

A METHOD AND A SYSTEM FOR GENERATION OF A CALIBRATED
SOUND FIELD

The present invention relates to a method and a
5 system for calibration of a sound field to be used
during fine-tuning of an auditory prosthesis.

An auditory prosthesis, such as a hearing aid, is
typically fine-tuned to an individual user by placing
the user with the auditory prosthesis in an auditory
10 test room in which various sound fields are generated
from a sound source. Each of the sound fields
corresponds to a sound field occurring in a real life
sound environment, such as in a concert hall, in an
environment with party noise, with traffic noise, with
15 no background noise, etc, etc. It is the object of the
fine-tuning procedure to adjust the auditory
prosthesis in such a way that the user's hearing loss
is compensated as well as possible in similar real
life sound environments.

20 In order to perform the required auditory
measurements accurately during auditory prosthesis
fine-tuning, the test room and the auditory fine-
tuning equipment must be calibrated to provide a
predetermined sound field at the position of the user.
25 It is well known that sound pressure in sound fields
generated with equipment that is not calibrated may
vary significantly. Many dispensers of hearing aids
constitute rather small entities for which investment
in calibration equipment represents a significant
30 burden.

It is an object of the present invention to
provide a method and a system for generation of a
calibrated sound field that reduces calibration
equipment requirements without substantially
35 compromising calibration accuracy.

According to the present invention the above-mentioned and other objects are fulfilled by an auditory prosthesis comprising a microphone for transforming an acoustic input signal into an electronic microphone signal, a filter bank with bandpass filters for dividing the microphone signal into a set of bandpass filtered microphone signals, a signal processor that is adapted to generate a processor output signal by individually processing each of the bandpass filtered microphone signals and summing the processed signals. The processor is further adapted to determine sound pressures based on the set of bandpass filtered microphone signals, and to provide a set of sound pressure signals representing the respective determined sound pressures. The prosthesis further comprises a signal output for provision of the set of sound pressure signals, and an output transducer for transforming the processor output signal into an acoustic output signal.

The auditory prosthesis may contain more than one microphone, e.g. for provision of directional characteristic capabilities, noise suppression capabilities, etc.

Preferably, sound pressure is determined as a sound pressure level in accordance with an accepted standard, such as ISO 131-1979, Acoustics - Expression of physical and subjective magnitudes of sound or noise in air. The sound pressure level is the sound pressure relative to a reference pressure, typically 20 μ Pa, preferably in dB.

In the following, the frequency ranges of the bandpass filters are also denoted channels.

In a simple embodiment of the invention, the auditory prosthesis is a single channel prosthesis,

i.e. the prosthesis processes incoming signals in one frequency band only. Thus, the filter bank consists of a single bandpass filter, and the single bandpass filter may be constituted by the bandpass filter that is inherent in the electronic circuitry and the transducers of the auditory prosthesis, i.e. no special circuitry provides the bandpass filter. Correspondingly, the summation in the processor of processed signals is reduced to simply providing the single processed signal at the output of the processor.

It is an important advantage of the present invention that resources already available in the auditory prosthesis are utilised for calibration of equipment used to generate the sound field corresponding to a specific sound environment used during fine-tuning.

Thus, utilisation of an auditory prosthesis for sound pressure determinations eliminates a need for dedicated sound pressure determining equipment, such as a calibrated microphone with a measuring apparatus for determination of sound pressure, e.g. a sound level meter according to IEC 651-1979, Sound level meters.

The auditory prosthesis may comprise a memory for storing sensitivity values of the microphone. The sensitivity may be the sound pressure level sensitivity. Sensitivity is defined as the ratio of generated electronic microphone signal magnitude to applied sound pressure. The magnitude may be the amplitude, RMS-value, etc. Typically, a set of sensitivity values is stored for a set of respective frequency ranges, and the stored sensitivity values are used in the determination of sound pressure.

The sensitivity values specified on the data

sheet provided by the manufacturer of the microphone may be stored in the memory.

Typically, sound pressure determinations made by auditory prostheses vary 1-2 dB so that calibration of sound field generating equipment with an auditory prosthesis according to the present invention may reduce sound pressure variations, e.g. from app. 20 dB to app. 2 dB. Typically, a 2 dB sound pressure ambiguity is sufficiently low for an optimum fine-tuning of an auditory prosthesis to be performed.

In a preferred embodiment of the present invention, a calibration of the microphone of the auditory prosthesis is performed for determination of sensitivity values of the microphone, and the determined sensitivity values are stored in the memory. Calibration of the sound field with an auditory prosthesis according to this embodiment is substantially as accurate as the calibration accuracy of the microphone.

Typically, hearing defects vary as a function of frequency in a way that is different for each individual user. Thus, in a preferred embodiment of the auditory prosthesis, the microphone signal is divided into a set of bandpass filtered signals with a filter bank of bandpass filters. Each of the bandpass filtered signals may be processed individually, e.g. amplified linearly or non-linearly with different gains, in the signal processor, and after processing the processed electrical signals are summed into a combined signal provided to the output transducer for conversion into an acoustic output signal.

In a preferred embodiment of the present invention, the processor is further adapted to determine sound pressures based on the set of bandpass filtered signals and to provide a corresponding set of

sound pressure signals at corresponding outputs of the auditory prosthesis.

Hereby, selective calibration of the equipment for sound field generation in each of the frequency
5 bands of the auditory prosthesis is facilitated. Further, a need for a dedicated frequency analyser is eliminated.

According to another aspect of the invention, a method for generation of a calibrated sound field is
10 provided, comprising the steps of positioning an auditory prosthesis as disclosed above in a test space (T), generating a sound field in the test space (T), and determining sound pressure with the auditory prosthesis.

15 In a preferred embodiment of the method, the step of positioning further comprises the steps of positioning the auditory prosthesis in the ear of a user, and positioning the user in the test space (T).

When the auditory prosthesis is positioned in the
20 ear of a user that is positioned in the test space (T) during sound field calibration, the need for a manikin or a test dummy, an occluded ear simulator, etc, is eliminated.

The method may further comprise the step of
25 modifying the generated sound field based on the generated set of sound pressure signals whereby a calibrated sound field is generated.

Thus, in the method the step of generating a sound field may comprise the steps of providing a
30 sound signal, modifying the sound signal according to a set of control parameters to provide a modified sound signal, and transforming the modified sound signal into a sound field in the test space (T). The method may further comprise the steps of supplying the
35 set of sound pressure signals to a controller for

calculation of new values of the set of control parameters for modification of the sound signal.

According to a further aspect of the invention, a system for generation of a calibrated sound field is provided, comprising an auditory prosthesis as disclosed above for determination of sound pressure.

The system may further comprise a sound signal generator for generation of a sound signal, a sound signal modifier that is adapted to receive and modify the sound signal in accordance with a set of control parameters for provision of a modified sound signal, a set of sound transducers, such as a set of loudspeakers, for transforming the modified sound signal into a sound field in the test space (T), and a controller that is adapted to receive the set of sound pressure signals from the auditory prosthesis and to calculate new values of the set of control parameters based on the received set of sound pressure signals.

It is not required to calibrate the sound field generating equipment before every fine-tuning of an auditory prosthesis to a user. Typically, it is sufficient to calibrate at regular intervals, e.g. during the first fine-tuning of a working day. However, when the sound field is calibrated with the auditory prosthesis worn by the user to whom the auditory prosthesis is subsequently fine-tuned, the additional advantage is obtained that the sound field is calibrated at the position of the auditory prosthesis during fine-tuning whereby ambiguity of sound pressure at the auditory prosthesis during fine-tuning is minimised.

The auditory prosthesis may be a hearing aid that is adapted to be programmed by an external programming device and to be connected to the programming device with a programming cable. Preferably, the signal

output is also adapted to be connected to the programming cable, and the set of sound level signals is supplied to the controller via the programming cable.

5 The auditory prosthesis may further comprise a transmitter for reception of the set of sound pressure signals from the signal processor and wireless transmission of corresponding respective signals.

10 The sound signal may be generated by reproduction of a signal recorded in a storage medium.

 The controller may be comprised in a personal computer comprising a memory for storage of the control parameters together with a computer programme for calculation of the control parameters, the
15 computer further comprising input means for receiving the set of sound pressure signals.

 In the following the invention will be further explained with reference to the accompanying drawing wherein

20 Fig. 1 is a block diagram of a prior art system for generation of a calibrated sound field,
 Fig. 2 is a block diagram of a first embodiment of the present invention,
 Fig 3 is a block diagram of a second embodiment
25 of the present invention,
 Fig. 4 is a block diagram of an embodiment of a hearing aid according to the present invention,
 Fig. 5 is a block diagram of an embodiment of the signal processor of a hearing aid according
30 to the present invention,
 Fig. 6 is a block diagram of a signal processor of the hearing aid shown in Fig. 2 or 3,
 Fig. 7 is a block diagram of another signal processor of the hearing aid shown in Fig. 2 or
35 3, and

Fig. 8 is a block diagram of a hearing aid according to the present invention comprising a multichannel signal processor.

A prior art sound field calibration system is shown in Fig. 1. A sound signal generator 1 generates a sound signal that is supplied to a sound signal modifier 2 wherein the level of the sound signal is modified as a function of frequency in accordance with a set of control parameters stored in a memory, not illustrated, in the sound signal modifier 2. The modified sound signal obtained from the signal modifier 2 is converted by a loudspeaker 3 into a sound field in a test space T.

The sound field is monitored in at least one observation point within the test space T by measuring means 4 comprising a precision calibrated microphone.

The measuring signal obtained from measuring means 4 includes level and/or frequency spectrum information and is supplied to control means comprising a signal analyser 5 for derivation of data representing the sound characteristic of the sound field in the test space and supplying the data to a control parameter calculator 6 for calculation of a new set of control parameters for use in the signal modifier 2.

In the embodiment of the present invention shown in Fig. 2, the sound signal generator 1, the signal modifier 2, and the control means including the measuring signal analyser 5 and the control parameter calculator 6 of the system illustrated in Fig. 1 have been combined into a computing device 7, such as a personal computer, comprising memory means 8, such as a hard disc, a keyboard 9, a display screen 10, and a sound interface that is connected with loudspeakers 12 for conversion of the sound signal into a sound field

in the test space T.

As further shown in Fig. 2 and in accordance with the invention, monitoring of the sound field in the test space T is performed by a microphone positioned
5 in a hearing aid that is carried by a user 13 who is seated in the test space T. The measuring signal obtained from one of or both of the hearing aids 14 is transmitted to the computer 7 through a cable 15, preferably the programming cable 15 that is connected
10 to a programming device 11 for programming of the hearing aid to suit various sound environments or listening situations by a computer assisted fine-tuning procedure.

Thereby the sound field calibration of the test
15 space T and the fine-tuning procedure may be combined into a single sequential operation using the same computer system 7 for the sound field calibration of the test space and for the fine-tuning procedure.

In an alternative embodiment of the present
20 invention shown in Fig. 3, the measuring signal obtained from hearing aids 14' is supplied to the computer 7 by wireless transmission means, such as IR or radio transmission from transmitters, not shown, integrated in each hearing aid 14', to an antenna 16
25 connected with a receiver 17 that is also connected to the cable 15.

In order to avoid possible discomfort to a user 13 during the calibration procedure, a pre-adjustment of the sound signal may be performed prior to
30 calibration. During the pre-adjustment the hearing aid is positioned at the observation point in the test space T without being carried by the user whereby the need for adjustment of the sound signal during calibration is minimised and so is possible user
35 discomfort.

In the simplified block diagram shown in Fig. 4, a hearing aid 14 for use in the implementation of the calibration method and system according to the invention comprises at least one microphone 18
5 connected with a signal processor 19, preferably comprising programmable signal processing parts, such as bandpass filters and amplifiers, from which a processor output signal is supplied to an output transducer 20, such as a hearing aid receiver.

10 It will be obvious for the person skilled in the art that the circuits shown in Fig. 4 may be realised using digital or analogue circuitry or any combination hereof. In the present embodiment, digital signal processing is employed and thus, the processor 19
15 comprises digital signal processing circuits. In the present embodiment, all the digital circuitry of the hearing aid may be provided on a single digital signal processing chip or, the circuitry may be distributed on a plurality of integrated circuit chips in any
20 appropriate way.

According to the invention, the hearing aid 14 also comprises interface means that is connected to the signal processor 19 for outputting the processor output signal. The interface means may comprise a
25 coupling terminal 21 for connection with the cable 15 as shown in Fig. 2, and the interface means may comprise wireless interface means as illustrated in Fig. 3.

In a programmable hearing aid according to the
30 present invention, a bi-directional communication link may be provided between the signal processor 19 and the computer 7 as shown in Figs. 2 and 3. Thus, data may flow in both directions in signal line 15 shown in Figs. 2 and 3. For a non-programmable hearing aid, it
35 is sufficient to provide a unidirectional

communication link between the processor 19 and the computer 7 for transmission of the measuring signal to the computer 7 for use in the calculation of calibration control parameters.

5 As shown in Fig. 5, the signal processor 19 comprises a sound pressure level signal generator 22 that is connected to the coupling terminal 21 for generation of the measuring signal. In a programmable hearing aid, the sound pressure level signal generator
10 may also serve as input/output interface for communication of programming data between the signal processor 19 and the programming computer.

As further illustrated in Fig. 6, the sound pressure level signal generator 22 may comprise an A/D
15 converter 23 for provision of a digital measuring signal for use in further signal processing in the processor 19, as indicated by line 24, and for use in the calibration of the sound field.

The measuring signal may be provided directly
20 from the A/D converter 23 to the interface means, e.g. the coupling terminal 21 as shown by the solid line 25, or, it may be further processed, e.g. averaged values may be calculated and provided to the interface means. In another embodiment of the invention, a
25 digital RMS-averaged signal is formed in a RMS-detector 26 and supplied to the interface means, e.g. the coupling terminal 21, via the dashed line 27.

As shown in Fig. 7, the measuring signal processor 22 may also include a pre-adjustment circuit
30 28 that is interconnected between the A/D converter 23 and the RMS detector 26 to provide pre-adjustment of the digital microphone signal into a calibrated microphone signal. The pre-adjustment circuit 28 comprises a memory for storing sensitivity values,
35 such as sound pressure level sensitivity values, of

the microphone defining ratios of electronic microphone signal amplitude to sound pressure at the microphone. Typically, a set of sensitivity values is stored for a set of respective frequency ranges, and
5 the stored sensitivity values are used in the determination of sound pressure. The sensitivity values specified on the data sheet provided by the manufacturer of the microphone may be stored in the memory, or, sensitivity values as determined by a
10 calibration measurement of the microphone 18 may be stored in the memory.

In the embodiment of the present invention shown in Fig. 7, the measuring signal obtained from the RMS detector 26 is supplied to a transmitter 29 feeding an
15 antenna 30 positioned at the hearing aid 14, 14' for wireless transmission of the measuring signal to the antenna 16 and the receiver 17 shown in Fig. 3.

Although the hearing aid 14, 14' in Figs. 4-7 is illustrated as a single channel hearing aid, it should
20 be understood that a hearing aid 14, 14' according to the present invention may contain any appropriate number of channels. A multichannel hearing aid according to the present invention is shown in Fig. 8 comprising a multichannel processor 31 wherein a
25 digital microphone signal supplied by the A/D converter 32 is filtered by adjustable band pass filters 33, 34, and 35 into, e.g. a high frequency signal, an intermediate signal and a low frequency signal. The filtered digital signals are further
30 processed in separate processing channels of the signal processor 31. Obviously, any number of channels may be provided in the hearing aid 14, 14'. The hearing aid may comprise an RMS detector 36 that is also divided into separate processing channels for
35 individually processing of the output signals from the

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band pass filters. The individually processed signals are transmitted to the computer 7 for adjustment of the control parameters.

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P A T E N T C L A I M S

1. An auditory prosthesis comprising
a microphone (18) for transforming an acoustic
input signal into an electronic microphone signal,
5 a signal processor (19) that is adapted to
generate a processor output signal by processing
the microphone signal,
determine sound pressures based on the microphone
signal, and
10 provide a set of sound pressure signals
representing the respective determined sound
pressures,
a signal output (21, 30, 38) for provision of the
set of sound pressure signals, and
15 an output transducer (20) for transforming the
processor output signal into an acoustic output
signal.
2. An auditory prosthesis according to claim 1,
further comprising a filter bank connected with the
20 microphone to receive the electronic microphone signal
therefrom, said filter bank having bandpass filters
(33, 34, 35) for dividing the microphone signal into a
set of bandpass filtered microphone signals, and
wherein the signal processor (19) is adapted to
25 generate the processor output signal by individually
processing each of the bandpass filtered microphone
signals, summing the processed signals to form the
processor output signal and determine sound pressures
based on the set of bandpass filtered microphone
30 signals.
3. An auditory prosthesis according to claim 1 or
2, further comprising a memory for storage of
sensitivity values of the microphone (18), and wherein
the signal processor (19) is further adapted to
35 determine sound pressure based on the stored

sensitivity values.

4. An auditory prosthesis according to claim 3, wherein the sensitivity values are specified by the manufacturer of the microphone.

5 5. An auditory prosthesis according to claim 3, wherein the sensitivity values are determined by calibration of the microphone (18).

6. An auditory prosthesis according to any of the preceding claims, further comprising a transmitter
10 (29, 37) for reception of the set of sound pressure signals from the signal processor (19) and wireless transmission of corresponding respective signals.

7. An auditory prosthesis according to any of the preceding claims, wherein the auditory prosthesis is a
15 hearing aid (14, 14') that is adapted to be programmed by an external programming device (11) and to be connected to the programming device with a programming cable (15), and wherein the signal output (21) is also adapted to be connected to the programming cable (15).

20 8. An auditory prosthesis according to any of the preceding claims, wherein the sound pressure signals are digital signals.

9. An auditory prosthesis according to any of the preceding claims, wherein the sound pressure signals
25 represent the RMS sound pressure.

10. A method for generation of a calibrated sound field, comprising the steps of positioning an auditory prosthesis according to any of the previous claims in a test space (T), generating a sound field in the test
30 space (T), and determining sound pressure with the auditory prosthesis.

11. A method according to claim 9, wherein the step of positioning further comprises the steps of positioning the auditory prosthesis in the ear of a
35 user, and of positioning the user in the test space

(T).

12. A method according to claim 10 or 11, wherein the step of generating a sound field comprises the steps of providing a sound signal, modifying the sound
5 signal according to a set of control parameters to provide a modified sound signal, transforming the modified sound signal into a sound field in the test space (T), and wherein the method further comprises the steps of supplying the set of sound pressure
10 signals to a controller (7) for calculation of new values of the set of control parameters for modification of the sound signal.

13. A method according to claim 12, wherein the controller (7) is comprised in a personal computer (7)
15 comprising a memory (8) for storage of the control parameters together with a computer programme for calculation of the control parameters, the computer (7) further comprising input means for receiving the set of sound pressure signals.

20 14. A method according to any of claims 10-13, wherein the auditory prosthesis is a hearing aid (14, 14') that is adapted to be programmed by an external programming device and to be connected to the programming device with a programming cable (15), and
25 wherein the signal output (21) is also adapted to be connected to the programming cable (15), the method further comprising the step of supplying the set of sound level signals to the controller (7) via the programming cable (15).

30 15. A method according to any of claims 10-13, wherein the auditory prosthesis further comprises a transmitter (29, 37) for reception of the set of sound pressure signals and wireless transmission of corresponding respective signals.

35 16. A method according to any of claims 10-15,

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further comprising the step of storing sensitivity values of the microphone (18), and wherein sound pressures are determined based on the stored sensitivity values.

5 17. A method according to claim 16, wherein the sensitivity values are specified by the manufacturer of the microphone.

18. A method according to claim 16, wherein the sensitivity values are determined by calibration of
10 the microphone (18).

19. A system for generation of a calibrated sound field, comprising an auditory prosthesis according to any of claims 1-9 for determination of sound pressure.

20. A system according to claim 19, further
15 comprising

a sound signal generator (1) for generation of a sound signal,

a sound signal modifier (2) that is adapted to receive and modify the sound signal in accordance with
20 a set of control parameters for provision of a modified sound signal,

a set of sound transducers (3) for transforming the modified sound signal into a sound field in a test space (T), and

25 a controller (7) that is adapted to receive the set of sound pressure signals from the auditory prosthesis and to calculate new values of the set of control parameters based on the set of sound pressure signals.

30 21. A system according to claim 20, comprising a personal computer (7) comprising the controller (7), a memory (8) for storage of the control parameters together with a computer programme for calculation of the control parameters, and input means for receiving
35 the set of sound pressure signals.

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22. A system according to claim 20 or 21, wherein the auditory prosthesis is a hearing aid (14, 14') that is adapted to be programmed by an external programming device and to be connected to the programming device with a programming cable (15), and wherein the signal output (21) is also adapted to be connected to the programming cable (15), the set of sound level signals being supplied to the controller (7) via the programming cable (15).

23. A system according to claim 20 or 21, wherein the auditory prosthesis further comprises a transmitter (29, 37) for reception of the set of sound pressure signals and wireless transmission of corresponding respective signals.

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