

Description

This invention relates to a connective tissue prosthesis, and in particular to a prosthesis for use in place of a natural ligament or tendon.

Numerous different constructions have been proposed for tendon and ligament prostheses. Early proposals were generally for prostheses in the form of a single load bearing element of a biocompatible material, and such constructions continue to be proposed. While such prostheses usually have the requisite tensile strength, their behaviour is very different from that of native collagenous soft tissue, because they display a substantially constant modulus of elasticity over a wide range of applied tensile loads. In contrast, a natural ligament or tendon displays a comparatively low modulus of elasticity under low tensile loads, and a greatly increased elastic modulus under high tensile loads. This means that natural ligaments and tendons are sufficiently resilient to provide enough movement to minimise the strain imposed on the connection with bone or soft tissue, but sufficiently resistant to large stresses to avoid excessive, and thus damaging, movement of joints.

Attempts have been made to produce prostheses which more closely mimic the mechanical properties of natural collagenous tissue. For example, British Patent Specification No. 1471837 discloses a tendon prosthesis consisting of a core and of a sheath. The preferred core consists of a knitted fabric or twisted fabric bundle embedded in an elastic oriented polymer. It is said that such a core gives a performance similar to that of a genuine tendon, and the prosthesis as a whole is said to be "physiologically inert".

More recently, the trend has been towards prostheses which are not physiologically inert, but which on the contrary, elicit the positive physiological response of fibrogenesis. Such a prosthesis is described in British Patent Specification No. 1602834. However, this prosthesis, being formed from a single material, suffers the same disadvantages as the earlier prior art prostheses as regards the nature of its response to increasing load.

US-A-4 301 551 discloses an artificial prosthetic ligament comprising an elongate elastic core having a low modulus of elasticity and a tensionable wrapping of thread (having a collective elastic modulus which is greater than that of the core), said wrapping being disposed in contact about the core in order to compress the core and to cause it to elongate axially upon opposite relative axial displacement of opposed ends of the wrapping secured to traction means.

The present invention seeks to provide an implantable prosthesis with a mechanical response similar to that of native soft collagenous connective

tissues, which is moreover capable of promoting a considerable degree of collagen fibrogenesis.

According to the present invention there is provided a biocompatible connective tissue prosthesis, comprising a first load bearing element and a bundle of fine filaments which are arranged to allow ingrowth of connective tissue, said filaments being of higher elastic modulus than the effective elastic modulus of the first element, and being attached to the first element at two or more spaced points along their length, the length of filament between said points being greater than the unstressed length of the first element between said points, such that the filaments are substantially unstressed unless the load on the prosthesis exceeds a predetermined value.

Thus, in contrast to the prosthesis disclosed in Specification No. 1471837, the high modulus material is available to be intertwined with collagen, following ingrowth of new tissue. We have found that the high modulus material should not be completely surrounded by the low modulus material (such as is the case in the prosthesis disclosed in Specification No. 1471837), because low modulus materials in general do not promote fibrogenesis.

The prosthesis of the present invention is capable of non-linear elastic deformation so that a comparatively large elastic stretch is obtained on the application of low tensile forces, but greatly increased forces produce comparatively little further deformation. Furthermore, in contrast to the prosthesis disclosed in Specification No. 1471837, there is substantially no shear interaction between the materials of different elastic modulus when the prosthesis is stretched as a whole.

The material or materials used in the prosthesis according to the invention must be biocompatible in the sense of inducing no adverse biological reaction, and being well tolerated by fibroblasts. It is also preferable that the material or materials are readily sterilizable by commonly used methods such as γ -irradiation, autoclaving and ethylene oxide treatment.

Preferably, the first load bearing element has an effective elastic modulus of from 0.1 to 2 MPa, for example 0.5 to 1.5 MPa, and the filaments preferably have a collective elastic modulus of from 100 to 3000 MPa, for example 1000 to 2000 MPa. The particular elastic modulus chosen for the first element and the filaments will depend on the use to which the prosthesis is to be put. For example, a prosthesis for use in a child will generally have a lower elastic modulus than a prosthesis for use in an adult, because connective tissue of children is generally more elastic than that of adults.

The term "effective elastic modulus", as used in relation to the first element, means the elastic modulus of the first element as a whole. This

elastic modulus may be derived from the inherent properties of the material from which it is made. Thus, for example, the first element may comprise one or more substantially straight filaments of the desired elastic modulus, such as medical grade silicone rubber.

In an alternative construction, the first element derives its effective elastic modulus not merely from the elastic modulus from which it is made, but also from the conformation in which this material is arranged. Thus, the first element may be in the form of a spring, such as a coil spring, of a material which has a relatively large elastic modulus, the desired elastic modulus being that of the spring as a whole.

The linear elastic strain limit of the first element will generally be greater than 20%, while the linear elastic strain limit of the filaments is preferably at least 2 to 3%.

It will be appreciated that the mechanical response of the prosthesis of the invention can be made to suit individual requirements not only by choosing materials having the desired elastic modulus and elastic strain limit, but also by varying the length of the filaments between the points of their attachment to the first element, relative to the relied length of the first element between those points. Generally, the fine filaments will be of such a length relative to the first element that the maximum degree to which the first element can be stretched without stressing the filaments is in the range 1 to 15%, and more preferably in the range 1 to 5%.

The prosthesis may be in the form of an elongate ligament or tendon prosthesis. Such a prosthesis is designed to bear tensile stresses essentially in a single direction, and may be referred to as a "one-dimensional" prosthesis. It will be understood, however, that the invention is equally applicable to two-, or even three-dimensional prostheses, i.e. to prostheses which are designed to bear stresses in two or three mutually perpendicular directions. Moreover, a ligament or tendon prosthesis may, if desired, be branched, the mechanical properties of each branch being tailored to match the mechanical properties of the branched ligament or tendon which the prosthesis is designed to replace.

The fine filaments will generally be formed from a plastics material, such as a polyester or polyamide, for example nylon. A ligament or tendon prosthesis according to the invention preferably comprises from 50 to 1500 yarns, each consisting of from 20 to 100 fine filaments. The number of fine filaments to be used in any prosthesis depends on the overall strength, elastic modulus, cross sectional area and extent of elastic stretch required of the prosthesis, and on the correspond-

ing properties of the individual fine filaments. The fine filaments preferably have a diameter in the range 8 to 20 microns.

When the fine filaments are provided in the form of filamentary yarns, these may be twisted or braided. In any such construction, however, care must be taken to ensure that the fine filaments are not so tightly packed that ingrowth of fresh collagenous tissue is prevented. The packing density of the fine filaments should preferably be slightly lower than that given by a close packed hexagonal arrangement of fine filaments.

The fibrogenicity of the prosthesis may be further enhanced by coating the fine filaments with agents which promote infiltration and adhesion, such as fibronectin and/or heparin.

The prosthesis may be sterilised, for example by gamma-irradiation, and may be hermetically sealed in a sterile envelope. One or both ends of the fine filaments may be collectively threaded through a surgical needle, so that the prosthesis is immediately ready for use by the surgeon.

The present invention also provides a method of making the prosthesis described above, the method comprising stretching a first load bearing element by a predetermined amount and then fixing a bundle of filaments at two or more spaced points along the length of the first element, such that the filaments are unstressed unless the first element is stretched by said predetermined amount.

A prosthesis according to the invention, and a method of making such a prosthesis, are now disclosed, by way, of example, with reference to the accompanying drawings, in which:-

Figure 1 is a schematic view of a prosthesis in a partially stretched state.

Figure 2 is a schematic view of the prosthesis of Figure 1 in a relaxed state.

Figure 3 is a graph showing the stress/strain curve of the prosthesis of Figure 1.

Figures 4 and 5 show schematic sections through alternative constructions of prosthesis, Figure 6 shows a prosthesis provided with needles for suturing.

Figure 7 illustrates a branched prosthesis, and Figure 8 shows a prosthesis adapted for receiving a load in two mutually perpendicular directions.

Referring to the drawings, a ligament prosthesis comprises a first load bearing element 1 in the form of a relatively thick silicone monofilament (e.g. SILASTIC silicone monofilament made by Dow Corning. SILASTIC is a Trade Mark). A bundle of fine polyester filaments 3, of 10 micron diameter, are connected to the first load bearing element 1 at spaced intervals as indicated at 5.

The prosthesis is made as follows. The silicone

monofilament 1, after washing in a detergent solution, is clamped between two clamps 7 and stretched so that the distance between two marker points AB is increased from the rest length l_0 to the desired stretched length l_1 . Fine filaments of polyester of length greater than l_1 are then washed in detergent solution and laid around the pre-stretched silicone, and fastened to the silicone at the points 5. Fastening can be effected by using non-toxic biologically tolerable glue, surgical staples or by tying with additional yarns of polyester. The fine polyester filaments 3 should be unstressed at this stage, as shown in Figure 1.

After the fine polyester filaments 3 are suitably attached to the silicone monofilament 1, the prosthesis is removed from the clamps, so that a distance AB reverts to l_0 .

In use, the elastic modulus of the prosthesis at small deformation is given by the elastic modulus of the silicone monofilament, since the fine polyester filaments are unstressed. As the deformation of the prosthesis increases so that the length AB exceeds l_1 , the elastic modulus of the prosthesis is given essentially by the elastic modulus of the fine polyester filaments. This is illustrated graphically in Figure 3.

As Figure 3 shows, applying an increasing tensile force to the prosthesis gives a comparatively large, and essentially linear increase in length of the prosthesis until the force reaches a value F_1 . This is the force required to stretch the distance between the markers AB from l_0 to l_1 .

As the applied force is increased, the fine filaments begin to stretch, and the stress/strain curve shows a transition from the low modulus linear response given by the first element, to the higher modulus, essentially linear response given by the fine filaments. This higher modulus linear response is seen until the applied force reaches F_e , at which point the length AB is given by l_e , the linear elastic limit of the fine filaments. Increasing the applied force still further produces non-elastic deformation of the prosthesis, and then ultimate failure. It is therefore preferable to construct the prosthesis so that in use it is never stretched beyond the length l_e .

It is not necessary for the first load bearing element to be constituted by a single monofilament or for such a monofilament to be located at the centre of the bundle of fine filaments. A plurality of elements of circular, rectangular, square or other cross sections may be dispersed among the fine filaments. For example, Figure 4 illustrates a section through a ligament prosthesis in which the first load bearing element is constituted by a central SILASTIC monofilament 41 and eight further SILASTIC monofilaments 42 disposed equiangularly around the central monofilament. Fine polyester

filaments 43 are arranged not only around the eight monofilaments 42, but also between these latter and the central monofilament 41.

Figure 5 shows a section through a prosthesis in which the first load bearing element is constituted by two sheets of SILASTIC silicone rubber 51, in a layered arrangement with fine polyester filaments 53.

As shown in Figure 6, the ends of the prosthesis may be inserted or fixed in connectors 64 to facilitate threading and fixation in surgical procedures. Alternatively, one or both ends of the protruding silicone monofilament may be cut off and the fine filament ends 66 prepared ready for suturing with surgical needles 68.

In the embodiment shown in Figure 7, the first load bearing element (not shown) is branched, with some of the fine filaments 73 being attached to one branch at 75, and other fine filaments 73' being attached to the other branch at 75'. The length of the fine filaments between the points 75, and the number of such filaments, need not necessarily be the same as the length and number of fine filaments between the points 75', so that the two branches display different mechanical properties.

For replacement of tissues which bear biaxial stresses, the form shown in Figure 8 may be adopted. In this construction the first load bearing element comprises a membrane 81 of low elastic modulus material which is pre-stretched in two mutually perpendicular directions (represented by X and Y) before attaching two crossed but distinct sets of fine filaments which are oriented respectively in the X and Y directions.

Claims

1. A biocompatible connective tissue prosthesis, comprising a first load bearing element (1), and a bundle of fine filaments (3) which are arranged to allow ingrowth of connective tissue, said filaments having a collective elastic modulus which is greater than the effective elastic modulus of the first element, and being attached to the first element (1) at two or more spaced points (5) along their length, the length of the filament between said points (5) being greater than the unstressed length of the first element between said points, such that the filaments are substantially unstressed unless the load on the prosthesis exceeds a predetermined value.
2. A prosthesis according to claim 1 wherein the first load bearing element has an elastic modulus of from 0.1 to 2 MPa.
3. A prosthesis according to claim 1 or claim 2

monofilament 1, after washing in a detergent solution, is clamped between two clamps 7 and stretched so that the distance between two marker points AB is increased from the rest length l_0 to the desired stretched length l_1 . Fine filaments of polyester of length greater than l_1 are then washed in detergent solution and laid around the pre-stretched silicone, and fastened to the silicone at the points 5. Fastening can be effected by using non-toxic biologically tolerable glue, surgical staples or by tying with additional yarns of polyester. The fine polyester filaments 3 should be unstressed at this stage, as shown in Figure 1.

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It is not necessary for the first load bearing element to be constituted by a single monofilament or for such a monofilament to be located at the centre of the bundle of fine filaments. A plurality of elements of circular, rectangular, square or other cross sections may be dispersed among the fine filaments. For example, Figure 4 illustrates a section through a ligament prosthesis in which the first load bearing element is constituted by a central SILASTIC monofilament 41 and eight further SILASTIC monofilaments 42 disposed equiangularly around the central monofilament. Fine polyester

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For replacement of tissues which bear biaxial stresses, the form shown in Figure 8 may be adopted. In this construction the first load bearing element comprises a membrane 81 of low elastic modulus material which is pre-stretched in two mutually perpendicular directions (represented by X and Y) before attaching two crossed but distinct sets of fine filaments which are oriented respectively in the X and Y directions.

Claims

1. A biocompatible connective tissue prosthesis, comprising a first load bearing element (1), and a bundle of fine filaments (3) which are arranged to allow ingrowth of connective tissue, said filaments having a collective elastic modulus which is greater than the effective elastic modulus of the first element, and being attached to the first element (1) at two or more spaced points (5) along their length, the length of the filament between said points (5) being greater than the unstressed length of the first element between said points, such that the filaments are substantially unstressed unless the load on the prosthesis exceeds a predetermined value.
2. A prosthesis according to claim 1 wherein the first load bearing element has an elastic modulus of from 0.1 to 2 MPa.
3. A prosthesis according to claim 1 or claim 2



wherein the fine filaments have a collective elastic modulus of from 100 to 3,000 MPa.

4. A prosthesis according to any preceding claim wherein the elastic strain limit of the first element is substantially greater than that of the filaments. 5
5. A prosthesis according to any preceding claim wherein the linear elastic strain limit of the fine filaments is from 2% to 3%. 10
6. A prosthesis according to any preceding claim wherein the maximum degree to which the first element can be stretched without stressing the fine filaments is in the range 1% to 15%. 15
7. A prosthesis according to any preceding claim wherein the first element comprises a single core surrounded by the fine filaments. 20
8. A prosthesis according to any of claims 1 to 6 wherein the first element is in the form of a spring having the required elastic modulus. 25
9. A prosthesis according to any of claims 1 to 6 wherein the first element comprises one or more substantially straight filaments. 30
10. A prosthesis according to claim 9 wherein the first element is a medical grade silicone rubber filament. 35
11. A prosthesis according to any preceding claim wherein the fine filaments are of a polyester or polyamide, and have a diameter in the range of 8 to 20 microns. 40
12. A prosthesis according to claim 11 comprising from 50 to 1500 filamentary yarns, each consisting of from 20 to 100 fine filaments. 45
13. A prosthesis according to any preceding claim wherein one or both ends of the fine filaments are threaded through a surgical needle. 50
14. A prosthesis according to any preceding claim wherein the fine filaments are wound, woven or braided around the first element. 55
15. A prosthesis according to any preceding claim wherein the fine filaments are coated with an agent promoting cell adhesion.
16. A method of making a prosthesis according to any preceding claim comprising stretching a first load bearing element by a predetermined amount and then fixing a bundle of fine fila-

ments at two or more spaced points along the length of the first element, such that the fine filaments are unstressed unless the first element is stretched by said predetermined amount.

Revendications

1. Prothèse biocompatible pour tissus conjonctif, comportant un premier élément (1) de reprise de la charge et un faisceau de fins filaments (3) disposés pour y permettre la croissance du tissu conjonctif, lesdits filaments ayant un module d'élasticité collectif qui est supérieur au module d'élasticité effectif du premier élément et étant fixés au premier élément (1) en deux ou plus points espacés (5) sur leur longueur, la longueur du filament entre lesdits points (1) étant supérieure à la longueur, à l'état non étiré, du premier élément entre lesdits points, de façon que les filaments ne soient sensiblement pas contraints à moins que la charge sur la prothèse dépasse une valeur prédéterminée.
2. Prothèse selon la revendication 1, dans laquelle le premier élément de reprise de la charge a un module d'élasticité allant de 0,1 à 2 MPa.
3. Prothèse selon la revendication 1 ou la revendication 2, dans laquelle les filaments ont un module d'élasticité collectif allant de 100 à 3000 MPa.
4. Prothèse selon l'une quelconque des revendications précédentes, dans laquelle la limite d'allongement élastique du premier élément est sensiblement supérieure à celle des filaments.
5. Prothèse selon l'une quelconque des revendications précédentes dans laquelle la limite d'allongement élastique linéaire des fins filaments est de 2 à 3%.
6. Prothèse selon l'une quelconque des revendications précédentes, dans laquelle le degré maximal auquel le premier élément peut être étiré sans contraindre les fins filaments va de 1% à 15%.
7. Prothèse selon l'une quelconque des revendications précédentes, dans laquelle le premier élément est constitué d'un unique noyau entouré par les fins filaments.
8. Prothèse selon l'une quelconque des revendications 1 à 6, dans laquelle le premier élément se présente sous forme d'un ressort ayant le



module d'élasticité demandé.

9. Prothèse selon l'une quelconque des revendications 1 à 6, dans laquelle le premier élément est constitué d'un ou plusieurs filaments sensiblement rectilignes.
10. Prothèse selon la revendication 9, dans laquelle le premier élément est un filament de caoutchouc silicone de qualité médicale.
11. Prothèse selon l'une quelconque des revendications précédentes dans laquelle les fins filaments sont en polyester ou polyamide et ont un diamètre allant de 8 à 20 microns.
12. Prothèse selon la revendication 11 constituée de 50 à 1500 fils de filaments, chaque filé comprenant de 20 à 100 fins filaments.
13. Prothèse selon l'une quelconque des revendications précédentes dans laquelle l'une des deux, ou les deux, extrémités des fins filaments se vissent par l'intermédiaire d'une aiguille chirurgicale.
14. Prothèse selon l'une quelconque des revendications précédentes, dans laquelle les fins filaments sont enroulés, tissés ou tressés autour du premier élément.
15. Prothèse selon l'une quelconque des revendications précédentes dans laquelle les fins filaments sont revêtus d'un agent favorisant l'adhérence des cellules.
16. Procédé de fabrication d'une prothèse conforme à l'une quelconque des revendications précédentes, comportant le fait d'étirer, d'une valeur prédéterminée, un premier élément de reprise de la charge et de fixer un faisceau de fins filaments en deux ou plus points espacés sur la longueur du premier élément, de façon que les fins filaments soient non contraints à moins que le premier élément soit étiré de ladite valeur prédéterminée.

Patentansprüche

1. Biologisch verträgliche Bindegewebsprothese, welche ein erstes lastentragendes Element (1) und ein Bündel von feinen Fäden (3) umfaßt, welche derart angeordnet sind, daß sie ein Einwachsen von Bindegewebe ermöglichen, und welche Fäden einen kollektiven Elastizitätsmodul aufweisen, welcher größer als der wirksame Elastizitätsmodul des ersten Elementes ist, und welche Fäden an zwei oder mehre-

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ren, im Abstand längs ihrer Längenerstreckung voneinander befindlichen Punkten (5) an dem ersten Element (1) befestigt sind, und wobei die Länge des Fadens zwischen diesen Punkten (5) größer als die unbelastete Längenerstreckung des ersten Elementes zwischen diesen Punkten ist, derart, daß die Fäden im wesentlichen unbelastet sind, sofern nicht die Belastung auf die Prothese einen vorbestimmten Wert überschreitet.

2. Prothese nach Anspruch 1, worin das erste lastentragende Element einen Elastizitätsmodul von 0,1 bis 2 MPa aufweist.

3. Prothese nach Anspruch 1 oder 2, worin die feinen Fäden einen kollektiven Elastizitätsmodul von 100 bis 3.000 MPa aufweisen.

4. Prothese nach einem der Ansprüche 1 bis 3, worin die der Elastizitätsgrenze entsprechende Beanspruchung des ersten Elementes wesentlich größer als jene der Fäden ist.

5. Prothese nach einem der Ansprüche 1 bis 4, worin die der Elastizitätsgrenze entsprechende lineare Beanspruchung der feinen Fäden 2 % bis 3 % beträgt.

6. Prothese nach einem der Ansprüche 1 bis 5, worin das maximale Ausmaß, in welchem das erste Element gestreckt werden kann, ohne die feinen Fäden zu beanspruchen, in einem Bereich von 1 % bis 15 % liegt.

7. Prothese nach einem der Ansprüche 1 bis 6, worin das erste Element einen einzelnen Kern umfaßt, welcher von den feinen Fäden umgeben ist.

8. Prothese nach einem der Ansprüche 1 bis 6, worin das erste Element in der Form einer Feder vorliegt, welche den erforderlichen Elastizitätsmodul aufweist.

9. Prothese nach einem der Ansprüche 1 bis 6, worin das erste Element einen oder mehrere, im wesentlichen gerade Fäden umfaßt.

10. Prothese nach Anspruch 9, worin das erste Element ein Faden aus Silikongummi von medizinischer Qualität ist.

11. Prothese nach einem der Ansprüche 1 bis 10, worin die feinen Fäden aus einem Polyester oder Polyamid bestehen und einen Durchmesser in einem Bereich von 8 bis 20 µm aufweisen.



12. Prothese nach Anspruch 11, welche 50 bis 1500 Fadengarne umfaßt, von denen ein jedes aus 20 bis 100 feinen Fäden besteht.



13. Prothese nach einem der Ansprüche 1 bis 12, worin eines oder beide Enden der feinen Fäden in einer chirurgischen Nadel eingefädelt sind.

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14. Prothese nach einem der Ansprüche 1 bis 13, worin die feinen Fäden um das erste Element herum gewickelt, gewebt oder geflochten sind.

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15. Prothese nach einem der Ansprüche 1 bis 14, worin die feinen Fäden mit einem Mittel überzogen sind, welches das Anhaften von Zellen fordert.

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16. Verfahren zur Herstellung einer Prothese nach einem der Ansprüche 1 bis 15, welches ein Strecken eines ersten lastentragenden Elementes um einen vorbestimmten Betrag und dann das Befestigen eines Bündels von feinen Fäden an zwei oder mehreren, im Abstand voneinander längs der Längenerstreckung des ersten Elementes befindlichen Punkten, derart, daß die feinen Fäden unbelastet sind, sofern nicht das erste Element um diesen vorbestimmten Betrag gestreckt wird, umfaßt.

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