

## **MEDICAL TUBE POSITION CONFIRMATION SYSTEM**

### **Technical Field**

**[0001]** The present invention relates to a medical tube position confirmation system.

### **Background Art**

**[0002]** Conventionally, in a medical setting, food is supplied directly into the stomach of a patient who finds oral ingestion of food difficult using a method known as nasal tube feeding. More specifically, a soft nasal tube is inserted through the nasal cavity of the patient until a tip end portion thereof reaches the stomach, whereupon liquid food and nutritional supplements are injected through a base end portion of the tube.

**[0003]** During nasal tube feeding, a method of inserting a nasal tube coated with lubricating jelly into the nostril, having the patient perform a swallowing action repeatedly while feeding the tip end portion of the tube more deeply little by little, and guiding the tip end portion of the nasal tube toward the esophagus side until the tip end portion reaches the stomach is implemented.

**[0004]** However, the back of the throat of a human bifurcates into two passages, namely the trachea and the esophagus, making the operation to insert the nasal tube extremely difficult, and when food or the like enters the lungs mistakenly, aspiration pneumonia or the like may occur. It is therefore necessary to perform an operation to confirm that the tip end portion of the nasal tube has reached the stomach.

**[0005]** Patent Document 1 discloses a detection line having a pair of insulated wires and a sensor portion formed on the tip end thereof. The detection line is inserted into a medical tube so that when the sensor portion comes into contact with gastric juice, a resistance value between the pair of insulated wires varies. Hence, by

detecting variation in the resistance value between the pair of insulated wires, it can be determined that the sensor portion has come into contact with gastric juice and accordingly that the medical tube has correctly reached the stomach.

**[0006]** Further, Patent Document 2 discloses a nasal tube tip end position confirmation device including a casing, a connecting portion that communicates with the outside from the casing and is connected to a base end side of a nasal tube inserted into the body of a patient, a sensor element disposed in the casing, an electronic circuit, and display means. The electronic circuit outputs air pressure variation received by the sensor element in the form of an electric signal, and the display means receives the output from the electronic circuit and displays the air pressure variation in a recognizable state. Hence, by pressing the abdomen of the patient from the outside, air pressure variation is generated in the stomach, and by having the display means display information indicating that the sensor element has received the air pressure variation, it is possible to determine whether or not the nasal tube has been inserted to an appropriate position.

## Citation List

### Patent Document

**[0007]** Patent Document 1: Patent Publication JP-A-2016-77450

Patent Document 2: Japanese Patent No. 6245870

## Summary

### Technical Problem

**[0008]** However, with a method employing a detection line, such as that of Patent Document 1, it is necessary for gastric juice to be secreted in an appropriate location. This means that the types of patients to which the method can be applied

are limited, and runs counter to the aim of determining the position of the medical tube with precision. Further, with a method employing air pressure variation, such as that of Patent Document 2, a complicated configuration is required to control the air pressure, leading to an increase in manufacturing cost.

**[0009]** An object of the present invention is therefore to provide a medical tube position confirmation system with which the position of a medical tube can be confirmed more easily.

#### Solution to Problem

**[0010]** A medical tube position confirmation system according to an aspect of the present invention is a medical tube position confirmation system for confirming the position of a medical tube that is used to supply nutrients to the interior of a body by means of tube feeding while an end portion thereof is inserted into (placed in) the stomach. The system includes a light guide that is configured to guide light entering through an incident end portion so that the light exits through an exit end portion and is inserted into the medical tube so that the exit end portion is disposed in the interior of the stomach, a light source for emitting light including a wavelength passing through a living body, the light source being optically connected to the incident end of the light guide so that the light enters the light guide, and a scattering part optically connected to the light guide on the exit end portion of the light guide so as to scatter light emitted by the light guide.

**[0011]** According to this aspect, the light emitted from the light source, which contains wavelengths that pass through a living body, is guided through the interior of the light guide inserted into the medical tube so as to exit through the exit end portion of the light guide, which is disposed in the stomach, and to be scattered extensively by the scattering portion. Since the emitted light is scattered

extensively, an operator can easily confirm the light which has passed through the stomach and the living body, which makes it easier to confirm the position of the medical tube.

#### **Advantageous Effects of Invention**

**[0012]** According to the present invention, it is possible to provide a medical tube position confirmation system with which the position of a medical tube can be confirmed more easily.

#### **Brief Description of Drawings**

**[0013]** Fig. 1 is a pattern diagram showing an example of a configuration of a medical tube position confirmation system 1 according to an embodiment of the present invention.

Fig. 2 is a schematic view showing an example of a functional configuration of a light 10.

Fig. 3 is a view illustrating wavelengths of light emitted by a light 10.

Fig. 4 is a diagram of a configuration of an exit end portion 20E side of an optical fiber 20.

Fig. 5 is a cross section according to the A-A' line in Fig. 4.

Fig. 6 is a schematic diagram showing an example of a functional configuration of a camera 30.

Fig. 7 is a schematic view showing an example of a functional configuration of a user terminal 40.

Fig. 8 is a view illustrating a configuration of another scattering portion 60.

#### **Description of Embodiments**

**[0014]** Referring to the attached figures, a preferred embodiment of the present invention will be described (note that in the figures, identical reference numerals denote identical or similar configurations).

**[0015]** [First Embodiment]

(1) Overall configuration

Fig. 1 is a pattern diagram showing an example of a configuration of a medical tube position confirmation system 1 according to an embodiment of the present invention. As shown in Fig. 1, the medical tube position confirmation system 1 includes, for example, a light 10, an optical fiber 20, a camera 30, a user terminal 40, and a database 50. The user terminal 40 is connected communicably to each of the light 10, the camera 30, and the database 50 via a communication network.

**[0016]** (2) Configurations of respective parts

(2-1) Light 10

Fig. 2 is a schematic view showing an example of a functional configuration of the light 10. The light 10 is an example of a light source that emits light containing wavelengths that pass through a living body. The light 10 is formed by providing a light-emitting unit 11, a drive circuit 12, a processing unit 13, a storage unit 14, and a communication unit 15 in a substantially cylindrical casing formed from metal, resin, or the like, for example.

**[0017]** The light-emitting unit 11 is constituted by a light-emitting LED, for example, and emits light containing wavelengths that pass through a living body. When the light 10 receives a supply of electric energy from a power supply (not shown) via the drive circuit 12 while a switch (not shown) provided on the light 10 is switched ON,

the light 10 emits light of predetermined wavelengths by converting the electric energy into optical energy. Note that the light-emitting unit 11 is not limited to a light-emitting LED and may be any light-emitting body that emits light containing a wavelength that passes through a living body.

**[0018]** The light 10 is optically connected to an incident end portion 20I of the optical fiber 20, to be described below, so that the light emitted by the light-emitting unit 11 of the light 10 enters the incident end portion 20I of the optical fiber 20.

**[0019]** The processing unit 13 is a CPU or the like, for example, having one or a plurality of processors and corresponding peripheral circuits, and performs overall control of the entire operation of the light 10 based on a program or the like stored in the storage unit 14.

**[0020]** The storage unit 14 is constituted by a nonvolatile memory or the like, such as an EEPROM (Electrically Erasable and Programmable Read Only Memory), for example, and stores preset control information and the like relating to the light 10.

**[0021]** The communication unit 15 includes a communication interface circuit for connecting the light 10 to the communication network, and communicates with the communication network. Note that the light 10 may have a simpler configuration not including the communication unit 15 and so on.

**[0022]** Here, using Fig. 3, the wavelengths of the light emitted by the light 10 will be described. Fig. 3 shows the light absorption coefficient of each of oxyhemoglobin, reduced hemoglobin, melanin, and water, which are the main constituent elements of a living body. On the graph in Fig. 3, the horizontal axis shows the wavelength (nm) and the vertical axis shows the absorption coefficient.

**[0023]** As shown in Fig. 3, absorption by blood (in other words, hemoglobin) is high in a wavelength region at or below approximately 650 nm, while absorption by water is high in a wavelength region exceeding approximately 950 nm. In a wavelength region of no less than approximately 650 nm and no more than approximately 950 nm, meanwhile, the respective absorption coefficients of hemoglobin and water are comparatively low. It can therefore be said that light in this wavelength region (no less than approximately 650 nm and no more than approximately 950 nm) passes through a living body more easily than light in another wavelength region.

**[0024]** There are no particular limitations on the wavelengths of the light emitted by the light-emitting unit 11 of the light 10 as long as wavelengths that pass through a living body are included therein, but as noted above, the wavelengths preferably include wavelengths within a range of no less than approximately 650 nm and no more than approximately 950 nm.

**[0025]** Further, as shown in Fig. 3, the absorption rate of oxyhemoglobin is particularly low in a wavelength region of no less than approximately 650 nm and no more than approximately 800 nm. Therefore, the wavelengths of the light emitted by the light-emitting unit 11 of the light 10 preferably include at least a part of a wavelength region of no less than approximately 650 nm and no more than approximately 800 nm.

**[0026]** Furthermore, as shown in Fig. 3, the absorption rate of reduced hemoglobin is particularly low in a wavelength range of no less than approximately 800 nm and no more than approximately 950 nm. Therefore, the wavelengths of the light emitted by the light-emitting unit 11 of the light 10 preferably include at least a part of a wavelength region of no less than approximately 800 nm and no more than approximately 950 nm.

**[0027]** Moreover, as shown in Fig. 3, the absorption rate of water is particularly low in a wavelength range of no less than approximately 650 nm and no more than approximately 700 nm. Therefore, the wavelengths of the light emitted by the light-emitting unit 11 of the light 10 preferably include at least a part of a wavelength region of no less than approximately 650 nm and no more than approximately 700 nm.

**[0028]** (2-2) Optical fiber 20

The optical fiber 20 is an example of a light guide that takes the shape of a narrow, flexible fiber, for example, and can be inserted into the interior of a medical tube T, as shown in Fig. 1. The optical fiber 20 has a two-layer structure constituted by, for example, a central core (not shown) formed from silica glass, plastic, or the like, and cladding (not shown) covering the periphery of the central core.

**[0029]** As shown in Fig. 1, the incident end portion 20I through which the light emitted by the light 10 and so on enters is formed on one end of the optical fiber 20. The incident end portion 20I is positioned so as to be optically connectable to the light 10 in a state where the optical fiber 20 is inserted into the interior of the medical tube T. The refractive index of the core of the optical fiber 20 is set to be higher than that of the cladding of the optical fiber 20. Therefore, the light entering from the incident end 20I propagates inside the optical fiber 20 while undergoing total reflection at the boundary of the core and cladding.

**[0030]** As shown in Fig. 1, an exit end portion 20E through which the light exits is formed on the other end of the optical fiber 20. When the optical fiber 20 correctly reaches the stomach while inserted into the interior of the medical tube T, the exit end portion 20E is disposed inside the stomach (indicated by a reference symbol S in Fig. 1).

**[0031]** Here, referring to Fig. 4, the configuration of the exit end portion 20E side of the optical fiber 20 will be explained. As shown in Fig. 4, a scattering portion 21 is optically connected to the exit end portion 20E of the optical fiber 20. The scattering portion 21 is composed of, for example, a light transmissive resin having a cylindrical shape containing a predetermined scattering material. The light that propagates through the core of the optical fiber 20 and reaches the exit end portion 20E is scattered in various directions by the scattering portion 21 after being emitted from the exit end portion 20E. The scattered light passes through the stomach and other body parts and exits the living body so as to partially reach the camera 30.

**[0032]** As a predetermined scattering material contained by the scattering portion 21, for example, a scattering material having the property that the degree of scattering against light is greater for light with a shorter wavelength is suitably used. The predetermined scattering material may be, for example, a fluorescent pigment. The scattering portion 21 may contain a plurality of types of scattering materials. The content rate of the scattering material of the scattering portion 21 may be uniform throughout the scattering portion 21. Alternatively, the content rate of the scattering material in the scattering portion 21 may be non-uniform throughout the scattering portion 21. For example, the content rate of the scattering material of the scattering portion 21 may be distributed with a predetermined gradient along the optical axis L or other directions, or may differ between the optical fiber 20 side and the other side of the optical fiber 20.

**[0033]** The protective portion 22 is composed of, for example, a light transmissive resin or synthetic quartz glass, etc., which presents a substantially cylindrical shape having a through hole along the axial direction. The protective portion 22 protects at least a part of the optical fiber 20 and at least a part of the scattering portion 21

along the optical axis L (see Fig. 5). The light scattered by the scattering portion 21 passes through the protective portion 22.

**[0034]** Here, referring to Fig. 5, the dimensions of the scattering portion 21 will be explained. Fig. 5 schematically shows the cross section according to the A-A' line in Fig. 4. In Fig. 5, the dotted arrow indicates the optical axis L of the optical fiber 20. The dimension of the scattering portion 21 in the direction parallel to the optical axis L is H, and the dimension of the scattering portion 21 in the direction perpendicular to the optical axis L is W. As shown in Fig. 5, the dimensions of the scattering portion 21 are set so that H is longer than W. As a result, the optical path with a smaller angular difference from the optical axis L generally has a longer distance to travel in the scattering portion 21, and the probability of light being scattered by the scattering material contained in the scattering portion 21 becomes higher. Therefore, the light emitted from the optical fiber 20 spreads out and travels in directions other than the direction of the optical axis L.

### **[0035]**(2-3) Camera 30

Fig. 6 is a schematic view showing an example of a functional configuration of the camera 30.

**[0036]** The camera 30 is an example of an imaging unit that generates image data by capturing an image of the living body (including a part of the living body) based at least on the light that passes through the living body after being scattered by a scattering portion 21. The camera 30 includes, for example, an image sensor 31, a processing unit 32, a storage unit 33, and a communication unit 34. The camera 30 may be an infrared sensor or an infrared camera that particularly has a high capability of sensing infrared rays, for example.

**[0037]** The image sensor 31 is constituted by a CCD (a Charge Coupled Device), a CMOS (a Complementary Metal Oxide Semiconductor), or the like, for example, and under the control of the processing unit 32, the image sensor 31 detects light that has been condensed by a lens, not shown in the figure, and converts the light into an electric signal.

**[0038]** The processing unit 32 is a CPU or the like, for example, having one or a plurality of processors and corresponding peripheral circuits, and performs overall control of the entire operation of the information processing device based on a program or the like stored in the storage unit 33. The processing unit 32 generates image data based on the electric signal generated by the image sensor 31, for example. Further, the processing unit 32 transmits the generated image data to the user terminal 40 or the database 50 via the communication unit 34.

**[0039]** The storage unit 33 includes at least one of a magnetic tape device, a magnetic disk device, and an optical disk device, for example, and stores a computer program, data, and so on used in the processing executed by the processing unit. The storage unit 33 is an example of an image data storage unit for storing the image data generated when the camera 30 captures an image of the living body.

**[0040]** The communication unit 34 includes a communication interface circuit for connecting the camera 30 to the communication network, and communicates with the communication network.

**[0041]** Note that the camera 30 may also include a display unit (not shown) for displaying the image data generated by the processing unit 32 and so on.

**[0042]** (2-4) User terminal 40

Fig. 6 is a schematic view showing an example of a functional configuration of the user terminal 40. The user terminal 40 may be any general-purpose information processing terminal and includes, for example, a communication unit 41, a storage unit 42, a processing unit 43, an operation unit 44, a display unit 45, and so on.

**[0043]** The communication unit 41 includes a communication interface circuit for connecting the user terminal 40 to the communication network, and communicates with the communication network.

**[0044]** The storage unit 42 includes at least one of a magnetic tape device, a magnetic disk device, and an optical disk device, for example, and stores a computer program, data, and so on used in the processing executed by the processing unit. The storage unit 42 is an example of the image data storage unit for storing the image data generated when the camera 30 captures an image of the living body.

**[0045]** The processing unit 43 is a CPU or the like, for example, having one or a plurality of processors and corresponding peripheral circuits, and performs overall control of the entire operation of the information processing device based on a program or the like stored in the storage unit. The processing unit 43 may determine whether or not the position of the medical tube T is appropriate by analyzing image data received from the camera 30 over the communication network. Further, the processing unit 13 may transmit the image data received from the camera 30 over the communication network to the database 50, for example. Furthermore, the processing unit 13 may transmit a control signal for switching the switch of the light 10 ON and OFF to the light 10, for example.

**[0046]** The operation unit 44 is constituted by a touch panel, key buttons, or the like, for example, and serves to receive operations performed by a user to input

alphabetic characters, numerals, symbols, and so on and supply signals corresponding to the operations to the processing unit.

**[0047]** The display unit 45 is constituted by a liquid crystal display, an organic EL (Electro-Luminescence) display, or the like, for example, and displays images based on display data supplied from the processing unit and so on.

**[0048]** (2-5) Database 50

The database 50 is a database managed by a medical institution such as a hospital, for example, and includes at least one of a magnetic tape device, a magnetic disk device, and an optical disk device. The database 50 receives image data from the camera 30 or the user terminal 40, for example, and stores the received image data. In other words, the database 50 is an example of the image data storage unit for storing the image data generated when the camera 30 captures an image of the living body. The database 50 may be connected to an external information processing device, such as a management server used by a medical institution or the like, for example, via a communication network. The external information processing device may obtain the image data stored in the database 50 and execute processing corresponding to various aims on the image data.

**[0049]** (3) Use method and operation

Next, a use method and an operation of the medical tube position confirmation system 1 will be described.

**[0050]** First, an operator checks the end portion of the medical tube T in the nasal cavity or the like of the patient and then inserts the optical fiber 20 into the interior of the medical tube T by a predetermined length, starting with the exit end portion 20E which is optically connected with a scattering portion 21.

**[0051]**Next, the switch (not shown) provided on the light 10 is switched ON so that the light 10 emits light. At this time, the operator may cause the light 10 to emit light by operating the switch of the light 10, for example. Alternatively, the operator may cause the light 10 to emit light by operating the user terminal 40 so that a control signal for switching the switch of the light 10 ON is transmitted from the user terminal 40 to the light 10.

**[0052]**When the light 10 emits light, the light emitted by the light 10 enters the incident end portion 20I of the optical fiber 20. The light that enters the incident end portion 20I propagates through the interior of the optical fiber 20 by total reflection so as to reach the exit end portion 20E. Having reached the exit end portion 20E, the light exits through the exit end portion 20E and then is scattered by a scattering portion 21, and a part of the light passes through the body of the patient.

**[0053]**The operator then checks the position of the light passing through the body of the patient in order to determine whether or not the position of the light is a position corresponding to the stomach. When the position of the light is a position corresponding to the stomach, it can be determined that the medical tube T has reached the stomach appropriately. When the position of the light is not a position corresponding to the stomach or when the presence of the light cannot be confirmed, it can be determined that the medical tube T has not reached the stomach. Here, the position of the light may be checked using either a method of visual confirmation by the operator or a method employing the image data generated by the camera 30. In the method employing the image data generated by the camera 30, for example, the user terminal 40 receives from the camera 30 the image data generated by the camera 30 based at least on the light passing through the stomach and other body

parts. The user terminal 40 then analyzes the image data to determine whether or not the position of the light is a position corresponding to the stomach.

#### **[0054](4) Miscellaneous**

Note that generally, the optical intensity required for light to pass from the interior of the stomach to the exterior of the body is lower than the optical intensity required for light to pass from the interior of the lungs and trachea to the exterior of the body. Therefore, the light source, such as the light 10, may be set to emit light at an intensity that equals or exceeds a first intensity required for light to pass from the interior of the stomach to the exterior of the body but is lower than a second intensity required for light to pass from the interior of the lungs and trachea to the exterior of the body. According to this configuration, there is no need to determine the position of the stomach during visual confirmation of the light by the operator or analysis of the image data, and it can be determined that the medical tube T has appropriately reached the stomach simply by determining whether or not the light can be confirmed.

#### **[0055][Modification]**

Figure 8 illustrates another scattering portion 60. Fig. 8 is a cross-sectional view similar to that of Fig. 5 described above. As shown in Fig. 8, a scattering portion 60 is coupled to the emit end portion 20E of the optical fiber 20 by an adhesive resin 61. The scattering portion 60 has a substantially conical shape formed from an apex 60T (protruded portion), a side surface 60R, and a bottom surface 60B. The apex 60T of the scattering portion 60 faces the optical fiber 20. The side surface 60R of the scattering portion 60 has a mirror surface formed, for example, by aluminum vapor deposition. The bottom surface 60B of the scattering portion 60 faces the opposite side of the optical fiber 20.

**[0056]** As shown by the solid arrows in Fig. 8, when the light propagating in the optical fiber 20 and emitted from the exit end portion 20E reaches the side surface 60R of the scattering portion 60, it is reflected by the side surface 60R. By adjusting the angle  $\theta$  formed between the optical axis L and the side surface 60R of the scattering portion 60, the direction of the reflected light can be adjusted. The value of the angle  $\theta$  is not particularly limited, but approximately 45 degrees is preferred.

**[0057]** The shape of the scattering portion 60 described above is an example, and the scattering portion 60 may present any shape as long as a reflective surface is formed to reflect the light propagating in the optical fiber 20 and emitted from the exit end portion 20E. The shape of the bottom surface of the scattering portion 60 (the surface provided on the opposite side of the optical fiber 20) is not particularly limited, but may include, for example, an ellipse, a polygon (including polygons in which the length of each side is not equal), or any other arbitrary shape in addition to a regular circle. These illustrated shapes may be abbreviated shapes that do not necessarily meet the geometric definition. The bottom surface of the scattering portion 60 may be shaped to cover only a part of the exit end portion 20E of the optical fiber 20 in a plane perpendicular to the optical axis L. As a result, a portion of the light emitted from the exit end portion 20E of the optical fiber 20 will travel toward the living body without being reflected by the scattering portion 60. By adjusting the size of the bottom surface of the scattering portion 60, it is possible to adjust the distribution of the light traveling direction.

**[0058]** As described above, the side surface 60R of the scattering portion 60 presents an abbreviated linear shape in the cross-sectional view shown in FIG. 8 (cross-sectional view by a plane passing through the optical axis L) and has a predetermined gradient ( $\theta$ ) with respect to the optical axis L. However, the side

surface of the scattering portion 60 may not present a straight line shape in the said cross-sectional view, and the gradient with respect to the optical axis L may vary depending on the position. Also, the side surface of the scattering portion 60 may have a mirror surface formed by a method other than aluminum vapor deposition. The side surface of the scattering portion 60 does not have to be a specular surface that reflects light, but may be, for example, a scattering surface that scatters light.

**[0059]** According to the embodiment (including variations) described above, light emitted from a light source and including a wavelength transmitting through a living body is guided inside a light guide inserted in a medical tube, and after being emitted from an output end portion of the light guide placed in the stomach, the light is scattered extensively by the scattering portion. Since the emitted light is widely scattered, the operator can easily check the light transmitted through the stomach and the living body from outside the living body, which makes it easier to confirm the position of the medical tube.

**[0060]** The embodiment (including variations) described above is to be used to facilitate understanding of the present invention, and the present invention is not limited thereto. The elements included in the embodiment, as well as the arrangements, materials, conditions, shapes, sizes, and so on thereof, are not limited to the cited examples and may be modified as appropriate. Moreover, configurations illustrated in different embodiments may be partially replaced or combined.

#### Reference Signs List

#### **[0061]**

- 1 Medical tube position confirmation system

|    |                     |
|----|---------------------|
| 10 | Light               |
| 11 | Light-emitting unit |
| 12 | Drive circuit       |
| 13 | Processing unit     |
| 14 | Storage unit        |
| 15 | Communication unit  |
| 20 | Optical fiber       |
| 21 | Scattering portion  |
| 22 | Protective portion  |
| 30 | Camera              |
| 31 | Image sensor        |
| 32 | Processing unit     |
| 33 | Storage unit        |
| 34 | Communication unit  |
| 40 | User terminal       |
| 41 | Communication unit  |
| 42 | Storage unit        |
| 43 | Processing unit     |
| 44 | Operation unit      |
| 45 | Display unit        |
| 60 | Scattering portion  |

60T Apex

60R Side surface

60B Bottom surface

What is claimed is:

1. A medical tube position confirmation system for confirming the position of a medical tube that is used to supply nutrients to the interior of a body by means of tube feeding while an end portion thereof is inserted into (placed in) the stomach, the system comprising:

a light guide that is configured to guide light entering through an incident end portion so that the light exits through an exit end portion, and is configured to be insertable into the medical tube so that the exit end portion is disposed in the interior of the stomach; and

a light source for emitting light including a wavelength passing through a living body, the light source being optically connected to the incident end of the light guide so that the light enters the light guide; and

a scattering part optically connected to the light guide on the exit end portion of the light guide so as to scatter light emitted by the light guide.

2. The medical tube position confirmation system according to claim 1, wherein the scattering part is composed of a resin containing a predetermined scattering material.

3. The medical tube position confirmation system according to claim 2, wherein the predetermined scattering material scatters light with a higher degree of scattering for a shorter wavelength.

4. The medical tube position confirmation system according to any one of claims 1 to 3, wherein the scattering part has longer dimensions in a direction parallel with a

direction of an optical axis of the light guide than in a direction perpendicular to the direction of the optical axis.

5. The medical tube position confirmation system according to claim 1, wherein the scattering part has a reflecting surface for reflecting light emitted by the light guide.

6. The medical tube position confirmation system according to claim 5, wherein the reflecting surface is formed by aluminum vapor deposition.

7. The medical tube position confirmation system according to claim 5 or 6, wherein the scattering part comprises:

a protruded portion facing the light guide; and

a reflecting surface extended from the protruded portion.

8. The medical tube position confirmation system according to claim 7, wherein the scattering part has a substantially conical shape with the protruded portion at an apex thereof and the reflecting surface on a side surface thereof.

9. The medical tube position confirmation system according to any one of claims 1 to 8, wherein the light source is set to emit light at an intensity that equals or exceeds a first intensity required for light to pass from the interior of the stomach to the exterior of the body but is lower than a second intensity required for light to pass from the interior of the lungs and trachea to the exterior of the body.

10. The medical tube position confirmation system according to any one of claims 1 to 9, further comprising an imaging unit for capturing an image of the living body based at least on the light that exits through the exit end portion of the light guide and passes through the living body.

11. The medical tube position confirmation system according to claim 10, further comprising an image data storage unit for storing image data generated when the imaging unit captures an image of the living body.