PALIPERIDONE IMPLANT FORMULATION

DESCRIPTION

TECHNICAL FIELD

The present invention relates to pharmaceutical composition for intramuscular injection comprising the drug paliperidone and/or its salts wherein the composition releases the drug with an immediate onset of action and continuously for at least 8 weeks, and wherein the composition has a pharmacokinetic profile in vivo that makes it suitable to be administered each 8 weeks or even longer periods. Specifically, the present invention is related to compositions for injectable *in-situ* forming biodegradable implants comprising paliperidone.

BACKGROUND ART

Paliperidone is an atypical antipsychotic drug with benzisoxazole and piperidine functional groups, which act as strong dopaminergic antagonist and selective serotonin receptor antagonist. One of the intrinsic problems that paliperidone-targeted patients usually face is the dissociation of some schizophrenic patients from the treatment, moreover when it consists of a daily medication, leading to irregular or inconstant treatments and favouring the appearance of psychotic crisis. Moreover, this kind of therapy gives rise to high differences in the plasma levels (measured as the difference between Cmax and Cmin) in patients, therefore usually affecting the patient's mood.

Therefore, paliperidone is a good drug candidate for incorporation into sustained delivery devices, where the patients would be covered or treated for long time periods with just one dose and without the need of caregivers to pay attention to a daily medication, and where more homogeneous plasma levels in the patient are desirable. Other indications may involve bipolar mania and schizoaffective disorder, and its possible use in autism and Asperger's syndrome and Tourette's disorder may be of benefit to the patients.

Many patients with these mental illnesses achieve symptom stability with available oral antipsychotic medications; however, it is estimated that up to 75% have difficulty adhering to a daily oral treatment regimen, i.e. compliance problems. Problems with adherence often result in worsening of symptoms, suboptimal treatment response, frequent relapses and re-hospitalizations, and an inability to benefit from rehabilitative and psychosocial therapies.

Paliperidone recently received marketing approval as the first oral atypical antipsychotic with an extended release, which is achieved by an osmotic-controlled release oral delivery system. Paliperidone ER (WO2006/17537) is marketed as Invega Sustenna® and unsaturated derivatives thereof are described in WO2008/128436. Other extended release oral dosage forms for paliperidone are under development.

Due the presence of a secondary hydroxyl group, paliperidone may be provided as a prodrug. WO2009/15828 details acid-labile low molecular weight prodrugs of paliperidone intended to undergo hydrolysis in the stomach.

Therefore, in view of the state of the art, it is of interest to develop very long-acting, injectable depots of paliperidone. There is great need to improve the compliance factor particularly in the treatment of schizophrenia. The development of once-weekly or even longer acting injectable depot formulations of those drugs will mark a significant step forward to ensure continuous and steady supply of the effective medication.

EP2234617 describes ester-linked prodrugs of paliperidone to provide sustained plasma concentrations of paliperidone when administered once monthly, which may greatly enhance compliance with dosing. The substance paliperidone palmitate is approved as a once-monthly atypical antipsychotic intramuscular injection for treating schizophrenia and preventing recurrence of its symptoms. Paliperidone palmitate is formulated in a submicrocrystalline form. Paliperidone palmitate due to its dissolution rate-limited absorption exhibits flip-flop kinetics, where the apparent half-life is controlled by the absorption rate constant. Additionally the volume of injected drug product also impacts

the apparent rate constant. It was also discovered that deltoid injections result in a faster rise in initial plasma concentration, facilitating a rapid attainment of potential therapeutic concentrations. Consequently, to facilitate patients' attaining a rapid therapeutic concentration of paliperidone it is preferred to provide the initial loading dose of paliperidone palmitate in the deltoids. The loading dose should be from about 100 mg-eq. to about 150 mg-eq. of paliperidone provided in the form of paliperidone palmitate. After the first or more preferably after the second loading dose injection patients will be approaching a steady state concentration of paliperidone in their plasma and may be injected in either the deltoid or the gluteal muscle thereafter. However, it is preferred that the patients receive further injections in the gluteal muscle. US2009/163519 outlines corresponding dosing regimen for long-acting injectable paliperidone esters of the palmitate type.

Other depot formulation it is described by the international application WO2011/42453. This specification describes a pharmaceutical composition for subcutaneous injection comprising a paliperidone compound. In particular the composition releases the paliperidone with an immediate onset of action and has an extended release time. Moreover, this specification relates to a pharmaceutical composition for subcutaneous injection comprising a paliperidone compound in a certain concentration.

Finally, another antipsychotic injectable depot composition is described in the international application number WO2011/151355. This application is directed to a composition that can be used to deliver an antipsychotic prodrug of risperidone, such as paliperidone, as an injectable in-situ forming biodegradable implant for extended release providing therapeutic plasma levels from the first day. The composition is in the form of drug suspension on a biodegradable and biocompatible copolymer or copolymers solution using water miscible solvents that is administered in liquid form. Once the composition contacts the body fluids, the polymer matrix hardens retaining the drug, forming a solid or semisolid implant that releases the drug in a continuous manner.

Paliperidone was formulated as an implant as is described in WO2011/151355. However, after the data was analyzed from the clinical trials of this formulation it was discovered that the absorption of paliperidone from these injections was far more complex than was originally anticipated for obtaining a release the drug with an immediate onset of action and continuously for at least 8 weeks. Additionally, attaining a potential therapeutic plasma level of paliperidone in patients was discovered to be dependent on the molecular weight of the biocompatible polymer based on lactic and glycolic acid having a monomer ratio of lactic to glycolic acid. Due to the challenging nature of ensuring an optimum plasma concentration-time profile for treating patients with paliperidone, it is desirable to develop a dosing regimen that fulfils this goal in patients in need of treatment.

SUMMARY OF THE INVENTION

Therefore, the compositions already described in the state of the art do not cover the existing needs in paliperidone compositions, kits and treatments for psychiatric disorders, and there still exists a need of compositions and devices to allow a controlled, constant release of the drug during prolonged periods of time during at least 8 weeks without a concomitant treatment or initial doses of risperidone and/or paliperidone.

The solution of this necessity is provided with an injectable intramuscular depot composition suitable for forming an in situ solid implant in a body, comprising a drug which is paliperidone, a biocompatible copolymer based on lactic and glycolic acid having a monomer ratio of lactic to glycolic acid in the range from 45:55 to 55:45 and preferably about 50:50 and a DMSO solvent, wherein the composition releases the drug with an immediate onset of action and continuously for at least 8 weeks and wherein the composition has a pharmacokinetic profile in vivo with substantially no burst release of the drug characterised in that the biocompatible copolymer has a molecular weight between 27 and 47 kDa, more preferably between 31 to 43 kDa and even more preferably 31 to 40 kDa and has an inherent viscosity in the range of 0.27-0.31dl/g ± 10%.

In one aspect of the present invention there is provided a dosing regimen for administering paliperidone to a psychiatric patient in need of treatment comprising administering intramuscularly a first dose from about 75 mg to about 250 mg of paliperidone formulated in a sustained release formulation on the first day of treatment; administering intramuscularly other following doses from about 75 mg to about 250 mg of paliperidone formulated in a sustained release formulation between about the 56th to 65th day of treatment.

DETAILED DESCRIPTION OF THE INVENTION

The compositions of the invention comprise at least a polymer or polymer matrix, a solvent and a drug.

One important aspect of this invention is an injectable intramuscular depot composition suitable for forming an in situ solid implant in a body, comprising a drug which is paliperidone or any pharmaceutically acceptable salt thereof in any combination, a biocompatible copolymer based on lactic and glycolic acid having a monomer ratio of lactic to glycolic acid in the range from 45:55 to 55:45 and preferably about 50:50, and a DMSO solvent, wherein the composition releases the drug with an immediate onset of action and continuously for at least 8 weeks and wherein the composition has a pharmacokinetic profile in vivo suitable to be administered between about 56th to 65th days after the preceding injection, characterised in that the biocompatible copolymer has a molecular weight between 27 and 47 kDa, more preferably between 31 and 43 kDa and even more preferably between 31 and 40 kDa and has an inherent viscosity in the range of 0.27-0.31dl/g ± 10%.

In a preferred embodiment of the invention, the biocompatible copolymer is gamma or beta irradiated in the dose range of 10-30 kGy ±10% measured at a temperature between –40ºC to +35ºC to adjust its molecular weight to a range between 27 and 47 kDa, more

preferably between 31 and 43 kDa and even more preferably 31 to 40 kDa, and its inherent viscosity to a range of of 0.27-0.31dl/g ± 10%.

In a more preferred embodiment, the polymer is radiated at 15-25 kGy ±10% measured at the temperature of 8 ºC.

A preferred composition has the particle size distribution of the drug as follows:

- less than 10% particles smaller than 10 microns;
- less than 10% particles larger than 225 and preferably larger than 200 microns, and
- a d0.5 value in the range of 40-90 microns.

If not otherwise specified, the particle size distribution was determined by light scattering technique using laser diffractor in wet mode. It is known that particle size distribution results can be altered as a function of the material treatment such the use of high concentrate surfactant agents and/or strong force energies (vortex, sonication, etc). If nothing else is mentioned, drug is not treated and samples are prepared by direct addition to the tank under moderate stirring (2000-3500 rpm). The methodology applied on present invention to determine the drug particle size distribution mimics in a more faithfully way the behavior of the drug powder on the injectable formulation herein described than other methods which apply force energies to the sample and/or use high concentrate surfactant agents for preparing the samples in order to achieve high degrees of powder disaggregation that cannot be simulated during the manual reconstitution process of the formulation.

According to another embodiment of the invention, the drug/(polymer+drug) mass ratio is about 33%, the content of drug is about 13% w/w of total formulation, and the viscosity of solution between polymer and DMSO is in the range of 1.2-2.5 Pa.s, preferably in the range of 1.5-2.1 Pa.s., and more preferably in the range of 1.7 – 1.8 Pa.s. ±10%.

In another embodiment, when the composition is formed, the drug is partially suspended with a solubility of drug in the DMSO solvent below 10 mg/ml.

In yet another embodiment, the composition is a sterile composition.

According to another aspect of the invention, the composition is a sterile composition and is suitable for the treatment of schizophrenia or bipolar disorders in the human body.

According to another aspect, the invention provides a pharmaceutical kit suitable for the in situ formation of a biodegradable implant in a body comprising the composition claimed, wherein the drug and the biocompatible polymer are contained in a first container, and the solvent is contained in a second, separate container. Preferably, at least one of the first and second containers is a syringe, a vial, a device or a cartridge, either disposable or not and more preferably both the first and the second containers are disposable syringes.

According to another aspect, the invention provides a method for the manufacturing of the said composition, comprising the step of providing a biocompatible copolymer having an initial polymer weight higher than required for the intramuscular depot composition and then adjusting its molecular weight to between 27 and 47 kDa and preferably 31 to 43 kDa and more preferably 31 to 40 kDa and its inherent viscosity to a range of 0.27-0.31 dl/g by irradiating it with gamma or beta radiation in the dose range of 10-30 kGy ±10% measured at a temperature between –40ºC and +35ºC ± 10%.

Preferably, when the biocompatible polymer has an initial molecular weight of about 50 kDa, it is irradiated with a radiation dose of about 16KGy measured at 8ºC to reduce its molecular weight to between 27 and 47 kDa, more preferably 31 to 43 kDa and even more preferably 31 to 40 kDa.

Preferably, when the biocompatible polymer has an initial molecular weight of about 54 kDa, it is irradiated with a radiation dose of about 25 kGy measured at 8ºC to reduce its molecular weight to between 31 and 43 kDa.

Preferably, when the biocompatible polymer has an initial molecular weight of about 63 kDa, it is irradiated with a radiation dose of about 30 kGy measured at 8ºC to reduce its molecular weight to between 30 and 43 kDa, preferably between 31 and 36 kDa.

According to another aspect, the invention provides a dosing regimen method for administering an injectable intramuscular depot composition according to the invention to a patient in need of psychiatric treatment comprising:

a) administering intramuscularly to the patient a first dose in the amount of 75 mg to 250 mg of the injectable depot composition, at a point of time between the 24th day and the 35th day counting from the previous administration day;

b) administering a subsequent dose of the injectable depot composition in the amount of 75 mg to 250 mg from about the 56th day to about the 65th day after the administration of said first dose; and

c) repeating step b) whenever required.

Preferably, said first dose is about 100 mg to about 200 mg and this is equivalent than other doses.

Preferably, the steps a) and b) are repeated as many times as required.

The **polymer** or polymer matrix is preferably a biocompatible and biodegradable polymer matrix. In order not to cause any severe damage to the body following administration, the preferred polymers are biocompatible, non-toxic for the human body, not carcinogenic, and do not induce significant tissue inflammation. The polymers are preferably biodegradable in order to allow natural degradation by body processes, so that they are readily disposable and do not accumulate in the body. The preferred polymeric matrices in the practice in this invention are selected from end-capped terminal carboxylic poly-lactide and poly-glycolic acid copolymers mixed in a ratio of ranging from 45:55 to 55:45, preferably about 50:50, with an average molecular weight in the range of 27 and 47 kDa

and preferably 31 to 43 kDa and more preferably 31 to 40 kDa and an inherent viscosity preferably in the range of 0.27-0.31dl/g ±10%.

A commercial polymer with the required molecular weight can certainly be used. However, we have determined that the essential range of its molecular weight is between 31 and 43 kDa and preferably between 31 and 40 kDa. Additionally we have determined in an in-house custom design that the molecular weight of the polymer can be varied by irradiating it with a radiation dose of between 10 and 30 kGy at a temperature between –40ºC and +35ºC, and this was not obvious in view of the state of the art to the skilled person (see figure 7). For example, the molecular weight of a commercially available polymer in a certain moment can be 50 kDa as an average value. We have determined a method for varying this molecular weight by irradiating the polymer with a certain dose of radiation that can be previously calculated. If done under controlled conditions, it is possible to obtain a mathematical model showing that the molecular weight of the polymer can be decreased with increasing irradiation doses.

Therefore, for example:

- When we need to use a PLGA polymer having a molecular weight between 31 and 43 kDa and an inherent viscosity value in the range of 0.27-0.31 dl/g ±10%, and we have as the starting polymer a polymer with 54 kDa of average molecular weight, we have determined that a radiation dose of 25 kGy is required to reduce its molecular weight to the cited range of 31-43 kDa, more preferably between 37-43 kDa.

- When we need to use a PLGA polymer having a molecular weight between 31 and 43 kDa, preferably between 31 and 40 kDa and an inherent viscosity value in the range of 0.27-0.31 dl/g ±10%., and we have as the starting polymer a polymer with 50 kDa of average molecular weight, we have determined that a radiation dose of 16 kGy is required to reduce its molecular weight to the cited range of 31-43 kDa, more preferably between 37-43 kDa ± 10%.

- When we need to use a PLGA polymer having a molecular weight between 31 and 43 kDa and an inherent viscosity value in the range of 0.27-0.31 dl/g ±10%, and we have as the starting polymer a polymer with 50 kDa of average molecular weight, we have determined that a radiation dose of 25 kGy is required to reduce its molecular weight to the cited range of 31-43 kDa, more preferably between 31-37 kDa.

- When we need to use a PLGA polymer having a molecular weight between 31 and 43 kDa and preferably between 31 and 40 kDa, and an inherent viscosity value in the range of 0.27-0.31 dl/g ±10% and we have as the starting polymer a polymer with 38 kDa of average molecular weight, we have determined that there is no need to use any radiation dose.

- When we need to use a PLGA polymer having a molecular weight between 31 and 43 kDa and preferably between 31 and 40 kDa, and an inherent viscosity value in the range of 0.27-0.31 dl/g ±10%, and we have as the starting polymer a polymer with 63 kDa of average molecular weight, we have determined that a radiation dose of 30 kGy is required to reduce its molecular weight to the cited range of 31 and 43 kDa, more preferably in the range of 31 and 40 kDa, and even more preferably in the range of 31-36 kDa.

In these experimental tests, the temperature conditions for the polymer during the irradiation were about 8ºC. However, other temperatures can be used, such as e.g. lower than 35ºC, or lower than 25ºC, although in these cases the relationships between the radiation dose and the resulting molecular weight may vary.

The procedure is especially suitable for the manufacturing of the compositions described in the present invention. Furthermore, the filling of the solid polymer into syringes represents a real challenge in the manufacturing of injectable formulations. The polymer, manufactured as a non-sterile product, requires undergoing sterilization in order to achieve a formulation that can be injected into human beings. Probably the best way to

solve this technical issue is to subject the polymer to sterilization by gamma or beta irradiation. Irradiation represents a challenging issue when using biodegradable polymers, as irradiation can disrupt the chains into fractions of smaller size. Control of the polymer molecular weight appears as again as the critical parameter to control the final characteristics of a product after a sterilization process.

As previously explained, chain size reduction by irradiation can be mathematically modelled or controlled in order to predict the final molecular weight of a polymer to be used as raw material having a molecular weight higher than desired. Therefore, once determined the fill weight of the polymer to be filled in a container (for example, the fill weight of the polymer in a syringe) and the bio-burden present in the polymer as raw material, the irradiation dose required to get the polymer sterile (as specified by ISO 11137) is selected for the required fill weight. Then the mathematical model describing the loss of molecular weight for a certain polymer versus the irradiated dose can identify the initial molecular weight of the polymer to be used as raw material required obtaining, after the irradiation process, a polymer with the desired final molecular weight for the formulation. As the availability of a polymer with a specific molecular weight can be somewhat limited, then we can alternatively select an available polymer with a molecular weight that is higher to what is required according to the irradiation dose identified, and then adjust the irradiation dose to a higher value in order to obtain a sterile polymer with the required molecular weight.

The concentration of the polymeric component in the compositions of the invention is preferably comprised in the range of 24-50%, (expressed as the percentage of polymer weight based on total formulation weight) and more preferably 25-27%.

For the purpose of the present invention, throughout the present specification the term intrinsic or inherent viscosity (η_{inh}) of the polymer is defined as the ratio of the natural logarithm of the relative viscosity, η_r, to the mass concentration of the polymer, c, i.e.:

$$\eta_{inh} = (\ln \eta_r)/c$$

and the relative viscosity (η_r) is the ratio of the viscosity of the solution η to the viscosity of the solvent η_s, i.e.:

$$\eta_r = \eta / \eta_s$$

If not otherwise specified, the intrinsic viscosity and molecular weight values throughout the present specification are to be understood as measured with the method explained in example 1. The value of intrinsic viscosity is considered in the present specification, as commonly accepted in the art, as an indirect indicator of the polymer molecular weight. In this way, a reduction in the intrinsic viscosity of a polymer, measured at a given concentration in a certain solvent, with same monomer composition and terminal end groups, is an indication of a reduction in the polymer molecular weight (IUPAC. Basic definitions of terms relating to polymers 1974. Pure Appl. Chem. 40, 477-491 (1974).

The preferred **solvents** are non-toxic, biocompatible and appropriate for parenteral injection. Solvents susceptible of causing toxicity should not be used for the injection of any material into any living body. More preferably, selected solvents are biocompatible in order not to cause any severe tissue irritation or necrosis at the injection site. Therefore, the solvent is preferably classified as class II or III, and more preferably class III, according to ICH Guidelines. For the formation of the *in-situ* implant, the solvent should preferably diffuse quickly from the polymeric solution towards surrounding tissues when is exposed to physiological fluids. Consequently, the solvent is preferably DMSO.

The **drug** is preferably paliperidone and/or its pharmaceutically acceptable salts and combinations thereof. This drug is preferably partially suspended in the solvent. Partially suspended means that the solubility of drug in the DMSO solvent is preferably below 10 mg/ml, when the formulation or implant is formed, is below 10 mg/ml in the total volume of DMSO and calculated at 25 ºC. The advantage of this low solubility is that the initial burst of the drug when the solvent diffuses to the external aqueous medium is greatly reduced. In addition, in the final compositions of the invention the drug is provided in a preferred concentration between 4 and 16 wt%, expressed as the percentage of the drug

in respect of the total composition weight. More preferably, the drug content is between 7 and 15%, and most preferably about 13% in respect of the total composition weight.

One of the factors contributing to control the initial release of the composition of the invention is the viscosity of the polymeric solution. The "polymeric solution", which is defined as the combination of the polymer matrix and the solvent where it is dissolved, has a preferred viscosity in the range of 1.5 to 2.5 Pa.s, more preferably in the range of 1.5-2.3Pa.s, and even more preferably between 1.5-2.1Pa.s ±10%.

A second factor contributing to control the initial release of the compositions of the invention is the biocompatible copolymer molecular weight that must be between 27 and 47 kDa and preferably 31 to 43 kDa and more preferably 31 to 40 kDa. The adequate balance in this composition between drug solubility in the solvent and the molecular weight of the polymer in the implant (that controls the polymer precipitation process and the final structural characteristics of the implant) allows the formulation to limit the amount of paliperidone that can be released in the solvent diffusion phase after the intramuscular injection. Once the formulation is injected in the intramuscular tissue, the DMSO is rapidly dissolved in the surrounding aqueous environment. The relative increase of the polymer concentration in DMSO over the polymer solubility in the solvent leads to the formation of a polymer precipitate that entraps the paliperidone that was not solubilized in the solvent. Molecular weight of the polymer has a great impact in this critical step, as too low weighed chains have delayed precipitation time compared to the chains having the weight in the adequate range. This delayed precipitation allows the drug to increase contact with the surrounding fluids towards the drug is being released. Therefore, low molecular weighed chains lead to an excessive release of paliperidone after the injection and potentially to obtain toxic plasma levels on the first days after the injection and/or to obtain a formulation that is not capable to cover a minimum of 8 weeks between injections. Molecular weight of the polymer also can affect the release of the drug from the intramuscularly injected implant after solvent diffusion and polymer precipitation. Molecular weights over the specified range are not capable to maintain adequate release rates of paliperidone by diffusion. Additionally, higher molecular weight

chains in the intramuscular tissue require longer hydrolysis times in order to provide soluble fractions that could release the drug entrapped in the polymer matrix. A higher remaining drug content to be released could lead to the obtention of undesirably high active moiety plasma values, or plasma values after 60 days post injection that could somehow interfere with the following dose as the formulation is intended to be injected several times into the human, each 8 weeks or more days.

The expression "about 50:50" as used in this description, refers to a monomer ratio of lactic to glycolic acid of biocompatible copolymer based on lactic and glycolic acid it is applied in the context of the invention for a monomer ratio measure with an standard technical error of ± 10% .

One important aspect of this invention is an injectable intramuscular depot composition suitable for forming an in situ solid implant in a body, comprising a drug which is paliperidone or any pharmaceutically acceptable salt thereof in any combination, a biocompatible copolymer based on lactic and glycolic acid having a monomer ratio of lactic to glycolic acid in the range from 45:55 to 55:45 and preferably about 50:50 and a DMSO solvent, wherein the composition releases the drug with an immediate onset of action and continuously for at least 8 weeks and wherein the composition has a pharmacokinetic profile in vivo suitable to be administered between about 56^{th} to 65^{th} days after the preceding injection, characterised in that the biocompatible copolymer has a molecular weight to a range between 31 and 43 and preferably between 31 and 40 kDa and has an inherent viscosity to a range of 0.27-0.31dl/g.

In the compositions cited previously, the polymer is radiated at a temperature lower than 35 º C, more preferably lower than 25 and more preferably lower than 8ºC.

This composition has the preferred particle size distribution of the drug as follows:

- less than 10% particles smaller than 10 microns;
- less than 10% particles larger than 200 microns and preferably larger than 225 microns, and
- a d0.5 value in the range of 40-90 microns.

According to an embodiment, the drug / (polymer+drug) mass ratio is about 33% about 33%, the content of drug is about 13% w/w of total formulation, and the viscosity of solution between polymer and DMSO is in the range of 1.5-2.5 Pa.s, more preferably in the range of 1.5-2.1 Pa.s and even more preferably in the range of 1.7 – 1.8 P.a.s.

According to another embodiment, when the composition is formed, the drug is partially suspended with a solubility of drug in the DMSO solvent below 10 mg/ml.

According to yet another embodiment, the composition is a sterile composition and is suitable for the treatment of schizophrenia or bipolar disorders in the human body.

According to another aspect the invention provides a pharmaceutical kit suitable for the in situ formation of a biodegradable implant in a body comprising the composition claimed, wherein the drug and the biocompatible polymer are contained in a first container, and the solvent is contained in a second, separate container. Preferably, at least one of the first and second containers is a syringe, a vial, a device or a cartridge, either disposable or not and more preferably both the first and the second containers are disposable syringes. This aspect of the invention is directed to a kit comprising a first container, preferably syringes, vials, devices or cartridges, all of them either being disposable or not, containing a polymer in solid form, such as PLGA and a drug in the appropriate amounts and a second container, likewise preferably syringes, vials, devices or cartridges, all of them being either disposable or not, containing the water-miscible solvent. When required, the contents of both containers are combined, for example through a connector or by using male-female syringes, and mixed each other so that the compositions according to the invention are reconstituted, for example by moving forwards and backwards the plungers of the syringes. Illustrative preferred embodiments are shown in Figure 5 (syringes connected through a connector device) and in Figure 6 (syringes connected through a direct thread).

According to another aspect, the invention provides a method for the manufacturing of the composition claimed comprising the step of providing a biocompatible copolymer having a polymer weight higher than required for the intramuscular depot composition and then

adjusting its molecular weight to between 31 and 43 and preferably between 31 and 40 kDa and its inherent viscosity to a range of 0.27-0.31 dl/g by irradiating it with gamma or beta radiation in the dose range of 10-30 kGy measured at a temperature between –40ºC and +35ºC.

Preferably, when the biocompatible polymer has an initial molecular weight of about 54 kDa, it is irradiated with a radiation dose of about 25KGy to reduce its molecular weight to between 31 and 43 kDa, and more preferably between 37 and 43 kDa.

Preferably, when the biocompatible polymer has an initial molecular weight of about 50 kDa, it is irradiated with a radiation dose of about 16KGy to reduce its molecular weight to between 35 and 43 kDa, preferably between 37 and 43 kDa.

Preferably, when the biocompatible polymer has an initial molecular weight of about 50 kDa, it is irradiated with a radiation dose of about 25KGy to reduce its molecular weight to between 31 and 37 kDa.

Preferably, when the biocompatible polymer has an initial molecular weight of about 63 kDa, it is irradiated with a radiation dose of about 30 kGy to reduce its molecular weight to between 31 and 43 kDa, and more preferably to 30-36 kDa.

According to another aspect the invention provides a dosing regimen method for administering an injectable intramuscular depot composition according to the invention to a patient in need of psychiatric treatment comprising:

a) administering intramuscularly to the patient a first dose in the amount of 75 mg to 250 mg of the injectable depot composition, at a point of time between the 24th day and the 35th day counting from the previous administration day;
b) administering a subsequent dose of the injectable depot composition in the amount of 75 mg to 250 mg from about the 56th day to about the 65th day after the administration of said first dose; and
c) repeating step b) whenever required.

Preferably, said first dose is about 100 mg to about 200 mg and this is equivalent than other doses.

In a preferred embodiment, the injectable depot composition is sterile as a finished product. In other preferred embodiment, the biocompatible polymer is sterilized previously to its aseptic filling process, preferably by irradiation in the range 15-30 kGy.

In the sense of the present invention, without limitation and in connection with the examples, all technical parameters having an standard technical measure error of ± 10%.

In the sense of the present invention, without limitation and in connection with the examples, it is important to explain that it might be necessary to use a starting regimen in order to accelerate obtaining the desired plasma levels before starting the 8 weekly dosing regimen. This starting regimen could be, for example but not limited to, as it is described in claim 15 or as described below:

A first intramuscular dose of the formulation at day 0, in a dose between 75 to 250 mg, followed by a second dose between days 5-10 with a dose in the range of 75 to 250 mg, followed by a third dose between days 28-35 after the first dose, with a dose in the range of 75-250 mg, and then subsequent 8 weekly doses of the formulation

- A first intramuscular dose of the formulation at day 0, in a dose between 75 to 250 mg, followed by a second dose between days 28-35 with a dose in the range of 75 to 250 mg, followed by a third dose between days 56-65 after the first dose, with a dose in the range of 75-250 mg, and then subsequent 8 weekly doses of the formulation

- Any other combination of strengths and intervals needed to obtain the plasma levels needed to start a 8 weekly administration.

BRIEF DESCRIPTION OF THE FIGURES

Fig 1.- Paliperidone levels profile in dog after the administration of the paliperidone formulation described in example 1 to Beagle dogs (n=3). Dose is 2.5 mg/kg. Results are expressed as ng/ml plasma values of paliperidone versus time. The table describes Area Under the Curve (AUC) of paliperidone plasma levels versus time. AUC all as well as AUC vs three different time frames are included. Units are expressed in h*ng/ml.

Fig 2.- Paliperidone levels profile in dog after the administration of the paliperidone formulation described in example 2 to two cohorts of Beagle dogs (each cohort n=6). Doses were 2.5 and 5 mg/kg. Results are expressed as ng/ml plasma values of paliperidone versus time. The table describes Area Under the Curve (AUC) of paliperidone plasma levels versus time. AUC all as well as AUC vs three different time frames are included. Units are expressed in h*ng/ml.

Fig 3.- Paliperidone levels profile in dog after the administration of the paliperidone formulation described in example 3 to Beagle dogs (n=3). Dose is 7.5 mg/kg. Results are expressed as ng/ml plasma values of paliperidone versus time. The table describes Area Under the Curve (AUC) of paliperidone plasma levels versus time. AUC all as well as AUC vs three different time frames are included. Units are expressed in h*ng/ml.

Fig 4.- Paliperidone levels profile in dog after the administration of the paliperidone formulation described in example 3 to Beagle dogs (n=3). Dose is 2.5 mg/kg. Results are expressed as ng/ml plasma values of paliperidone versus time. The table describes Area Under the Curve (AUC) of paliperidone plasma levels versus time. AUC all as well as AUC vs three different time frames are included. Units are expressed in h*ng/ml.

Fig 5.- Drawing of a kit suitable for the preparation of paliperidone compositions comprising two male syringes linked by a connector. Polymer+paliperidone are contained in one syringe and DMSO filled in the second syringe.

Fig 6.-Drawing of a kit suitable for the preparation of paliperidone compositions comprising a female syringe linked to a male syringe. Polymer+paliperidone can be contained in one syringe and DMSO filled in the second syringe. Preferably female syringe contains polymer+paliperidone as a solids and male syringe is filled with DMSO.

Fig 7- Loss of molecular weight percentage in the custom design. The molecular weight of the polymer can be varied by irradiating it with a certain radiation dose. The table describes the percentage of loss of polymer weight versus radiation dose.

EXAMPLES

The following examples illustrate the invention and should not be considered in a limitative sense thereof.

In the sense of the present invention, without limitation and in connection with the *in vivo* examples, for "Initial Burst" or initial release it is meant the addition of the plasma levels of paliperidone, from the moment of the injection until the third day after the administration. In a similar way, an "adequate plasma level profile" is considered as not more than the 45% of the AUC of the paliperidone occurring between the moment of the injection until day 21, between 35% and 45% of the AUC of the paliperidone occurring between day 21 and day 49, and not more than 35% of the AUC of the paliperidone occurring after day 49. These percentages represent an adequate balance between the different periods in which paliperidone is being released from the implant in order to have a formulation to be injected each 8W or each 60 days capable to obtain therapeutic plasma levels of paliperidone in a human since the first day of the injection, capable to obtain the desired average paliperidone plasma concentrations during the period between injections and with reduced peak-valley plasma values of paliperidone that could lead to toxicity or lack of efficacy. Also in the sense of this invention, without limitation and in connection with the examples, acceptable plasma levels of paliperidone during the initial burst phase are below 75 ng/ml in Beagle dogs when doses administered are 2.5 mg/kg paliperidone.

Example 1: Depot formulation with Resomer® 503

In the present example, the following formulation was prepared:

Female 2.25 ml syringe	Ingredient	Amount (mg)
	Lactic-co-glycolic acid copolymer (N-capped) with 50% content of each of the two organic acid monomers and a molecular weight of 32.5KDa	50
	Paliperidone	25
Male 2.25 ml syringe	Ingredient	Amount (mg)
	Dimethyl sulfoxide	117

Paliperidone particle size was characterized by light scattering and provided the following distribution of particle size: d(0.1) = 17.41 µm, d(0.5) = 51.61 µm and d(0.9) = 175.32 µm.

Polymer has been characterized for its molecular weight according to the following technique:

Equipment

GPC chromatograph with triple detector (laser diffraction, viscosimetry, refraction index)

- Viscotek® GPCmax VE 2001 GPC SOLVENT/SAMPLE MODULE
- Viscotek® TDA 305 TRIPLE DETECTOR ARRAY

Reagents

- Tetrahydrofurane (THF) grade GPC stabilized with butyl hydroxyl toluene (BHT) 250 ppm
- Polystyrene narrow standard (preferable about a molecular weight of 90 or 99 kDa)

Sample preparation

- 1-2 mg/ml Standard Sample
- 10 mg/ml Test sample: 3 samples for each polymer to be tested

Pre-conditioning

Condition and stabilize column and detectors with mobile phase (THF) until reaching working flow rate of 1 ml/min and purge viscometer and refraction index detectors, checking at the end that all signals are stable and adequate.

Chromatographic conditions:

- Column: 2 serial columns i-MBMMW-3078 (CLM1012, Viscotek)
- Delay column: medium delay (CLM9002, Viscotek)
- Column temperature 30ºC
- Flux rate 1 ml/min
- Injection volume: 100 µl
- Run time: 35 minutes
- Eluent: stabilized THF (pre-heated to 30ºC and under 100 rpm agitation)

System verification

- Inject 100 µl of eluent and check there is no response in signals related with molecular weight determination
- Inject 100 µl of polystyrene narrow standard and check adequacy of the measurement. Repeat at least twice.

  Acceptance Criteria: ±5% of the nominal Molecular Weight and ±3% Intrinsic Viscosity declared by manufacturer standard certificate.

Calibration

Not necessary if system verification complies and no previous chromatographic conditions are changed.

In case it would be required to calibrate:

- Inject 100 µl of polystyrene standard at least twice.

- Use first sample's data for triple calibration by creating a new multidetectors - homopolymer's method.
- Introduce into the method all the data needed for internal calibration such standard values of MW, IV, dn/dc, dA/dc and refractive index of the solvent.
- Calibrate the system as the equipment specify and save the new method.
- Check with the new method the adequacy of the measurement for the second injection of the standard.

Procedure

Inject by triplicate 100 µl of the test sample

Polymer molecular weight measured according to the technique specified resulted in 32.5KDa. According to a similar technique, inherent viscosity of the polymer resulted in a value of 0.27dl/g. It is important to mention that inherent viscosity values correspond to those obtained with the technique described, specially related to temperature conditions and eluent used. Any change in measurement conditions mean the obtention of different values as directly depend on them.

The paliperidone implantable formulation was prepared by connecting male and female syringes and moving the plungers forwards and backwards upon complete dissolution of the polymer and the formation of a homogeneous suspension of the paliperidone in the polymer dissolution.

In vivo plasma levels after intramuscular administration to Beagle dog:

The paliperidone composition of this example was intramuscularly injected to Beagle dogs weighing an average of 10 kg. The amount injected corresponded to a dose of 25 mg paliperidone and the composition was intramuscularly placed in the left hind leg using a syringe with a 20G needle. Total number of dogs was 3. After injection, plasma levels were

obtained at 0, 4h, 1d, 2d, 3d, 5d, 7d, 10d, 14d, 17d, 21d, 24d, 28d, 31d, 36d, 38d, 42d, 45d, 49d, 52d, 55d, 59d, 63d, 73d, 80d, 87d, 94d, 108d and 118d.

The kinetics of the plasma levels corresponding to the paliperidone was evaluated by tandem mass HPLC. The profile of the plasma levels of the paliperidone is shown in Figure 1. The results are expressed as paliperidone concentrations (ng/ml) as the function of time. As it can be observed in this Figure, the injection of an amount of composition equivalent to 25 mg paliperidone to Beagle dogs resulted in very high control of the initial burst release followed by a slow, sustained decrease, with continuous plasma levels from day 1 onwards. The plasma levels profile for the paliperidone, as previously described, can be considered adequate as provide very low risk of having toxic plasma levels just after the injection. This property is crucial for a formulation intended to be administered at least each 8 weeks, as the dose needed to be injected is high compared to existing monthly regimens and, therefore, the risk of reaching toxic plasma levels with small variations of the drug fraction released at this stage is potentially very high. In this formulation, drug release during polymer precipitation process is controlled by the drug solubility in the solvent, the amount of solvent (ratio drug to solvent) and the polymer concentration and molecular weight.

The results also indicate that the formulation can release paliperidone over a period of more than two months in a prolonged manner, with reduced peak to valley plasma concentration fluctuations of the drug. An adequate control of the drug to polymer ratio and the polymer molecular weight are crucial to achieve this target.

Once the formulation is injected in the intramuscular tissue, the DMSO is rapidly dissolved in the surrounding aqueous environment. The relative increase of the polymer concentration in DMSO over the polymer solubility in the solvent leads to the formation of a polymer precipitate that entraps the paliperidone that was not solubilized in the solvent. Molecular weight of the polymer has a great impact in this critical step, as too low weighed chains have delayed precipitation time compared to the chains having the weight in the adequate range. This delayed precipitation allows the drug to increase contact with the surrounding fluids towards the drug is being released. Therefore, low molecular weighed chains lead to an excessive release of paliperidone after the injection and potentially to

obtain toxic plasma levels on the first days after the injection. Molecular weight of the polymer also can affect the release of the drug from the intramuscularly injected implant after solvent diffusion and polymer precipitation. Molecular weights over the specified range are not capable to maintain adequate release rates of paliperidone by diffusion. This phase is particularly prolonged in a bi-monthly formulation compared to a formulation intended to be administered each 4 weeks, and the control of the polymer molecular weight becomes particularly crucial. Additionally, higher molecular weight chains can lead to formulations that are too viscous to be injected at the required concentration (more than 3.0 Pa.s) and once injected in the intramuscular tissue require longer hydrolysis times in order to provide soluble fractions that could release the drug entrapped in the polymer matrix. A higher remaining drug content to be released could lead to the obtention of undesirably low paliperidone plasma values, between days 24 and 49 that could lead to obtain under therapeutic plasma concentrations of the drug.

	AUC all	AUC_{0-21} days	AUC_{21-49} days	$AUC_{42-last}$
	(h*ng/ml)	(h*ng/ml)	(h*ng/ml)	(h*ng/ml)
Dose 2.5 mg/kg	5985.5	2615.9	2666.28	703.32

Example 2: Depot formulation with Resomer® 504 radiated to 16KGy. 2 doses.

Preparation of sterile formulations to be used in vivo can require the use of procedures, such as irradiation, that have the potential to affect the polymer molecular structure. The example shows that the polymer molecular weight loss that occur upon polymer irradiation can be measured and controlled in order to achieve a sterile polymer with the desired characteristics in order to obtain adequate plasma levels profile of paliperidone.

In this example, a lactic-co-glycolic acid copolymer with 50% content of each of the two organic acid monomers and a molecular weight of 50 kDa was sterilized by beta irradiation at 16 kGy under controlled temperature and moisture conditions. The resultant polymer was characterized for its molecular weight according to the method described in example 1. Molecular weight after irradiation process was 40KDa.

Female 2.25 ml syringe	Ingredient	Amount (mg)
	Lactic-co-glycolic acid copolymer (N-capped) with 50% content of each of the two organic acid monomers and a molecular weight of 50 kDa, beta-irradiated as a bulk with a 16 kGy dose achieving a final molecular weight of 40KDa.	100
	Paliperidone	50
Male 2.25 ml syringe	Ingredient	Amount (mg)
	Dimethyl sulfoxide	234

Paliperidone particle size was characterized by light scattering and provided the following distribution of particle size: d(0.1) = 17.41 μm, d(0.5) = 51.61 μm and d(0.9) = 175.32 μm.

Inherent viscosity of the irradiated polymer, as calculated by the technique described in example 1 was 0.31dl/g.

The paliperidone implantable formulation was prepared by connecting male and female syringes and moving the plungers forwards and backwards upon complete dissolution of the polymer and the formation of a homogeneous suspension of the paliperidone in the polymer dissolution.

In vivo plasma levels after intramuscular administration to Beagle dog:

The paliperidone composition of this example was intramuscularly injected to two cohorts of Beagle dogs weighing an average of 10 kg. The amount injected corresponded to a dose of 25 mg paliperidone in one cohort and to a dose of 50 mg paliperidone in a second cohort. The compositions were intramuscularly placed in the left hind leg using a syringe with a 20G needle. Total number of dogs was 3 for each cohort. After injection, plasma levels were obtained at 0, 4h, 1d, 2d, 3d, 5d, 7d, 10d, 14d, 17d, 21d, 24d, 28d, 31d, 36d, 38d, 42d, 45d, 49d, 52d, 55d, 59d, 63d, 73d, 80d, 87d, 94d, 108d and 118d.

The kinetics of the plasma levels corresponding to the paliperidone was evaluated by tandem mass HPLC. The profile of the plasma levels of the paliperidone is shown in Figure 2. The results are expressed as paliperidone concentrations (ng/ml) as the function of time. As it can be observed in this Figure, the injection of an amount of composition equivalent to 25 mg paliperidone to Beagle dogs resulted in a paliperidone plasma levels profile that was similar to that observed in Example 1, representing a polymer that was not irradiated.

The example shows how can be adjusted by the sterilization process the polymer molecular weight in order to obtain a polymer that is sterile, and that confers the formulation the desired release properties. Possible changes in terminal end groups of the polymer after irradiation process do not significantly change in vivo release properties in the specified range, meaning that molecular weight is the major factor that controls degradation process in this composition.

	AUC all	AUC $_{0\text{-}21}$ days	AUC $_{21\text{-}49}$ days	AUC $_{42\text{-last}}$
	(h*ng/ml)	(h*ng/ml)	(h*ng/ml)	(h*ng/ml)
Dose 5 mg/kg	14991.22	4842.82	5521.8	4626.6
Dose 2.5 mg/kg	7077.38	2503.94	2708.16	1865.28

Example 3: Depot formulation with Lakeshore Biomaterials® 5050DLG 5E radiated to 25KGy.

Preparation of sterile formulations to be used in vivo can require the use of procedures, such as irradiation, that have the potential to affect the polymer molecular structure. The example shows that the polymer molecular weight loss that occur upon polymer irradiation can be measured and controlled in order to achieve a sterile polymer with the desired characteristics in order to obtain adequate plasma levels profile of paliperidone.

In this example, a lactic-co-glycolic acid copolymer with 50% content of each of the two organic acid monomers and a molecular weight of 54 kDa was sterilized by beta irradiation at 25 kGy under controlled temperature and moisture conditions. The resultant polymer

was characterized for its molecular weight according to the method described in example 1. Molecular weight after irradiation process was 42KDa.

Female 2.25 ml syringe	Ingredient	Amount (mg)
	Lactic-co-glycolic acid copolymer (N-capped) with 50% content of each of the two organic acid monomers and a molecular weight of 54 kDa, beta-irradiated as a bulk with a 25 kGy dose achieving a final molecular weight of 42KDa.	100
	Paliperidone	50
Male 2.25 ml syringe	Ingredient	Amount (mg)
	Dimethyl sulfoxide	234

Paliperidone particle size was characterized by light scattering and provided the following distribution of particle size: d(0.1) = 17.41 µm, d(0.5) = 51.61 µm and d(0.9) = 175.32 µm.

Inherent viscosity of the irradiated polymer, as calculated by the technique described in example 1 was 0.31dl/g.

The paliperidone implantable formulation was prepared by connecting male and female syringes and moving the plungers forwards and backwards upon complete dissolution of the polymer and the formation of a homogeneous suspension of the paliperidone in the polymer dissolution.

In vivo plasma levels after intramuscular administration to Beagle dog:

The paliperidone composition of this example was intramuscularly injected to Beagle dogs weighing an average of 10 kg. The amount injected corresponded to a dose of 75 mg paliperidone. The composition was intramuscularly placed in the left hind leg using a syringe with a 20G needle. Total number of dogs was 3. After injection, plasma levels were obtained at 0, 4h, 1d, 3d, 5d, 7d, 10d, 14d, 17d, 21d, 24d, 28d, 31d, 34d, 41d, 49d and 56d.

The kinetics of the plasma levels corresponding to the paliperidone was evaluated by tandem mass HPLC. The profile of the plasma levels of the paliperidone is shown in Figure 3. The results are expressed as paliperidone concentrations (ng/ml) as the function of time. As it can be observed in this Figure, the injection of an amount of composition equivalent to 75 mg paliperidone to Beagle dogs resulted in a paliperidone plasma levels profile that was similar to that observed in Example 1, representing a polymer that was not irradiated and Example 2 representing a polymer radiated to 16KGy.

The example shows how can be adjusted by the sterilization process the polymer molecular weight in order to obtain a polymer that is sterile, and that confers the formulation the desired release properties. Possible changes in terminal end groups of the polymer after irradiation process do not significantly change in vivo release properties in the specified range, meaning that molecular weight is the major factor that controls degradation process in this composition.

	AUC all	AUC_{0-21} days	AUC_{21-49} days	$AUC_{42-last}$
	(h*ng/ml)	(h*ng/ml)	(h*ng/ml)	(h*ng/ml)
Dose 7.5 mg/kg	19537.55	8049.47	8750.54	2737.54

Example 4: Depot formulation with Resomer® 504 radiated to 25KGy

The current example demonstrates that an excessive reduction in the polymer molecular weight can lead to a shortening of the duration of paliperidone plasma levels profile that makes the formulation not suitable to be administered each 8 weeks or more.

A lactic-co-glycolic acid copolymer with 50% content of each of the two organic acid monomers and a molecular weight of 38KDa was sterilized by beta irradiation at 25KGy under controlled temperature and moisture conditions. The resultant polymer was characterized for its molecular weight according to the method described in example 1. Molecular weight after irradiation process was 29KDa.

Female 2.25 ml syringe	Ingredient	Amount (mg)
	Lactic-co-glycolic acid copolymer (N-capped) with 50% content of each of the two organic acid monomers and a molecular weight of 38KDa, beta-irradiated as a bulk with a 25 kGy dose achieving a final molecular weight of 29KDa.	50
	Paliperidone	25
Male 2.25 ml syringe	Ingredient	Amount (mg)
	Dimethyl sulfoxide	117

Paliperidone particle size was characterized by light scattering and provided the following distribution of particle size: d(0.1) = 17.41 µm, d(0.5) = 51.61 µm and d(0.9) = 175.32 µm.

Inherent viscosity of the irradiated polymer, as calculated by the technique described in example 1 was 0.31 dl/g.

The paliperidone implantable formulation was prepared by connecting male and female syringes and moving the plungers forwards and backwards upon complete dissolution of the polymer and the formation of a homogeneous suspension of the paliperidone in the polymer dissolution.

In vivo plasma levels after intramuscular administration to Beagle dog:

The paliperidone composition of this example was intramuscularly injected to Beagle dogs weighing an average of 10 kg. An amount of formulation equivalent to a dose of 2.5 mg/kg of paliperidone was intramuscularly placed in the left hind leg using a syringe with a 20G needle. Total number of dogs per cohort was 3. After injection, plasma levels were obtained at 0, 4h, 1d, 2d, 3d, 5d, 7d, 10d, 14d, 17d, 21d, 24d, 28d, 31d, 35d, 38d, 42d, 45d, 49d, 52d, 56d, 59d, 63d, 70d, 77d.

The kinetic of the plasma levels corresponding to paliperidone was evaluated and is shown in Figure 4. The results are expressed as paliperidone concentrations (ng/ml) as the function of time. As it can be observed in this Figure, the injection of an amount of

composition equivalent to 2.5 mg/kg to Beagle dogs resulted in a shortened plasma levels profile. A reduction of 4 kDa from 33to 29increases significantly drug diffusion throughout the polymer matrix, leading to a reduced availability of the drug to be released after 30 days post injection.

5

	AUC all	AUC $_{0-21}$ days	AUC $_{21-49}$ days	AUC $_{42\text{-last}}$
	(h*ng/ml)	(h*ng/ml)	(h*ng/ml)	(h*ng/ml)
Dose 2.5 mg/kg	10542.26	7142.06	3128.04	272.16

CLAIMS

1.- An injectable intramuscular depot composition suitable for forming an in situ solid implant in a body, comprising a drug which is paliperidone and/or its pharmaceutical acceptable salts in any combination thereof, a biocompatible copolymer based on lactic and glycolic acid having a monomer ratio of lactic to glycolic acid in the range of 50:50 and DMSO as solvent, wherein the composition releases the drug with an immediate onset of action and continuously for at least 8 weeks and wherein the composition has a pharmacokinetic profile *in vivo* suitable for the formulation to be administered each 8 weeks or longer periods, characterised in that the biocompatible copolymer has a molecular weight in the range of between 31 and 40 kDa and an inherent viscosity in the range of between 0.27-0.31 dl/g.

2.- The composition of claim 1, wherein the biocompatible copolymer is gamma or beta irradiated in the dose range of 10-30 KGy measured at a temperature between –40ºC and +35ºC to adjust its molecular weight to a range between 31 and 40 kDa and its inherent viscosity to a range of between 0.27-0.31 dl/g.

3.- The composition claims 1 or 2, wherein the particle size distribution of the drug is:

- less than 10% particles smaller than 10 microns;
- less than 10% particles larger than 225 microns, and
- a d0.5 value in the range of 40-130 microns.

4.- The composition according to any one of claims 1 to 3, wherein the drug/(polymer+drug) mass ratio is about 33%.

5.- The composition according to any one of claims 1 to 4, wherein the content of drug is about 13% w/w of total formulation and the viscosity of the solution comprising the polymer and the DMSO is in the range of 1.7 – 1.8 P.a.s.

6.- The composition of any one of previous claims for the treatment of schizophrenia or bipolar disorders in the human body.

7.- A pharmaceutical kit suitable for the in situ formation of a biodegradable implant in a body comprising the composition of any one of claims 1-6, wherein the drug and the biocompatible polymer are contained in a first container, and the solvent is contained in a second, separate container.

8.- The pharmaceutical kit according to claim 7, wherein at least one of the first and second containers is a syringe, a vial, a device or a cartridge, either disposable or not.

9.- A method for the manufacturing of a composition according to any one of previous claims 1-6, comprising the step of providing a biocompatible copolymer having an initial polymer weight higher than required for the intramuscular depot composition and then adjusting its molecular weight to between 31 and 40kDa and its inherent viscosity to a range of 0.27-0.31 dl/g by irradiating it with gamma or beta radiation in the dose range of 10-30 KGy measured at a temperature between –40ºC and +35ºC.

10. Method according to claim 9 wherein the dose range irradiated to the polymer is in the range of 16-25 KGy measured at the temperature of 8ºC.

11.- Method according to claims 9 or 10 wherein, when the biocompatible polymer has an initial molecular weight of about 50 kDa, it is irradiated with a radiation dose of about 16 KGy to reduce its molecular weight to between 35 and 38 kDa.

12.- Method according to claims 9 or 10 wherein, when the biocompatible polymer has an initial molecular weight of about 63 kDa, it is irradiated with a radiation dose of about 30 KGy to reduce its molecular weight to between 30 and 36 kDa.