

ACTIVE MINIATURIZED SENSING SYSTEM AND METHOD

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Description

The present invention relates to a non-invasive active sensing system for determining a physiological parameter in a bodily fluid of subject. Further, the present invention relates to a non-invasive method for determining a physiological parameter in a bodily fluid of a subject.

Background

In the year 2016, about 415 million people suffered from diabetes. For 2040, an increase to more than 640 million people can be expected. Since people with diabetes are at risk for complications such as blindness, kidney diseases, heart diseases and stroke, there is a need to control the disease by closely monitoring blood glucose level.

Presently, determination of blood glucose is mainly based on invasive system and methods, wherein either a blood sample is taken and subsequently subjected to an *in vitro* test or a sensor is implanted for determining the glucose level *in vivo*. These invasive systems and methods are disadvantageous in that they are painful or inconvenient.

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Thus, there is a need for developing a system and methods which allow a reliable non-invasive determination of glucose and or physiological parameters.

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Summary of the invention

According to the present invention, a simple, rapid and reliable determination of a physiological parameter is feasible using non-invasive systems and methods. These systems and methods involve irradiation of a body part of a subject, particular a human subject, with visual (VIS)/near-infrared (NIR) radiation in the range of about 400 nm to about 1500 nm or about 500 nm to about 1500 nm and detecting emitted IR radiation from the irradiated body part of said subject in the range of about 5 μ m to about 12 μ m. Surprisingly, the present inventor has found that irradiating a body part, e.g. a fingertip, an earlobe, a wrist or a forearm with short-wavelength radiation and detecting emitted long-wavelength radiation from the irradiated body part allows determination for physiological parameters such as glucose in a bodily fluid such as blood.

Irradiation of a body part with VIS/NIR radiation according to the present invention causes energy absorption within an area of the irradiated body part. Energy absorption in this irradiated area, i.e. the absorption area, results in a local increase of tissue temperature within the irradiated body part, particularly within the absorption area, which again causes an increased emission of IR radiation from the irradiated body part, particularly from the absorption area, including an increased emission of IR radiation in the range of about 5 μ m to about 12 μ m. Thus, detection of emitted IR radiation from the irradiated body part is facilitated and substantially improved.

A first aspect of the invention relates to a non-invasive system for determining a physiological parameter, particularly glucose, in a bodily fluid of a subject comprising:

- (a) a radiation source adapted for emitting visual (VIS)/near-infrared (NIR) radiation in the range of about 400 nm to about 1500 nm, or about 500 nm to about 1500 nm into a body part of said subject, wherein the

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body part is particularly selected from a fingertip, an earlobe, a wrist, and a forearm, and upper arm,

- 5 (b) a sensing unit for detecting emitted IR radiation from the irradiated body part of said subject in the range of about 5 μm to about 12 μm , wherein said sensing unit is adapted for (i) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said
- 10 subject, and for (ii) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of the physiological parameter in the bodily fluid of said subject, and
- 15 (c) an analyzing unit for the qualitative and/or quantitative determination of the physiological parameter based on the IR radiation detected in the sensing unit (b).

A further aspect of the invention relates to the use of the above system for

20 non-invasively determining a physiological parameter in a bodily fluid of a subject, particularly wherein the physiological parameter is glucose, and the bodily fluid is blood.

A still further aspect of the invention relates to a method for non-invasively

25 determining a physiological parameter, particularly glucose in a bodily fluid of a subject comprising the steps:

- (a) irradiating a body part of said subject with visual (VIS)/near-infrared (NIR) radiation in the wavelength range of about 400 nm to about
- 30 1500 nm, or about 500 nm to about 1500 nm,
- (b) detecting emitted IR radiation from the irradiated body part of said subject in the wavelength range of about 5 μm to about 12 μm ,

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- comprising separately (i) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject, and (ii) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of the physiological parameter in the bodily fluid of said subject, and
- (c) analyzing the detected IR radiation for the qualitative and/or quantitative determination of the physiological parameter.

Detailed description

- The present invention involves determination of a physiological parameter by detecting IR radiation from previously irradiated body parts of a subject, particularly a human subject in the wavelength range of about 5 μm to about 12 μm , particularly in the range of about 8 μm to about 10 μm . The physiological parameter may be any compound having characteristic absorption bands in this wavelength range. For example, the physiological parameter is glucose or another clinically relevant analyte such as lactate or troponin.

- In a certain embodiment of the invention, the system is adapted for the non-invasive determination of glucose in blood. In this embodiment, IR radiation is detected at a glucose-specific wavelength or wavelength range where glucose has a characteristic absorption band and where the intensity of the detected IR radiation is dependent from the concentration of glucose in the blood. More particularly, the glucose-specific wavelength or wavelength range is selected from a wavelength of about 9.2 μm , a wavelength of about 9.4 μm , a wavelength of about 9.6 μm , a wavelength range comprising at least two of the wavelengths of about 9.2 μm , about 9.4 μm and about 9.6 μm , a wavelength range comprising all three of the wavelengths of about 9.2

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μm, about 9.4 μm and about 9.6 μm or any combination thereof. Additionally, IR radiation is detected at a reference wavelength or wavelength range where glucose has no characteristic absorption band and particularly an absorption minimum and where the intensity of the detected IR radiation is substantially independent from the concentration of glucose in blood. More particularly, the reference wavelength or wavelength range is selected from a wavelength or wavelength range between about 8.7 μm to about 9.0 μm, a wavelength or a wavelength range between about 9.7 μm to about 10.2 μm or any combination thereof.

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As outlined above, the invention is based on the irradiation of body tissue with electromagnetic radiation in the wavelength range between about 500 nm to about 1500 nm (VIS/NIR radiation) and detection of electromagnetic radiation emitted from the irradiated body part in the wavelength range between about 5 μm to about 15 μm (IR radiation). Irradiation of the body part with VIS/NIR radiation results in an enhanced self-emission of IR radiation from said body part due to local energy absorption, which causes a local increase in temperature. Thus, self-emission of IR radiation from the irradiated body part is increased by previous irradiation of said body part with VIS/NIR radiation. Consequently, irradiation of the body part with an external source of IR radiation in the wavelength range between about 5 μm to about 15 μm is not required. Thus, in certain embodiments, the system of the invention does not include an external IR radiation source, particularly in certain embodiments the system of the invention does not include an external IR radiation source adapted to irradiate the body part from which the detected IR radiation is emitted.

Figure 1 shows the penetration depth of electromagnetic radiation into body tissue [mm] depending from the wavelength [nm]. It can be seen that the penetration depth is dependent from the wavelength. In the visual (VIS)/near-infrared (NIR) wavelength range between about 400 nm to about 1500 nm, particularly in the range of about 500 nm to about 1500 nm or in the range of

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about 400 nm to about 1200 nm, more particularly in the range of about 550 nm to about 1200 nm, there is a penetration depth of about 1 mm or more, particularly about 3 mm or more. Thus, a body part irradiated with radiation will absorb electromagnetic energy resulting in a local increase of tissue temperature. This again results in an increased emission of longer-wavelength IR radiation, e.g. IR radiation in the wavelength range of about 5 μm to about 12 μm , where certain organic compounds present in bodily fluids, i.e. physiological parameters, show absorption bands. This allows a quantitative or qualitative determination of such parameters according to the above aspects of the present invention.

In certain embodiments, the VIS/NIR radiation emitted into the body part is in the range of about 550 nm to about 1000 nm, particularly in the range of about 800 nm to about 820 nm, e.g. about 810 nm, and/or in the range of about 590 nm to about 660 nm, e.g. at about 600 nm, and/or in the range of about 920 nm to about 980 nm, e.g. at about 940 nm. In certain embodiments, the VIS/NIR radiation emitted into the body is in the range of about 450 nm to about 800 nm.

Figure 2 shows relative absorption coefficients of certain compounds present in the human body depending from the wavelength in the range between 400 nm and 1100 nm. The wavelengths of about 600 nm and about 810 nm, at which radiation may be emitted into the body part, are specifically indicated. In the wavelength range of about 500 nm to about 1050 nm, there is a relatively low absorption of water (H_2O). Further, the major blood constituents hemoglobin (Hb) and oxyhemoglobin (Hboxy) show similar absorption coefficients. The skin pigment melamine shows an absorption coefficient which decreases with increasing wavelength.

In an embodiment of the invention, the radiation source (a) is adapted for emitting VIS/NIR radiation in the range of about 920 nm to about 960 nm, e.g. about 940 nm into a body part. This irradiation wavelength may be used

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alone or in combination with at least one further irradiation wavelength. As shown in **Figure 3**, glucose has an absorption band at a wavelength of 940 nm. Thus, irradiation at a wavelength of about 940 nm leads to a selective excitation of glucose molecules and may result in a stronger absorption of glucose molecules in the IR wavelength range, particularly in the wavelength range of about 5 μm to about 12 μm .

According to an embodiment of the invention, the radiation source (a) is adapted for emitting VIS/NIR radiation in the range of about 920 nm to about 980 nm, e.g. about 940 nm into a body part of said subject, and the sensing unit (b) is further adapted for detecting VIS/NIR radiation having a wavelength of about 940 nm, where the intensity of the detected VIS/NIR radiation is dependent from the concentration of glucose. The measurement signal in the VIS/NIR wavelength range may be combined with the measurement signals in the IR range as described above, e.g. by means of a comparator.

In a still further embodiment, VIS/NIR irradiation occurs at a combination of at least 2 different wavelengths, particularly at a combination of a first wavelength of about 800 nm to about 820 nm, e.g. about 810 nm, and a second wavelength of about 920 nm to about 980 nm, e.g. about 940 nm.

Figure 4 shows an embodiment of a system of the present invention. A body part (1), e.g. a fingertip, is placed into contact with the system, which is adapted to irradiate an absorption area (2) within the body part (1).

The system comprises a cover (3) which is at least partially made of a material, which is optically transparent. For example, the cover is at least partially made of CaF_2 and/or BaF_2 or of a plastic material which is transparent in the IR wavelength range of about 5 μm to about 12 μm or a sub-range thereof, e.g. of about 8 μm to about 12 μm , and which is optionally transparent in the VIS/NIR wavelength range of about 400 nm to about 1500

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nm or a sub-range thereof. Suitable IR-transparent plastic materials are e.g. the PolyIR plastic materials commercially available from Fresnel Technologies, Fort Worth, Texas, USA. In certain embodiments, the cover may have a thickness of about 0.2 mm to about 2 mm, particularly of about
5 0.5 mm to about 1.5 mm, more particularly about 1 mm.

The system further comprises at least one sensor (4) which may be provided with a filter element (5) and optionally a lens element (not shown), which e.g. may be arranged between a sensor (4) and a filter element (5). The sensor
10 (4) may be mounted on a circuit board (6). Further, the system comprises at least one radiation source (9, 9a). For example, the system may comprise a radiation source (9) located on the same side as the sensor (4) and/or a radiation source (9a) located on an opposite side of the body part (1) with regard to the sensor (4). If desired, a further sensor (4) may be provided
15 without filter element (5) for monitoring the exact skin temperature of the subject.

The system contains one or more sensors (4). In the embodiment of Figure 4, the system comprises four different sensors (4). The sensor may be an
20 optical detector, particularly an optical photovoltaic detector, e.g. an InAsSb-based detector, which may be used in combination with a lock-in amplifier, if desired. A photovoltaic detector, e.g. an InAsSb-based detector has a rise time of only few nanoseconds and is particularly useful in a set-up wherein the body part is irradiated intermittently. In other embodiments, the sensor
25 may be heat detector, e.g. a thermopile or a bolometer. Suitable sensors include a photovoltaic detector (e.g. Hamamatsu P13894), a thermopile (e.g. Heimann HCS C21 F8-14) or other types of IR sensors (e.g. Sensirion STS21 or Melexis MLX90632). If desired, a sensor (4) may be provided with a filter element (5) capable of selectively transmitting radiation of a desired
30 wavelength or wavelength range. The filter element may have narrow bandwidth, e.g. of about 50 to 100 nm, or a broader bandwidth, e.g. of about 400 nm or more. A filter may be made from germanium or other filter

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materials, which are optically transmissive for the respective wavelengths. Further, a sensor may be provided with a lens element, e.g. a micro-lens capable of focusing the light falling onto the sensor.

- 5 In certain embodiments, the sensor surface may be coated with a noble metal such as Au or Ag, particularly Au, in order to increase its sensitivity. Such a coating which may be shaped as a Bundt baking-pan is described by Awad (Nature Scientific Reports 9:12197 (2019)), the content of which is herein incorporated by reference.

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In certain embodiments, the sensor is a miniaturized sensor having an area of about 1 mm² to about 10,000 mm², e.g. of about 10 mm² to about 1,000 mm². In certain embodiments, the sensor may be even more miniaturized, e.g. an ASIC (application-specific integrated circuit).

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- In the sensing unit of the invention, at least one sensor may be an analyte-specific sensor, i.e. a sensor which is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject, and at least on
20 sensor may be a reference sensor, i.e. a sensor which is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of the physiological parameter in the bodily fluid of
25 said subject.

- In certain embodiments, the sensing unit (b) is adapted for detecting self-emitted IR radiation from the previously irradiated body part, i.e. IR radiation generated by the body heat of the subject without irradiation by an external
30 IR source. Further, the sensing unit (b) may be adapted for detecting emitted IR radiation from an absorption area within the previously irradiated body part wherein the absorption area has a locally increased temperature and exhibits

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an increased emission of IR radiation in the wavelength range of about 5 μm to about 12 μm .

In certain embodiments, at least one further sensor may be present, e.g. a
5 sensor which (i) is adapted for detecting unspecific IR radiation, (ii) is adapted for detecting unspecific VIS/NIR radiation, (iii) is adapted for detecting VIS/NIR radiation having a wavelength, where the intensity of the detected VIS/NIR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject, and/or (iv) a
10 temperature sensor for measuring the temperature of the body part.

In certain embodiments, at least one further analyte-specific sensor may be present, i.e. a sensor which is adapted for detecting VIS/NIR radiation having at least one wavelength or wavelength range where the intensity of the
15 detected VIS/NIR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject. For example, at least one further sensor adapted for detecting VIR/NIR radiation having a wavelength of about 940 nm may be present.

20 Further, the device may comprise a circuit board (7) on which the light source (9) is mounted and an active and/or passive heat sink (8).

The VIS/NIR radiation source (9, 9a, 9b) may be adapted for emitting collimated radiation, e.g. a laser-based light source, and/or adapted for
25 emitting non-collimated radiation, e.g. an LED-based light source. For example, the light source may be selected from an LED, a laser diode, a VCSEL (vertical-cavity surface-emitting laser) or a laser. In certain embodiments, a broadband VIS/NIR radiation emitter is used which may be adapted for emitting VIS/NIR radiation in the range of about 650 nm to about
30 950 nm, particularly in the range of about 750 nm to about 850 nm and more particularly in the range of about 780 nm to about 820 nm. Suitable VIS/NIR

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emitters are e.g. the OSOLON products from Osram such as OSOLON SFH 4763.

5 The radiation source is adapted for emitting VIS/NIR radiation in the range of about 400 nm to about 1500 nm, particularly in the range of about 500 nm to about 1500 nm. The VIS/NIR radiation may be emitted continuously or intermittently throughout a predetermined time interval.

10 In a certain embodiment, the radiation source is adapted to cause a local increase in the temperature of the irradiated body part, e.g. a fingertip, and particularly a local increase in the temperature of the absorption area within the irradiated body part. The local increase in temperature may be in the range of between about 1°C to about 15°C, particularly about 2°C to about 10°C, and more particularly in the range of about 3°C to about 5°C. The
15 locally increased temperature of the irradiated body part, e.g. a fingertip, may be in temperature range up to about 45°C, up to about 40°C or up to about 37°C, for example in the temperature range between about 30°C to about 35°C or about 30°C to about 32°C. This local temperature increase results in an enhanced self-emission of IR radiation from the irradiated body part and
20 particularly from the absorption area within the irradiated body part.

In a certain embodiment, the radiation source may be adapted for emitting radiation continuously at a power of about 10 mW to about 1 W, particularly for about 20 mW to about 500 mW, more particularly of about 50 mW to
25 about 250 mW, and even more particularly of about 100 mW to about 200 mW, e.g. about 150 mW, for a time interval of about 0.1 to about 20 s, particularly of about 0.2 s to about 5 s, and more particularly of about 0.5 s to about 2 s, e.g. about 1 s.

30 In a further embodiment, the radiation source may be adapted for emitting radiation intermittently at a power of about 10 mW to about 5 W, particularly of about 20 mW to about 1 W, and more particularly of about 50 mW to about

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500 mW for a time interval of about 0.1 s to about 20 s, particularly of about 0.2 s to about 5 s, and more particularly of about 0.5 s to about 2 s. The radiation may be emitted intermittently with a pulse frequency of about 1 Hz to about 1 MHz.

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In a further embodiment, the radiation source may be adapted to emit VIS/NIR radiation at a plurality of different wavelengths, e.g. at 2, 3, 4, 5, 6, 7, 8 or even more different wavelengths. For example, the radiation source may be multi LED chip. The use of a multi-wavelength radiation source
10 allows adjusting a predetermined penetration depth of electromagnetic radiation into the tissue of the irradiated body part depending on specific characteristics of the body part, e.g. pigmentation, skin thickness, presence or absence of horny skin. As shown in Figure 1, supra, the penetration depth into body tissue varies with the wavelength and the use of VIS/NIR radiation
15 with different wavelengths or with combinations of different wavelengths can be adapted for each subject and/or each body part individually, if desired.

In certain embodiments, the radiation source (a) is a multi-wavelength radiation source is adapted to emit VIS/NIR radiation at several different
20 wavelengths or wavelength ranges, for example, between about 400 nm to about 1200 nm, more particularly between about 450 nm and about 900 nm, e.g. at least 2, 3 4, 6 or 8 wavelengths which may be selected from wavelengths at about 470 nm, about 520 nm, about 590 nm, about 650 nm, about 750 nm and about 810 nm.

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A further embodiment of the system of the invention is shown in **Figure 5**. Here, a single radiation source (9a) is provided on a side of the body part (1) which is opposite to a sensing unit comprising at least one sensor (4) provided with a filter (5) and a further sensor (4a) provided with a filter (5a).
30 In certain embodiments, sensor (4a) is an optical sensor, e.g. a photodiode. It is adapted for a reference measurement of transmission radiation from radiation source (9a), e.g. for measuring radiation at a wavelength of about

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600 nm and/or about 810 nm and/or about 940 nm. For this purpose, filter element (5a) may be a bandpass filter at about 600 nm and/or 810 nm and/or 940 nm.

5 Still a further embodiment of the invention is shown in **Figure 6**. Here, a radiation source (9b) is provided on a side of the body part (1), e.g. a fingertip, wherein direct access to an absorption area (2) within the body part (1) is provided through the skin of the body part without the radiation passing through a cover structure of the device and/or without passing through a
10 horny structure on the body surface, e.g. a finger nail and/or horny skin. Thereby, interference, e.g. interference from the cover structure or from keratinic horny skin or nail material and optionally nail varnish can be reduced or eliminated. According to this embodiment, a single radiation source (9b) or a plurality of radiation sources (9b), e.g. 2, 3, 4, 6 or 8
15 radiation sources may be provided at a position around the circumference of the body part (1), e.g. a fingertip. If a plurality of radiation sources is present, they are preferably adapted to emit radiation into a single absorption area (2) within the body part, which may be about 3 mm to about 5 mm below the body surface.

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Still a further embodiment of the invention is shown in **Figure 7**. In this embodiment, a cover (3) is provided which is adapted for focusing IR radiation emitted from the body part to the at least one sensor (4) of the sensing unit. Thereby, the radiation intensity on the sensor and thus the
25 sensitivity and/or accuracy of the measurement may be increased. The cover (3) is made of a material, e.g. plastic, metal, metal oxide or composite material, which is substantially transparent for IR radiation in the wavelength range to be detected on the sensor, particularly for IR radiation in the wavelength range of about 5 μm to about 12 μm or a sub-range thereof, e.g.
30 of about 8 μm to about 12 μm . Suitable materials are e.g. the PolyIR plastic materials, c.f. supra. In this embodiment, the cover (3) may comprise an IR Fresnel lens, i.e. a lens of large aperture and short focal length capable of

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efficiently focusing IR radiation passing therethrough, or an array comprising a plurality e.g. up to 10 or more IR Fresnel lenses. In certain embodiments, the array may comprise IR Fresnel micro-lenses, e.g. up to 100 or 1000 micro-lenses, which may have diameters in the range of about 50 nm to about 500 μm . In certain embodiments, the IR Fresnel lens may have a back focal length of about 3 mm to about 10 mm, e.g. about 5 mm and may be manufactured from an IR-transparent plastic. For example, a suitable IR Fresnel lens, which is optically transparent in the wavelength range of 8-14 μm is commercially available from Edmund Optics (product family no. 2042).

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Further, Figure 7 shows a radiation source (9a) provided on the opposite side of the body part with regard to the position of the sensing unit, which comprises a sensor (4). It should be noted, however, that one or more radiation sources may also be arranged in a circumferential arrangement around the body part (1), e.g. as shown in Figure 6. It should further be noted, that in this embodiment a plurality of different sensors may be present, e.g. as shown in Figures 4 and 5.

As shown in Figures 4 and 5, the system of the invention may comprise a plurality of different sensors (4). In certain embodiments, the system may comprise a plurality of analyte-specific, e.g. glucose-specific sensors wherein a first sensor is adapted for detecting radiation at a first wavelength or wavelength range, e.g. at a wavelength of about 9.2 μm and at least another first sensor is adapted for detecting IR radiation at a second wavelength range which encompasses the first wavelength or wavelength range and further comprises another wavelength or wavelength range. For example, the other first sensor may be adapted for detecting IR radiation at a wavelength of about 9.2 μm and additionally at a wavelength of about 9.4 μm and/or about 9.6 μm , particularly at a wavelength of about 9.4 μm and a wavelength of about 9.6 μm .

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Further, the sensing unit may comprise a plurality of reference sensors adapted for detecting reference radiation at different wavelengths or wavelength ranges. For example, when determining glucose, a reference sensor may be adapted for detecting radiation having a wavelength range
5 between about 8.6 μm and about 9.0 μm . Another reference sensor is adapted for detecting radiation at a wavelength or wavelength range between about 9.8 μm and about 10.2 μm .

Still a further embodiment of the invention is shown in **Figure 8**. In this
10 embodiment, a support (16) for the body part (1), e.g. a fingertip, is provided wherein said support (16) comprises an opening adapted to receive a portion (15) of the body part (1). For example, the support may comprise an annular structure with an opening, e.g. a substantially circular opening, in its center. The system is adapted for pressing the body part (1) onto the opening in the
15 support (16) such that a portion (15) of the body part (1), e.g. a portion of the fingertip, is forced into the opening. Thus, the tissue including the blood vessels within portion (15) is compressed resulting in an enhanced amount of capillary blood within portion (15). Thereby, the signal intensity and thus the sensitivity and/or accuracy of the measurement may be increased.

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Further, the system of Figure 8 includes a cover (3) which may be formed as an IR Fresnel lens as described above in the context of Figure 7. It should be noted, however, that other covers are also suitable. Furthermore, a radiation source (9a) is shown which is provided on the opposite side of the body part
25 with regard to the position of the sensing unit, which comprises a sensor (4). It should be noted, however, that one or more radiation sources may also be arranged in a circumferential arrangement around the body part (1), e.g. as shown in Figure 6. It should further be noted, that in this embodiment a plurality of different sensors may be present, e.g. as shown in Figures 4 and
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In **Figure 9**, measurement at a plurality of analyte-specific wavelengths/wavelength ranges and reference wavelengths/wavelength ranges is shown.

5 The absorption signal of glucose (24) has three different peaks at about 9.2 μm , at about 9.4 μm and about 9.6 μm . A first glucose-specific sensor may be adapted for measuring only the peak at 9.2 μm . Such a sensor would be adapted with a filter element capable of transmitting radiation only in a narrow range (22). Thus, the sensor is capable of selectively detecting
10 radiation within this narrow range. A further glucose-specific sensor may be adapted for measuring radiation at a broader range between about 9.1 μm and about 9.7 μm , thereby encompassing the peaks at about 9.2 μm , 9.4 μm and 9.6 μm . This sensor may be adapted with a filter element capable of transmitting radiation in a broader range (21).

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Two reference sensors may be provided, wherein said reference sensors are provided with filter elements capable of transmission of radiation with a wavelength in the range of about 8.6 μm and about 9.0 μm , particularly of about 8.8 μm - 8.9 μm (20) and/or radiation with a wavelength in the range of
20 about 9.8 μm and about 10.2 μm , particularly of about 9.9 μm - 10.1 μm (23), respectively.

Parallel and separate measurements at a wavelength of about 9.2 μm on the one hand and at a wavelength range including the peak at 9.2 μm , but also at
25 least one of the other peaks, particularly the peak at about 9.6 μm have a further advantage, since they allow determination whether the subject's blood contains ethanol. Since ethanol and other alcohols have an absorption band at a wavelength of about 9.6 μm , but not at a wavelength of about 9.2 μm , the ratio between the peak at 9.2 μm and 9.6 μm may be used to determine
30 and optionally correct a disturbance caused by blood alcohol.

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In an alternative embodiment, a first glucose-specific sensor may be adapted for measuring only the peak at 9.6 μm . Such a sensor would be provided with a filter element capable of transmitting radiation only in a narrow range. A further glucose-specific sensor may be adapted for measuring radiation at a
5 broader range between about 9.4 μm and about 9.6 μm , thereby encompassing the peaks at about 9.4 μm and about 9.6 μm and not encompassing the peak at 9.2 μm . This sensor may be provided with a filter element capable of transmitting radiation in a broader range.

10 In a further alternative embodiment, a reference sensor may be provided, which is provided with a filter element capable of transmission of radiation with a wavelength in the range of about 7.8 μm and about 8.2 μm , particularly of about 7.9 μm - 8.1 μm , optionally in combination with at least
15 one further reference sensor, which is provided with a filter element capable of transmission of radiation with a wavelength in the range of about 8.8 μm - 9.2 μm and/or radiation with a wavelength of about 9.8 μm - 10.2 μm , respectively

In a still further embodiment of the invention, the system may comprise a
20 sensor, which is adapted for a time-dependent detection of IR radiation having different wavelengths or wavelength ranges. In this embodiment, the system may be provided with a sensor comprising a plurality of filters adapted for transmitting IR radiation having different wavelengths or wavelength ranges wherein said filters may be placed on a sensor during
25 different stages of a measurement cycle thereby allowing detection of different wavelengths or wavelength ranges within a measurement cycle. Such an embodiment is shown in **Figure 10**. Here, a system is provided comprising a filter wheel (10) capable of rotating around an axis (11) and a shutter wheel (13) capable of rotating around an axis. The filter wheel and
30 the shutter wheel are provided with illumination holes (15) through which light from the radiation source (not shown) may pass into the body part of the subject (not shown). Reflected light from the irradiated body part may pass

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through different holes (14) of the filter wheel (10) which may be provided with analyte-specific filter elements and/or reference filter elements as described above. The filter wheel's (10) and the shutter wheel's (13) position may be monitored with a magnet (12) in combination with a magnetic sensor.

- 5 In operation, they may be rotated with predetermined frequencies, thereby allowing time-dependently passing of radiation from the radiation source into the body part and time-dependently passing of radiation emitted from the body part at predetermined time intervals through the different holes (14) of the filter wheel (10) to a sensor (not shown).

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In an alternative embodiment (not shown), a sensor which is adapted for a time-dependent detection of IR radiation having different wavelengths or wavelength ranges, may be a Fabry-Perot interferometer, e.g. a MEMS spectrometer for the desired IR wavelength range (cf. Tuohinieni et al., J. Micromech. Microeng. 22 (2012), 115004; Tuohinieni et al., J. Micromech. Microeng. 23 (2013), 075011).

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In certain embodiments, the system comprises a single sensor, which is adapted for a time-dependent detection of IR radiation having different
20 wavelengths or wavelength ranges. This sensor may be provided with different filters, e.g. with a filter wheel, or be a Fabry-Perot interferometer as described above.

The system of the present invention further comprises an analyzing unit (c)
25 for the qualitative and/or quantitative determination of a physiological parameter based on the IR radiation detected in the sensing unit (b). The analyzing unit may comprise, for example, an A/D converter and a microcontroller. The analysis of the measured signal may be based on the intensity and/or the decay time.

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A still further embodiment of the invention is shown in **Figure 11**. The system of this embodiment is adapted for being permanently fixed to the subject's

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body. This system is particularly adapted for carrying out a plurality of measurements in predetermined time intervals. The system comprises a housing (30) and a strap (31) for fixing the housing around the body (33), e.g. a wrist or forearm. Further, the system comprises a radiation source for emitting VIS/NIR light into an absorption area (34) of the body part (33) and sensors for detecting IR radiation emitted from the irradiated body part.

A still further embodiment of the invention is shown in **Figure 12**. The system of this embodiment is adapted for being permanently fixed to the subject's body and particularly adapted for carrying out a plurality of measurements in predetermined time intervals. The system comprises a housing (30) and a strap (31) for fixing the housing around the body (33), e.g. a wrist or forearm. Further, the system comprises a plurality of radiation sources, e.g. 2 radiation sources, for emitting VIS/NIR light into an absorption area (34) of the body part (33) and sensors for detecting IR radiation emitted from the irradiated body part. The light emitted from these sources may fall at angle, e.g. at an angle of about 30° to about 75° onto the surface of the body part (33).

In **Figure 13**, a schematic view of the system of Figure 4 is shown.

Figure 14 shows a heat map of a fingertip after irradiation with light of 810 nm for a time period of 2 s.

Figure 15 is diagram showing the time-dependent thermal power output in addition to the self-emission of a fingertip during intermittent irradiation with light of 810 nm with a power of 2 mW and a frequency of 0.1 Hz.

Figure 16a shows a block diagram of an embodiment of the sensing unit the present invention. A Region of Interest (ROI), i.e. the skin tissue of a subject, particularly a human subject, is irradiated with a first light source emitting VIS/NIR radiation having a wavelength of 940 nm, a second light source emitting VIS/NIR radiation having a wavelength of about 810 nm and

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optionally a third light source emitting VIS/NIR radiation having a wavelength of about 600 nm. Radiation transmitted through the Region of Interest or reflected from the Region of Interest is analyzed by a sensing unit. Further, the device comprises a temperature sensor.

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The sensing unit comprises a plurality of sensors, for example analyte-specific IR sensors (1) and (2) and reference sensors, e.g. IR sensor (4). For the determination of glucose, an IR sensor (1) may be provided with a first optical filter, which is transmissive for a wavelength of about 9.2 μm and an
10 IR sensor (2) may be provided with a second optical filter, which is transmissive for a wavelength range between about 9.2 μm and about 9.6 μm . A reference sensor (4) may be provided with a fourth optical filter which is transmissive for a wavelength or wavelength range between about 8.6 μm and about 9.0 μm and/or a wavelength or wavelength range between about
15 9.8 μm and about 10.2 μm . Further, the sensing unit comprises an NIR sensor for detecting VIS/NIR radiation having a wavelength of about 940 μm where glucose has a strong absorption band. The NIR sensor is provided with a suitable optical filter, which is transmissive for this wavelength. Further, the sensing unit may comprise a temperature sensor for measuring
20 the temperature of the skin tissue in the Region of Interest. The respective sensors may be coupled to amplifiers (AMP) for first signal amplification. Signals from individual sensors may be referenced with signals from other sensors by means of a comparator, thereby improving the measurement accuracy and/or signal quality. For example, the measurement signal from
25 the NIR sensor at 940 nm may be referenced with the measurement signal from analyte-specific IR sensor (1). Alternatively or additionally, the measurement signal from the NIR sensor at 940 nm may be referenced with the measurement signals from analyte-specific IR sensor (1) and/or analyte-specific IR sensor (2) and/or reference IR sensor (4). The measured and
30 optionally referenced signals are further amplified by a lock-in amplifier unit and transmitted to a microcontroller unit. A feedback control from the lock-in amplifier to the light sources may be provided. From the microcontroller unit,

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the signal and/or the result of internal algorithms may be transmitted to a display unit and/or another device, e.g. by a direct connection or via Bluetooth and/or WLAN.

- 5 **Figure 16b** shows a block diagram of a further embodiment of the sensing unit of the present invention, which is similar to the sensing unit shown in Fig. 16a. Here, additionally or alternatively, a multi-wavelength light source, e.g. a multi-wavelength LED comprising a plurality of individual diodes is provided. The multi-wavelength light source may e.g. have a wavelength range from
- 10 400 nm to about 700 nm is provided and may be operated by the microcontroller unit. Further, a temperature sensor coupled to an amplifier (AMP) is present. This temperature sensor may also be operated by the microcontroller unit.
- 15 In a still further embodiment of the invention, the system may comprise a spectral or line sensor or spectral or line sensor array, typically a bolometer or thermopile array, which is adapted for detecting an IR spectrum within the wavelength range of interest, e.g. including the range of about 7 μm to about 12 μm , particularly including the range of about 8 μm to about 10 μm . An IR
- 20 spectrum may be generated by passing the IR radiation from the irradiated body part through a spectral splitting or diffracting device and then to the sensor or sensor array. Such an embodiment is shown in **Figure 17**. Emitted IR radiation (70) from the irradiated body part (71), e.g. a fingertip, is optionally focused by a focusing element (72) adapted for focusing IR
- 25 radiation, e.g. a lens or concave mirror element, and then passed to an spectral splitting or diffracting element (73), e.g. a prism or an transmissive or reflective optical grating, where the IR radiation is split according to its wavelength. From there the diffracted radiation is passed to a spectral sensor or line sensor or sensor array (74), typically a bolometer or thermopile array,
- 30 where an IR spectrum in the wavelength range of interest, e.g. between 8 μm and about 20 μm including analyte-specific wavelengths or wavelength ranges and reference wavelengths or wavelength ranges, e.g. as described

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above, is detected. The amount of the physiological parameter of interest, e.g. glucose may be determined by spectral analysis according to the relative intensities of predetermined analyte-specific and reference wavelengths.

- 5 The system and the method of the invention allow qualitative and/or quantitative determination of the physiological parameter to be measured, particularly qualitative and/or quantitative determination of glucose in blood.

In certain embodiments, the concentration of the physiological parameter, e.g. the concentration of glucose in blood, is quantitatively determined. In certain embodiments, the alteration rate of the measured amount of the physiological parameter, e.g. glucose, is determined. These embodiments may involve a non-quantitative measurement, e.g. a relative measurement of the alteration of the analyte amount per time unit, i.e. the increase of the
10 analyte amount or the decrease of the analyte amount per time unit. In case the alteration of the analyte amount into a single direction, i.e. increase or decrease, exceeds a predetermined level and/or time period, the system will provide an alert. This embodiment is particularly useful for systems as shown in Figure 11 and Figure 12, which may be permanently fixed at the body of
15 the subject, e.g. around the wrist, forearm or upper arm. This embodiment may be adapted for steady glucose level monitoring.
20

In certain embodiments, the system of the invention is adapted for performing both non-quantitative measurements and quantitative
25 measurements. For example, the system may be adapted for performing non-quantitative measurements, e.g. qualitatively measuring the alteration, e.g. the increase or decrease, of the analyte amount over time during standard operation. Non-quantitative measurements may e.g. be performed as continuous and/or intermittent monitoring measurements, as required. In
30 case the alteration of the analyte amount exceeds a predetermined level and/or time period, the system is adapted to switch to a quantitative measurement in order to provide more detailed information. In these

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embodiments, a system adapted to be permanently fixed to the body, e.g. to an arm wrist, or to an ankle, may be used. Specific embodiments of such systems are shown in Figure 11 and Figure 12.

- 5 In certain embodiments, the system is adapted to perform non-quantitative measurements, e.g. continuous and/or intermittent monitoring measurements, and quantitative measurements on several different body parts. For example, the system may be adapted to perform non-quantitative measurements on a first body part, e.g. a body part to which the system may
- 10 be permanently fixed, such as an arm wrist or an ankle, and to perform quantitative measurements on a second body part, e.g. a body part where capillary vessels are more accessible, such as an earlobe or a fingertip. For performing a measurement on the second body part, the system is removed from the first body part and brought into contact, particularly into direct
- 15 contact with the second body part. After performing the measurement on the second body part, the system may be removed therefrom and brought again into contact with the first body part, e.g. by fixing the system to the first body part. In specific embodiments, the first body part is an arm wrist and/or the second body part is a fingertip.

20

A still further aspect of the invention is a non-invasive system for determining glucose in blood, which allows identification and optional correction of disturbances caused by blood alcohol comprising a sensing unit for detecting emitted IR radiation from a body part of said subject in the range of about 5

25 μm to about 12 μm ,

- wherein said sensing unit is adapted for (i) detecting IR radiation at a wavelength of about 9.2 μm and separately therefrom for detecting IR radiation at a wavelength of at least about 9.2 μm and about 9.6 μm , particularly at a wavelength range encompassing the wavelength of about
- 30 9.2 μm , about 9.4 μm and about 9.6 μm , and an analyzing unit for the separate determination of glucose from the above sensing units.

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Still a further aspect of the invention is a method for non-invasively determining glucose in blood of a subject using this system.

Preferred features of these aspects are as previously indicated in the above
5 specification.

Still a further aspect of the present invention is the use of an InAsSb sensor, optionally in combination with a lock-in amplifier for the measure of IR radiation emitted from a body part.

10 Preferred features of this aspect are as previously indicated in the above specification.

Still a further aspect of the present invention is a system and method for the
15 non-quantitative measurement of glucose involving a plurality of measurements during a predetermined time interval and determining an alteration of the measurement signal indicating an alteration of the amount of analyte and providing an alter if the alteration of the glucose amount to one direction, i.e. increase or decrease, exceeds a certain level in a
20 predetermined time period. This system and method may be adapted for steady glucose level monitoring.

Preferred features of this aspect are as previously indicated in the above
25 specification.

In the following, certain aspects and embodiments of the present invention are described as part of the specification.

Embodiments of the Specification

30 1. A non-invasive system for determining a physiological parameter in a bodily fluid of a subject comprising:

- 25 -

5 (a) a radiation source adapted for emitting visual (VIS)/near-infrared (NIR) radiation in the range of about 400 nm to about 1500 nm, or about 500 nm to about 1500 nm into a body part of said subject, wherein the irradiated body part absorbs electromagnetic energy resulting in a local increase of tissue temperature and in an increased emission of IR radiation in the wavelength range of about 5 μm to about 12 μm ,

10 (b) a sensing unit for detecting emitted IR radiation from the previously irradiated body part of said subject in the range of about 5 μm to about 12 μm ,

wherein said sensing unit is adapted for (i) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject,

15 and for (ii) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of the physiological parameter in the bodily fluid of said subject, and

20

(c) an analyzing unit for the qualitative and/or quantitative determination of the physiological parameter based on the IR radiation detected in the sensing unit (b).

25

2. The system of embodiment 1, which does not comprise an external radiation source for emitting IR radiation in the wavelength range of about 5 μm to about 12 μm .

30 3. The system of embodiment 1 or 2, wherein the physiological parameter is selected from compounds having at least one

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characteristic absorption band in the IR range of about 5 μm to about 12 μm , particularly in the range of about 8 μm to about 10 μm .

4. The system of any one of the preceding embodiments, wherein the physiological parameter is glucose.
5. The system of any one of the preceding embodiments, wherein the bodily fluid is blood.
6. The system of any one of the preceding embodiments which is adapted for determining glucose in blood, wherein said sensing unit is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of glucose in the blood of said subject, wherein said at least one wavelength or wavelength range is particularly selected from a wavelength of about 9.2 μm , a wavelength of about 9.4 μm , a wavelength of about 9.6 μm , a wavelength range comprising at least two of the wavelengths of about 9.2 μm , about 9.4 μm and about 9.6 μm , a wavelength range comprising all three of the wavelengths of about 9.2 μm , about 9.4 μm and about 9.6 μm or any combination thereof.
7. The system of any one of the preceding embodiments which is adapted for determining glucose in blood, wherein said sensing unit is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of glucose in the blood of said subject, wherein said at least one wavelength or wavelength range is particularly selected from a wavelength or wavelength range between about 8.7 μm to about 9.0 μm , a wavelength or wavelength range between about 9.7 μm to about 10.2 μm or any combination thereof.

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8. The system of any one of the preceding embodiments, which comprises a single radiation source (a).
- 5 9. The system of any one of embodiments 1-7 which comprises a plurality of radiation sources (a), e.g. 2, 3, 4 or more and e.g. up to 10 individual radiation sources (a).
- 10 10. The system of any one of the preceding embodiments, wherein the radiation source (a) is adapted for emitting VIS/NIR radiation in the range of about 400 nm to about 1200 nm, particularly in the range of about 550 nm to about 1100 nm, particularly in the range of about 800 nm to about 820 nm, e.g. at about 810 nm, and/or in the range of about 590 nm to about 660 nm, e.g. at about 600 nm, and/or in the range of about 920 nm to about 980 nm, e.g. at about 940 nm.
15
11. The system of any one of the preceding embodiments, wherein the radiation source (a) is adapted for emitting collimated radiation and/or adapted for emitting non-collimated radiation.
20
12. The system of any one of the preceding embodiments, wherein the radiation source (a) is a LED, a laser diode, a vcsel (vertical-cavity surface-emitting laser) or a laser.
- 25 13. The system of any one of the preceding embodiments, wherein the radiation source (a) is adapted for emitting VIS/NIR radiation continuously or intermittently throughout a predetermined time interval.
- 30 14. The system of any one of the preceding embodiments, wherein the radiation source (a) is adapted for emitting VIS/NIR radiation to obtain a local increase in temperature in the irradiated body part, particularly in

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an absorption area within the irradiated body part in the range of about 2°C to about 10°C, particularly in the range of about 3°C to about 5°C.

- 5 15. The system of embodiment 13 or 14, wherein the radiation source (a) is adapted for emitting VIS/NIR radiation continuously at a power of about 10 mW to about 1 W, particularly of about 20 mW to about 500 mW, and more particularly of about 50 mW to about 250 mW.
- 10 16. The system of embodiment 13, 14 or 15, wherein the radiation source (a) is adapted for emitting VIS/NIR radiation continuously for a time interval of about 0.1 s to 20 s, particularly of about 1 s to about 5 s, and more particularly of about 0.5 s to about 2 s.
- 15 17. The system of embodiment 13 or 14, wherein the radiation source (a) is adapted for emitting VIS/NIR radiation intermittently at a power of about 10 mW to about 5 W, particularly of about 20 mW to about 1 W, and more particularly of about 50 mW to about 500 mW.
- 20 18. The system of embodiment 13, 14 or 17, wherein the radiation source (a) is adapted for emitting VIS/NIR radiation intermittently for a time interval of about 0.1 s to about 20 s, particularly of about 0.2 s to about 5 s, and more particularly of about 0.5 s to about 2 s.
- 25 19. The system of embodiment 13, 14, 17 or 18, wherein the radiation source (a) is adapted for emitting VIS/NIR radiation intermittently with a pulse frequency of about 1 Hz to about 1 MHz.
- 30 20. The system of any one of the preceding embodiments, wherein the radiation source (a) is a multi-wavelength radiation source, particularly wherein the radiation source is adapted to emit VIS/NIR radiation at several, e.g. 2, 3, 4, 6, 8, 10 or more different wavelengths or wavelength ranges between about 400 nm to about 1200 nm, more

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particularly between about 450 nm and about 900 nm, e.g. at least 2, 3, 4, 6 or 8 wavelengths, which may be selected from about 470 nm, about 520 nm, about 590 nm, about 650 nm, about 750 nm and about 810 nm.

5

21. The system of any one of the preceding embodiments, wherein the radiation source (a) is provided on a side of the body part which is located opposite to the sensing unit (b).

10 22. The system of any one of the preceding embodiments, wherein at least one radiation source (a) is provided on a side of the body part which allows for emitting radiation directly into the body part without passing through a part of the system.

15 23. The system of any one of the preceding embodiments, wherein at least one radiation source (a) is provided on a side of the body part which allows for emitting radiation directly into the body part without passing through a horny part of the body surface, e.g. a finger nail.

20 24. The system of any one of the preceding embodiments, wherein the sensing unit (b) is adapted for detecting self-emitted IR radiation from the previously irradiated body part.

25 25. The system of any one of the preceding embodiments, wherein the sensing unit (b) is adapted for detecting emitted IR radiation from an absorption area within the previously irradiated body part wherein the absorption area has a locally increased temperature and exhibits an increased emission of IR radiation in the wavelength range of about 5 μm to about 12 μm .

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26. The system of any one of the preceding embodiments, wherein the sensing unit (b) comprises at least one first sensor, at least one second sensor, and optionally at least one third sensor, wherein the at least one first sensor is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject,
- 5 wherein the at least one second sensor is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of the physiological parameter in the bodily fluid of said subject, and
- 10 wherein the at least one third sensor, if present, (i) is adapted for detecting unspecific IR radiation, (ii) is adapted for detecting unspecific VIS/NIR radiation, (iii) is adapted for detecting VIS/NIR radiation having a wavelength, where the intensity of the detected VIS/NIR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject, and/or (iv) is
- 15 a temperature sensor for measuring the temperature of the body part.
- 20
27. The system of embodiment 26, wherein the at least one first sensor and the at least one second sensor are each provided with filter elements and optionally lens elements which are optically transparent in a predetermined wavelength or wavelength range.
- 25
28. The system of embodiment 26 or 27 comprising at least two different first sensors, which are adapted for detecting IR radiation having at least two different wavelengths or wavelength ranges.
- 30
29. The system of embodiment 26, 27 or 28, wherein at least one first sensor is adapted for detecting IR radiation having a first wavelength

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5 or wavelength range and at least one other first sensor is adapted for detecting IR radiation having a second wavelength range wherein the second wavelength range comprises the first wavelength or wavelength range and further comprises another wavelength or wavelength range.

10 30. The system of embodiment 29 for determining glucose in blood, wherein a first sensor is adapted for detecting IR radiation having a wavelength of about 9.2 μm and another first sensor is adapted for detecting IR radiation having a wavelength range between about 9.2 μm and about 9.6 μm .

15 31. The system of embodiment 29 for determining glucose in blood, wherein a first sensor is adapted for detecting IR radiation having a wavelength of about 9.6 μm and another first sensor is adapted for detecting IR radiation having a wavelength range between about 9.4 μm and about 9.6 μm .

20 32. The system of any one of embodiments 26-31 comprising at least two different second sensors, which are adapted for detecting IR radiation having at least two different wavelengths or wavelength ranges.

25 33. The system of embodiment 32 for determining glucose in blood, wherein a second sensor is adapted for detecting IR radiation having a wavelength or wavelength range between about 8.6 μm and 9.0 μm and another second sensor is adapted for detecting IR radiation having a wavelength or wavelength range between about 9.8 μm and about 10.2 μm .

30 34. The system of any one of embodiments 26-32 for determining glucose in blood, wherein a second sensor is adapted for detecting IR radiation having a wavelength or wavelength range between about 7.8

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5 μm and about 8.2 μm and optionally at least one further second sensor is adapted for detecting IR radiation having a wavelength or wavelength range between about 8.6 μm and 9.0 μm and/or for detecting IR radiation having a wavelength or wavelength range between about 9.8 μm and about 10.2 μm .

10 35. The system of any one of embodiments 26-34 for determining glucose in blood comprising at least one third sensor adapted for detecting VIS/NIR radiation, particularly VIS/NIR radiation having a wavelength of about 940 nm.

15 36. The system of any of the preceding embodiments, wherein the sensing unit (b) comprises at least one sensor adapted for time-dependently and separately detecting IR radiation having different wavelengths or wavelength ranges,
wherein in at least one first time interval the sensor is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily
20 fluid of said subject, and
wherein in at least one second time interval the sensor is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of the physiological parameter in
25 the bodily fluid of said subject.

30 37. The system of embodiment 36, wherein the sensing unit (b) comprises at least one sensor, which is provided with a plurality of filters adapted for transmitting IR radiation having different wavelengths or wavelength ranges.

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38. The system of embodiment 36 or 37, wherein the sensor is provided with a shutter wheel and/or a filter wheel.
- 5 39. The system of embodiment 38, wherein the shutter wheel comprises a plurality of openings wherein at least some of said openings are provided with filter elements and optionally lens elements which are optically transparent in a predetermined wavelength or wavelength range.
- 10 40. The system of embodiment 36, wherein the sensing unit (b) comprises at least one sensor, which is a Fabry-Perot interferometer.
- 15 41. The system of any one of the preceding embodiments, wherein the sensing unit (b) comprises at least one spectral sensor or line sensor or a spectral or line sensor array.
42. The system of any one of embodiments 36-41, wherein the sensing unit (b) comprises a single sensor.
- 20 43. The system of any one of the preceding embodiments, wherein the sensing unit (b) comprises at least one sensor, which is an optical detector, particularly an optical photovoltaics detector, more particularly an InAsSb-based detector.
- 25 44. The system of any one of the preceding embodiments, wherein the sensing unit (b) comprises at least one sensor, which is a thermopile or a bolometer.
- 30 45. The system of any one of the preceding embodiments, wherein the analyzing unit (c) comprises a microcontroller adapted for quantitatively determining the concentration of the physiological

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parameter and/or for non-quantitatively determining the alteration rate of the physiological parameter.

- 5 46. The system of any one of the preceding embodiments, which is adapted for detecting IR radiation from a body part which is selected from a fingertip, an ear lobe, a wrist, a forearm and an upper arm.
- 10 47. The system of any one of the preceding embodiments, wherein the radiation source (a) and the sensing unit (b) are arranged on the same side of the body part.
- 15 48. The system of any one of the preceding embodiments, wherein the radiation source (a) and the sensing unit (b) are arranged on different sides, particularly on opposite sides of the body part.
- 20 49. The system of any one of the preceding embodiments, wherein a first radiation source (a) is arranged on the same side of the body part as the sensing unit (b) and a further radiation source (a) is arranged on a different side, particularly on an opposite side of the body part as the sensing unit.
- 25 50. The system of any one of the preceding embodiments further comprising a cover, wherein said cover is at least partially made of a material, which is optically transparent for VIS/NIR radiation emitted by the radiation source (a) and/or for IR radiation detected by the sensing unit (b).
- 30 51. The system of embodiment 50, wherein the cover is at least partially made of CaF_2 and/or BaF_2 and/or of a plastic material, which is transparent for IR radiation and optionally transparent for VIS/NIR radiation.

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52. The system of embodiment 50 or 51, wherein the optically transparent material of the cover has a thickness of about 0.2 mm to about 2 mm, particularly of about 0.5 mm to about 1.5 mm, more particularly about 1 mm.
- 5
53. The system of any one of the preceding embodiments further comprising a cover, wherein said cover is at least partially made of a material which is optically transparent for IR radiation to be detected by the sensing unit, particularly in the IR wavelength range between about 5 μm to about 12 μm or a sub-range thereof and wherein said material is optionally substantially optically impermeable for VIS/NIR radiation emitted by the radiation source (a).
- 10
54. The system of any one of the preceding embodiments further comprising a cover which focuses IR radiation from the body part to the sensing unit (b), particularly to the at least one sensor of the sensing unit (b).
- 15
55. The system of embodiment 54 wherein the cover comprises an IR Fresnel lens or an array comprising a plurality of IR Fresnel lenses.
- 20
56. Use of the system of any one of the preceding embodiments for non-invasively determining a physiological parameter in a bodily fluid of a subject.
- 25
57. The use of embodiment 56, wherein the physiological parameter is glucose and the bodily fluid is blood.
58. The use of embodiment 56 or 57, wherein the physiological parameter is quantitatively determined.
- 30

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59. The use of embodiment 56, 57 or 58, wherein the alteration rate of the physiological parameter rate is non-quantitatively determined.
60. A method for non-invasively determining a physiological parameter in a bodily fluid of a subject comprising the steps:
- (a) irradiating a body part of said subject with visual (VIS)/near-infrared (NIR) radiation in the wavelength range of about 500 nm to about 1500 nm, or about 500 nm to about 1500 nm, wherein the irradiated body part absorbs electromagnetic energy resulting in a local increase of tissue temperature and in an increased emission of IR radiation in the wavelength range of about 5 μ m to about 12 μ m,
- (b) detecting emitted IR radiation from the previously irradiated body part of said subject in the wavelength range of about 5 μ m to about 12 μ m, comprising separately (i) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject, and
- (ii) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of the physiological parameter in the bodily fluid of said subject, and
- (c) analyzing the detected IR radiation for the qualitative and/or quantitative determination of the physiological parameter.
61. The method of embodiment 60, wherein the body part is not irradiated with an external source of IR radiation in the wavelength range of about 5 μ m to about 12 μ m.

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62. The method of embodiment 60 or 61, wherein the physiological parameter is glucose and the bodily fluid is blood.
63. The method of embodiment 60, 61 or 62, wherein the physiological parameter is quantitatively determined.
64. The method of any one of embodiments 60-63, wherein the alteration rate of the physiological parameter rate is non-quantitatively determined.

CLAIMS

1. A non-invasive system for determining a physiological parameter in a
5 bodily fluid of a subject comprising:
- (a) a radiation source adapted for emitting visual (VIS)/near-infrared
(NIR) radiation in the range of about 400 nm to about 1500 nm or 500
10 nm to about 1500 nm into a body part of said subject, wherein the
body part is particularly selected from a fingertip, an ear lobe, a wrist,
a forearm, and upper arm, and wherein the irradiated body part
absorbs electromagnetic energy resulting in a local increase of tissue
temperature and in an increased emission of IR radiation in the
wavelength range of about 5 μm to about 12 μm ,
15
- (b) a sensing unit for detecting emitted IR radiation from the previously
irradiated body part of said subject in the range of about 5 μm to about
12 μm ,
wherein said sensing unit is adapted for (i) detecting IR radiation
20 having at least one wavelength or wavelength range where the
intensity of the detected IR radiation is dependent from the
concentration of the physiological parameter in the bodily fluid of said
subject,
and for (ii) detecting IR radiation having at least one wavelength or
25 wavelength range where the intensity of the detected IR radiation is
substantially independent from the concentration of the physiological
parameter in the bodily fluid of said subject, and
- (c) an analyzing unit for the qualitative and/or quantitative
30 determination of the physiological parameter based on the IR radiation
detected in the sensing unit (b).

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2. The system of claim 1, which does not comprise an external radiation source for emitting IR radiation in the wavelength range of about 5 μm to about 12 μm .
- 5 3. The system of claim 1 or 2, wherein the physiological parameter is glucose and the bodily fluid is glucose.
4. The system of any one of the preceding claims which is adapted for determining glucose in blood, wherein said sensing unit is adapted for
10 detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of glucose in the blood of said subject, wherein said at least one wavelength or wavelength range is particularly selected from a wavelength of about 9.2 μm , a wavelength of about
15 9.4 μm , a wavelength of about 9.6 μm , a wavelength range comprising at least two of the wavelengths of about 9.2 μm , about 9.4 μm and about 9.6 μm , a wavelength range comprising the wavelengths of about 9.2 μm , about 9.4 μm and about 9.6 μm or any combination thereof.
20
5. The system of any one of the preceding claims, wherein the radiation source (a) is adapted for emitting VIS/NIR radiation in the range of about 550 nm to about 1200 nm, particularly in the range of about 800 nm to about 820 nm, e.g. at about 810 nm, and/or in the range of
25 about 590 nm to about 610 nm, e.g. at about 600 nm, and/or in the range of about 920 nm to about 980 nm, e.g. at about 940 nm.
6. The system of any one of the preceding claims, wherein the radiation source (a) is a LED, a laser diode, a vcsel (vertical-cavity surface-emitting laser) or a laser.
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7. The system of any one of the preceding claims, wherein the radiation source (a) is a multi-wavelength radiation source.
8. The system of claim any one of the preceding claims, wherein the sensing unit (b) comprises at least one first sensor, at least one second sensor, and optionally at least one third sensor, wherein the at least one first sensor is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject, wherein the at least one second sensor is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of the physiological parameter in the bodily fluid of said subject, and wherein the at least one third sensor, if present, (i) is adapted for detecting unspecific IR radiation, (ii) is adapted for detecting unspecific VIS/NIR radiation, (iii) is adapted for detecting VIS/NIR radiation having a wavelength, where the intensity of the detected VIS/NIR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject, and/or (iv) is a temperature sensor for measuring the temperature of the body part.
9. The system of claim 8, wherein at least one first sensor is adapted for detecting IR radiation having a first wavelength or wavelength range and at least one other first sensor is adapted for detecting IR radiation having a second wavelength range, wherein the second wavelength range comprises the first wavelength or wavelength range and further comprises another wavelength or wavelength range,

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- wherein the system is particularly adapted for determining glucose in blood, wherein a first sensor is adapted for detecting IR radiation having a wavelength of about 9.2 μm and another first sensor is adapted for detecting IR radiation having a wavelength range between about 9.2 μm and about 9.6 μm which comprises the first wavelength of about 9.2 μm and further comprises at least one wavelength of about 9.4 μm and about 9.6 μm , and particularly further comprises a wavelength of about 9.4 μm and about 9.6 μm .
- 10 10. The system of claim 8 or 9 comprising at least two different second sensors, which are adapted for detecting IR radiation having at least two different wavelengths or wavelength ranges, wherein the system is particularly adapted for determining glucose in blood, wherein a second sensor is adapted for detecting IR radiation having a wavelength or wavelength range between about 8.6 μm and 9.0 μm and another second sensor is adapted for detecting IR radiation having a wavelength or wavelength range between about 9.8 μm and about 10.2 μm .
- 20 11. The system of any of the preceding claims, wherein the sensing unit (b) comprises at least one sensor adapted for time-dependently and separately detecting IR radiation having different wavelengths or wavelength ranges, wherein in at least one first time interval the sensor is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject, and wherein in at least one second time interval the sensor is adapted for detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially

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independent from the concentration of the physiological parameter in the bodily fluid of said subject.

12. The system of any one of the preceding claims, wherein the sensing unit (b) comprises a single sensor.
13. The system of any one of the preceding claims, wherein the sensing unit (b) comprises at least one sensor which is an optical detector, particularly an optical photovoltaics detector, more particularly an InAsSb-based detector.
14. The system of any one of the preceding claims further comprising a cover, wherein said cover is at least partially made of a material which is optically transparent for IR/VIS radiation emitted by the radiation source (a) and for IR radiation detected by the sensing unit (b), wherein the cover is at least partially made of CaF_2 and/or BaF_2 and and/or of a plastic material which is transparent for IR radiation and optionally transparent for VIS/NIR radiation, wherein the optically transparent material of the cover has a thickness of about 0.2 mm to about 2 mm, particularly of about 0.5 mm to about 1.5 mm, more particularly about 1 mm.
15. The system of any one of the preceding claims further comprising a cover which focuses IR radiation from the body part to the sensing unit (b), particularly to the at least one sensor of the sensing unit (b), particularly wherein the cover comprises an IR Fresnel lens or an array comprising a plurality of IR Fresnel lenses.
16. Use of the system of any one of the preceding claims for non-invasively determining a physiological parameter in a bodily fluid of a subject, wherein the physiological parameter is glucose and the bodily

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fluid is blood, and wherein the alteration rate of the amount of glucose in blood is determined.

17. A method for non-invasively determining a physiological parameter in a bodily fluid of a subject comprising the steps:
- (a) irradiating a body part of said subject with visual (VIS)/near-infrared (NIR) radiation in the wavelength range of about 400 nm to about 1500 nm, or about 500 nm to about 1500 nm, wherein the irradiated body part absorbs electromagnetic energy resulting in a local increase of tissue temperature and in an increased emission of IR radiation in the wavelength range of about 5 μm to about 12 μm ,
- (b) detecting emitted IR radiation from the previously irradiated body part of said subject in the wavelength range of about 5 μm to about 12 μm , comprising separately (i) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is dependent from the concentration of the physiological parameter in the bodily fluid of said subject, and
- (ii) detecting IR radiation having at least one wavelength or wavelength range where the intensity of the detected IR radiation is substantially independent from the concentration of the physiological parameter in the bodily fluid of said subject, and
- (c) analyzing the detected IR radiation for the qualitative and/or quantitative determination of the physiological parameter.
18. The method of claim 17, wherein the body part is not irradiated with an external source of IR radiation in the wavelength range of about 5 μm to about 12 μm .

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19. The method of claim 17 or 18, wherein the physiological parameter is glucose and the bodily fluid is blood.
- 5 20. The method of any one of claims 17-19, wherein the concentration of the physiological parameter is quantitatively determined, and/or wherein the alteration rate of the amount of the physiological parameter is determined, particularly non-quantitatively determined.