

ENDOTRACHEAL TUBE AND INTUBATION SYSTEM INCLUDING SAME

FIELD AND BACKGROUND OF THE INVENTION

The present invention relates to endotracheal tubes for mechanically ventilating patients, and also to an intubation system including such tubes.

In the medical treatment of patients requiring breathing assistance, it is frequently necessary to insert an endotracheal tube into the trachea of the patient, by way of the mouth or nose and to connect the tube to a ventilator which periodically forces air into the lungs through the tube. The inner or distal end of the tube is typically provided with an inflatable cuff which is inflated into contact with the interior wall of the trachea.

In using such endotracheal tubes, however, problems arise with respect to bodily secretions which pass progressively between the inner surface of the trachea and the outer surface of the cuff. The evacuation of secretions accumulated in the subglottal region above the cuff is required to prevent a ventilator-associated lung infection, commonly called VAP or Ventilator Associated Pneumonia. Attempts have been made in the past to overcome these problems by regulating cuff pressure and/or by suctioning secretions from between the trachea's wall and the endotracheal tube. The removal of such secretions by suction generally requires the insertion into the subglottal region of an external lumen having a suction inlet port located above the sealing cuff. Another alternative is to use a suction lumen integrally formed in the wall of the endotracheal tube. In either case, the suction lumen is connected to a negative pressure source, thus drawing out secretions within the subglottal region.

However, there is a tendency for the suction lumen to become blocked, particularly during long-term intubation. Attempts have made to prevent or reduce such suction lumen blockage by irrigating the suction channel between successive suction. Such attempts, however, have frequently been unsuccessful, thereby subjecting the patient to an increase in the risk of lung infection.

BRIEF SUMMARY OF THE INVENTION

Embodiments of the present invention seek to provide an endotracheal tube, and also an intubation system, having advantages in the above respects. Embodiments of the invention also seek to provide such a tube and intubation system which can reduce the chances of blockage of the suction inlet port of the suction lumen, and more effectively

evacuate secretions and/or rinsing fluid from the subglottal region during the mechanical ventilation of the patient.

In studying the problem to be overcome, it was noted that the blockage of the suction lumen during the mechanical ventilation of the patient was frequently caused by the movement of a portion of the cuff, or by tracheal mucosal tissue of the patient, over the suction inlet port during the negative pressure condition in the suction lumen. It was accordingly found that by forming the distal end of the endotracheal tube with an outer surface configuration effective to prevent blockage of the suction inlet port by the cuff, or by tracheal mucosal tissue of the patient, the secretions, and/or rinsing fluid, could be more effectively removed from the subglottal region during the mechanical ventilation of the patient with reduced danger of blockage of the suction lumen.

In studying the above problem, it was further noted that the negative pressure exerted by the suction lumen caused the creation of a confined space between the vocal cords and the upper side of the cuff, causing the adhesion of cuff or tissue to the suction port. It was accordingly found that by venting the subglottal space with an external or embedded lumen, blockage of the suction inlet port by the cuff, or by tracheal mucosal tissue of the patient and or the secretions, could be more effectively prevented during the mechanical ventilation of the patient.

According to an aspect of the present invention, there is provided an endotracheal tube for mechanically ventilating patients, including a distal end for insertion into the patient's airway, past the vocal chords, through the subglottal region, and into the patient's lung; and a proximal end for connection to a mechanical ventilator; a cuff at said distal end of the endotracheal tube to be located in the subglottal region of

the patient below the vocal chords; an inflating lumen for inflating said cuff; a suction lumen having a suction inlet port leading from the outer surface of said endotracheal tube, and to be located in said subglottal region, for evacuating secretions and/or rinsing fluid from said subglottal region during the mechanical ventilation of the patient; a venting lumen leading from the outer surface of the endotracheal tube and also to be located in the patient's subglottal region, for venting the subglottal region to the atmosphere; and a separate rinsing lumen for connection to a rinsing-fluid source for circulating a rinsing fluid through said subglottal region to be removed by said suction lumen wherein said distal end is formed with an outer surface configuration effective to prevent blockage of said suction inlet port by said cuff or by tracheal mucosal tissue of the patient during a negative pressure condition in said suction lumen.

According to further features in the preferred embodiments of the invention described below, the endotracheal tube comprises a venting lumen leading from the outer surface of the endotracheal tube and also to be located in the patient's subglottal

region, for venting the subglottal region to the atmosphere to prevent the creation of vacuum within subglottal space.

According to further features in some described preferred embodiments, the outer surface configuration of the endotracheal tube includes a protuberance adjacent to the suction inlet port and projecting radially outwardly of the outer surface of the endotracheal tube at the suction inlet port effective to prevent such blockage of the suction inlet port. In one described embodiment, the protuberance is integrally formed in the wall of the endotracheal tube as a thickened portion thereof, and in another described embodiment, it is in the form of an inflatable element carried by the wall of the endotracheal tube.

In the described preferred embodiments, the venting lumen is used intermittently for venting and for analyzing air leaked from the lungs, particularly the CO₂, within the subglottal region.

In some described embodiments, the proximal end of the suction lumen is constructed for selective connection to a suction source, or to a rinsing-fluid source for circulating a rinsing fluid through the subglottal region. In such embodiments, therefore, the suction lumen is also used as the rinsing-fluid lumen. Other embodiments are described, however, wherein separate suction and rinsing-fluid lumens are provided in the endotracheal tube.

According to the disclosure herein, there is provided an endotracheal tube for mechanically ventilating patients, including: a distal end for insertion into the patient's airway, past the vocal chords, through the subglottal region, and into the patient's lung, and a proximal end for connection to a mechanical ventilator; a cuff at the distal end of the endotracheal tube to be located in the subglottal region of the patient below the vocal chords; an inflating lumen for inflating the cuff; a suction lumen integrally formed in a wall of the endotracheal tube and having a suction inlet port located for evacuating secretions and/or rinsing fluid from the subglottal region during the ventilation of the patient; and a rinsing lumen integrally formed in a wall of the tracheal tube and having a rinsing outlet port to be located in the patient's subglottal region for circulating a rinsing fluid through the subglottal region to be removed by the suction lumen.

In the described preferred embodiment, the endotracheal tube further comprises a venting lumen integrally formed in a wall of the endotracheal tube and having an air suction inlet located for pumping air into a CO₂ analyzer or for venting

the subglottal space during suction of secretions to prevent under pressurized vacuum conditions in the subglottal space.

According to further features in that described preferred embodiment, the outer wall of the endotracheal tube further includes at least one recess extending at one side of the suction and rinsing lumens from the proximal end of the endotracheal tube to the distal end to be located in the patient's subglottal region, the suction inlet port and the rinsing outlet port being located within the recess such as to reduce the possibility of blockage of the suction inlet port by the cuff or by endotracheal mucosal tissue of the patient during a negative pressure condition in the suction lumen.

Preferably, the outer wall of the endotracheal tube includes two of the recesses straddling the suction and rinsing lumens, there being a suction inlet port and a rinsing-liquid outlet port in each of the recesses.

As will be described more particularly below, endotracheal tubes constructed in accordance with the foregoing features more effectively evacuate secretions and/or rinsing fluid from the subglottal region during the mechanical ventilation of the patient, and prevent blockage of the suction inlet port by the cuff, or by tracheal mucosal tissue of the patient, during the negative pressure condition in the suction lumen.

Further features and advantages of the invention will be apparent from the description below.

BRIEF DESCRIPTION OF THE DRAWINGS

The invention is herein described, by way of example only, with the reference to the accompanying drawings, wherein:

Fig. 1 diagrammatically illustrates one form of prior art intubation system to which the present invention relates;

Fig. 2 is an enlarged fragmentary view illustrating the distal end of the endotracheal tube used in the system of Fig. 1, and particularly the subglottal region through which the tube passes;

Fig. 3 is a transverse sectional view along line III -- III of Fig. 2;

Figs. 4 and 5 are fragmentary views illustrating two ways in which it was found that the suction lumen frequently becomes blocked during the mechanical ventilation of a patient, thereby preventing evacuation of the secretions from the subglottal region;

Fig. 6 illustrates one construction of the endotracheal tube in accordance with the present invention to prevent blockage of the suction lumen,

Fig. 7 is a transverse sectional view along lines VII -- VII of Fig. 6;

Fig. 8 illustrates a modification in the construction of the endotracheal tube of

5 Fig. 6, particularly in the location of the protuberance preventing blockage of the suction inlet port;

Fig. 9 illustrates a further modification in the construction of the endotracheal tube, particularly in the nature of the protuberance to prevent blockage of the suction inlet port;

10 Fig. 10 illustrates a further modification in the construction of the endotracheal tube, to include separate suction and rinsing-fluid lumens;

Fig. 11 is a flowchart illustrating the operation of an intubation system using the endotracheal tube of Figs. 7 or 8, for example;

15 Fig. 12 is a timing diagram of the operation illustrated in the flowchart of Fig. 11;

Fig. 13 is a flowchart illustrating the operation of an intubation system using the endotracheal tube of Fig. 10, having separate suction and rinsing-fluid lumens;

Fig. 14 is a timing diagram of the operation illustrated in the flowchart of Fig. 13;

20 Fig. 15 is an elevational view illustrating another endotracheal tube constructed in accordance with the present invention; and

Fig. 16 is a transverse sectional view along line XVI -- XVI of Fig. 15.

It is to be understood that the foregoing drawings, and the description below, are provided primarily for purposes of facilitating understanding the conceptual
25 aspects of the invention and possible embodiments thereof, including what is presently considered to be a preferred embodiment. In the interest of clarity and brevity, no attempt is made to provide more details than necessary to enable one skilled in the art, using routine skill and design, to understand and practice the described invention. It is to be further understood that the embodiments described are
30 for purposes of example only, and that the invention is capable of being embodied in other forms and applications than described herein.

DESCRIPTION OF PREFERRED EMBODIMENTS

The Intubation System of Figs. 1–5

The preferred embodiments of the present invention to be described below relate primarily to the type of intubation system for mechanically ventilating patients as illustrated in Figs. 1–3. Such a system utilizes an endotracheal tube, generally designated 10, having a distal end 10a for insertion into the patient's airway 2, past the vocal chords 3, through the subglottal region 4 and into the patient's lungs 5. The proximal end 10b of endotracheal tube 10 is connectable to a mechanical ventilator 6, as well as to a number of control devices as will be described more particularly below.

As indicated earlier, such endotracheal tubes generally include a main lumen 11 for ventilating the patient, and a cuff 12 at the distal end 10a of the tube to be located in the subglottal region 4 of the patient, below the vocal chords. Such tubes also include an inflating lumen 13 extending through the tube for inflating the cuff by a cuff inflator 7 at the proximal end 10b of the tube; and a suction lumen 14 having an inlet port 14a leading from the outer surface of the endotracheal tube, and to be located in the subglottal region 4. Suction lumen 14 is connected, at the proximal end 10 of the endotracheal tube, to a suction device 8 or to a wall provided vacuum port for evacuating secretions from the subglottal region during the mechanical ventilation of the patient. In an embodiment of the invention described below, the subglottal region is also irrigated with a rinsing fluid, in which case suction lumen 14 would be used for evacuating the rinsing fluid introduced into the subglottal region as well as the secretions from the subglottal region.

In some intubation systems, the proximal end of suction lumen 14 may be connected either to a suction device 8, or to a monitor 9 for monitoring the composition, particularly the CO₂ content, of the air from the lungs removed via the suction lumen 14. Monitoring the composition of the exhaled air can be used for controlling the cuff-inflation pressure in order to minimize leakage while at the same time avoiding damage to the patient's airway.

As indicated earlier, the evacuation of secretions via the suction lumen 14 was frequently hindered by blockage of the suction lumen particularly during the long-term intubation. It was found that this was generally caused by blockage of the suction inlet port 14a either by the cuff 12 (as shown in Fig. 4), or by tracheal mucosal tissue of the patient, as shown in Fig. 5, during the negative-pressure condition of the suction lumen.

The Embodiment of Figs. 6 and 7

Figs. 6 and 7 illustrate one embodiment of an endotracheal tube, generally designated 20, particularly its distal end 20a, constructed in accordance with the present invention for avoiding the above problems. Endotracheal tube 20 includes the usual main lumen 21, cuff 22, and inflation lumen 23 for inflating the cuff. It further includes a suction lumen 24 having a suction inlet port 24a leading from the outer surface of the tube and to be located in the subglottal region, as described above with respect to Figs. 1–3, for evacuating secretions and/or rinsing fluid from the subglottal region during the mechanical ventilation of the patient.

According to the present invention, the distal end 20a of the endotracheal tube 20 is formed with an outer configuration effective to prevent blockage of the suction inlet port 24a by the cuff 22, or by tracheal mucosal tissue of the patient, during a negative-pressure condition in the suction lumen.

In the embodiment of the invention illustrated in Figs. 6 and 7, the outer surface of the endotracheal tube is formed with a protuberance 25 adjacent to the suction inlet port 24a and projecting radially outwardly of the outer surface of the tube at the section inlet port, such as to be effective to prevent blockage of the suction inlet port either by cuff 22, or tracheal mucosal tissue within airway 2 of the patient, during a negative pressure condition in the suction lumen.

In the embodiment of the invention illustrated in Figs. 6 and 7, the protuberance is integrally formed in the wall of the endotracheal tube 20 as a thickened portion thereof and is located in the space between the suction inlet port 24a and the cuff 22. Preferably, the protuberance should have a rounded outer surface projecting radially outwardly of the suction inlet port 24a so as to prevent blockage of that port either by the cuff 22 or by tracheal mucosal tissue.

The endotracheal tube illustrated in Figs. 6 and 7 includes a further feature, namely a venting lumen 26 integrally formed with, and extending through, the wall of the endotracheal tube 20 for venting the subglottal region to the atmosphere. Such a venting lumen thereby prevents an undue build-up of negative pressure within the subglottal region 4 such that the suction inlet port 24a of the suction lumen 24 may become blocked by the cuff 22 or by tracheal mucosal tissue.

As will be described below, venting lumen 26 may also be used for monitoring the composition, particularly the CO₂ of the leaking exhaled air evacuated from the subglottal region, similar to the function performed in the prior art via the suction lumen 14 and CO₂ monitor 9 in Fig. 1.

The Embodiment of Fig. 8

Fig. 8 illustrates the distal end 30a of another endotracheal tube 30 constructed in accordance with the present invention, also including the basic elements described above with respect to Figs. 6 and 7, mainly a main lumen 31, a cuff 32, an inflating lumen 33, and a suction lumen 34 having a suction inlet port 34a to be located in the subglottal region of the patient. In this case, the distal end of the endotracheal tube is formed with a protuberance 35 located adjacent to, but on the opposite side of the suction inlet port 24a such as to project radially outwardly of the outer surface of the endotracheal tube at the suction inlet port and to be effective to prevent blockage of the suction inlet port.

Endotracheal tube 30 illustrated in Fig. 8 also includes the venting lumen 36 integrally formed in the wall of the tube and having a port 36a to be located in the subglottal region 4 so as to prevent undue buildup of a negative pressure within that region during the mechanical ventilation of the patient. As will be described more particularly below, and as described above with respect to venting lumen 26 in Figs. 6 and 7, venting lumen 36 in Fig. 8 may also be used, not only for venting the subglottal region to the atmosphere, but also for analyzing the composition, particularly the CO₂ content, of the exhaled air from the lungs leaking into that region, e.g., to control the pressure within cuff 32 in order to produce the desired tissue contact without damage to the surrounding tissue.

The Embodiment of Fig. 9

Fig. 9 illustrates the distal end 40a of another endotracheal tube 40 constructed in accordance with the present invention of similar structure as described above with respect to Fig. 8. In endotracheal tube 40 of Fig. 9, however, the protuberance, thereby generally designated 45, is in the form of an inflatable element or balloon which, when inflated, projects radially outwardly of the outer surface of the tube at the suction inlet port, and thereby effectively prevents blockage of the suction inlet port. Inflatable element 45 may be of a blister configuration as shown, or of another configuration, e.g., annular configuration.

In all other respects, the endotracheal tube 40 illustrated in Fig. 9 is constructed and used in the same manner as described above with respect to Fig. 8.

The Embodiment of Fig. 10

Fig. 10 illustrates the distal end 50a of an endotracheal tube 50 constructed similar to that in Figs. 6 and 7, except that the endotracheal tube of Fig. 10 further includes a rinsing lumen 57 for rinsing or irrigating the subglottal region 4. In such

case, the rinsing lumen 57 has an outlet port 57a communicating with the subglottal region, preferably at the distal end thereof adjacent to the cuff 52.

By thus providing the endotracheal tube with a separate rinsing lumen 57, separate from the suction lumen 54, each lumen may be controlled to maximize its respective function, namely for rinsing the subglottal region via the rinsing lumen, and extracting secretions, as well as the rinsing fluid, from the subglottal region via the suction lumen. Where a separate rinsing lumen is not provided, as described above with respect to Figs. 5–9, for example, the suction lumen would also be used for rinsing the subglottal region, and therefore would be controlled to perform its suction function and rinsing function alternatively, as will be described below with respect to Figs. 11 and 12.

In all other respects, endotracheal tube 50 illustrated in Fig. 10 is constructed in the same manner as described above, to include a main lumen 51, cuff 52, inflating lumen 53, suction line 54 having an inlet port 54a, protuberance 55 and venting lumen 56.

Examples of Operation

The flowchart of Fig. 11, and timing diagram of Fig. 12, illustrate one example of operation of the above-described endotracheal tube illustrated in Figs. 6–8, wherein there is no separate rinsing lumen, but rather the suction lumen is also used for rinsing. The corresponding flow chart and timing diagram of Figs. 13 and 14 illustrate the corresponding operation of the endotracheal tube where a separate rinse lumen is provided, such as illustrated in Fig. 9. During both types of operations, the venting lumen e.g., 26, 36, 46, 56, is used intermittently, alternating for venting the subglottal region to the atmosphere, and for measuring the CO₂ content of the exhaled air leaking from the lungs and discharged from the subglottal region.

Thus, in the case where no separate rinsing lumen is provided (Figs. 10 and 11), the suction lumen (e.g., 24) is also used for rinsing, and is therefore controlled to alternately perform its suction and rinsing functions as shown by blocks 60–68, Fig. 10. The venting lumen 26 is also used intermittently, for alternately performing its venting function and CO₂ measurement functions. In the example operation illustrated in Figs. 11 and 12, it will be seen that the suction step is accompanied by the venting step to prevent the formation of underpressure. As noted by step 67 in Fig. 11, after the rinse line connected to suction lumen 24 has been closed, the venting lumen, e.g., 26, is used to enable completion of the measurement step 68.

Figs. 13 and 14 are corresponding flow and timing diagrams illustrating the operation of the endotracheal tube where a separate rinse lumen is provided as in the case of rinse lumen 57 in Fig. 10, such that the rinse may be a continuous operation, whereas the suction is periodically applied in synchronism with the venting operation. As shown by blocks 70–77 in Fig. 13, and in the functional timing of Fig. 14, the CO₂ measuring operation, however, is performed in between the suction operations and is combined with the venting operations.

The Embodiment of Figs. 15 and 16

Figs. 15 and 16 illustrate an endotracheal tube to include all the foregoing lumens formed as passageways through the wall of the endotracheal tube, generally designated 80. Thus, endotracheal tube 80 includes a main lumen 81, a cuff 82 at the distal end 81a of the tube, an inflating lumen 83 for inflating/deflating the cuff, a suction lumen 84 for evacuating secretions and/or rinsing fluid from the subglottal region 4, a venting lumen 86 for venting the subglottal region to the atmosphere, and a rinsing lumen 87 for introducing a rinsing or irrigating fluid into the subglottal region.

It will be seen from Fig. 16 that the suction lumen 84 and rinsing lumen 87 are formed in the same side of the endotracheal tube in radial alignment, and are separated by a partition 88 integrally formed with the wall of the endotracheal tube.

It will also be seen from Fig. 16 that the outer surface of the endotracheal tube 80 is formed with a pair longitudinally-extending recesses 85a, 85b on opposite sides of the suction lumen 84 and rinsing lumen 87. Suction lumen 84 includes two suction inlet ports 84a, 84b, one in each of the two recesses 85a, 85b; similarly, rinsing lumen 87 includes two exit ports 87a, 87b, one in each of the recesses 85a, 85b, for introducing the rinsing fluid into the subglottal region.

It will thus be appreciated that the outer surface of the endotracheal tube 80 on opposite sides of the two recesses 85a, 85b, project outwardly of the two suction inlet ports 84a, 84b, and are therefore effective to prevent blockage of those ports either by the cuff 82, or by tracheal mucosal tissue of the patient, during a negative pressure condition in the suction lumen. It will also be appreciated that the two rinsing-fluid exit ports 87a and 87b of the rinsing lumen 87, also formed in recesses 85a and 85b adjacent to the suction inlet ports 84a, 84b, further reduce the possibility of blocking those inlet ports during the mechanical ventilation of the patient.

Endotracheal tube 80 further includes a radio opaque strip 89 integrally formed in the wall of the tube at the opposite side of the inflation lumen 83.

As one example, endotracheal tube 80 illustrated in Figs. 15 and 16 may be made of silicon having an inner diameter of 8 mm, and an outer diameter of 11.5 mm. The Shore Hardness should be the maximum available. The outer diameter of the tube may be increased, but preferably not to exceed 12.5 mm. Other preferred dimensions appear on the drawings. It will be appreciated, however, that other materials could be used, e.g., polyvinyl chloride, and that the dimensions could be varied according to the requirements of any particular application.

While the invention has been described with respect to several preferred embodiments, it will be appreciated that these are set forth merely for purposes of example, and that many other variations, modifications and applications of the invention may be made.

WHAT IS CLAIMED IS:

1. An endotracheal tube for mechanically ventilating patients, including a distal end for insertion into the patient's airway, past the vocal chords, through the subglottal region, and into the patient's lung; and a proximal end for connection to a mechanical ventilator;

a cuff at said distal end of the endotracheal tube to be located in the subglottal region of the patient below the vocal chords;

an inflating lumen for inflating said cuff;

a suction lumen having a suction inlet port leading from the outer surface of said endotracheal tube, and to be located in said subglottal region, for evacuating secretions and/or rinsing fluid from said subglottal region during the mechanical ventilation of the patient;

a venting lumen leading from the outer surface of the endotracheal tube and also to be located in the patient's subglottal region, for venting the subglottal region to the atmosphere; and

a separate rinsing lumen for connection to a rinsing-fluid source for circulating a rinsing fluid through said subglottal region to be removed by said suction lumen

wherein said distal end is formed with an outer surface configuration effective to prevent blockage of said suction inlet port by said cuff or by tracheal mucosal tissue of the patient during a negative pressure condition in said suction lumen.

2. The endotracheal tube according to Claim 1, wherein said outer surface configuration includes a protuberance adjacent to said suction inlet port and projecting radially outwardly of the outer surface of the endotracheal tube at said suction inlet port.

3. The endotracheal tube according to Claim 2, wherein said protuberance is integrally formed in the wall of said endotracheal tube as a thickened portion thereof.

4. The endotracheal tube according to Claim 2, wherein said protuberance is in the form of an inflatable element carried by the wall of said endotracheal tube.

5. The endotracheal tube according to Claim 2, wherein said protuberance is located between said cuff and said suction inlet port of the suction lumen.

6. The endotracheal tube according to Claim 2, wherein said protuberance is located on the side of said suction inlet port facing the proximal end of the endotracheal tube.

7. The endotracheal tube according to Claim 1, wherein the proximal end of said suction lumen is constructed for selective connection to a suction source, or to a rinsing-fluid source for circulating a rinsing fluid through said subglottal region.

8. The endotracheal tube according to Claim 2, wherein said venting lumen is constructed for selective connection to the atmosphere or to an analyzing device for analyzing the composition of air leaking from the lungs into said subglottal region.

9. An intubation system, comprising:
an endotracheal tube according to Claim 7;
a suction source connectable to the proximal end of said endotracheal tube;
a rinsing-fluid source connectable to the proximal end of said endotracheal tube;
and a control device for selectively connecting said proximal end of the endotracheal tube to either said suction source or to said rinsing-fluid source.

10. The intubation system according to Claim 9, wherein:
said endotracheal tube further comprises a venting lumen;

said intubation system further comprises an analyzing device connected to the proximal end of said venting lumen for analyzing air leaking from the lungs into said subglottal region;

and said control device also selectively connects said proximal end of the venting lumen to the atmosphere or to said analyzing device.

11. An intubation system comprising:
an endotracheal tube according to Claim 1;
a suction source connected to the proximal end of said suction lumen;
and a rinsing-fluid source connectable to the proximal end of said rinsing lumen for circulating a rinsing liquid through said subglottal region to be removed by said suction lumen.

12. The intubation system according to Claim 11, further comprising an analyzing device connected to the proximal end of said venting lumen for analyzing air leaking from the lungs into said subglottal region;
and a control device which selectively connects said proximal end of the venting lumen to the atmosphere or to said analyzing device.

13. The endotracheal tube according to Claim 1, wherein:
said suction lumen is integrally formed in a wall of said endotracheal tube;
outer surface of said wall is formed with a recess extending from said suction inlet port to the proximal end of said endotracheal tube;
and said suction inlet port is formed in said recess in the outer surface of said endotracheal tube such that the outer surface of the endotracheal tube adjacent to said recess projects radially outwardly of said recess and thereby prevents said blockage of the suction inlet port.

14. The endotracheal tube according to Claim 13, wherein there are two of said recesses formed in the outer surface of said endotracheal tube wall on opposite

sides of said suction lumen, said suction lumen including a suction inlet port in each of said two recesses.

15. The endotracheal tube according to Claim 1, wherein said rinsing lumen is formed through a wall of the endotracheal tube and has a rinsing-liquid outlet at its distal end.

16. The endotracheal tube according to Claim 15, wherein said suction lumen and said rinsing lumen are formed in radially-aligned relation in said wall of the endotracheal tube between said two recesses and are separated by a partition integrally formed in said wall of the endotracheal tube; and wherein said rinsing lumen includes a said rinsing-liquid outlet in each of said two recesses.

17. The endotracheal tube according to Claim 16, wherein said inflating lumen is formed through another wall portion of the endotracheal tube.

18. The endotracheal tube according to Claim 17, wherein the endotracheal tube further comprises a radio opaque strip in a wall portion thereof opposite to that formed with said inflating lumen.

19. The endotracheal tube according to Claim 17, wherein said endotracheal tube further comprises a venting lumen formed through a wall thereof opposite to that of said suction lumen and rinsing lumen, said venting lumen having an inlet port to be located in the patient's subglottal region for alternatingly venting the subglottal region to the atmosphere, and for supplying a sample of air leaking from the lungs into said subglottal region for analysis.