APPARATUS AND TECHNIQUES FOR REDUCING THE EFFECTS OF GENERAL ANESTHETICS

TECHNICAL FIELD

The present invention relates generally to apparatus and techniques for reversing the effects of inhaled general anesthetics. More particularly, the present invention relates to use of ventilation and rebreathing apparatus and, optionally, respiratory monitoring apparatus, in conjunction with one another to reverse the effects of inhaled general anesthetics.

BACKGROUND

General anesthesia is often administered to subjects as surgical procedures are being performed. Typically, a subject who is subject to general anesthesia is "hooked up" to a ventilator by way of a breathing circuit. One or more sensors may communicate with the breathing circuit to facilitate monitoring of the subject's respiration, the anesthesia, and, possibly, the subject's blood gases and blood flow. One or more anesthetic agents are typically administered to the subject through the breathing circuit.

Examples of breathing circuits that are used while anesthesia is being administered to a patient include circular breathing circuits, which are also referred to in the art as "circle systems," and Mapleson or Bain type breathing circuits, which are also referred to herein as Bain systems for the sake of simplicity.

Circle systems are typically used with adult patients. The expiratory and inspiratory limbs of a breathing circuit of a circle system communicate with one another, with a carbon dioxide remover, such as a soda lime can, being disposed therebetween. As the expiratory and inspiratory limbs communicate with one another, a circle system will typically include two or more sets of one-way valves to prevent a patient from rebreathing just-expired, CO_2-rich gases.

Bain systems are typically used with smaller patients (*e.g.*, children). Bain systems include linear tubes through which both inspiratory and expiratory gases flow. Fresh gases are typically directed toward a patient interface to remove the just-expired gases therefrom before the patient can rebreathe them. As long as the fresh gas flow is higher than the flow of the patient's ventilation, there is little or no rebreathing.

When a general anesthesia is administered to a subject, respiratory or inhaled anesthetics are delivered to a patient in low concentrations, typically being diluted to a concentration of about 1% to about 6%, depending on the type of anesthetic agent used. As the subject inhales a general anesthetic agent, the anesthetic agent is carried into the lungs, where it enters the bloodstream, and is carried by the blood to various other body tissues. Once the concentration of the anesthetic reaches a sufficient level, or threshold level, in the brain, which depends upon a variety of subject-specific factors, including the size and weight of the subject, the subject becomes anesthetized. The subject remains anesthetized so long as the concentration of the anesthetic agent in the brain of the subject remains above the threshold level.

Once the procedure, typically surgery, for which the general anesthesia is given, has been completed, it is usually desirable to reverse the effects of the general anesthetic as soon as possible. Reversal of the effects of general anesthesia allows the surgical team to vacate the operating room, thereby freeing it up for subsequent surgeries and possibly reducing the cost of surgery, and also permits the anesthetist to tend to other patients, and conserves the typically expensive anesthetic agents that are used. In addition, for safety reasons, it is desirable to minimize the time a subject is under general anesthesia. Other benefits of quickly reversing anesthesia include better cognitive function for elderly patients immediately following surgery and enabling patients to protect their own airway sooner.

Reversal or discontinuation of the general anesthetic state requires that levels of the anesthetic agent in the brain decrease below the threshold level, or that the anesthetic agent be removed from the subject's brain.

It has long been known that activated charcoal and other substances can be used to selectively adsorb gaseous anesthetic agents. Accordingly, activated charcoal has found conventional use in adsorbers, such as that described in U.S. Patent 5,471,979, issued to Psaros et al., that prevents anesthetic agents from escaping the breathing circuit and entering the operating room. In this regard, activated charcoal adsorbers are typically placed in the exhaust flow of the anesthesia delivery system. The potentially deleterious effects of exhaust anesthetic gases into the operating room are thereby avoided. Further, as most halocarbon anesthetics are considered to be atmospheric pollutants, the charcoals or other adsorbents of conventional anesthetic agent adsorbers

prevent pollution that may be caused if gaseous anesthetic agents were otherwise released into the environment.

U.S. Patent 5,094,235, issued to Westenskow et al. (hereinafter "Westenskow"), describes the use of activated charcoal to hasten the removal of gaseous anesthetic agents from breathing circuits. While such a technique would be useful for preventing the reinhalation of previously exhaled anesthetic agents, more could be done to hasten the rate at which anesthetic agents are removed from the subject's brain.

Typically, the rate at which blood flows through the brain and a subject's breathing rate and breathing volume are the primary factors that determine the rate at which the levels of anesthetic agent are removed from the brain of the subject. The rate of blood flow through the brain is a determining factor because the blood carries anesthetic agents away from the brain and to the lungs. The breathing rate and breathing volume are important since they increase the rate at which anesthetic agent may be removed from the blood and transported out of the body through the lungs.

Hyperventilation has been used to increase the breath volume and/or rate of a subject and, thereby, to facilitate the removal of anesthetic agents from the subject's lungs. However, hyperventilation typically results in a reduced level of carbon dioxide (CO_2) in blood of the subject (P_aCO_2). When P_aCO_2 levels are decreased, the brain is less likely to signal the lungs to breathe on their own and the patient remains dependent on the ventilation from an artificial respirator. *See* U.S. Patent 5,320,093, issued to Raemer (hereinafter "Raemer"). Additionally, the reduced P_aCO_2 levels that result from hyperventilation are known to cause a corresponding reduction in the rate at which blood flows through the brain, which actually decreases the rate at which the blood can carry anesthetic agents away from the brain.

Rebreathing processes, in which a subject "rebreathes" previously exhaled, CO_2-rich air, have been used to prevent significant decreases in P_aCO_2 levels during such hyperventilation. The apparatus that have been conventionally used to effect such processes, however, do not filter anesthetic agent from the exhaled air before the subject rebreathes the same. Consequently, the patient also rebreathes the previously exhaled anesthetic agent, which effectively prolongs the process of reversing the general anesthesia.

The computerized system described in Raemer was designed to overcome purported deficiencies with hyperventilation and rebreathing. The system of Raemer

infuses CO_2 from an external source into the breathing circuit and, thus, into the subject's lungs (*i.e.*, the CO_2 is not rebreathed by the subject) as general anesthesia is being reversed to speed the rate of reversal and, thus, recovery of the subject from the general anesthesia. The teachings of Raemer with respect to infusion of CO_2 from an external source are limited to avoidance of reintroducing anesthetic agents into the subject's brain while increasing the subject's P_aCO_2 to a level that will facilitate reinitiation of spontaneous breathing by his or her brain as early as possible. As the technique and system that are taught in Raemer do not include increases in the breathing rate or breathing volume of a subject, they do not accelerate the rate at which a subject recovers from anesthesia.

Accordingly, there are needs for processes and apparatus which increase the rate at which blood carries anesthetic agents from the brain, as well as the rate at which the lungs expel the anesthetic agents from the body in order to minimize the time required to reverse the levels of anesthetic agents in the brain to reverse the effects thereof.

DISCLOSURE OF INVENTION

The present invention includes methods and apparatus for accelerating the rate at which a subject recovers from general anesthesia, or for reversing the effects of anesthetic agents. These methods and apparatus maintain or increase the rate at which blood flows through the subject's brain, increase the subject's rate of respiration and respiratory volume, and prevent the subject from re-inhaling previously exhaled anesthetic agents.

A method according to the present invention includes increasing the rate at which the subject inhales or the volume of gases inhaled by the subject while causing the subject to at least periodically breathe gases including an elevated fraction of CO_2. This may be effected by having or causing the subject to rebreathe at least some of the gases that the subject has already exhaled or by otherwise increasing the amount of CO_2 in gases that are to be inhaled by the subject. The rebreathed gases are filtered to at least partially remove some of the previously exhaled anesthetic agent or agents therefrom. It is currently preferred that substantially all anesthetic agents be removed from the exhaled gases prior to rebreathing thereof.

An apparatus that incorporates teachings of the present invention is configured to facilitate breathing by a subject at a rapid (*i.e.*, above-normal) rate, while

maintaining CO_2 levels in the subject's blood, thereby at least maintaining the rate at which blood flows to and through the subject's brain. Such an apparatus includes a filter to selectively remove anesthetic agents from gases that have been exhaled by the subject, as well as a component that is configured to effect partial rebreathing by the subject, which is also referred to herein as a "rebreathing element," or another component which is configured to increase the levels of CO_2 inhaled by the subject. The rebreathing or other CO_2 level-elevating component of the apparatus facilitates an increase in the rate of ventilation of the subject, while CO_2 levels in blood of the subject (*i.e.*, P_aCO_2) remain normal or elevated. The rebreathing or other CO_2 level-elevating component further allows the patient to be ventilated at a high volume or rate while maintaining high or normal levels of CO_2.

Other features and advantages of the present invention will become apparent to those of ordinary skill in the art through consideration of the ensuing description, the accompanying drawings, and the appended claims.

BRIEF DESCRIPTION OF DRAWINGS

In the drawings, which illustrate various aspects of exemplary embodiments of the present invention:

FIG. 1 is a schematic representation of an example of an anesthesia reversal system according to the present invention, including at least a portion of a breathing circuit, an element for increasing a concentration of carbon dioxide inhaled by a subject that is recovering from anesthesia, and an anesthesia filter and Y-connector positioned along the breathing circuit;

FIGs. 1A and 1B schematically illustrate variations of the anesthesia reversal system shown in FIG. 1;

FIG. 2 schematically depicts an exemplary embodiment of the anesthesia reversal system shown in FIG. 1, which includes a rebreathing tube positioned along a breathing circuit, between the anesthesia filter and the Y-connector, which are also positioned along the breathing circuit;

FIG. 3 is a cross-sectional representation of another exemplary embodiment of the anesthesia reversal system of FIG. 1, in which a rebreathing tube extends from and back to the anesthesia filter housing;

FIG. 4 is a cross-sectional representation of another embodiment of anesthesia reversal system of the present invention, in which the anesthesia filter thereof includes an additional deadspace volume which is configured to effect rebreathing;

FIG. 5 is a cross-sectional representation of still another embodiment of anesthesia reversal system that incorporates teachings of the present invention, in which the anesthesia filter includes a volume-adjustable deadspace to effect rebreathing;

FIGs. 6 through 6B schematically illustrate, in cross-section, another exemplary embodiment of anesthesia reversal system, comprising a switch or valve for selectively controlling filtration of respiratory gases;

FIG. 7 schematically illustrates, in cross-section, an exemplary embodiment of anesthesia reversal system that includes a mask;

FIGs. 8A and 8B are schematic depictions of yet another embodiment of anesthesia reversal system of the present invention, in which one or more conduits and valves are positioned between inspiratory and expiratory limbs that branch off of the Y-connectors;

FIG. 9 schematically depicts use of an anesthesia reversal system according to the present invention along a conventional circular system;

FIG. 10 schematically illustrates use of an anesthesia reversal system of the present invention with a conventional Bain system; and

FIG. 11 is a schematic representation of yet another embodiment of anesthesia reversal system of the type shown in FIG. 1, in which the element that increases a concentration of carbon dioxide inhaled by the subject comprises a carbon dioxide infuser.

Unless otherwise indicated, like numbers, including numbers preceded by additional digits or followed by primes or other symbols, represent similar elements that may have the same or similar characteristics.

BEST MODE(S) FOR CARRYING OUT THE INVENTION

With reference to FIG. 1, an anesthesia reversal system 10 according to the present invention, which may be positioned along a portion of a breathing circuit 50, between a subject I and a Y-connector 60, and includes a filter 20 and a rebreathing component 30. An inspiratory limb 52 and an expiratory limb 54 may be coupled to Y-connector 60 and, thus, to breathing circuit 50. Notably, the inspiratory and

expiratory limbs of some breathing circuits are coaxial. Nonetheless, the junction between the inspiratory and expiratory hoses of such breathing circuits is still referred to as a "Y-connector."

As depicted, filter 20 is positioned near the endotracheal tube for an intubated patient or over the mouth and/or nose of a subject I when breathing through a mask or mouthpiece so as to remove exhaled anesthetic agents before they flow into the remainder of anesthesia reversal system 10, where they might otherwise be adsorbed by the surfaces of anesthesia reversal system 10 to remove inhalation anesthetics and be subsequently inhaled by the subject. Of course, placement of filter 20 at alternative locations of anesthesia reversal system 10 is also within the scope of the present invention, so long as filter 20 is positioned between the subject I and rebreathing component 30.

Filter 20 may include a housing 22 with a proximal (relative to subject I) port 24 and a distal port 26, which, in the depicted example, are on opposite sides of filter 20. In addition, an anesthesia filter member 28 is contained within housing 22, in communication with both proximal port 24 and distal port 26.

Proximal port 24 and distal port 26 may both be configured for connection to standard breathing circuit fittings. For example, proximal port 24 and distal port 26 may be configured to connect to standard 15 mm or 22 mm respiratory fittings. As such, once reversal of general anesthesia or other inhaled anesthesia is desired, filter 20 may be positioned along a breathing circuit 50 which is already in communication with an airway (*i.e.*, the mouth or nose, trachea, and lungs) of subject I.

Anesthesia filter member 28 may comprise any type of filter which is known to selectively adsorb one or more types of anesthetic agents. By way of example and not to limit the scope of the present invention, anesthesia filter member 28 may comprise an activated charcoal, or activated carbon, filter, a crystalline silica molecular sieve, a lipid-based absorber (*e.g.*, which operates in accordance with the teachings of U.S. Patent 4,878,388 to Loughlin et al.), a condensation-type filter, or any other type of filtering mechanism which captures or otherwise removes anesthetic vapors from the gases that have been exhaled by subject I. If filter member 28 comprises a particulate material, such as activated charcoal or crystalline silica, the particulate material may be contained by a porous member, a screen, or the like.

As anesthesia filter member 28 communicates with both proximal port 24 and distal port 26, it will remove anesthetic agents from gases that are inhaled by subject I, as well as from gases that are exhaled by subject I.

Optionally, filter 20 may also include an antimicrobial filter member 29 of a type known in the art, such as 3M FILTRETE® filter media or other electrostatic polypropylene fiber based filter media. Like anesthesia filter member 28, antimicrobial filter member 29 communicates with breathing circuit 50 (*e.g.*, by way of proximal port 24 and distal port 26 of filter 20). Accordingly, antimicrobial filter member 29 may be positioned to receive substantially all of the gases that are inhaled or exhaled by subject I and, thus, to remove bacteria, viruses, or other pathogens from those gases. Of course, anesthesia reversal systems that include antimicrobial filters that are separate from filter 20 are also within the scope of the present invention.

As another option, a system that incorporates teachings of the present invention may be configured to selectively restrict the direction in which gases flow through filter 20. This may be desirable since directing exhaled gases through filter 20 may result in a high concentration of anesthesia at the subject-side of anesthesia filter member 28 (*i.e.*, the side of anesthesia filter member 28 located closest to proximal port 24 of filter 20). A high anesthesia concentration at the subject-side of anesthesia filter member 28 may, in turn, result in the reintroduction of anesthesia into gases that are inhaled by subject I.

An exemplary embodiment of a selective flow restrictor 100, shown in FIG. 1A, includes a bypass conduit 101 and at least two one-way valves 102 and 103 (*e.g.*, flap valves of known configuration). Bypass conduit 101 is positioned parallel to filter 20. Valve 102 is positioned at an end of or along bypass conduit 101 and is oriented so as to open when subject I exhales and close when subject I inhales. Valve 103 is positioned adjacent to filter 20 and is oriented to close when subject I exhales and open when subject I inhales. As shown, valve 103 is positioned adjacent to distal port 26 of filter 20, but may be positioned between filter 20 and subject I. Of course, other configurations of selective flow restrictors, which perform the same functions, are also within the scope of the present invention.

Valves 102 and 103 work in concert to control the flow of gases through filter 20. When subject I exhales, the positive pressure closes valve 103 and opens valve 102. The closure of valve 103 results in a restriction adjacent to filter 20, which

causes the majority of exhaled gases to pass through bypass conduit 101, bypassing filter 20 and preventing anesthesia from collecting at the proximal (relative to subject I) side of anesthesia filter member 28. Conversely, when subject I inhales, the negative pressure draws valve 102 closed, which prevents the inhaled gases from passing through bypass conduit 101. Instead, the inhaled gases must pass through filter 20, where anesthesia in the gases may be removed by anesthesia filter member 28 before subject I inhales the gases. During mechanical ventilation, inhaled gas is forced through the device into the patient, hence there is no negative pressure on the valve 102. Nevertheless, there is pressure difference that closes valve 102 and opens valve 103 during inspiration.

FIG. 1B schematically depicts a bypass switch 105, which is also referred to herein as a "switching element," that may optionally be included in an anesthesia reversal system according to the present invention and positioned along a breathing circuit 50. When positioned in a first orientation, bypass switch 105 allows gases to flow through filter 20 and, optionally, into rebreathing component 30 (FIG. 1) when anesthesia reversal is desired. When anesthesia reversal or use of an anesthesia reversal system is not desired, for example, during surgery or after withdrawal of anesthesia but while a subject is mechanically ventilated, switch 105 may be positioned in a second orientation, in which respiratory gases bypass filter 20 and, optionally, rebreathing component 30.

With returned reference to FIG. 1, filter 20 and rebreathing component 30 are in direct communication with one another. As will be shown in greater detail hereinafter, rebreathing component 30 may actually be a part of filter 20, rather than separate therefrom.

Rebreathing component 30 may be configured to provide a volume or an amount of deadspace which will maintain a particular level of CO_2 in the blood (*i.e.*, P_aCO_2) of subject I. In the depicted example, rebreathing component 30 comprises conduit 31 including a section 32 of expandable tubing that can be extended to increase or compressed to decrease the amount of deadspace for containing previously exhaled gases which are to be rebreathed by subject I. Of course, other types of rebreathing apparatus, such as one of those (excepting the tracheal gas insufflation device) described in U.S. Patent 6,227,196, issued to Orr et al., or any other known type of

partial rebreathing apparatus, may be used in anesthesia reversal system 10 as rebreathing component 30.

It is also within the scope of the present invention to include another element, such as a respiratory flow sensor or gas sampling port 40a therefor, or a capnometer or gas sampling port 40b therefor, as known in the art, at any position along an anesthesia reversal system 10 according to the present invention (*e.g.*, close to subject I, between filter 20 and rebreathing component 30, close to Y-connector 60, etc.). For example, when gas sampling ports 40a, 40b are used, they may be of conventional configuration (*e.g.*, for facilitating gas sampling at a rate of about 50 ml/min to about 250 ml/min), such as fittings that are configured to be disposed at an end or along the length of breathing circuit 50 or an inspiratory or expiratory limb 52, 54 in communication therewith.

Turning now to FIGs. 2 through 8B, specific examples of anesthesia reversal systems that incorporate teachings of the present invention are shown.

The embodiment of anesthesia reversal system 10′ shown in FIG. 2 includes a rebreathing component 30′ that comprises a section of rebreathing conduit 31′, which communicates with breathing circuit 50 at two locations 34′ and 35′ between filter 20 and Y-connector 60. Rebreathing conduit 31′ may include a section 32′ which is volume-adjustable in a manner known in the art (*e.g.*, by way of corrugations, etc.). One or more valves 36′, flow restrictors 37′, or a combination thereof may be positioned along breathing circuit 50 or rebreathing conduit 31′ to control the flow of gases into and out of conduit 31′.

Another embodiment of anesthesia reversal system 10″, which is shown in FIG. 3, includes a rebreathing component 30″ that communicates directly with a filter 20″ rather than with breathing circuit 50. As shown, rebreathing component 30″ may be configured as a loop of conduit 31″. One or both ends 38″ and 39″ of conduit 31″ may communicate with filter 20″ at a location which is on the distal side of anesthesia filter member 28 relative to the location of subject I (FIG. 1) (*e.g.*, between anesthesia filter member 28 and distal port 26) such that gases are filtered before and/or after passage thereof through conduit 31″. Like rebreathing component 30′ (FIG. 2), rebreathing component 30″ may include a volume-adjustable section 32″.

FIG. 4 depicts another embodiment of anesthesia reversal system 10‴, in which filter 20‴ is configured to provide a deadspace volume 30‴ in which at least some

carbon dioxide rich gases are collected as subject I exhales. As shown, deadspace volume 30''' is located on the distal side of anesthesia filter member 28, such that the exhaled gases that have collected therein are filtered as they flow therein and, later, as they are drawn therefrom (*e.g.*, as subject I (FIG. 1) subsequently inhales).

Yet another embodiment of anesthesia reversal system 10'''' that incorporates teachings of the present invention is pictured in FIG. 5. Anesthesia reversal system 10'''' is much like anesthesia reversal system 10''', which is shown in and described with reference to FIG. 4. The primary difference between anesthesia reversal system 10'''' and anesthesia reversal system 10''' is that the deadspace volume 30'''' of anesthesia reversal system 10'''', which is at least partially defined by body 22'''' of filter 20'''', is adjustable, for example, by enlarging or reducing the amount of space occupied by body 22'''' (*e.g.*, by the illustrated sliding motion or as otherwise will be readily apparent to those of ordinary skill in the art).

FIGs. 6 through 6B illustrate an anesthesia reversal system 110' that is configured to be positioned along a breathing circuit 50. A switch 105' of anesthesia reversal system 110' is positioned along breathing circuit 50, as described above in reference to FIG. 1B, so that gases may be selectively directed into anesthesia reversal system 110' or selectively bypass anesthesia reversal system 110'. A housing 111' of anesthesia reversal system 110' includes a proximal opening 112' and a distal opening 114', and contains a filter 120' and a rebreathing component 130'. Rebreathing component 130' is illustrated as including a compact, somewhat convoluted pathway of sufficient length to hold carbon dioxide-rich gases.

Switch 105' may comprise a rotatable valve of the type illustrated in FIGs. 6 through 6B, which includes a vane 106' that controls the direction in which gases may flow. Alternatively, switch 105' may comprise a sliding switch, a diaphragm, or any other suitable switching or valve mechanism.

When switch 105' is in a first position, as shown in FIG. 6, gases may flow directly and substantially unimpeded through breathing circuit 50 and, therefore, bypass anesthesia reversal system 110'. When switch 105' is in a second position, as shown in FIGs. 6A and 6B, it restricts gas flow through breathing circuit 50, causing respiratory gases to flow into and pass through anesthesia reversal system 110'.

Additionally, a bypass conduit 101' and a pair of one-way valves 102' and 103' or other selective flow restrictor 100' may be positioned within housing 111' so as to

control the direction in which gases flow through anesthesia reversal system 110′. In the illustrated example, bypass conduit 101′ and one-way valves 102′ and 103′ are positioned on the proximal side of filter 120′ in an arrangement that prevents exhaled gases from flowing into filter 120′ and that causes inhaled gases to flow through filter 120′.

As shown in FIG. 6A, when a subject exhales, as illustrated by the arrows, one-way valve 102′ opens, causing the exhaled gases to flow through bypass conduit 101′ and, thus, to prevent the exhaled gases from flowing into filter 120′. The exhaled gases enter rebreathing component 130′ through bypass conduit 101′. As the volume of exhaled gases may exceed the volume of rebreathing component 130′, excess exhaled gases flow out of rebreathing component 130′ and housing 111′ of anesthesia reversal system 110′ through distal opening 114′.

As shown in FIG. 6B, when the subject inhales, one-way valve 103′ is drawn to a closed position. The negative pressure draws gases from a distal section of breathing circuit 50, into housing 111′ through distal opening 114′, into and along rebreathing component, through filter 120′, and back into breathing circuit 50 through proximal opening 112′ of housing 111′.

Another embodiment of anesthesia reversal system 110″, which is illustrated in FIG. 7, includes a mask 115″. Mask 115″ is configured to interface with the mouth or nose of a subject I. In addition to mask 115″, anesthesia reversal system 110″ includes a housing 111″ with a proximal opening 112″ and a distal opening 114″. Housing 111″ contains a rebreathing component 130″, as well as a filter 120″.

Proximal opening 112″ communicates mask 115″ and, thus, with the airway of subject I (*e.g.*, through one or both of the mouth and nose of subject I). Distal opening 114″ may be configured to communicate with subject I's surrounding environment, as illustrated.

Rebreathing component 130″, which is located along a flow path between proximal opening 112″ and distal opening 114″, is configured to hold at least a portion of the relatively carbon dioxide-rich gases that are exhaled by subject I. While rebreathing component 130″ may have any suitable configuration, rebreathing component 130″ is illustrated as including a plurality of concentrically arranged, serially connected passageways 130a″, 130b″, 130c″, etc. A proximal end 132″ of rebreathing component 130″ communicates with a distal end of filter 120″ which, in

turn, communicates with proximal opening 112″ of housing 111″ and, thus, with mask 115″.

Anesthesia reversal system 111″ may optionally include a selective flow restrictor 100″, such as a bypass conduit 101″ and a pair of one-way valves 102″ and 103″, arranged or positioned to control the flow of respiratory gases through filter 120″. For example, when subject I exhales, valve 102″ is forced into a closed position, which prevents the exhaled gases from entering filter 120″. In addition, valve 103″ is forced into an open position, causing the exhaled gases to flow into bypass conduit 101″ and directly into rebreathing component 130″. As the volume of rebreathing component 130″ is fixed, excess exhaled gases may exit housing 111″ through distal opening 114″. When subject I inhales, valve 103″ is forced into a closed position, while valve 102″ is forced into an open position. As a result, gases may be drawn from rebreathing component 130″ and through filter 120″ before exiting housing 111″ through proximal opening 112″ and entering the subject I's airway.

As another alternative, pictured in FIGs. 8A and 8B, an anesthesia reversal system 10″″ of the present invention may include one or more shunt lines 56″″ positioned between an inspiratory limb 52″″ and an expiratory limb 54″″ to provide a selectively sized deadspace in the circuit. In this embodiment, inspiratory limb 52″″ and expiratory limb 54″″ act as part of the deadspace. A two-way shunt valve 58″″ is positioned along each shunt line 56″″ to selectively direct the flow of inspired and expired gas.

During normal or baseline breathing, as depicted in FIG. 8A, the two-way shunt valve 58″″ will be in a closed position and exhaled gases, which are represented by the shaded area, will enter the expiratory limb 54″″.

In order to facilitate rebreathing, as pictured in FIG. 8B, two-way shunt valve 58″″ is opened, permitting exhaled gases to fill a portion of inspiratory limb 52″″, substantially all of expiratory limb 54″″, and shunt line 56″″, all of which serve as deadspace.

The deadspace may be rendered adjustably expandable by using an expandable conduit for all or part of one or more of inspiratory limb 52″″, expiratory limb 54″″, and shunt line 56″″.

Turning now to FIGs. 9 and 10, use of an anesthesia reversal system 10 of the present invention in combination with various anesthesia delivery systems is shown.

In FIG. 9, a circle system 70 is illustrated. Circle system 70, which includes an interconnected (*e.g.*, in the configuration of a circle, or loop) inspiratory limb 52′ and expiratory limb 54′. Inspiratory limb 52′ and expiratory limb 54′ are coupled to a Y-connector 60 which, in turn, is coupled to a breathing circuit 50′. Breathing circuit 50′ is configured to interface with a subject I (FIG. 1) in a known manner (*e.g.*, by intubation, with a mask, with a nasal cannula, etc.). Circle system 70 also includes at least two one-way valves 72 and 74, which are positioned across inspiratory limb 52′ and expiratory limb 54′, respectively, at opposite sides of Y-connector 60. One way valves 72 and 74 restrict the flow of gases through circle system 70 to a single direction, such that expired gases are prevented from flowing directly into inspiratory limb 52′ and to prevent subject I from inhaling gases directly from expiratory limb 54′.

Inspiratory limb 52′ of circle system 70 includes at least one gas inlet 75, such as a port that facilitates coupling to an anesthesia delivery system 300, a mechanical ventilator, or a breathing bag, or which permits air from an environment external to circle system 70 (*e.g.*, an operating room, a patient room in a hospital, etc.) to flow therein. An expiratory element 76, such as an expiratory spill valve of a known type is positioned along expiratory limb 54′ of circle system 70.

As shown, expiratory limb 54′ and inspiratory limb 52′ are joined at a location which is distal relative to Y-connector 60 and subject I by a carbon dioxide removal element 77, such as a soda lime canister. As one-way valve 72 prevents exhaled gases entering inspiratory limb 52′, the exhaled gases are directed through expiratory limb 54′ and, depending upon the positioning of a bypass valve 78 positioned along expiratory limb 54′, possibly into carbon dioxide removal element 77, which reduces the amount of carbon dioxide present in such gases.

Additionally, circle system 70 includes an anesthesia reversal system. While any anesthesia reversal system that incorporates teachings of the present invention may be included in circle system 70, for the sake of simplicity, circle system 70 is described as including anesthesia reversal system 10. As shown, anesthesia reversal system 10 selectively communicates, by way of bypass valve 78, with expiratory limb 54′ of circle system 70 and is positioned in parallel to carbon dioxide removal element 77. The volume of deadspace that may be present within circle system 70 depends upon whether or not expiratory element 76 causes exhaled gases to remain within expiratory limb 54′ and upon whether bypass valve 78 is positioned to permit exhaled gases to

bypass carbon dioxide removal element 77. In addition, when a mechanical ventilator is coupled to gas inlet 75, the volume of deadspace within circle system 70 depends upon the proximity of the gas inlet 75 to a junction 80 of anesthesia reversal system 10 with inspiratory limb 52'.

If expiratory element 76 is at least partially closed, depending upon the positioning of bypass valve 78, at least some of the gases that have been exhaled by subject I and which are flowing through expiratory limb 54' may be diverted from carbon dioxide removal element 77 into anesthesia reversal system 10. If bypass valve 78 is adjustable to more than two positions, exhaled gases may be directed into both anesthesia reversal system 10 and carbon dioxide removal element 77. Thus, it may be possible to carefully regulate the amounts of exhaled gases that are directed into anesthesia reversal system 10 and carbon dioxide removal element 77, providing control over the amount of carbon dioxide that is rebreathed by subject I. Further, if bypass valve 78 is positioned such that the previously exhaled gases flow through anesthesia reversal system 10, the amount of carbon dioxide that remains in gases that pass through anesthesia reversal system 10 will be relatively high, while the amount of anesthesia present in such gases will be reduced by filter 20.

Then, when subject I inhales or is caused to inhale, at least a portion of the gases that are inhaled (*i.e.*, the gases that remain within breathing circuit 50' and anesthesia reversal system 10) will be previously exhaled, CO_2-rich gases.

As circle system 70 may itself serve as a deadspace from which a subject I may be caused to rebreathe previously exhaled, carbon dioxide rich gases, an anesthesia reversal system 10 that is used in a circle system 70 may lack additional deadspace, such as a rebreathing component 30.

Referring now to FIG. 10, a Bain system 90 that incorporates teachings of the present invention is depicted. Bain system 90 includes a linear breathing circuit 50", a patient interface 92 located at one end 51" of breathing circuit 50", and a fresh gas inlet 94, which is configured to communicate with an anesthesia delivery system 300 of a known type, a mechanical ventilator, a breathing bag, or the environment external to Bain system 90, positioned along the length of breathing circuit 50". In addition, Bain system 90 includes an anesthesia reversal system 10 that communicates with breathing circuit 50". Anesthesia reversal system 10 is preferably positioned proximate to patient interface 92 so as to optimize the amount of anesthesia removed from the exhaled gases

and, thus, minimize the amount of anesthetic agent rebreathed by a subject I as the affects of the anesthesia are being reversed.

While FIGs. 2 through 10 illustrate various systems that are useful for providing a deadspace volume from which a subject I may rebreathe as subject I is being withdrawn from anesthesia, any other method, apparatus, or system that induces rebreathing of carbon dioxide in a mechanical breathing circuit for the purpose of reversing the affects of anesthesia on a subject are also within the scope of the present invention.

Turning now to FIG. 11, an anesthesia reversal system 110 that includes a carbon dioxide infusion element 130 rather than a rebreathing component is depicted. As illustrated, carbon dioxide infusion element 130 communicates with a breathing conduit 150. A filter 120 of anesthesia reversal system 110 is also positioned along breathing conduit 150, proximate to subject I (FIG. 1), so as to reduce the amount of anesthesia in gases that are exhaled by subject I and, thus, to minimize the amount of anesthesia that remains in any gases that are withdrawn from breathing conduit 150 and rebreathed by subject I.

With returned reference to FIG. 1 (although anesthesia reversal system 110 shown in and described with reference to FIG. 11 may be used in a similar manner), anesthesia reversal system 10 may be used by placing the same in communication with a breathing circuit or anesthesia delivery circuit (*e.g.*, those shown in FIGs. 9 and 10). It is currently preferred that filter 20 be positioned proximate to subject I and that rebreathing component 30 be positioned closer to Y-connector 60. In the case of anesthesia recovery system 110 (FIG. 11), the position of carbon dioxide infusion element 130 relative to that of filter 120 is irrelevant.

A deadspace (*e.g.*, in the form of the volume within a rebreathing component 30) may be adjusted by an anesthetist to provide the desired volume of deadspace therein in order to facilitate rebreathing. For example, when the deadspace volume is at least partially located within corrugated tubing, the deadspace volume may be adjusted by extending or contracting the length of the corrugated tubing. As another example, when a fixed volume of deadspace is present, or even with a volume-adjustable deadspace, the amount of carbon dioxide within the deadspace may be tailored by adjusting the flow of "fresh" gases, including recycled gas from which

carbon dioxide has been removed. When the flow of "fresh" gases is lower than the flow of subject I's ventilation, rebreathing of gases within the deadspace may occur.

Once anesthesia reversal system 10 has been positioned in communication with a breathing circuit or anesthesia delivery system, gases that are exhaled by subject I pass into and through filter 20, which removes at least some anesthetic agents from the exhaled gases. At least a portion of the volume of the filtered, exhaled gases enters and at least temporarily remains within the deadspace (*e.g.*, rebreathing component 30). Also, by reducing levels of anesthetic agents in gases that are exhaled by subject I, filter 20 may effectively reduce levels of anesthetic agents that escape into the environment (*e.g.*, the operating room, recovery room, atmosphere, etc.) when subject I exhales.

When subject I inhales, at least a portion of the inhaled gases are drawn from the deadspace (*e.g.*, from rebreathing component 30), with any other gases being drawn from either the air or from a source of inspiratory gases that communicate with a ventilator. As the inhaled gases are drawn through breathing circuit 50, they pass through filter 20, where at least some of the remaining anesthetic agents therein are removed therefrom. Notably, in most anesthesia systems, very high concentrations of oxygen (> 90%) are used. Thus, subject I may rebreathe the same gas many times and still be sufficiently oxygenated.

It is currently preferred that partial rebreathing processes (*i.e.*, only a portion of the gases inhaled by the patient were previously exhaled, while the other portion of gases are "fresh") be used in reversing the effects of inhaled anesthesia. This is because subject I requires some oxygen during the reversal. Of course, the use of total rebreathing processes is also within the scope of the invention. The manner in which rebreathing is effected may be varied or controlled to provide the desired affects, while providing subject I with sufficient oxygen.

Of course, a gas sensor and monitor 210 (*e.g.*, an anesthetic gas monitor of a known type) that measures carbon dioxide or oxygen may be used to monitor the ventilatory gases of subject I. A respiratory flow sensor and monitor 212 may also be used to monitor the flow of ventilation of subject I. Gas concentrations may be determined by a processing element 220 (*e.g.*, a computer processor or controller, a smaller group of logic circuits, etc.) that communicates with gas sensor and monitor 210 and flow sensor and monitor 212, as known in the art. If the carbon

dioxide or oxygen levels (*e.g.*, blood gas content, respiratory fraction, etc.) reach undesirable levels, adjustments may be made to the deadspace volume (*e.g.*, within rebreathing component 30), or volume of rebreathed gases, to the concentration of oxygen or carbon dioxide in the other inhaled gases, or to any combination of the foregoing. Such adjustment may be made automatically, such as by processing element 220, which, of course, operates under control of appropriate programming and communicates with one or more of a ventilator and valves (*e.g.*, bypass valve 78 (FIG. 9)) of the anesthesia reversal system 10. Alternatively, adjustment of the deadspace may be effected semiautomatically, such as in accordance with instructions provided by a processing element, or manually.

By combining a filter 20 and an element for increasing the amount of carbon dioxide inhaled by subject I (*e.g.*, with a rebreathing component 30 or carbon dioxide infusion element 130) in an anesthesia reversal apparatus of the present invention, ventilation of a subject I may be increased while maintaining normal to high P_aCO_2 levels, which maintains or increases blood flow levels and, thus, the rate at which anesthetic agents may be removed from the brain as the increased ventilation improves the rate at which anesthetic agents are removed from the blood and, thus, exhaled by subject I.

While much of the description provided herein focuses on the reversal of general anesthesia, it should be appreciated that the apparatus and methods of the present invention are useful for reversing the effects of any type of inhaled anesthesia, whether or not such inhaled anesthetic agents have a general anesthetic effect.

Although the foregoing description contains many specifics, these should not be construed as limiting the scope of the present invention, but merely as providing illustrations of some of the presently preferred embodiments. Similarly, other embodiments of the invention may be devised which do not depart from the spirit or scope of the present invention. Features from different embodiments may be employed in combination. The scope of the invention is, therefore, indicated and limited only by the appended claims and their legal equivalents, rather than by the foregoing description. All additions, deletions and modifications to the invention as disclosed herein which fall within the meaning and scope of the claims are to be embraced thereby.

CLAIMS

What is claimed:

1. A method for facilitating emergence of a subject from inhaled anesthesia, comprising:

bypassing a filter for removing anesthesia during exhalation by the subject; and

drawing gases through the filter before they are inhaled by the subject.

2. The method of claim 1, wherein drawing comprises drawing inhaled gases including an above-ambient concentration of carbon dioxide through the filter.

3. The method of claim 1, wherein bypassing is effected with at least one valve.

4. The method of claim 1, wherein drawing is effected with at least one valve.

5. A method for ventilating a subject, comprising:

establishing communication between an airway of the subject and a ventilator with an apparatus including a breathing circuit with a switching element positioned along a length thereof and an anesthesia reversal system that selectively communicates with the breathing circuit through the switching element;

causing the switching element to direct respiratory gases through the anesthesia reversal system when expedited reversal of an effect of the anesthesia is desired; and

causing the switching element to prevent respiratory gases from flowing through the anesthesia reversal system when expedited reversal of an effect of the anesthesia is not desired.

6. The method of claim 5, wherein establishing communication comprises establishing communication between the airway and an anesthesia reversal system including a filter for removing anesthesia at least from gases to be inhaled by the subject.

7. The method of claim 6, further comprising, upon causing the switching element to direct respiratory gases through the anesthesia reversal system:
preventing exhaled gases from passing through the filter; and
causing gases to pass through the filter before they are inspired.

8. A system for facilitating emergence of a subject from inhaled anesthesia, comprising:
a filter for at least partially removing anesthesia from gases exhaled by the subject;
a CO_2 level-elevating component for causing the subject to inhale gases including an above-normal amount of CO_2; and
a selective restrictor for causing:
exhaled gases to bypass the filter and enter the CO_2 level-elevating component; and
inhaled gases to be drawn from the CO_2 level-elevating component and through the filter.

9. The system of claim 8, wherein the selective restrictor comprises a bypass conduit and a pair of valves, at least one valve of the pair being positioned at an end of the bypass conduit or along a length of the bypass conduit.

10. The system of claim 9, wherein the at least one valve is positioned at an end of the bypass conduit most proximate to a subject with which the system may be used.

11. The system of claim 8, further comprising:
a mask in communication with the bypass conduit.

12. A system for facilitating emergence of a subject from inhaled anesthesia, comprising:

a filter for at least partially removing anesthesia from gases exhaled by the subject;

a CO_2 level-elevating component for causing the subject to inhale gases including an above-normal amount of CO_2; and

a mask in communication with the filter and the CO_2 level-elevating component.

13. A respiratory system, comprising:

a breathing circuit;

an anesthesia reversal system; and

a switching element positioned along a length of or at an end of the breathing circuit for facilitating selective communication between the breathing circuit and the anesthesia reversal system.

14. The respiratory system of claim 13, wherein the switching element configures a switch configured to be oriented in:

a first position that allows respiratory gases to flow substantially unimpeded along the breathing circuit but restricts flow of respiratory gases into the anesthesia reversal system; and

a second position that restricts flow of respiratory gases along the breathing circuit and directs respiratory gases into and through the anesthesia reversal system.

15. The system of claim 13, wherein the anesthesia reversal system includes:

a filter; and

a CO_2 level-elevating component for causing the subject to inhale gases including an above-normal amount of CO_2 located distally relative to the filter.

16. The system of claim 15, wherein the filter removes anesthesia at least from gases to be inhaled by a subject.

17. The system of claim 15, wherein the CO_2 level-elevating component comprises a rebreathing component configured to receive gases exhaled by a subject.

18. The system of claim 15, wherein the anesthesia reversal system further includes:

a selective restrictor for causing:

exhaled gases to bypass the filter and enter the CO_2 level-elevating component; and

inhaled gases to be drawn from the CO_2 level-elevating component and through the filter.

19. The system of claim 18, wherein the selective restrictor comprises a bypass conduit and a pair of valves, at least one valve of the pair being positioned at an end of the bypass conduit or along a length of the bypass conduit.

20. A method for further reversing anesthesia of a spontaneously breathing subject, comprising:

placing a mask over at least a portion of a face of the subject, in communication with an airway of the subject;

directing at least some exhaled gases into a rebreathing component in communication with the mask; and

drawing gases within the rebreathing component through an anesthesia removal filter and into the airway of the subject as the subject inhales.

21. The method of claim 20, further comprising:

preventing the exhaled gases from passing through the anesthesia removal filter.