

CLOSURE SYSTEM, AND MANUFACTURING METHOD OF CLOSURE DEVICE

BACKGROUND

5 Field

[0001]

An embodiment of the present disclosure relates to a closure system comprising a closure device for closing a hole or duct in a tissue related to a cardiac disease. In addition, an
10 embodiment of the present disclosure relates to a manufacturing method of a closure device.

Background Art

[0002]

15 In cardiac diseases such as atrial septal defect, ventricular septal defect, patent ductus arteriosus, patent foramen ovale, etc., a hole or duct is formed in a tissue such as atrial septum, pulmonary artery, etc. A closure device is used as a tool for closing the hole or duct. For example, Patent Literature 1
20 discloses a method of closing a hole using a mesh structure formed of woven metal wires. When pushed out from a catheter inserted in a heart, the mesh structure can expand like a disc in the heart.

Patent Literature

25 [0003]

Patent Literature 1: JP 6661539 B

Non Patent Literature

[0004]

Non patent Literature 1: Zahid Amin, Echocardiographic
30 Predictors of Cardiac Erosion After Amplatzer Septal Occluder

Placement, Catheterization and Cardiovascular Interventions
(2014) 83:84-92

Non Patent Literature 2: Tadaaki Abe; Shinya Tsukano;
Yuko Tosaka, Pericardial tamponade due to erosion of a Figulla
5 Flex II device after closure of an atrial septal defect, Catheter
Cardiovasc Interv. (2019) 94:1003-1005.

Non Patent Literature 3: Masataka Kitano; Satoshi Yazaki;
Hisashi Sugiyama; Shin-ichi Ohtsuki; Hideshi Tomita, Risk Factors
and Predictors of Cardiac Erosion Discovered from 12 Japanese
10 Patients Who Developed Erosion After Atrial Septal Defect Closure
Using Amplatzer Septal Occluder, Pediatric Cardiology (2020)
41:297-308

Non Patent Literature 4: Preetham Kumar; James L.
Orford; Jonathan M. Tobis, Two cases of pericardial tamponade
15 due to nitinol wire fracture of a gore septal occluder, Catheter
Cardiovasc Interv. (2020) 96:219-224.

SUMMARY

[0005]

20 The use of the mesh structure limits a planar shape of the
closure device. This may make it difficult to properly close a hole
or duct, depending on a position and a shape of the hole or duct.

[0006]

For example, Non Patent Literatures 1 to 4 introduce
25 examples in which a hole of atrial septal defect is closed by using
an Amplatzer septal occluder (hereinafter referred to also as
ASO). The ASO comprises a mesh structure formed of woven
metal wires. Non Patent Literatures 1 to 3 report a mechanical
damage (referred to also as erosion), such as cardiac perforation
30 formed in a tissue, which is caused by contact with the ASO. Non

Patent Literature 4 reports that some of the metal wires in the mesh structure were damaged, which results in erosion. If breeding or the like occurs because of the erosion, there is a risk of cardiac tamponade. The cardiac tamponade is a state in which a heart is unable to sufficiently dilate due to increase in inner pressure of cardiac sac caused by increase in cardiac sac fluid.

[0007]

The object of the present disclosure is to provide a closure device and a closure system capable of effectively solving such a problem.

[0008]

An embodiment of the present disclosure is a closure system for closing a hole or duct in a tissue related to a cardiac disease, comprising:

a catheter having an internal diameter D1 [mm]; and

a closure device to be delivered to the hole or duct in the tissue through the catheter;

wherein:

the closure device comprises: a first plate including a first center part, and a first extension part extending around the first center part and containing a resin having elastic restorability; and a waist part connected to the first center part;

the elastic restorability is a property by which the first extension part returns from a state in which the first extension part is folded such that surface portions of the first extension part face to each other, to a state in which the first extension part is extended around the first center part;

the first extension part has a thickness A1 [mm];

the waist part has a maximum dimension T1 [mm] in a

plan view; and

the internal diameter $D1$ of the catheter is larger than $2 \times A1 + T1$.

[0009]

5 In the closure system according to the present disclosure, the first extension part may have a maximum dimension $B1$ [mm] in a plan view, and

$A1/B1$ may be $1/50$ or more.

[0010]

10 In the closure system according to the present disclosure, the first plate may include a base layer extending around the first center part and containing fluororesin, polyester, polyamide, urethane, silicone, or polyetherketone, and

a thickness of the base layer may be 50% or more of the
15 thickness $A1$ of the overall first plate.

[0011]

In the closure system according to the present disclosure, the first extension part may have a tensile strength between 20 MPa or more and 150 MPa or less.

20 [0012]

In the closure system according to the present disclosure, the first extension part may include, in a plan view, a first portion, and a second portion having a shape asymmetric to the first portion with respect to a center of the first center part.

25 [0013]

The closure system according to the present disclosure may comprise a second plate connected to the waist part, wherein

the second plate may comprise a second center part connected to the waist part, and a second extension part
30 extending around the second center part and containing a resin

having elastic restorability.

[0014]

In the closure system according to the present disclosure, the second extension part may have a thickness $A2$ [mm], and

5 the internal diameter $D1$ of the catheter may be larger than $2 \times A1 + 2 \times A2 + T1$.

[0015]

The closure system according to the present disclosure may comprise an IC chip embedded in the resin.

10 [0016]

In the closure system according to the present disclosure, the IC chip may include a power generating element that generates electric power using pulses of a heart.

[0017]

15 In the closure system according to the present disclosure, the first plate may comprise a surface layer containing a fluororesin.

[0018]

In the closure system according to the present disclosure, 20 the first plate may comprise a plurality of projections positioned on a contact surface facing the tissue.

[0019]

In the closure system according to the present disclosure, the first extension part may comprise a linearly running 25 reinforcement part.

[0020]

In the closure system according to the present disclosure, the cardiac disease may be atrial septal defect, ventricular septal defect, patent ductus arteriosus, or patent foramen ovale.

30 [0021]

The closure system according to the present disclosure may comprise a handle for operating the closure device.

[0022]

In the closure system according to the present disclosure,
5 the closure device may include a marker provided on the first plate, and

the handle may include a lever that controls a rotational angle of the first plate.

[0023]

10 An embodiment of the present disclosure is a manufacturing method of a closure device for closing a hole or duct in a tissue related to a cardiac disease, wherein:

the closure device comprises a first plate to cover the hole or duct;

15 the first plate comprises a first center part, and a first extension part extending around the first center part and containing a resin having elastic restorability;

the elastic restorability is a property by which the first extension part returns from a state in which the first extension
20 part is folded such that surface portions of the first extension part face to each other, to a state in which the first extension part is extended around the first center part;

the manufacturing method comprises a producing step that produces the closure device based on information on a shape
25 and a position of the hole or duct in the tissue; and

the producing step comprises a first plate designing step using a learning model that is trained with a training data in such a manner that the information on the shape and the position of the hole or duct in the tissue are inputted to the learning model,
30 and that the learning model outputs design information including

any of a planar shape, a thickness, and/or a material of the first extension part, wherein the training data includes shapes and positions of holes or ducts in tissues of patients having cardiac disease as input objects, and wherein the training data includes
5 design information including any of planar shapes, thicknesses, and/or materials of first extension parts as output values.

[0024]

In the manufacturing method according to the present disclosure, the producing step may comprise a first plate
10 producing step that produces the first plate by means of a 3D printer.

[0025]

In the manufacturing method according to the present disclosure, the first extension part may have a thickness A1 [mm]
15 and a maximum dimension B1 [mm] in a plan view, and A1/B1 may be 1/50 or more.

[0026]

In the manufacturing method according to the present disclosure, the first plate may contain fluororesin, polyester,
20 polyamide, urethane, silicone, or polyetherketone.

[0027]

In the manufacturing method according to the present disclosure, the closure device may comprise a waist part connected to the second center part, and a second plate
25 connected to the waist part,

the second plate may comprise a second center part connected to the waist part, and a second extension part extending around the second center part and containing a resin having elastic restorability, and

30 the producing step may comprise a second plate designing

step using a learning model that is trained with training data in such a manner that the information on the shape and the position of the hole or duct in the tissue are inputted to the learning model, and that the learning model outputs design information including
5 any of a planar shape, a thickness, and/or a material of the second extension part, wherein the training data includes shapes and positions of holes or ducts in tissues of patients having cardiac disease as input objects, and wherein the training data includes design information including any of planar shapes,
10 thicknesses, and/or materials of second extension parts as output values.

[0028]

The present disclosure can provide a closure device and a closure system capable of appropriately various holes or ducts.

15

BRIEF DESCRIPTION OF THE DRAWINGS

[0029]

Fig. 1 is a view showing an example in which a duct by an arterial duct is formed between an aorta and a pulmonary artery.

20 Fig. 2 is a view showing that the arterial duct of Fig. 1 is closed by a closure device.

Fig. 3 is a view showing an example of the closure device.

Fig. 4 is a view illustrating elastic restorability of the closure device.

25 Fig. 5 is a view showing a first plate seen from a non-contact surface side.

Fig. 6 is a sectional view of the first plate of Fig. 5 seen from a VI-VI direction.

30 Fig. 7 is a view showing examples of materials forming a base layer of the first plate.

Fig. 8 is a view showing examples of materials forming a fiber of the first plate.

Fig. 9 is a view showing examples of materials forming a second surface layer of the first plate.

5 Fig. 10 is a view showing an example of a manufacturing method of the closure device.

Fig. 11A is a view showing an example of a method of closing an arterial duct using the closure device.

10 Fig. 11B is a view showing the example of the method of closing the arterial duct using the closure device.

Fig. 11C is a view showing the example of the method of closing the arterial duct using the closure device.

Fig. 11D is a view showing the example of the method of closing the arterial duct using the closure device.

15 Fig. 12 is a view showing an example of a closure system.

Fig. 13 is a view showing an example of a heart including an atrial septum in which a hole is formed.

Fig. 14 is a view showing an example of the closure system.

20 Fig. 15 is a view showing that the hole in the atrial septum is closed by the closure device of Fig. 14.

Fig. 16 is a view illustrating dimensions of the closure device of Fig. 14.

Fig. 17A is a view showing an example of a method of closing a hole using the closure device.

25 Fig. 17B is a view showing the example of the method of closing the hole using the closure device.

Fig. 17C is a view showing the example of the method of closing the hole using the closure device.

30 Fig. 17D is a view showing the example of the method of closing the hole using the closure device.

Fig. 18 showing an example of a heart including an atrial septum in which a hole is formed.

Fig. 19 is a view showing an example of the closure device for closing the hole of Fig. 18.

5 Fig. 20 is a view showing that the hole in the atrial septum of Fig. 19 is closed by the closure device.

Fig. 21 is a view showing that a hole in an interventricular septum is closed by the closure device.

Fig. 22 is a view showing an example of the closure device.

10 Fig. 23 is a view showing an example of a handle for operating the closure device.

DESCRIPTION OF EMBODIMENTS

[0030]

15 A closure device according to the present disclosure is described in detail with reference to the drawings. An embodiment described below is a mere example, and the present disclosure is not construed as limited to the embodiment. In the drawings to which the reference is made in this embodiment, the same or similar reference numeral is given to parts that are
20 identical or have similar functions, and repeated description may be omitted. Dimensional proportions in the drawings may differ from actual proportions for the sake of explanation, and some components may be omitted from the drawings.

25 [0031] (Closure System)

Fig. 1 shows an example of a tissue related to a cardiac disease. In the example shown in Fig. 1, the cardiac disease is patent ductus arteriosus. The patent ductus arteriosus is a condition in which an arterial duct 73 connecting an aorta 71 and
30 a pulmonary artery 72 is not closed, so that the arterial duct 73

remains.

[0032]

Fig. 2 is a view showing that the arterial duct 73 of Fig. 1 is treated by a closure system 10. The closure system 10 comprises a catheter 11 to be inserted into a body, and a closure device 20 to be delivered through the catheter 11 to the arterial duct 73. The closure device 20 is configured to close the arterial duct 73.

[0033]

Fig. 3 is a view showing an example of the closure system 10. The closure system 10 may comprise a delivery cable 12 joined to the closure device 20. By moving the delivery cable 12 inside the catheter 11, the closure device 20 can be moved inside the catheter 11, and the closure device 20 can be pushed out from the closure device 20. After the closure device 20 has been attached to a tissue of a heart 1, the delivery cable 12 is detached from the closure device 20.

[0034]

The closure device 20, which is in a folded state, is inserted into the catheter 11, and is delivered to the arterial duct 73. After having been delivered to the arterial duct 73 or the aorta 71, the closure device 20 is pushed out from the catheter 11 by the delivery cable 12. After having been pushed out from the catheter 11, the closure device 20 can unfold and elastically restore to its extending state as shown in Fig. 3.

[0035] (Closure Device)

The closure device 20 is described in detail. The closure device 20 at least comprises a first plate 30 to cover the arterial duct 73. The closure device 20 may comprise a waist part 50 to be installed in the arterial duct 73. The waist part 50 may

include a joint 51 joined to the delivery cable 12. The joint 51 includes an opening into which the delivery cable 12 is inserted, for example. The opening of the joint 51 may have a structure for facilitating attachment to the delivery cable 12 and detachment from the delivery cable 12. For example, threads may be formed on a wall surface of the opening of the joint 51.

[0036] (First Plate)

The first plate 30 is described in detail. As shown in Fig. 3, the first plate 30 includes a contact surface 31 and a non-contact surface 32. The contact surface 31 is a surface that faces and contacts the tissue related to the cardiac disease. In this embodiment, the contact surface 31 faces and contacts a wall surface of the aorta 71. The non-contact surface 32 is a surface opposite the contact surface 31.

[0037]

A shape of the first plate 30 in a plan view is described. "Plan view" means that the closure device 20 is seen along a normal direction of the contact surface 31 or the non-contact surface 32. In the example shown in Fig. 3, the first plane 30 has a circular shape in a plan view. In the description below, a shape in a plan view is referred to as planar shape.

[0038]

As shown in Fig. 3, the first plate 30 includes a first center part 33, and a first extension part 34 extending around the first center part 33. The first center part 33 is connected to the waist part 50. The first center part 33 may be integral with the waist part 50. "Integral" means that there is no interface between two components. The first extension part 34 contains a resin having elastic restorability. The elastic restorability is a property by which the first extension part 34 returns from a state in which

the first extension part 34 is folded such that surface portions of the first extension part 34 face to each other, to a state in which the first extension part 34 is extended around the first center part 33. The first extension part 34 may be integral with the first center part 33.

[0039]

The elastic restorability is described with reference to Fig. 4.

First, as shown in the left side of Fig. 4, a force F_1 is applied to the first plate 30. Thus, the first extension part 34 is folded such that the contact surface 31 of a first portion 34a of the first extension part 34 and the contact surface 31 of a second portion 34b thereof face to each other. The second portion 34b is positioned on an opposite side of the first portion 34a with respect to a center of the first center part 33. In the example shown in Figs. 3 and 4, the first portion 34a is positioned below the first center part 33, and the second portion 34b is positioned above the first center part 33. A reference numeral S of Fig. 4 represents a distance between a distal end of the first portion 34a and a distal end of the second portion 34b in the folded state. The distance S is $B_1/3$, for example. B_1 is a maximum dimension of the contact surface 31 in a plan view. When the first plate 30 is circular, the maximum dimension B_1 is a diameter of the first plate 30, as shown in Fig. 3.

Following thereto, the force F_1 is removed from the first plate 30. Thus, as shown in the right side of Fig. 4, the first plate 30 unfolds and elastically restores to its extending shape. In Fig. 4, θ_1 represents an angle defined between a direction along which the first portion 34a unfolds and a direction along which the second portion 34b unfolds. In this patent application,

when the angle $\theta 1$ is between 135° or more and 225° or less, it can be said that the first extension part 34 has elastic restorability. The angle $\theta 1$ may be between 150° or more and 210° or less.

[0040]

5 As shown by a reference numeral L1 in Fig. 4, the direction along which the first portion 34a unfolds is defined by a direction along which the first portion 34a unfolds in a boundary between the first center part 33 and the first portion 34a. Similarly, as shown by a reference numeral L2 in Fig. 4, the direction along
10 which the second portion 34b unfolds is defined by a direction along which the second portion 34b unfolds in a boundary between the first center part 33 and the second portion 34b. The direction L1, the direction L2, and the angle $\theta 1$ are calculated by laterally imaging the first plate 30 and by analyzing an obtained
15 image.

[0041]

 The elastic restorability of the first extension part 34 can be realized by various methods. For example, the elastic restorability can be realized by appropriately setting a
20 relationship between a thickness A1 [mm] of the first extension part 34 and the maximum dimension B1 [mm] of the first extension part 34 in a plan view. A1/B1 is, for example, 1/50 or more, may be 1/30 or more, or may be 1/20 or more. On the other hand, the first plate 30 having an excessively large
25 thickness A1 is hard to fold, which makes it difficult to deliver the closure device 20 through the catheter 11. In consideration of this point, A1/B1 may be 1/3 or less, may be 1/5 or less, or may be 1/10 or less. As described below, the elastic restorability of the first extension part 34 may be realized based on a mechanical
30 property such as tensile strength.

[0042]

As shown in Fig. 4, in a state where the first plate 30 is extended, the waist part 50 has a maximum dimension T1 in a plan view. When the waist part 50 is circular in a plan view, the maximum dimension T1 is a diameter of the waist part 50.

[0043]

As shown in Fig. 3, a plurality of projections 31a may be formed on the contact surface 31 of the first plate 30. The provision of the projections 31a can increase a contact surface area of the contact surface 31 with the wall surface of the aorta 71. This can suppress detachment of the first plate 30 from the tissue. A height, a shape, a distribution density, etc., of the projections 31a are set to improve adhesiveness of the first plate 30 to the tissue, while avoiding damage which may be given by the projection 31a to the tissue. The height of the projection 31a is, for example, 10 μm or more, may be 100 μm or more, or may be 1mm or more. The height of the projection 31a is, for example, 20 mm or less, may be 10 mm or less, or may be 5 mm or less.

[0044]

In Figs. 3 and 4, a reference numeral 30e represents an outer edge of the first plate 30. The outer edge 30e is preferably free of hard material such as a metal. For example, the outer edge 30e is preferably formed of a resin such as a biocompatible material described below. This can suppress generation of erosion in the tissue, which may be caused by contact between the tissue and the outer edge 30e.

[0045]

In Figs. 3 and 4, a reference numeral 50e represents an outer circumferential surface of the waist part 50. The outer

circumferential surface 50e is preferably free of hard material such as a metal. For example, the outer circumferential surface 50e is preferably formed of a resin such as a biocompatible material described below. This can suppress generation of erosion in the tissue, which may be caused by contact between the tissue and the outer circumferential surface 50e.

[0046]

Next, a structure of the non-contact surface 32 of the first plate 30 is described. Fig. 5 is a view showing the first plate seen from the non-contact surface side. As shown in Fig. 5, a linearly running reinforcement part 35 may be formed on the non-contact surface 32. The reinforcement part 35 is raised from the non-contact surface 32. The provision of the reinforcement part 35 can improve the elastic restorability of the first extension part 34. Although not shown, the reinforcement part 35 may be formed on the contact surface 31.

[0047]

As shown in Fig. 5, the reinforcement part 35 may run from the first center part 33 toward the outer edge of the first plate 30. In other words, the reinforcement part 35 may run along a radial direction of the first plate 30. Although not shown, the reinforcement part 35 may run along another direction. For example, the reinforcement part 35 may run in a direction parallel to the outer edge of the first plate 30. In addition, the first plate 30 may include both the reinforcement part 35 running from the first center part 33 toward the outer edge of the first plate 30, and the reinforcement part 35 running in a direction parallel to the outer edge of the first plate 30.

[0048]

A width W1 of the reinforcement part 35 is, for example,

1 mm or more, may be 3 mm or more, or may be 5 mm or more. In addition, the width W1 of the reinforcement part 35 is, for example, 20 mm or less, may be 15 mm or less, or may be 10 mm or less.

5 [0049]

Next, a layer structure of the first plate 30 is described with reference to Fig. 6. The first plate 30 comprises at least a base layer 63. The base layer 63 is a layer that occupies most of the first extension part 34 of the first plate 30. A thickness of
10 the base layer 63 is, for example, 50% or more of the thickness A1 of the overall first plate 30, may be 60% or more, or may be 70% or more. The elastic restorability of the first extension part 34 mainly depends on a property of the base layer 63.

[0050]

15 The base layer 63 contains a biocompatible material having suitable elasticity. For example, the base layer 63 contains fluororesins, polyesters, polyamides, urethanes, silicones, polyetherketones, or other biocompatible polymers, and combinations thereof.

20 [0051]

Examples of fluororesins include polytetrafluoroethylene (PTFE), tetrafluoroethylene hexafluoropropylene copolymer (FEP), tetrafluoroethylene ethylene copolymer (ETFE), tetrafluoroethylene ethylene copolymer (PVDF), etc.

25 Examples of polyesters include polyethylene terephthalate, polyester-based elastomers (TPEE), etc. Elastomer is a material which is soft and fluid when heated, and returns to a rubbery state when cooled.

Examples of polyamides include PC12, polyamide
30 elastomers (TPAE), etc..

Urethanes are compounds with urethane bonds formed by reaction of alcohols and isocyanates. Examples of urethanes include polyurethane elastomers (TPU), etc..

Silicones are silicone rubber (SR), etc., for example.

5 Examples of polyetherketones include polyetheretherketone (PEEK), etc.

Fig. 7 shows examples of materials forming the base layer 63 and mechanical properties of the respective materials.

[0052]

10 As shown in Fig. 6, the first plate 30 may include a first surface layer 64 forming the contact surface 31. The first surface layer 64 may be stacked on the base layer 63. The first surface layer 64 may be formed of a biocompatible or biodegradable material. This can suppress elimination reaction
15 of a living body to the first plate 30. The first surface layer 64 may preferably contain fluororesin. This can improve the adhesiveness of the first plate 30 to the tissue.

[0053]

Examples of biocompatible materials are the following
20 biocompatible polymers.

ePTFE (porous material), fluororesin such as PTFE, polyamides, urethane-based polymers, PEEK

Examples of biodegradable materials are the following biodegradable polymers.

25 Lactide cabrolactan copolymers, ePTFE+ [collagen/extracellular matrix]

[0054]

As shown in Fig. 6, the first plate 30 may include a second surface layer 65 forming the non-contact surface 32. The second
30 surface layer 65 may be stacked on the base layer 63. The

second surface layer 65 is preferably formed such that a coefficient of friction between the second surface layer 65 and the catheter 11 is low. This allows the closure device 20 to be smoothly delivered inside the catheter 11.

5 [0055]

For example, the second surface layer 65 contains fluororesins, polyesters, polyamides, urethanes, or other biocompatible polymers, and combinations thereof.

[0056]

10 Examples of fluororesins include ePTFE, PTFE, FEP, ETFE, etc.

Examples of polyamides include PC12, polyamide elastomers (TPAE), etc.

15 Fig. 8 shows examples of materials forming the second surface layer 65 and mechanical properties of the respective materials.

[0057]

20 As shown in Fig. 6, the reinforcement part 35 may include a bundle of fibers 66. The fibers 66 run along a direction in which the reinforcement part 35 runs in a plan view. The fibers 66 are embedded in the base layer 63, for example.

[0058]

25 The fiber 66 preferably has a tensile strength higher than the base layer 63. Examples of the fibers 66 include carbon fibers, aramid fibers, polyparaphenylene benzobisoxazole, polyarylate, nylon, ultra high molecular weight polyethylene fibers, etc.

Fig. 9 shows examples of materials forming the fiber 66 and mechanical properties of the respective materials.

30 [0059]

A height H1 of the reinforcement part 35 is, for example, 1 mm or more, may be 3 mm or more, and may be 5 mm or more. In addition, the height H1 of the reinforcement part 35 is, for example, 20 mm or less, may be 15 mm or less, or may be 10 mm or less.

[0060]

Preferable mechanical properties of the first extension part 34 are described.

A tensile strength of the first extension part 34 is, for example, 20 MPa or more, may be 25 MPa or more, or may be 30 MPa or more. In addition, the tensile strength of the first extension part 34 is, for example, 150 MPa or less, may be 130 MPa or less, may be 100 MPa or less, or may be 80 MPa or less.

A tensile rupture strain of the first extension part 34 is, for example, 50% or more, may be 80% or more, may be 100% or more, or may be 150% or more. In addition, the tensile rupture strain of the first extension part 34 is, for example, 550% or less, may be 450% or less, may be 400% or less, or may be 300% or less.

The tensile strength and the tensile rupture strain of the first extension part 34 are measured in line with JIS K 7161. As shown by one-dot chain lines indicated by a reference numeral 30S in Fig. 5, for example, a measurement sample is obtained by cutting a portion of the first extension part 34 along a direction from the first center part 33 toward the outer edge of the first plate 30.

[0061]

A layer structure of the waist part 50 may be entirely the same as the layer structure of the first plate 30, may be partially the same, or may be different therefrom. For example, the waist

part 50 may include a layer integrally formed by the same material as that of the base layer 63 of the first plate 30.

[0062]

As shown in Fig. 6, the closure device 20 may comprise an
5 IC chip 36 embedded in the resin of the closure device 20. The IC chip 36 includes, for example, a MEMS.

The IC chip 36 has a sensor function, for example. For example, the IC chip 36 can function as a heart rate sensor that electrically measures pulses of the heart 1.

10 The IC chip 36 may have a radar function. For example, the IC chip 36 may include a transceiver that transmits and receives radio waves. This allows an object around the closure device 20 to be detected.

The IC chip 36 may have a function of detecting sound.
15 For example, the IC chip 36 may include a sound pickup microphone that detects sound, and a converter that converts detected sound to an electric signal.

Since the IC chip 36 is embedded in the resin, detachment of the IC chip 36 from the closure device 20 can be suppressed.
20 Data obtained by the IC chip 36 are transmitted to an external apparatus by wireless communication or the like.

[0063]

The IC chip 36 may include a power generating element 36a. The power generating element 36a generates electric
25 power using pulses of the heart 1, for example. The use of the power generating element 36a allows a continuous operation of the IC chip 36 over a long period of time.

[0064] (Manufacturing Method of Closure Device)

Next, a manufacturing method of the closure device 20 is
30 described with reference to Fig. 10. First, a measuring step S1

that measures a shape and a position of a hole or duct in a tissue related to a cardiac disease is performed. A shape and a position of the arterial duct 73 are measured by echo, etc., for example.

[0065]

5 Following thereto, a producing step that produces the closure device 20 is performed based on the information on the shape and the position of the arterial duct 73. The producing step may include a step of designing and producing a part of the closure device 20 in accordance with the measuring result of the
10 shape and the position of the arterial duct 73. For example, as shown in Fig. 10, the producing step may include a first plate designing step S2 and a first plate producing step S3. This can provide the closure device 20 comprising the first plate 30 which is more suited to individual cases of patients. A predetermined
15 design or a previously produced component may be used for a part of the closure device 20, which is less dependent on individual cases.

[0066]

 In the first plate designing step S2, design information of
20 the first extension part 34 may be generated based on a learning model. For example, the design information of the first extension part 34 can be obtained by inputting the shape and the position of the arterial duct 73, which are obtained in the measuring step S1, to a computer comprising a learning model.
25 The design information includes at least one of a planar shape, a thickness, and a material of the first extension part 34. The design information may include any two of the planar shape, the thickness, and the material of the first extension part 34. The design information may include the planar shape, the thickness,
30 and the material of the first extension part 34.

[0067]

A learning model of the first plate 30 can be obtained by means of a computer trained by a training data. The training data includes shapes and positions of holes or ducts in tissues of patients having cardiac disease as input objects. The training data includes the aforementioned design information of the first extension part 34 as output values. Input to the learning model may further include other information such as an inner diameter of the catheter 11, a coefficient of friction of the catheter 11, etc.

[0068]

Input to the computer comprising the learning model may include physical characteristics of a patient, such as a height, a weight, etc. Input to the computer comprising the learning model may include information such as patient's age, gender, etc. The computer may output the design information based on prediction of future changes that may occur in a tissue such as a heart. For example, when a patient is determined as a child from the input information, the computer may output the design information based on prediction of growth that may occur in a tissue of a heart, etc. This allows the closure device 20 to properly function after the patient has grown.

[0069]

The first plate producing step S3 may produce the first plate 30 by means of a 3D printer. This allows the closure device 20 to be quickly produced based on the information obtained in the measuring step S1.

[0070]

The producing step may include a waist part designing step and a waist part producing step. Similarly to the first plate designing step S2, the waist part designing step may generate

design information of the waist part 50 based on a learning model. In this case, the learning model may use, as an input, information on a thickness in the tissue of the aorta 71, etc. Similarly to the first plate producing step S3, the waist part producing step may
5 produce the waist part 50 by means of a 3D printer.

[0071]

In a treatment, such as ASO, which uses a conventional closure device, a closure device suited to a patient is selected depending on a shape of a cardiac disease of a patient. For
10 example, suppose that lineups of a conventional closure device prepare closure devices every 1 mm in diameter. When a diameter of a hole of a cardiac disease is 19.3 mm, a closure device having a diameter of 20 mm is used. Namely, a ready-made closure device is used. This may result in erosion because
15 of the excessive dimension of the closure device.

[0072]

On the other hand, when the closure device 20 is produced by means of a 3D printer, the closure device 20 can have a shape corresponding to a shape of a cardiac disease of a patient.
20 Namely, a custom-made closure device 20 can be provided. Thus, there is less possibility that the closure device 20 has an excessive dimension. This can suppress a problem such as erosion. A resolution of a 3D printer is, for example, 500 μm or less. Thus, the dimension of the closure device 20 can have an
25 accuracy of 500 μm . The resolution of a 3D printer may be 300 μm or less, may be 100 μm or less, or may be 50 μm or less.

[0073]

The producing step such as the first plate designing step may be realized by a software running on a computer. By
30 installing a program in a computer, for example, the computer

may execute the first plate designing step using a learning model.

[0074]

The program may be pre-installed on a computer when the computer is shipped. Alternatively, the program may be
5 installed on the computer after it has been shipped by using a computer readable non-transitory storage medium in which the program is stored. A type of the storage medium is not particularly limited, and various types may be considered. Namely, the storage medium may be a portable storage medium
10 such as a magnetic disk or an optical disk, a fixed storage medium such as a hard disk and a memory, etc. The program may be distributed via a communication line such as an internet. When the program is distributed via a communication line, a storage medium storing the program according to this embodiment is at
15 least temporarily present on a server for distribution.

[0075] (Using Method of Closure Device)

Next, a using method of the closure device 20 is described with reference to Figs. 11A to 11D.

[0076]

20 First, the catheter 11 is inserted into a body. Then, as shown in Fig. 11A, the catheter 11 is moved until the distal end of the catheter 11 reaches the aorta 71 through the arterial duct 73. In addition, the delivery cable 12 is attached to the waist part 50 of the closure device 20, and the closure device 20 is
25 inserted into the catheter 11. Then, as shown in Fig. 11A, the closure device 20 is moved closer to the distal end of the catheter 11. The closure device 20 is positioned inside the catheter 11, with at least the first plate 30 being folded.

[0077]

30 As shown in Fig. 11A, when the closure device 20 is

positioned inside the catheter 11, the waist part 50 may be compressed in the radial direction by a force received from the inner wall of the catheter 11. The compressed waist part 50 has a dimension smaller than the internal diameter of the catheter 11 in the radial direction. The radial direction means a direction from the first center part 33 toward the outer edge of the first extension part 34, in a state where the first extension part 34 is extended around the first center part 33. After having been taken out from the catheter 11, the waist part 50 preferably has a dimension larger than the internal diameter of the catheter 11 in the radial direction.

[0078]

As shown in Fig. 11B, the closure device 20 is further moved so that the first plate 30 of the closure device 20 is pushed out from the catheter 11. Then, as shown in Fig. 11C, the first extension part 34 elastically restores, i.e., unfolds to extend around the first center part 33. Since the waist part 50 is released from the force received from the catheter 11, it can expand in the radial direction.

[0079]

Following thereto, as shown in Fig. 11D, the delivery cable 12 is retracted so that the contact surface 31 of the first plate 30 comes into contact with the wall surface of the aorta 71. The waist part 50 also comes into contact with the wall surface of the arterial duct 73. Thus, the arterial duct 73 can be closed. Thereafter, the delivery cable 12 is detached from the closure device 20. In addition, the catheter 11 together with the delivery cable 12 is pulled out from the body.

[0080] (Effect of Embodiment)

In this embodiment, the first plate 30 of the closure device

20 comprises the first extension part 34 containing a resin having elastic restorability. Thus, the first plate 30 of the closure device 20, which is delivered in the folded state, can elastically restore to its extending shape. Thus, the first plate 30 can close the
5 arterial duct 73. As compared with the use of a conventional mesh structure, the first plate 30 has a higher degree of freedom in the planar shape, and is easy to manufacture. For example, the first plate 30 having a desired shape can be quickly produced by means of a 3D printer. Thus, the first plate 30 suited for
10 various shapes of the arterial duct 73 can be easily provided. This can suppress generation of erosion, which may be caused by an excessive dimension of the closure device 20.

[0081]

This embodiment can close a cardiac disease of the arterial
15 duct 73 or the like without using a mesh structure made of metal wires. Since the closure device 20 includes no mesh structure, generation of erosion, which may be caused by damaged metal wire, can be suppressed.

[0082]

20 By suppressing erosion, dangerous conditions such as cardiac tamponade can be suppressed.

[0083]

The above embodiment can be variously modified. Modification examples are described below, with reference to the
25 drawings according to need. In the following description and the drawings used in the following description, the same reference numeral as that used for the part that can be structure in the same way as in the above embodiment, and redundant description is omitted. In addition, when the effect obtained in
30 the above embodiment is obtained in the modification examples,

its description may be omitted.

[0084] (Modification Example of Closure System)

Fig. 12 is a view showing an example of the closure system 10. The catheter 11 has an internal diameter D1 [mm]. The internal diameter D1 may be larger than $2 \times A1 + T1$. A1 is a thickness of the first extension part 34 of the first plate 30. T1 is a maximum dimension of the waist part 50 in a plan view. When the internal diameter D1 is larger than $2 \times A1 + T1$, compression of the waist part 50 in the radial direction of the catheter 11 can be suppressed. This can reduce a frictional force between the inner wall of the catheter 11 and the closure device 20, whereby the closure device 20 can be easily moved inside the catheter 11. This allows the closure device 20 to be delivered quickly to the tissue of the body.

15 [0085] (Modification Example of Cardiac Disease)

The above embodiment shows the example in which the patent ductus arteriosus is treated using the closure device 20. However, the cardiac disease in which the closure device 20 is used is not limited to the patent ductus arteriosus. For example, another cardiac disease, such as atrial septal defect, ventricular septal defect, patent foramen ovale, etc., may be treated using the closure device 20. Fig. 13 is a view showing an example of a cardiac disease of the heart 1.

[0086]

25 The heart 1 includes a left atrium 2, a right atrium 3, an atrial septum 4, a left ventricle 5, a right ventricle 6, and an interventricular septum 7, which are positioned inside an atrial wall 1a. The atrial septum 4 is positioned between the left atrium 2 and the right atrium 3. The interventricular septum 7 is positioned between the left ventricle 5 and the right ventricle

30

6. In the example shown in Fig. 13, the atrial septum 4 has a hole 4a. Namely, the cardiac disease of the heart 1 is ventricular septal defect.

[0087]

5 Fig. 14 is a view showing an example of the closure device 20. As shown in Fig. 14, the closure device 20 may comprise, in addition to the first plate 30 and the waist part 50, a second plate 40 connected to the waist part 50. The second plate 40 is arranged inside the heart 1 such that the hole 4a of the atrial
10 septum 4 is sandwiched between the second plate 40 and the first plate 30. Fig. 15 is a view showing that the hole 4a of the atrial septum 4 is closed by the closure device 20 of Fig. 14.

[0088]

 As shown in Fig. 14, the second plate 40 includes a contact
15 surface 41 and a non-contact surface 42. The contact surface 41 faces the contact surface 31 of the first plate 30. The contact surface 41 may contact the atrial septum 4. The non-contact surface 42 is a surface opposite the contact surface 41.

[0089]

20 As shown in Fig. 14, the second plate 40 has a second center part 43, and a second extension part 44 extending around the second center part 43. The second center part 43 is connected to the waist part 50. The second center part 43 may be integral with the waist part 50. The second extension part 44
25 may be integral with the second center part 43.

[0090]

 Similarly to the first extension part 34, the second extension part 44 contains a resin having elastic restorability. Thus, the second extension part 44 can return from a state in
30 which the second extension part 44 is folded such that surface

portions of the second extension part 44 face to each other, to a state in which the second extension part 44 is extended around the second center part 43.

[0091]

5 Fig. 16 is a view illustrating dimensions of the closure device 20 of Fig. 14. The second extension part 44 has a thickness $A2$ [mm]. The second extension part 44 has a maximum dimension $B2$ [mm] in a plan view. When the second plate 40 is circular, the maximum dimension $B2$ is a diameter of
10 the second plate 40. $A2/B2$ is, for example, $1/50$ or more, may be $1/30$ or more, or may be $1/20$ or more. $A2/B2$ may be $1/3$ or less, may be $1/5$ or less, or may be $1/10$ or less.

[0092]

 An outer edge 40e of the second plate 40 is preferably free
15 of hard material such as a metal. For example, the outer edge 40e is preferably formed of a resin such as the aforementioned biocompatible material. This can suppress generation of erosion in the tissue, which may be caused by contact between the tissue and the outer edge 40e.

20 [0093]

 A layer structure of the second extension part 44 may be similar to the layer structure of the first extension part 34. For example, the second extension part 44 comprises at least the aforementioned base layer 63. The second extension part 44
25 may include the aforementioned first surface layer 64 forming the contact surface 41. In addition, the second extension part 44 may include the aforementioned second surface layer 65 forming the non-contact surface 42.

[0094]

30 Since preferable mechanical properties of the second

extension part 44 are similar to those of the first extension part 34, description is omitted.

[0095]

Next, a manufacturing method of the closure device 20 of
5 Fig. 14 is described. Also in this modification example, a measuring step S1 that measures a shape and a position of the hole 4a in the tissue is performed. At this time, a thickness of the tissue, e.g., a thickness of the atrial septum 4 may further be measured.

10 [0096]

Following thereto, a producing step that produces the closure device 20 is performed based on the information on the shape and the position of the hole 4a. The producing step may include the aforementioned first plate designing step S2 and the
15 first plate producing step S3. In addition, the producing step may include a second plate designing step and a second plate producing step.

[0097]

Similarly to the first plate designing step S2, the second
20 plate designing step may generate design information of the second extension part 44 based on a learning model. For example, the design information of the second extension part 44 can be obtained by inputting the shape and the position of the arterial duct 73, which are obtained in the measuring step S1, to
25 a computer comprising a learning model. The design information includes at least one of a planar shape, a thickness, and a material of the second extension part 44. The design information may include any two of the planar shape, the thickness, and the material of the second extension part 44. The
30 design information may include the planar shape, the thickness,

and the material of the second extension part 44.

[0098]

A learning model of the second plate 40 can be obtained by means of a computer trained by a training data. The training
5 data includes shapes and positions of holes or ducts in tissues of patients having cardiac disease as input objects. The training data includes the aforementioned design information of the second extension part 44 as output values. Input to the learning
10 model may further include other information such as an inner diameter of the catheter 11, a coefficient of friction of the catheter 11, etc.

[0099]

Similarly to the first plate producing step S3, the second plate producing step may produce the second plate 40 by means
15 of a 3D printer.

[0100]

The producing step may include a waist part designing step and a waist part producing step. Similarly to the first plate designing step S2, the waist part designing step may generate
20 design information of the waist part 50 based on a learning model. In this case, the learning model may use, as an input, information of a thickness of the tissue such as the atrial septum 4. Similarly to the first plate producing step S3, the waist part producing step may produce the waist part 50 by means of a 3D printer.

25 [0101]

Next, a using method of the closure device 20 of Fig. 14 is described with reference to Figs. 17A to 17D.

[0102]

First, the catheter 11 is inserted from a blood vessel at the
30 base of a leg. Then, as shown in Fig. 17A, the catheter 11 is

moved until the distal end of the catheter 11 reaches the left atrium 2 through the hole 4a of the atrial septum 4. In addition, the delivery cable 12 is attached to the waist part 50 of the closure device 20, and the closure device 20 is inserted into the catheter 11. Then, as shown in Fig. 17A, the closure device 20 is moved closer to the distal end of the catheter 11. The closure device 20 is positioned inside the catheter 11, with the first plate 30 and the second plate 40 being folded.

[0103]

The internal diameter D1 of the catheter 11 may be larger than $2 \times A1 + 2 \times A2 + T1$. A1 is a thickness of the first extension part 34 of the first plate 30. A2 is a thickness of the second extension part 44 of the second plate 40. T1 is a maximum dimension of the waist part 50 in a plan view. When the internal diameter D1 is larger than $2 \times A1 + 2 \times A2 + T1$, compression of the waist part 50 in the radial direction of the catheter 11 can be suppressed. This can reduce a frictional force between the inner wall of the catheter 11 and the closure device 20, whereby the closure device 20 can be easily moved inside the catheter 11.

[0104]

As shown in Fig. 17B, the closure device 20 is further moved so that the first plate 30 of the closure device 20 is pushed out from the catheter 11. Then, as shown in Fig. 17C, the extension part 34 elastically restores, i.e., unfolds to extend around the first center part 33.

[0105]

Following thereto, as shown in Fig. 17C, the delivery cable 12 is retracted so that the contact surface 31 of the first plate 30 comes into contact with the atrial septum 4. Then, the catheter 11 is retracted so that the second plate 40 is discharged from the

catheter 11. Then, as shown in Fig. 17D, the second extension part 44 elastically restores, i.e., unfolds to extend around the second center part 43. Thus, the atrial septum 4 can be sandwiched between the first plate 30 and the second plate 40.

- 5 This can more securely close the hole 4a in the atrial septum 4. In addition, detachment of the closure device 20 from the tissue can be suppressed.

[0106]

- As compared with the use of a conventional mesh structure,
 10 the closure device 20 in this modification example also has a higher degree of freedom in the planar shape, and is easy to manufacture. For example, the first plate 30 and the second plate 40 each having a desired shape can be quickly produced by means of a 3D printer. Thus, the first plate 30 and the second
 15 plate 40 which are suited for various shapes of the hole 4a of the atrial septum 4 can be easily provided. This can suppress generation of erosion, which may be caused by an excessive dimension of the closure device 20. In addition, since the closure device 20 includes no mesh structure, generation of
 20 erosion, which may be caused by damaged metal wire, can be suppressed.

[0107] (Modification Example of Closure System)

- When the closure device 20 is positioned inside the catheter 11, the waist part 50 of the closure device 20 comprising
 25 the first plate 30 and the second plate 40 may be compressed in the radial direction, although not shown. Namely, the internal diameter D1 of the catheter 11 may be smaller than $2 \times A1 + 2 \times A2 + T1$. In this case, similarly to the example shown in Fig. 11D, after having been pushed out from the catheter 11, the
 30 waist part 50 of the closure device 20 may be in contact with the

wall surface of the hole 4a.

[0108] (Modification Example of Hole Position)

An example in which the hole 4a is positioned close to the atrial wall 1a, as shown in Fig. 18, is described. When a
5 conventional closure device formed of a mesh structure is used, a part of the closure device contacts the atrial wall 1a. Thus, there is a possibility that the closure device cannot appropriately close the hole 4a.

[0109]

10 On the other hand, since the first plate 30 has a high degree of freedom in the planar shape, this patent application can provide a closure device 20 as shown in Fig. 19, for example. In the example shown in Fig. 19, the first extension part 34 of the first plate 30 has a first portion 34a, and a second portion 34b
15 having a shape asymmetric to the first portion 34a with respect to a center of the first center part 33. For example, the first portion 34a is semicircular, while the second portion 34b has a shape obtained by cutting a part of a semicircular arc along a line parallel to the diameter. By machining the second portion 34b
20 in this manner, contact between the first plate 30 and the atrial wall 1a of the heart 1 can be suppressed, as shown in Fig. 20. Thus, the closure device 20 can appropriately close the hole 4a. By suppressing contact with the atrial wall 1a, generation of erosion in the atrial wall 1a can be suppressed.

25 [0110]

In Fig. 19, reference numerals R1 and R2 respectively represent a dimension of the first portion 34a and a dimension of the second portion 34b in a direction along which they are arranged side by side. The dimension R2 of the second portion
30 34b is smaller than the dimension R1 of the first portion 34a.

The dimension R2 is, for example, 9/10 or less of the dimension R1, may be 8/10 or less, or may be 7/10 or less.

[0111]

Similarly to the first plate 30, the second plate 40 has a high degree of freedom in the planar shape. As shown in Fig. 19, the second extension part 44 of the second plate 40 may include a third portion 44a, and a fourth portion 44b having a shape asymmetric to the first portion 44a with respect to a center of the second center part 43. For example, the third portion 44a is semicircular, while the fourth portion 44b has a shape obtained by cutting a part of a semicircular arc along a line parallel to the diameter. By machining the fourth portion 44b in this manner, contact between the second plate 40 and the atrial wall 1a of the heart 1 can be suppressed, as shown in Fig. 20. Thus, the closure device 20 can appropriately close the hole 4a. By suppressing contact with the atrial wall 1a, generation of erosion in the atrial wall 1a can be suppressed.

[0112] (Modification Example of Manufacturing Method of Closure Device)

Although the above embodiment shows the example in which the closure device 20 is designed based on a learning model, the closure device 20 may be designed using another method. For example, a person may design the closure device 20 based on experience.

[0113]

In addition, although the above embodiment shows the example in which the closure device 20 is produced by means of a 3D printer, the closure device 20 may be produced using another method. For example, the closure device 20 may be produced by a molding method such as sheet molding.

[0114] (Modification Example of Cardiac Disease)

The above embodiment shows the example in which the ventricular septal defect is treated using the closure device 20. However, the cardiac disease in which the closure device 20 is used is not limited to the ventricular septal defect. For example, another cardiac disease, such as atrial septal defect, patent ductus arteriosus, patent foramen ovale, etc., may be treated using the closure device 20. Fig. 21 is a view showing an example in which a hole 7a in the interventricular septum 7 is closed using the closure device 20.

[0115] (Modification Example of Closure Device)

Fig. 22 is a view showing an example of the closure device 20. The first plate 30 does not have rotational symmetry. For example, similarly to the example of Fig. 19, the closure device 20 has a first portion 34a, and a second portion 34b having a shape asymmetric to the first portion 34a with respect to the center of the first center part 33. In this case, in order to appropriately close a hole or duct of a cardiac disease, it is necessary to control positions of the first portion 34a and the second portion 34b. In order to appropriately perform the control, it is necessary to monitor the positions of the first portion 34a and the second portion 34b, while the closure device 20 is being inserted in a body.

[0116]

In this modification example, the first plate 30 includes a first marker 38. The first marker 38 is positioned on the first portion 34a, for example. While the closure device 20 is being inserted in the body, the position of the first portion 34a can be determined by detecting the first marker 38 by means of echo or the like. Thus, a rotational angle of the first plate 30 can be

calculated, for example.

[0117]

The first marker 38 can have any structure, as long as the position of the marker 38 can be detected from outside the body
5 by an inspection method such as echo. For example, the first marker 38 may have a structure raised from a surface of the first plate 30. Alternatively, the first marker 38 may have a structure recessed from the surface of the first plate 30. The first marker 38 may contain a material, such as a metal, which is different
10 from that of an element surrounding the first marker 38.

[0118]

Fig. 23 is a view showing an example of a handle 80 for operating the closure device 20. The handle 80 includes a lever 81 for controlling a rotational angle of the closure device 20. For
15 example, by moving the lever 81 in a rotational direction A, the closure device 20 can be rotated in a rotational direction B. A rotational angle of the closure device 20 can be controlled by operating the lever 81 while monitoring a rotational angle of the closure device 20 by means of the marker 38.

20 [0119]

Any driving mechanism for rotating the closure device 20 will do. For example, the closure device 20 may be rotated by rotating the delivery cable 12 or the catheter 11.

[0120]

25 Although not shown, the closure device 20 may include a plurality of markers.

For example, the first plate 30 may include, in addition to the first marker 38 positioned on the first portion 34a, a second marker positioned on the second portion 34b. The first marker
30 38 and the second marker may be different from each other in

shape, dimension, material, etc.

Alternatively, the first plate 30 may include 12 markers that are equidistantly arranged along a circumference, similarly to hour marks on a clock.

5 [0121]

Fig. 22 shows the example in which the first marker 38 is positioned on the contact surface 31 of the first plate 30. However, the position of the first marker 38 is not limited thereto, and the first marker 38 may be positioned on the non-contact
10 surface 32 of the first plate 30. The first marker 38 may be positioned on the contact surface 41 or the non-contact surface 42 of the second plate 40.

[0122]

Although not shown, an IC chip, a microactuator, a marker,
15 etc., may be provided on a component of the closure system 10, which is other than the closure device 20. For example, the catheter 11, the delivery cable 12, etc., may include an IC chip, a microactuator, a marker, etc.

[0123] (Modification Example of Using Method of Closure
20 Device)

The above embodiment shows the example in which the closure device 20 is delivered into the heart 1 through the catheter 11. However, the means for delivering the closure device 20 to the heart 1 is not limited to the catheter 11. For
25 example, the heart 1 may be surgically cut, and the closure device 20 may be delivered into the heart 1 through an incision. In this case, the closure device 20 may be sutured to the tissue using a thread and a needle.

In this modification example, since the first extension part
30 34 has the elastic restorability, the closure device 20 can be

passed through the incision, with the first extension part 34 being in the folded state. In addition, the first extension part 34 can be easily adhered to the tissue by means of the elasticity of the first extension part 34. In addition, since the first extension part 34 has high degree of freedom in the planar shape, a hole or duct in a tissue related to a cardiac disease can be appropriately closed.

[0124]

Some modification examples on the above embodiment have been described, it goes without saying that the modification examples can be suitably combined and applied.

[0125]

- 1 Heart
- 1a Atrial wall
- 2 Left atrium
- 15 3 Right atrium
- 4 Atrial septum
- 4a Hole
- 5 Left ventricle
- 6 Right ventricle
- 20 7 Interventricular septum
- 7a Hole
- 8 Lower great vein
- 10 Closure system
- 11 Catheter
- 25 12 Delivery cable
- 20 Closure device
- 30 First plate
- 31 Contact surface
- 31a Projection
- 30 32 Non-contact surface

	33	First center part
	34	First extension part
	34a	First portion
	34b	Second portion
5	35	Reinforcement part
	36	IC chip
	36a	Power generating element
	38	Marker
	40	Second plate
10	41	Contact surface
	42	Non-contact surface
	43	Second center part
	44	Second extension part
	50	Waist part
15	51	Joint
	63	Base layer
	64	First surface layer
	65	Second surface layer
	66	Fiber
20	71	Aorta
	72	Pulmonary artery
	73	Arterial duct
	80	Handle
	81	Lever
25		

CLAIMS

1. A closure system for closing a hole or duct in a tissue related to a cardiac disease, comprising:

a catheter having an internal diameter D1 [mm]; and

a closure device to be delivered to the hole or duct in the tissue through the catheter;

wherein:

the closure device comprises: a first plate including a first center part, and a first extension part extending around the first center part and containing a resin having elastic restorability; and a waist part connected to the first center part;

the elastic restorability is a property by which the first extension part returns from a state in which the first extension part is folded such that surface portions of the first extension part face to each other, to a state in which the first extension part is extended around the first center part;

the first extension part has a thickness A1 [mm];

the waist part has a maximum dimension T1 [mm] in a plan view; and

the internal diameter D1 of the catheter is larger than $2 \times A1 + T1$.

2. The closure system according to claim 1, wherein

the first extension part has a maximum dimension B1 [mm] in a plan view, and

$A1/B1$ is 1/50 or more.

3. The closure system according to claim 1 or 2, wherein

the first plate includes a base layer extending around the first center part and containing fluoro-resin, polyester, polyamide, urethane, silicone, or polyetherketone, and

a thickness of the base layer is 50% or more of the thickness A1 of the overall first plate.

4. The closure system according to any one of claims 1 to 3, wherein

the first extension part has a tensile strength between 20 MPa or more and 150 MPa or less.

5. The closure system according to any one of claims 1 to 4, wherein

the first extension part includes, in a plan view, a first portion, and a second portion having a shape asymmetric to the first portion with respect to a center of the first center part.

6. The closure system according to any one of claims 1 to 5, comprising a second plate connected to the waist part, wherein

the second plate comprises a second center part connected to the waist part, and a second extension part extending around the second center part and containing a resin having elastic restorability.

7. The closure system according to claim 6, wherein

the second extension part has a thickness A2 [mm], and

the internal diameter D1 of the catheter is larger than $2 \times A1 + 2 \times A2 + T1$.

8. The closure system according to any one of claims 1 to 7,

comprising an IC chip embedded in the resin.

9. The closure system according to claim 8, wherein
the IC chip includes a power generating element that generates electric power using pulses of a heart.
10. The closure system according to any one of claims 1 to 9, wherein
the first plate comprises a surface layer containing a fluororesin.
11. The closure system according to any one of claims 1 to 10, wherein
the first plate comprises a plurality of projections positioned on a contact surface facing the tissue.
12. The closure system according to any one of claims 1 to 11, wherein
the first extension part comprises a linearly running reinforcement part.
13. The closure system according to any one of claims 1 to 12, wherein
the cardiac disease is atrial septal defect, ventricular septal defect, patent ductus arteriosus, or patent foramen ovale.
14. The closure system according to any one of claims 1 to 13, comprising a handle for operating the closure device.
15. The closure system according to claim 14, wherein

the closure device includes a marker provided on the first plate, and

the handle includes a lever that controls a rotational angle of the first plate.

16. A manufacturing method of a closure device for closing a hole or duct in a tissue related to a cardiac disease, wherein:

the closure device comprises a first plate to cover the hole or duct;

the first plate comprises a first center part, and a first extension part extending around the first center part and containing a resin having elastic restorability;

the elastic restorability is a property by which the first extension part returns from a state in which the first extension part is folded such that surface portions of the first extension part face to each other, to a state in which the first extension part is extended around the first center part;

the manufacturing method comprises a producing step that produces the closure device based on information on a shape and a position of the hole or duct in the tissue; and

the producing step comprises a first plate designing step using a learning model that is trained with a training data in such a manner that the information on the shape and the position of the hole or duct in the tissue are inputted to the learning model, and that the learning model outputs design information including any of a planar shape, a thickness, and/or a material of the first extension part, wherein the training data includes shapes and positions of holes or ducts in tissues of patients having cardiac disease as input objects, and wherein the training data includes design information including any of planar shapes, thicknesses,

and/or materials of first extension parts as output values.

17. The manufacturing method according to claim 16, wherein the producing step comprises a first plate producing step that produces the first plate by means of a 3D printer.

18. The manufacturing method according to claim 16 or 17, wherein

the first extension part has a thickness $A1$ [mm] and a maximum dimension $B1$ [mm] in a plan view, and $A1/B1$ is $1/50$ or more.

19. The manufacturing method according to any one of claims 16 to 18, wherein

the first plate contains fluororesin, polyester, polyamide, urethane, silicone, or polyetherketone.

20. The manufacturing method according to any one of claims 16 to 19, wherein

the closure device comprises a waist part connected to the second center part, and a second plate connected to the waist part,

the second plate comprises a second center part connected to the waist part, and a second extension part extending around the second center part and containing a resin having elastic restorability, and

the producing step comprises a second plate designing step using a learning model that is trained with a training data in such a manner that the information on the shape and the position of the hole or duct in the tissue are inputted to the learning model,

and that the learning model outputs design information including any of a planar shape, a thickness, and/or a material of the second extension part, wherein the training data includes shapes and positions of holes or ducts in tissues of patients having cardiac disease as input objects, and wherein the training data includes design information including any of planar shapes, thicknesses, and/or materials of second extension parts as output values.