

DESCRIPTION

Alpha-Tricalcium Phosphate Ceramic and Production
Method Thereof

5 TECHNICAL FIELD

The present invention relates to an α -tricalcium phosphate ceramic having a superior biocompatibility for use mainly as a bone filler and a method for producing the same.

10 BACKGROUND ART

In the past, hydroxyapatite and β -tricalcium phosphate have been known as ceramics for use as bone fillers. These ceramics are known to be bioactive materials and can bond directly with a natural bone. In general, when these materials are implanted in bone, a thin layer of bioapatite forms in the body at the interface between the bone and the materials. A new bone is said to be formed starting from this point. That is, after bioapatite is formed at the surface of the materials, it is believed that the materials are not dissolved or absorbed much at all. In fact, these materials have slow rates of absorption into the body and are never completely replaced by a new bone.

On the other hand, α -tricalcium phosphate is said not to exhibit formation of a bioapatite layer at the interface of the bone with the material, has a faster rate of absorption in the body compared with hydroxyapatite and β -tricalcium phosphate, and has an extremely high ability to form a new bone. The ideal bone filler should have a high bone-forming ability and should completely disappear and be completely replaced by bone. For a long time, it has been thought that if production of a shaped article made of α -tricalcium phosphate were possible, it could be an extremely favorable bone filler. However, α -tricalcium phosphate has been difficult to fabricate as a ceramic up to now due to the difficulty of formation by a wet method, the

unavoidable formation of cracks at the time of sintering, and other reasons.

DISCLOSURE OF INVENTION

Accordingly, the objects of the present invention
5 are to provide a high purity α -tricalcium phosphate ceramic and a method for producing an α -tricalcium phosphate ceramic, which is expected to use as a material for an ideal bone filler.

In accordance with the present invention, there is
10 provided a method for producing an α -tricalcium phosphate ceramic comprising the steps of: sintering the shaped powder after shaping a powder material under pressure, or simultaneously with the shaping under pressure; and, further cooling the sintered product.

15 In accordance with the present invention, there is also provided a method for producing an α -tricalcium phosphate ceramic comprising the steps of: shaping a powder material prepared by a wet method using the monoaxial press method or CIP method (i.e., cold
20 isostatic pressing method); sintering the shaped powder material at a temperature of 1100 to 1500°C for 1 to 200 hours; and, further cooling the sintered product at a cooling rate of 100 to 2000°C/hrs.

In accordance with the present invention, there is
25 further provided a method for producing an α -tricalcium phosphate ceramic comprising the step of: sintering a powder material prepared by a wet method using a hot press method or HIP method (i.e., hot isostatic pressing method) at a temperature of 200 to 1500°C for 1 to
30 200 hours.

BRIEF DESCRIPTION OF DRAWINGS

The present invention will be further explained in detail with reference to the accompanying drawings.

Fig. 1 is a graph showing the relationship between
35 the sintering temperature and the relative density (Example 3);

Fig. 2 is a photograph of a non-decalcified sample

(implanted 3 months) of an α -tricalcium phosphate ceramic when implanted in the femur of an osteophoresis model rat (Example 4); and

5 Fig. 3 is a photograph of a non-decalcified sample (implanted 3 months) of a hydroxyapatite ceramic when implanted in the femur of an osteophoresis model rat (Example 4).

BEST MODE FOR CARRYING OUT THE INVENTION

10 The method for producing an α -tricalcium phosphate ceramic according to the present invention will now be explained in detail below.

The α -tricalcium phosphate in the present invention is the high temperature stable phase of tricalcium phosphate and is expressed in chemical composition as
15 $\text{Ca}_3(\text{PO}_4)_2$. Tricalcium phosphate has β -phase (low temperature phase), γ -phase (high pressure phase), and α -phase (high temperature phase), which are the same in composition. The stable region of the α -phase is 1125 to 1500°C.

20 The method of production of a dense ceramic of α -tricalcium phosphate is as follows. As an example of the wet method, an aqueous solution of phosphoric acid is gradually added dropwise to, for example, a 0.5M suspension of calcium hydroxide. This is stirred and a
25 uniform reaction is caused to obtain amorphous tricalcium phosphate. This amorphous tricalcium phosphate is filtered, then dried at, for example, 60°C, then pulverized by a kneader. The resultant powder is provisionally sintered at a temperature of 600 to 1200°C
30 is homogeneously mixed with a thickening agent, then is shaped using a press at a pressure of 50 to 200 MPa. Note that during the sintering, amorphous tricalcium phosphate is formed in the temperature range of 600 to 750°C, β -tricalcium phosphate in the temperature range of
35 775 to 1100°C, and α -tricalcium phosphate in the temperature range of 1125 to 1200°C. The shaped article

is sintered at a temperature of 1150 to 1500°C, preferably 1350 to 1450°C, for 1 to 200 hours, more preferably 50 to 100 hours, and further cooled at a cooling rate of 500 to 1000 °C/hr. The press used may be
5 a monoaxial press, hot press, rubber press, etc.

The method of production of the porous ceramic of α -tricalcium phosphate is as follows. A powder of tricalcium phosphate prepared by the above-mentioned method is homogeneously mixed with a thickening agent,
10 then the mixture is made into a slurry by addition of water or ethanol. The slurry is then uniformly impregnated into, for example, a plastic sponge and subjected to the same sintering as with the above dense body.

15 By sintering at a high temperature over a long period as mentioned above, it is possible to fabricate a single phase α -tricalcium phosphate ceramic. Further, by changing the conditions of synthesis, conditions of sintering, etc., it is also possible to fabricate shaped
20 articles containing other calcium phosphates such as hydroxyapatite, β -tricalcium phosphate, tetracalcium phosphate.

EXAMPLES

The present invention will now be further
25 illustrated by, but is, of course, by no means limited to the following Examples.

Example 1

α -tricalcium phosphate powder and β -tricalcium phosphate powder prepared by a wet method were fabricated
30 into disk shaped articles having diameters of about 28 mm and thicknesses of about 5 mm by using a monoaxial press. These were sintered at a temperature range of 1000 to 1500°C and were identified in phase by the powder X-ray diffraction method. As a result, it was found that a
35 single phase, high purity α -tricalcium phosphate ceramic having a mole ratio of Ca/P of about 1.50 was obtained from α -tricalcium phosphate powder when sintered at



conditions of 1400 to 1450°C and a single phase, high purity α -tricalcium phosphate ceramic having a mole ratio of Ca/P of about 1.50 was obtained from β -tricalcium phosphate powder when sintered at conditions of 1150 to 1400°C. Further, depending on the conditions, it was also possible to fabricate a tricalcium phosphate ceramic with an α -phase at the surface and a β -phase inside. The relationship between the sintering temperature and phase is shown in Table 1.

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Table 1

Sintering temperature (°C)	α -TCP		β -TCP	
	Ceramic surface	After pulverization	Ceramic surface	After pulverization
1150	$\alpha+\beta$	$\alpha+\beta$	α	α
1200	$\alpha+\beta$	$\alpha+\beta$	α	α
1250	$\alpha+\beta$	$\alpha+\beta$	α	α
1300	α	$\alpha+\beta$	α	α
1350	α	$\alpha+\beta$	α	α
1400	α	α	α	α
1450	α	α	-	-

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In the Table, the α -TCP and β -TCP are the α -tricalcium phosphate powder and β -tricalcium phosphate powder of the starting materials. "Ceramic surface" is the information of the powder X-ray diffraction from the surface of the sintered body, while "After pulverization" is the information from the powder after pulverization of the sintered body.

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Next, the relative densities of α -type tricalcium phosphate ceramics obtained when sintering shaped articles of α -tricalcium phosphate powder at a fixed 1400°C, but changing the sintering time were found. The relative density increased along with the sintering time and that an approximately 95% dense body was obtained with a sintering time of 100 hours.

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Example 2

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Alpha-tricalcium phosphate powder prepared by a wet



method was heat treated under pressure using a hot press under conditions of 80 MPa and 1350°C, whereupon a high purity α -tricalcium phosphate ceramic was obtained.

Example 3

5 Alpha-tricalcium phosphate powder, β -tricalcium phosphate powder, and amorphous tricalcium phosphate powder prepared by a wet method were made into slurries by adding 50% of water. These were then impregnated into polyurethane sponges, then dried and sintered at a
10 sintering temperature of 1400°C and a sintering time of 50 hours, whereupon high purity α -type tricalcium phosphate ceramics were obtained. These had sufficient practical strength as a bone filler (see Fig. 1).

Example 4

15 Dense bodies of α -tricalcium phosphate and hydroxyapatite cut into rectangular columns of 0.7 mm $\times$ 0.7 mm $\times$ 5 mm were implanted into the femur of osteophoresis model rats subjected to ovariectomies to observe the reaction with bone tissue. As a result, in
20 the case of α -tricalcium phosphate, new bone was formed directly around the specimen. There was no interposition of fibrous connecting tissue observed. The new bone and the material bonded directly. Further, the new bone
25 substantially completely covered the surface of the specimen and the rectangular column material became rounded, and therefore, there were signs of absorption over time and the possibility was suggested of complete disappearance with long term implantation (see Fig. 2).

 On the other hand, in the case of the
30 hydroxyapatite, fibrous connecting tissue was formed around the specimen. There was little formation of new bone. Further, the shape of the article remained the same as at the time of implantation, and therefore, there was no sign of dissolution and it was believed that there
35 would be no absorption even with long-term implantation (see Fig. 3).

INDUSTRIAL APPLICABILITY

As explained above in detail, according to the present invention, it is possible to obtain a ceramic usable as a bone filler, superior in biocompatibility, high in the ability to form bone, and having the ability
5 of being replaced by bone.

CLAIMS

1. A method for producing an α -tricalcium phosphate ceramic comprising the steps of: sintering the shaped powder, after shaping a powder material under pressure, or simultaneously with the shaping under pressure; and, further, cooling the sintered product.
2. A method for producing an α -tricalcium phosphate ceramic comprising the steps of: shaping a powder material prepared by a wet method using the monoaxial press method or CIP method; sintering the shaped powder material at a temperature of 1100 to 1500°C for 1 to 200 hours; and, further cooling the sintered product at a cooling rate of 100 to 2000°C/hr.
3. A method for producing an α -tricalcium phosphate ceramic according to claim 2, wherein the powder material obtained by the wet method is impregnated in a porous plastic material, followed by sintering.
4. A method for producing an α -tricalcium phosphate ceramic comprising the step of: sintering a powder material prepared by a wet method using a hot press method or HIP method at a temperature of 200 to 1500°C for 1 to 200 hours.
5. A method for producing an α -tricalcium phosphate ceramic according to any one of claims 2 to 5, wherein the powder material prepared by a wet method is at least one powder selected from the group consisting of β -tricalcium phosphate powder, α -tricalcium phosphate powder, and amorphous calcium phosphate powder, and mixtures of these powders with hydroxyapatite.
6. An α -tricalcium phosphate ceramic having an α -type single phase.