

ELECTRONIC OPHTHALMIC LENS WITH LID POSITION SENSOR

BACKGROUND OF THE INVENTION

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1. Field of the Invention

The present invention relates to a powered or electronic ophthalmic lens, and more particularly, to a powered or electronic ophthalmic lens having a sensor and
10 associated hardware and software for detecting eyelid position.

2. Discussion of the Related Art

As electronic devices continue to be miniaturized, it is becoming increasingly
15 more likely to create wearable or embeddable microelectronic devices for a variety of uses. Such uses may include monitoring aspects of body chemistry, administering controlled dosages of medications or therapeutic agents via various mechanisms, including automatically, in response to measurements, or in response to external control signals, and augmenting the performance of organs or tissues. Examples of
20 such devices include glucose infusion pumps, pacemakers, defibrillators, ventricular assist devices and neurostimulators. A new, particularly useful field of application is in ophthalmic wearable lenses and contact lenses. For example, a wearable lens may incorporate a lens assembly having an electronically adjustable focus to augment or enhance performance of the eye. In another example, either with or without adjustable
25 focus, a wearable contact lens may incorporate electronic sensors to detect concentrations of particular chemicals in the precorneal (tear) film. The use of embedded electronics in a lens assembly introduces a potential requirement for communication with the electronics, for a method of powering and/or re-energizing the

electronics, for interconnecting the electronics, for internal and external sensing and/or monitoring, and for control of the electronics and the overall function of the lens.

The human eye has the ability to discern millions of colors, adjust easily to shifting light conditions, and transmit signals or information to the brain at a rate exceeding that of a high-speed internet connection. Lenses, such as contact lenses and intraocular lenses, currently are utilized to correct vision defects such as myopia (nearsightedness), hyperopia (farsightedness), presbyopia and astigmatism. However, properly designed lenses incorporating additional components may be utilized to enhance vision as well as to correct vision defects.

Contact lenses may be utilized to correct myopia, hyperopia, astigmatism as well as other visual acuity defects. Contact lenses may also be utilized to enhance the natural appearance of the wearer's eyes. Contact lenses or "contacts" are simply lenses placed on the anterior surface of the eye. Contact lenses are considered medical devices and may be worn to correct vision and/or for cosmetic or other therapeutic reasons. Contact lenses have been utilized commercially to improve vision since the 1950s. Early contact lenses were made or fabricated from hard materials, were relatively expensive and fragile. In addition, these early contact lenses were fabricated from materials that did not allow sufficient oxygen transmission through the contact lens to the conjunctiva and cornea which potentially could cause a number of adverse clinical effects. Although these contact lenses are still utilized, they are not suitable for all patients due to their poor initial comfort. Later developments in the field gave rise to soft contact lenses, based upon hydrogels, which are extremely popular and widely utilized today. Specifically, silicone hydrogel contact lenses that are available today combine the benefit of silicone, which has extremely high oxygen permeability, with the proven comfort and clinical performance of hydrogels. Essentially, these silicone hydrogel based contact lenses have higher oxygen permeability and are generally more comfortable to wear than the contact lenses made of the earlier hard materials.

Conventional contact lenses are polymeric structures with specific shapes to correct various vision problems as briefly set forth above. To achieve enhanced functionality, various circuits and components have to be integrated into these polymeric structures. For example, control circuits, microprocessors, communication devices, power supplies, sensors, actuators, light-emitting diodes, and miniature antennas may be integrated into contact lenses via custom-built optoelectronic components to not only correct vision, but to enhance vision as well as provide additional functionality as is explained herein. Electronic and/or powered contract lenses may be designed to provide enhanced vision via zoom-in and zoom-out capabilities, or just simply modifying the refractive capabilities of the lenses. Electronic and/or powered contact lenses may be designed to enhance color and resolution, to display textural information, to translate speech into captions in real time, to offer visual cues from a navigation system, and to provide image processing and internet access. The lenses may be designed to allow the wearer to see in low-light conditions. The properly designed electronics and/or arrangement of electronics on lenses may allow for projecting an image onto the retina, for example, without a variable-focus optic lens, provide novelty image displays and even provide wakeup alerts. Alternately, or in addition to any of these functions or similar functions, the contact lenses may incorporate components for the noninvasive monitoring of the wearer's biomarkers and health indicators. For example, sensors built into the lenses may allow a diabetic patient to keep tabs on blood sugar levels by analyzing components of the tear film without the need for drawing blood. In addition, an appropriately configured lens may incorporate sensors for monitoring cholesterol, sodium, and potassium levels, as well as other biological markers. This, coupled with a wireless data transmitter, could allow a physician to have almost immediate access to a patient's blood chemistry without the need for the patient to waste time getting to a laboratory and having blood drawn. In addition, sensors built into the lenses may be utilized to detect light incident on the eye to compensate for ambient light conditions or for use in determining blink patterns.

The proper combination of devices could yield potentially unlimited functionality; however, there are a number of difficulties associated with the incorporation of extra components on a piece of optical-grade polymer. In general, it is difficult to manufacture such components directly on the lens for a number of reasons, as well as mounting and interconnecting planar devices on a non-planar surface. It is also difficult to manufacture to scale. The components to be placed on or in the lens need to be miniaturized and integrated onto just 1.5 square centimeters of a transparent polymer while protecting the components from the liquid environment on the eye. It is also difficult to make a contact lens comfortable and safe for the wearer with the added thickness of additional components.

Given the area and volume constraints of an ophthalmic device such as a contact lens, and the environment in which it is to be utilized, the physical realization of the device must overcome a number of problems, including mounting and interconnecting a number of electronic components on a non-planar surface, the bulk of which comprises optic plastic. Accordingly, there exists a need for providing a mechanically and electrically robust electronic contact lens.

As these are powered lenses, energy or more particularly current consumption, to run the electronics is a concern given battery technology on the scale for an ophthalmic lens. In addition to normal current consumption, powered devices or systems of this nature generally require standby current reserves, precise voltage control and switching capabilities to ensure operation over a potentially wide range of operating parameters, and burst consumption, for example, up to eighteen (18) hours on a single charge, after potentially remaining idle for years. Accordingly, there exists a need for a system that is optimized for low-cost, long-term reliable service, safety and size while providing the required power.

In addition, because of the complexity of the functionality associated with a powered lens and the high level of interaction between all of the components

comprising a powered lens, there is a need to coordinate and control the overall operation of the electronics and optics comprising a powered ophthalmic lens. Accordingly, there is a need for a system to control the operation of all of the other components that is safe, low-cost, and reliable, has a low rate of power consumption and is scalable for incorporation into an ophthalmic lens.

Powered or electronic ophthalmic lenses may have to account for certain unique physiological functions from the individual utilizing the powered or electronic ophthalmic lens. More specifically, powered lenses may have to account for blinking, including the number of blinks in a given time period, the duration of a blink, the time between blinks and any number of possible blink patterns, for example, if the individual is dosing off. Blink detection may also be utilized to provide certain functionality, for example, blinking may be utilized as a means to control one or more aspects of a powered ophthalmic lens. Additionally, external factors, such as changes in light intensity levels, and the amount of visible light that a person's eyelid blocks out, have to be accounted for when determining blinks. For example, if a room has an illumination level between fifty-four (54) and one hundred sixty-one (161) lux, a photosensor should be sensitive enough to detect light intensity changes that occur when a person blinks.

Ambient light sensors or photosensors are utilized in many systems and products, for example, on televisions to adjust brightness according to the room light, on lights to switch on at dusk, and on phones to adjust the screen brightness. However, these currently utilized sensor systems are not small enough and/or do not have low enough power consumption for incorporation into contact lenses.

It is also important to note that different types of blink detectors may be implemented with computer vision systems directed at one's eye(s), for example, a camera digitized to a computer. Software running on the computer can recognize visual patterns such as the eye open and closed. These systems may be utilized in ophthalmic clinical settings for diagnostic purposes and studies. Unlike the above

described detectors and systems, these systems are intended for off eye use and to look at rather than look away from the eye. Although these systems are not small enough to be incorporated into contact lenses, the software utilized may be similar to the software that would work in conjunction with powered contact lenses. Either
5 system may incorporate software implementations of artificial neural networks that learn from input and adjust their output accordingly. Alternately, non-biology based software implementations incorporating statistics, other adaptive algorithms, and/or signal processing may be utilized to create smart systems.

10 Accordingly, there exists a need for a means and method for detecting certain physiological functions, such as a blink, and utilizing them to activate and/or control an electronic or powered ophthalmic lens according to the type of blink sequence detected by a sensor. The sensor being utilized having to be sized and configured for use in a contact lens. In addition there exists a need to detect the position of a user's eyelids.
15 One indicator of a user's need to focus near is that the top eyelids drop, for example when holding paper to read. Detecting this change in eyelid position could be used as an input to a variable-focus lens to correct presbyopia. An eyelid position sensor could also be used to detect if a user is squinting, perhaps in an attempt to focus far away. An eyelid position sensor could be used to detect that a user is falling asleep, for
20 example to trigger an appropriate alert to keep the user awake. There are existing systems for detecting lid position; however they are limited to devices like camera imagers, image recognition, and infrared emitter/detector pairs which rely on reflection off the eye and eyelid. Existing systems to detect lid position also rely on the use of spectacles or clinical environments and are not easily contained within a contact lens.

SUMMARY OF THE INVENTION

30 The electronic ophthalmic lens with lid position sensor in accordance with the present invention overcomes the limitations associated with the prior art as briefly

described above. This lid position sensor may be integrated into a contact lens instead of requiring a clinical environment or spectacles as is common for existing eye-facing detection systems. The lid position sensor is of the appropriate size and current consumption for use in a contact lens. It also outputs the information necessary for contact lens applications, for example correcting presbyopia or alerting a user to drowsiness.

In accordance with one aspect, the present invention is directed to a powered ophthalmic lens. The powered ophthalmic lens comprises a contact lens including an optic zone and a peripheral zone, and an eyelid position sensor system incorporated into the peripheral zone of the contact lens, the eyelid position sensor system including a sensor array having a plurality of individual sensors to detect eyelid position, a system controller configured to sample each individual sensor in the sensor array to detect eyelid position and provide an output control signal, and at least one actuator configured to receive the output control signal and implement a predetermined function.

In accordance with another aspect, the present invention is directed to a powered ophthalmic lens. The powered ophthalmic lens comprises a contact lens, and an eyelid position sensor system incorporated into the contact lens, the eyelid position sensor system including a sensor array having a plurality of individual sensors to detect eyelid position, a system controller configured to sample each individual sensor in the sensor array to detect eyelid position and provide an output control signal, and at least one actuator configured to receive the output control signal and implement a predetermined function.

In accordance with yet another aspect, the present invention is directed to a powered ophthalmic lens. The powered ophthalmic lens comprises an intraocular lens, and an eyelid position sensor system incorporated into the intraocular lens, the eyelid position sensor system including a sensor array having a plurality of individual sensors to detect eyelid position, a system controller configured to sample each individual

sensor in the sensor array to detect eyelid position and provide an output control signal, and at least one actuator configured to receive the output control signal and implement a predetermined function.

The present invention relates to a powered or electronic ophthalmic lens which may incorporate an eyelid or lid position sensor. It is known that the eyelids protect the globe in a number of ways, including the blink reflex and the tear spreading action. The
5 blink reflex of the eyelids prevents trauma to the globe by rapidly closing upon a perceived threat to the eye. Blinking also spreads tears over the globe's surface to keep it moist and rinse away bacteria and other foreign matter. But the movement of the eyelids may also indicate other actions or functions at play. For example, when an individual focuses on a near object, the top eyelid drops. Accordingly, detection of this
10 movement may be utilized as an input into an electronic ophthalmic lens with a variable focus optic to correct for a loss in accommodation associated with presbyopia. Alternately, when an individual attempts to focus on a distant object, he or she may squint. The eyelid motion associated with squinting may be utilized as an input into an electronic ophthalmic lens with a variable focus optic to focus or zoom in on a distant
15 object. In addition, an eyelid position sensor may also be utilized to alert an individual wearing an electronic ophthalmic lens that he or she is in danger of falling asleep.

The present invention more generally relates to a powered contact lens comprising an electronic system, which performs any number of functions, including
20 actuating a variable-focus optic if included. The electronic system includes one or more batteries or other power sources, power management circuitry, one or more sensors, clock generation circuitry, control algorithms and circuitry, and lens driver circuitry.

Control of a powered ophthalmic lens may be accomplished through a manually
25 operated external device that communicates with the lens wirelessly, such as a hand-held remote unit. Alternately, control of the powered ophthalmic lens may be accomplished via feedback or control signals directly from the wearer. For example,

sensors built into the lens may detect blinks and/or blink patterns. Based upon the pattern or sequence of blinks, the powered ophthalmic lens may change state, for example, its refractive power in order to either focus on a near object or a distant object.

5 The blink detection algorithm is a component of the system controller which detects characteristics of blinks, for example, if the lid is open or closed, the duration of the blink open or closed, the inter-blink duration, and the number of blinks in a given time period. The exemplary algorithm in accordance with the present invention relies on sampling light incident on the eye at a certain sample rate. Pre-determined blink
10 patterns are stored and compared to the recent history of incident light samples. When patterns match, the blink detection algorithm triggers activity in the system controller, for example, to activate the lens driver to change the refractive power of the lens.

 The blink detection algorithm and associated circuitry of the present invention
15 preferably operate over a reasonably wide range of lighting conditions and is preferably able to distinguish an intentional blink sequence from involuntary blinks. It is also preferred that minimal training is required to utilize intentional blinks to activate and/or control the powered ophthalmic lens. The blink detection algorithm and associated circuitry of the present invention provides a safe, low cost, and reliable means and
20 method for detecting blinks via a powered or electronic contact lens, which also has a low rate of power consumption and is scalable for incorporation into an ophthalmic lens, for at least one of activating or controlling a powered or electronic ophthalmic lens.

 The present invention is also directed to a powered or electronic ophthalmic lens
25 that incorporates an eyelid or lid position sensor.

BRIEF DESCRIPTION OF THE DRAWINGS

The foregoing and other features and advantages of the invention will be apparent from the following, more particular description of preferred embodiments of the invention, as illustrated in the accompanying drawings.

5 Figure 1 illustrates an exemplary contact lens comprising a blink detection system in accordance with some embodiments of the present invention.

Figure 2 illustrates a graphical representation of light incident on the surface of the eye versus time, illustrating a possible involuntary blink pattern recorded at various
10 light intensity levels versus time and a usable threshold level based on some point between the maximum and minimum light intensity levels in accordance with the present invention.

Figure 3 is an exemplary state transition diagram of a blink detection system in
15 accordance with the present invention.

Figure 4 is a diagrammatic representation of a photodetection path utilized to detect and sample received light signals in accordance with the present invention.

20 Figure 5 is a block diagram of digital conditioning logic in accordance with the present invention.

Figure 6 is a block diagram of digital detection logic in accordance with the
25 present invention.

Figure 7 is an exemplary timing diagram in accordance with the present
invention.

Figure 8 is a diagrammatic representation of a digital system controller in
30 accordance with the present invention.

Figure 9 is an exemplary timing diagram for automatic gain control in accordance with the present invention.

5 Figure 10 is a diagrammatic representation of light-blocking and light-passing regions on an exemplary integrated circuit die in accordance with the present invention.

Figure 11 is a diagrammatic representation of an exemplary electronic insert, including a blink detector, for a powered contact lens in accordance with the present
10 invention.

Figure 12 is a diagrammatic representation of an exemplary eyelid position sensor in accordance with the present invention.

15 Figure 13 is a diagrammatic representation of two exemplary eyelid position sensors having a communication channel for synchronizing operation between two eyes in accordance with the present invention.

Figure 14A is a diagrammatic representation of a first exemplary electronic
20 system incorporated into a contact lens for detecting eyelid position in accordance with the present invention.

Figure 14B is an enlarged view of the first exemplary electronic system of Figure
14A.

25 Figure 15 is a diagrammatic representation of exemplary outputs from eyelid position sensors in accordance with the present invention.

Figure 16A is a diagrammatic representation of a second exemplary electronic system incorporated into a contact lens for detecting eyelid position in accordance with the present invention.

5 Figure 16B is an enlarged view of the second exemplary electronic system of Figure 16A.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

10 Conventional contact lenses are polymeric structures with specific shapes to correct various vision problems as briefly set forth above. To achieve enhanced functionality, various circuits and components may be integrated into these polymeric structures. For example, control circuits, microprocessors, communication devices, power supplies, sensors, actuators, light-emitting diodes, and miniature antennas may
15 be integrated into contact lenses via custom-built optoelectronic components to not only correct vision, but to enhance vision as well as provide additional functionality as is explained herein. Electronic and/or powered contact lenses may be designed to provide enhanced vision via zoom-in and zoom-out capabilities, or just simply modifying the refractive capabilities of the lenses. Electronic and/or powered contact lenses may
20 be designed to enhance color and resolution, to display textural information, to translate speech into captions in real time, to offer visual cues from a navigation system, and to provide image processing and internet access. The lenses may be designed to allow the wearer to see in low light conditions. The properly designed electronics and/or arrangement of electronics on lenses may allow for projecting an image onto the retina,
25 for example, without a variable focus optic lens, provide novelty image displays and even provide wakeup alerts. Alternately, or in addition to any of these functions or similar functions, the contact lenses may incorporate components for the noninvasive monitoring of the wearer's biomarkers and health indicators. For example, sensors built into the lenses may allow a diabetic patient to keep tabs on blood sugar levels by
30 analyzing components of the tear film without the need for drawing blood. In addition,

an appropriately configured lens may incorporate sensors for monitoring cholesterol, sodium, and potassium levels, as well as other biological markers. This coupled with a wireless data transmitter could allow a physician to have almost immediate access to a patient's blood chemistry without the need for the patient to waste time getting to a laboratory and having blood drawn. In addition, sensors built into the lenses may be utilized to detect light incident on the eye to compensate for ambient light conditions or for use in determining blink patterns.

The powered or electronic contact lens of the present invention comprises the necessary elements to correct and/or enhance the vision of patients with one or more of the above described vision defects or otherwise perform a useful ophthalmic function. In addition, the electronic contact lens may be utilized simply to enhance normal vision or provide a wide variety of functionality as described above. The electronic contact lens may comprise a variable focus optic lens, an assembled front optic embedded into a contact lens or just simply embedding electronics without a lens for any suitable functionality. The electronic lens of the present invention may be incorporated into any number of contact lenses as described above. In addition, intraocular lenses may also incorporate the various components and functionality described herein. However, for ease of explanation, the disclosure will focus on an electronic contact lens to correct vision defects intended for single-use daily disposability.

The present invention may be employed in a powered ophthalmic lens or powered contact lens comprising an electronic system, which actuates a variable-focus optic or any other device or devices configured to implement any number of numerous functions that may be performed. The electronic system includes one or more batteries or other power sources, power management circuitry, one or more sensors, clock generation circuitry, control algorithms and circuitry, and lens driver circuitry. The complexity of these components may vary depending on the required or desired functionality of the lens.

Control of an electronic or a powered ophthalmic lens may be accomplished through a manually operated external device that communicates with the lens, such as a hand-held remote unit. For example, a fob may wirelessly communicate with the powered lens based upon manual input from the wearer. Alternately, control of the
5 powered ophthalmic lens may be accomplished via feedback or control signals directly from the wearer. For example, sensors built into the lens may detect blinks and/or blink patterns. Based upon the pattern or sequence of blinks, the powered ophthalmic lens may change state, for example, its refractive power in order to either focus on a near object or a distant object.

Alternately, blink detection in a powered or electronic ophthalmic lens may be used for other various uses where there is interaction between the user and the electronic contact lens, such as activating another electronic device, or sending a command to another electronic device. For example, blink detection in an ophthalmic
15 lens may be used in conjunction with a camera on a computer wherein the camera keeps track of where the eye(s) moves on the computer screen, and when the user executes a blink sequence that it detected, it causes the mouse pointer to perform a command, such as double-clicking on an item, highlighting an item, or selecting a menu item.

A blink detection algorithm is a component of the system controller which detects characteristics of blinks, for example, is the lid open or closed, the duration of the blink, the inter-blink duration, and the number of blinks in a given time period. The algorithm in accordance with the present invention relies on sampling light incident on the eye at a
25 certain sample rate. Pre-determined blink patterns are stored and compared to the recent history of incident light samples. When patterns match, the blink detection algorithm may trigger activity in the system controller, for example, to activate the lens driver to change the refractive power of the lens.

Blinking is the rapid closing and opening of the eyelids and is an essential function of the eye. Blinking protects the eye from foreign objects, for example, individuals blink when objects unexpectedly appear in proximity to the eye. Blinking provides lubrication over the anterior surface of the eye by spreading tears. Blinking also serves to remove contaminants and/or irritants from the eye. Normally, blinking is done automatically, but external stimuli may contribute as in the case with irritants. However, blinking may also be purposeful, for example, for individuals who are unable to communicate verbally or with gestures can blink once for yes and twice for no. The blink detection algorithm and system of the present invention utilizes blinking patterns that cannot be confused with normal blinking response. In other words, if blinking is to be utilized as a means for controlling an action, then the particular pattern selected for a given action cannot occur at random; otherwise inadvertent actions may occur. As blink speed may be affected by a number of factors, including fatigue, eye injury, medication and disease, blinking patterns for control purposes preferably account for these and any other variables that affect blinking. The average length of involuntary blinks is in the range of about one hundred (100) to four hundred (400) milliseconds. Average adult men and women blink at a rate of ten (10) involuntary blinks per minute, and the average time between involuntary blinks is about 0.3 to seventy (70) seconds.

An exemplary embodiment of the blink detection algorithm may be summarized in the following steps.

1. Define an intentional "blink sequence" that a user will execute for positive blink detection.
2. Sample the incoming light level at a rate consistent with detecting the blink sequence and rejecting involuntary blinks.
3. Compare the history of sampled light levels to the expected "blink sequence," as defined by a blink template of values.
4. Optionally implement a blink "mask" sequence to indicate portions of the template to be ignored during comparisons, e.g. near transitions. This may allow for a user to deviate from a desired "blink sequence," such as a plus or minus one (1) error

window, wherein one or more of lens activation, control, and focus change can occur. Additionally, this may allow for variation in the user's timing of the blink sequence.

An exemplary blink sequence may be defined as follows:

- 5 1. blink (closed) for 0.5 s
2. open for 0.5 s
3. blink (closed) for 0.5 s

At a one hundred (100) ms sample rate, a twenty (20) sample blink template is
10 given by

blink_template = [1,1,1, 0,0,0,0,0, 1,1,1,1,1, 0,0,0,0,0, 1,1].

The blink mask is defined to mask out the samples just after a transition (0 to mask out or ignore samples), and is given by

15 blink_mask = [1,1,1, 0,1,1,1,1, 0,1,1,1,1, 0,1,1,1,1, 0,1].

Optionally, a wider transition region may be masked out to allow for more timing uncertainty, and is given by

20 blink_mask = [1,1,0, 0,1,1,1,0, 0,1,1,1,0, 0,1,1,1,0, 0,1].

Alternate patterns may be implemented, e.g. single long blink, in this case a 1.5s blink with a 24-sample template, given by

blink_template = [1,1,1,1,0,0, 0,0,0,0,0,0, 0,0,0,0,0,0, 0,1,1,1,1,1].

25 It is important to note that the above example is for illustrative purposes and does not represent a specific set of data.

Detection may be implemented by logically comparing the history of samples against the template and mask. The logical operation is to exclusive-OR (XOR) the
30 template and the sample history sequence, on a bitwise basis, and then verify that all

unmasked history bits match the template. For example, as illustrated in the blink mask samples above, in each place of the sequence of a blink mask that the value is logic 1, a blink has to match the blink mask template in that place of the sequence. However, in each place of the sequence of a blink mask that the value is logic 0, it is not necessary
5 that a blink matches the blink mask template in that place of the sequence. For example, the following Boolean algorithm equation, as coded in MATLAB®, may be utilized.

matched = not (blink_mask) | not (xor (blink_template, test_sample)),

10 wherein test_sample is the sample history. The matched value is a sequence with the same length as the blink template, sample history and blink_mask. If the matched sequence is all logic 1's, then a good match has occurred. Breaking it down, not (xor (blink_template, test_sample)) gives a logic 0 for each mismatch and a logic 1 for each
15 match. Logic oring with the inverted mask forces each location in the matched sequence to a logic 1 where the mask is a logic 0. Accordingly, the more places in a blink mask template where the value is specified as logic 0, the greater the margin of error in relation to a person's blinks is allowed. MATLAB® is a high level language and implementation for numerical computation, visualization and programming and is a
20 product of MathWorks, Natick, Massachusetts. It is also important to note that the greater the number of logic 0's in the blink mask template, the greater the potential for false positive matched to expected or intended blink patterns. It should be appreciated that a variety of expected or intended blink patterns may be programmed into a device with one or more active at a time. More specifically, multiple expected or intended blink
25 patterns may be utilized for the same purpose or functionality, or to implement different or alternate functionality. For example, one blink pattern may be utilized to cause the lens to zoom in or out on an intended object while another blink pattern may be utilized to cause another device, for example, a pump, on the lens to deliver a dose of a therapeutic agent.

Figure 1 illustrates, in block diagram form, a contact lens 100, comprising an electronic blink detector system, in accordance with an exemplary embodiment of the present invention. In this exemplary embodiment, the electronic blink detector system may comprise a photosensor 102, an amplifier 104, an analog-to-digital converter or ADC 106, a digital signal processor 108, a power source 110, an actuator 112, and a system controller 114.

When the contact lens 100 is placed onto the front surface of a user's eye the electronic circuitry of the blink detector system may be utilized to implement the blink detection algorithm of the present invention. The photosensor 102, as well as the other circuitry, is configured to detect blinks and/or various blink patterns produced by the user's eye.

In this exemplary embodiment, the photosensor 102 may be embedded into the contact lens 100 and receives ambient light 101, converting incident photons into electrons and thereby causing a current, indicated by arrow 103, to flow into the amplifier 104. The photosensor or photodetector 102 may comprise any suitable device. In one exemplary embodiment, the photosensor 102 comprises a photodiode. In a preferred exemplary embodiment, the photodiode is implemented in a complimentary metal-oxide semiconductor (CMOS process technology) to increase integration ability and reduce the overall size of the photosensor 102 and the other circuitry. The current 103 is proportional to the incident light level and decreases substantially when the photodetector 102 is covered by an eyelid. The amplifier 104 creates an output proportional to the input, with gain, and may function as a transimpedance amplifier which converts input current into output voltage. The amplifier 104 may amplify a signal to a useable level for the remainder of the system, such as giving the signal enough voltage and power to be acquired by the ADC 106. For example, the amplifier may be necessary to drive subsequent blocks since the output of the photosensor 102 may be quite small and may be used in low-light environments. The amplifier 104 may be implemented as a variable-gain amplifier, the gain of which

may be adjusted by the system controller 114, in a feedback arrangement, to maximize the dynamic range of the system. In addition to providing gain, the amplifier 104 may include other analog signal conditioning circuitry, such as filtering and other circuitry appropriate to the photosensor 102 and amplifier 104 outputs. The amplifier 104 may
5 comprise any suitable device for amplifying and conditioning the signal output by the photosensor 102. For example, the amplifier 104 may simply comprise a single operational amplifier or a more complicated circuit comprising one or more operational amplifiers. As set forth above, the photosensor 102 and the amplifier 104 are configured to detect and isolate blink sequences based upon the incident light intensity
10 received through the eye and convert the input current into a digital signal usable ultimately by the system controller 114. The system controller 114 is preferably preprogrammed or preconfigured to recognize various blink sequences and/or blink patterns in various light intensity level conditions and provide an appropriate output signal to the actuator 112. The system controller 114 also comprises associated
15 memory.

In this exemplary embodiment, the ADC 106 may be used to convert a continuous, analog signal output from the amplifier 104 into a sampled, digital signal appropriate for further signal processing. For example, the ADC 106 may convert an
20 analog signal output from the amplifier 104 into a digital signal that may be useable by subsequent or downstream circuits, such as a digital signal processing system or microprocessor 108. A digital signal processing system or digital signal processor 108 may be utilized for digital signal processing, including one or more of filtering, processing, detecting, and otherwise manipulating/processing sampled data to permit
25 incident light detection for downstream use. The digital signal processor 108 may be preprogrammed with the blink sequences and/or blink patterns described above. The digital signal processor 108 also comprises associated memory. The digital signal processor 108 may be implemented utilizing analog circuitry, digital circuitry, software, or a combination thereof. In the illustrate exemplary embodiment, it is implemented in
30 digital circuitry. The ADC 106 along with the associated amplifier 104 and digital signal

processor 108 are activated at a suitable rate in agreement with the sampling rate previously described, for example every one hundred (100) ms.

A power source 110 supplies power for numerous components comprising the blink detection system. The power may be supplied from a battery, energy harvester, or other suitable means as is known to one of ordinary skill in the art. Essentially, any type of power source 110 may be utilized to provide reliable power for all other components of the system. A blink sequence may be utilized to change the state of the system and/or the system controller. Furthermore, the system controller 114 may control other aspects of a powered contact lens depending on input from the digital signal processor 108, for example, changing the focus or refractive power of an electronically controlled lens through the actuator 112.

The system controller 114 uses the signal from the photosensor chain; namely, the photosensor 102, the amplifier 104, the ADC 106 and the digital signal processing system 108, to compare sampled light levels to blink activation patterns. Referring to Figure 2, a graphical representation of blink pattern samples recorded at various light intensity levels versus time and a usable threshold level is illustrated. Accordingly, accounting for various factors may mitigate and/or prevent error in detecting blinks when sampling light incident on the eye, such as accounting for changes in light intensity levels in different places and/or while performing various activities. Additionally, when sampling light incident on the eye, accounting for the effects that changes in ambient light intensity may have on the eye and eyelid may also mitigate and/or prevent error in detecting blinks, such as how much visible light an eyelid blocks when it is closed in low-intensity light levels and in high-intensity light levels. In other words, in order to prevent erroneous blinking patterns from being utilized to control, the level of ambient light is preferably accounted for as is explained in greater detail below.

For example, in a study, it has been found that the eyelid on average blocks approximately ninety-nine (99) percent of visible light, but at lower wavelengths less

light tends to be transmitted through the eyelid, blocking out approximately 99.6 percent of visible light. At longer wavelengths, toward the infrared portion of the spectrum, the eyelid may block only thirty (30) percent of the incident light. What is important to note; however, is that light at different frequencies, wavelengths and intensities may be transmitted through the eyelids with different efficiencies. For example, when looking at a bright light source, an individual may see red light with his or her eyelids closed. There may also be variations in how much visible light an eyelid blocks based upon an individual, such as an individual's skin pigmentation. As is illustrated in Figure 2, data samples of blink patterns across various lighting levels are simulated over the course of a seventy (70) second time interval wherein the visible light intensity levels transmitted through the eye are recorded during the course of the simulation, and a usable threshold value is illustrated. The threshold is set at a value in between the peak-to-peak value of the visible light intensity recorded for the sample blink patterns over the course of the simulation at varying light intensity levels. Having the ability to preprogram blink patterns while tracking an average light level over time and adjusting a threshold may be critical to being able to detect when an individual is blinking, as opposed to when an individual is not blinking and/or there is just a change in light intensity level in a certain area.

Referring now again to Figure 1, in further alternate exemplary embodiments, the system controller 114 may receive input from sources including one or more of a blink detector, eye muscle sensors, and a fob control. By way of generalization, it may be obvious to one skilled in the art that the method of activating and/or controlling the system controller 114 may require the use of one or more activation methods. For example, an electronic or powered contact lens may be programmable specific to an individual user, such as programming a lens to recognize both of an individual's blink patterns and an individual's ciliary muscle signals when performing various actions, for example, focusing on an object far away, or focusing on an object that is near. In some exemplary embodiments, using more than one method to activate an electronic contact lens, such as blink detection and ciliary muscle signal detection, may give the ability for

each method to be crosschecked with another before activation of the contact lens occurs. An advantage of crosschecking may include mitigation of false positives, such as minimizing the chance of unintentionally triggering a lens to activate. In one exemplary embodiment, the crosschecking may involve a voting scheme, wherein a certain number of conditions are met prior to any action taking place.

The actuator 112 may comprise any suitable device for implementing a specific action based upon a received command signal. For example, if a blink activation pattern is matched compared to a sampled light level as described above, the system controller 114 may enable the actuator 112, such as a variable-optic electronic or powered lens. The actuator 112 may comprise an electrical device, a mechanical device, a magnetic device, or any combination thereof. The actuator 112 receives a signal from the system controller 114 in addition to power from the power source 110 and produces some action based on the signal from the system controller 114. For example, if the system controller 114 signal is indicative of the wearer trying to focus on a near object, the actuator 112 may be utilized to change the refractive power of the electronic ophthalmic lens, for example, via a dynamic multi-liquid optic zone. In an alternate exemplary embodiment, the system controller 114 may output a signal indicating that a therapeutic agent should be delivered to the eye(s). In this exemplary embodiment, the actuator 112 may comprise a pump and reservoir, for example, a microelectromechanical system (MEMS) pump. As set forth above, the powered lens of the present invention may provide various functionality; accordingly, one or more actuators may be variously configured to implement the functionality.

Figure 3 illustrates a state transition diagram 300 for an exemplary blink detection system in accordance with the blink detection algorithm of the present invention. The system starts in an IDLE state 302 waiting for an enable signal bl_go to be asserted. When the enable bl_go signal is asserted, for example, by an oscillator and control circuit which pulses bl_go at a one hundred (100) ms rate commensurate with the blink sampling rate, the state machine then transitions to a WAIT_ADC state

304 in which an ADC is enabled to convert a received light level to a digital value. The ADC asserts an `adc_done` signal to indicate its operations are complete, and the system or state machine transitions to a SHIFT state 306. In the SHIFT state 306 the system pushes the most recently received ADC output value onto a shift register to hold the history of blink samples. In some exemplary embodiments, the ADC output value is first compared to a threshold value to provide a single bit (1 or 0) for the sample value, in order to minimize storage requirements. The system or state machine then transitions to a COMPARE state 308 in which the values in the sample history shift register are compared to one or more blink sequence templates and masks as described above. If a match is detected, one or more output signals may be asserted, such as one to toggle the state of the lens driver, `bl_cp_toggle`, or any other functionality to be performed by the powered ophthalmic lens. The system or state machine then transitions to the DONE state 310 and asserts a `bl_done` signal to indicate its operations are complete.

Figure 4 illustrates an exemplary photosensor or photodetector signal path `pd_rx_top` that may be used to detect and sample received light levels. The signal path `pd_rx_top` may comprise a photodiode 402, a transimpedance amplifier 404, an automatic gain and low pass filtering stage 406 (AGC/LPF), and an ADC 408. The `adc_vref` signal is input to the ADC 408 from the power source 110 (see Figure 1) or alternately it may be provided from a dedicated circuit inside the analog-to-digital converter 408. The output from the ADC 408, `adc_data`, is transmitted to the digital signal processing and system controller block 108/114 (see Figure 1). Although illustrated in Figure 1 as individual blocks 108 and 114, for ease of explanation, the digital signal processing and system controller are preferably implemented on a single block 410. The enable signal, `adc_en`, the start signal, `adc_start`, and the reset signal, `adc_rst_n` are received from the digital signal processing and system controller 410 while the complete signal, `adc_complete`, is transmitted thereto. The clock signal, `adc_clk`, may be received from a clock source external to the signal path, `pd_rx_top`, or from the digital signal processing and system controller 410. It is important to note that

the adc_clk signal and the system clock may be running at different frequencies. It is also important to note that any number of different ADCs may be utilized in accordance with the present invention which may have different interface and control signals but which perform a similar function of providing a sampled, digital representation of the output of the analog portion of the photosensor signal path. The photodetect enable, pd_en, and the photodetect gain, pd_gain, are received from the digital signal processing and system controller 410.

Figure 5 illustrates a block diagram of digital conditioning logic 500 that may be used to reduce the received ADC signal value, adc_data, to a single bit value pd_data. The digital conditioning logic 500 may comprise a digital register 502 to receive the data, adc_data, from the photodetection signal path pd_rx_top to provide a held value on the signal adc_data_held. The digital register 502 is configured to accept a new value on the adc_data signal when the adc_complete signal is asserted and to otherwise hold the last accepted value when the adc_complete signal is received. In this manner the system may disable the photodetection signal path once the data is latched to reduce system current consumption. The held data value may then be averaged, for example, by an integrate-and-dump average or other averaging methods implemented in digital logic, in the threshold generation circuit 504 to produce one or more thresholds on the signal pd_th. The held data value may then be compared, via comparator 506, to the one or more thresholds to produce a one-bit data value on the signal pd_data. It will be appreciated that the comparison operation may employ hysteresis or comparison to one or more thresholds to minimize noise on the output signal pd_data. The digital conditioning logic may further comprise a gain adjustment block pd_gain_adj 508 to set the gain of the automatic gain and low-pass filtering stage 406 in the photodetection signal path via the signal pd_gain, illustrated in Figure 4, according to the calculated threshold values and/or according to the held data value. It is important to note that in this exemplary embodiment six bit words provide sufficient resolution over the dynamic range for blink detection while minimizing complexity.

In one exemplary embodiment, the threshold generation circuit 504 comprises a peak detector, a valley detector and a threshold calculation circuit. In this exemplary embodiment, the threshold and gain control values may be generated as follows. The peak detector and the valley detector are configured to receive the held value on signal
5 adc_data_held. The peak detector is further configured to provide an output value, pd_pk, which quickly tracks increases in the adc_data_held value and slowly decays if the adc_data_held value decreases. The operation is analogous to that of a classic diode envelope detector, as is well-known in the electrical arts. The valley detector is further configured to provide an output value pd_vl which quickly tracks decreases in
10 the adc_data_held value and slowly decays to a higher value if the adc_data_held value increases. The operation of the valley detector is also analogous to a diode envelope detector, with the discharge resistor tied to a positive power supply voltage. The threshold calculation circuit is configured to receive the pd_pk and pd_vl values and is further configured to calculate a mid-point threshold value pd_th_mid based on an
15 average of the pd_pk and pd_vl values. The threshold generation circuit 504 provides the threshold value pd_th based on the mid-point threshold value pd_th_mid.

The threshold generation circuit 504 may be further adapted to update the values of the pd_pk and pd_vl levels in response to changes in the pd_gain value. If the
20 pd_gain value increases by one step, then the pd_pk and pd_vl values are increased by a factor equal to the expected gain increase in the photodetection signal path. If the pd_gain value decreases by one step, then the pd_pk and pd_val values are decreased by a factor equal to the expected gain decrease in the photodetection signal path. In this manner the states of the peak detector and valley detectors, as held in the pd_pk
25 and pd_vl values, respectively, and the threshold value pd_th as calculated from the pd_pk and pd_vl values are updated to match the changes in signal path gain, thereby avoiding discontinuities or other changes in state or value resulting only from the intentional change in the photodetection signal path gain.

In a further exemplary embodiment of the threshold generation circuit 504, the threshold calculation circuit may be further configured to calculate a threshold value `pd_th_pk` based on a proportion or percentage of the `pd_pk` value. In a preferred exemplary embodiment the `pd_th_pk` may be advantageously configured to be seven
5 eighths of the `pd_pk` value, a calculation which may be implemented with a simple right shift by three bits and a subtraction as is well-known in the relevant art. The threshold calculation circuit may select the threshold value `pd_th` to be the lesser of `pd_th_mid` and `pd_th_pk`. In this manner, the `pd_th` value will never be equal to the `pd_pk` value, even after long periods of constant light incident on the photodiode which may result in
10 the `pd_pk` and `pd_vl` values being equal. It will be appreciated that the `pd_th_pk` value ensures detection of a blink after long intervals. The behavior of the threshold generation circuit is further illustrated in Figure 9, as discussed subsequently.

Figure 6 illustrates a block diagram of digital detection logic 600 that may be
15 used to implement an exemplary digital blink detection algorithm in accordance with an embodiment of the present invention. The digital detection logic 600 may comprise a shift register 602 adapted to receive the data from the photodetection signal path `pd_rx_top`, Figure 4, or from the digital conditioning logic, Figure 5, as illustrated here on the signal `pd_data`, which has a one bit value. The shift register 602 holds a history of
20 the received sample values, here in a 24-bit register. The digital detection logic 600 further comprises a comparison block 604, adapted to receive the sample history and one or more blink templates `bl_tpl` and blink masks `bl_mask`, and is configured to indicate a match to the one or more templates and masks on one or more output signals that may be held for later use. The output of the comparison block 604 is latched via a
25 D flip-flop 606. The digital detection logic 600 may further comprise a counter 608 or other logic to suppress successive comparisons that may be on the same sample history set at small shifts due to the masking operations. In a preferred exemplary embodiment the sample history is cleared or reset after a positive match is found, thus requiring a full, new matching blink sequence to be sampled before being able to
30 identify a subsequent match. The digital detection logic 600 may still further comprise a

state machine or similar control circuitry to provide the control signals to the photodetection signal path and the ADC. In some exemplary embodiments the control signals may be generated by a control state machine that is separate from the digital detection logic 600. This control state machine may be part of the digital signal processing and system controller 410.

Figure 7 illustrates a timing diagram of the control signals provided from a blink detection subsystem to an ADC 408 (Figure 4) used in a photodetection signal path. The enable and clock signals `adc_en`, `adc_rst_n` and `adc_clk` are activated at the start of a sample sequence and continue until the analog-to-digital conversion process is complete. In one exemplary embodiment the ADC conversion process is started when a pulse is provided on the `adc_start` signal. The ADC output value is held in an `adc_data` signal and completion of the process is indicated by the analog-to-digital converter logic on an `adc_complete` signal. Also illustrated in Figure 7 is the `pd_gain` signal which is utilized to set the gain of the amplifiers before the ADC. This signal is shown as being set before the warm-up time to allow the analog circuit bias and signal levels to stabilize prior to conversion.

Figure 8 illustrates a digital system controller 800 comprising a digital blink detection subsystem `dig_blink` 802. The digital blink detection subsystem `dig_blink` 802 may be controlled by a master state machine `dig_master` 804 and may be adapted to receive clock signals from a clock generator `clkgen` 806 external to the digital system controller 800. The digital blink detection subsystem `dig_blink` 802 may be adapted to provide control signals to and receive signals from a photodetection subsystem as described above. The digital blink detection subsystem `dig_blink` 802 may comprise digital conditioning logic and digital detection logic as described above, in addition to a state machine to control the sequence of operations in a blink detection algorithm. The digital blink detection subsystem `dig_blink` 802 may be adapted to receive an enable signal from the master state machine 804 and to provide a completion or done indication and a blink detection indication back to the master state machine 804.

Figure 9 provides waveforms, Figures 9A – 9G, to illustrate the operation of the threshold generation circuit and automatic gain control (Figure 5). Figure 9A illustrates an example of photocurrent versus time as might be provided by a photodiode in response to varying light levels. In the first portion of the plot, the light level and resulting photocurrent are relatively low compared to in the second portion of the plot. In both the first and second portions of the plot a double blink is seen to reduce the light and photocurrent. Note that the attenuation of light by the eyelid may not be one hundred (100) percent, but a lower value depending on the transmission properties of the eyelid for the wavelengths of light incident on the eye. Figure 9B illustrates the `adc_data_held` value that is captured in response to the photocurrent waveform of Figure 9A. For simplicity, the `adc_data_held` value is illustrated as a continuous analog signal rather than a series of discrete digital samples. It will be appreciated that the digital sample values will correspond to the level illustrated in Figure 9B at the corresponding sample times. The dashed lines at the top and bottom of the plot indicate the maximum and minimum values of the `adc_data` and `adc_data_held` signals. The range of values between the minimum and maximum is also known as the dynamic range of the `adc_data` signal. As discussed below, the photodetection signal path gain is different (lower) in the second portion of the plot. In general the `adc_data_held` value is directly proportional to the photocurrent, and the gain changes only affect the ratio or the constant of proportionality. Figure 9C illustrates the `pd_pk`, `pd_vl` and `pd_th_mid` values calculated in response to the `adc_data_held` value by the threshold generation circuit. Figure 9D illustrates the `pd_pk`, `pd_vl` and `pd_th_pk` values calculated in response to the `adc_data_held` value in some exemplary embodiments of the threshold generation circuit. Note that the `pd_th_pk` value is always some proportion of the `pd_pk` value. Figure 9E illustrates the `adc_data_held` value with the `pd_th_mid` and `pd_th_pk` values. Note that during long periods of time where the `adc_data_held` value is relatively constant the `pd_th_mid` value becomes equal to the `adc_data_held` value as the `pd_vl` value decays to the same level. The `pd_th_pk` value always remains some amount below the `adc_data_held` value. Also illustrated in Figure 9E is the selection of

pd_th where the pd_th value is selected to be the lower of pd_th_pk and pd_th_mid. In this way the threshold is always set some distance away from the pd_pk value, avoiding false transitions on pd_data due to noise on the photocurrent and adc_data held signals. Figure 9F illustrates the pd_data value generated by comparison of the
5 adc_data_held value to the pd_th value. Note that the pd_data signal is a two-valued signal which is low when a blink is occurring. Figure 9G illustrates a value of tia_gain versus time for these example waveforms. The value of tia_gain is set lower when the pd_th starts to exceed a high threshold shown as agc_pk_th in Figure 9E. It will be appreciated that similar behavior occurs for raising tia_gain when pd_th starts to fall
10 below a low threshold. Looking again at the second portion of each of the Figures 9A through 9E the effect of the lower tia_gain is clear. In particular note that the adc_data_held value is maintained near the middle of the dynamic range of the adc_data and adc_data_held signals. Further, it is important to note that the pd_pk and pd_vl values are updated in accordance with the gain change as described above such
15 that discontinuities are avoided in the peak and valley detector states and values due solely to changes in the photodetection signal path gain.

Figure 10 illustrates exemplary light-blocking and light-passing features on an integrated circuit die 1000. The integrated circuit die 1000 comprises a light passing
20 region 1002, a light blocking region 1004, bond pads 1006, passivation openings 1008, and light blocking layer openings 1010. The light-passing region 1002 is located above the photosensors (not illustrated), for example an array of photodiodes implemented in the semiconductor process. In a preferred exemplary embodiment, the light-passing region 1002 permits as much light as possible to reach the photosensors thereby
25 maximizing sensitivity. This may be done through removing polysilicon, metal, oxide, nitride, polyimide, and other layers above the photoreceptors, as permitted in the semiconductor process utilized for fabrication or in post processing. The light-passing area 1002 may also receive other special processing to optimize light detection, for example an anti-reflective coating, filter, and/or diffuser. The light-blocking region 1004
30 may cover other circuitry on the die which does not require light exposure. The

performance of the other circuitry may be degraded by photocurrents, for example shifting bias voltages and oscillator frequencies in the ultra-low current circuits required for incorporation into contact lenses, as mentioned previously. The light-blocking region 1004 is preferentially formed with a thin, opaque, reflective material, for example aluminum or copper already use in semiconductor wafer processing and post-processing. If implemented with metal, the material forming the light-blocking region 1004 must be insulated from the circuits underneath and the bond pads 1006 to prevent short-circuit conditions. Such insulation may be provided by the passivation already present on the die as part of normal wafer passivation, e.g. oxide, nitride, and/or polyimide, or with other dielectric added during post-processing. Masking permits light blocking layer openings 1010 so that conductive light-blocking metal does not overlap bond pads on the die. The light-blocking region 1004 is covered with additional dielectric or passivation to protect the die and avoid short-circuits during die attachment. This final passivation has passivation openings 1008 to permit connection to the bond pads 1006.

Figure 11 illustrates an exemplary contact lens with an electronic insert comprising a blink detection system in accordance with the present embodiments (invention). The contact lens 1100 comprises a soft plastic portion 1102 which comprises an electronic insert 1104. This insert 1104 includes a lens 1106 which is activated by the electronics, for example focusing near or far depending on activation. Integrated circuit 1108 mounts onto the insert 1104 and connects to batteries 1110, lens 1106, and other components as necessary for the system. The integrated circuit 1108 includes a photosensor 1112 and associated photodetector signal path circuits. The photosensor 1112 faces outward through the lens insert and away from the eye, and is thus able to receive ambient light. The photosensor 1112 may be implemented on the integrated circuit 1108 (as shown) for example as a single photodiode or array of photodiodes. The photosensor 1112 may also be implemented as a separate device mounted on the insert 1104 and connected with wiring traces 1114. When the eyelid closes, the lens insert 1104 including photodetector 1112 is covered, thereby reducing

the light level incident on the photodetector 1112. The photodetector 1112 is able to measure the ambient light to determine if the user is blinking or not.

Additional embodiments of the blink detection algorithm may allow for more variation in the duration and spacing of the blink sequence, for example by timing the start of a second blink based on the measured ending time of a first blink rather than by using a fixed template or by widening the mask “don’t care” intervals (0 values).

It will be appreciated that the blink detection algorithm may be implemented in digital logic or in software running on a microcontroller. The algorithm logic or microcontroller may be implemented in a single application-specific integrated circuit, ASIC, with photodetection signal path circuitry and a system controller, or it may be partitioned across more than one integrated circuit.

It is important to note that the blink detection system of the present invention has broader uses than for vision diagnostics, vision correction and vision enhancement. These broader uses include utilizing blink detection to control a wide variety of functionality for individuals with physical disabilities. The blink detection may be set up on-eye or off-eye.

In accordance with another exemplary embodiment, a powered or electronic ophthalmic lens may incorporate an eyelid or lid position sensor. It is known that the eyelids protect the globe in a number of ways, including the blink reflex and the tear spreading action. The blink reflex of the eyelids prevents trauma to the globe by rapidly closing upon a perceived threat to the eye. Blinking also spreads tears over the globe’s surface to keep it moist and rinse away bacteria and other foreign matter. But the movement of the eyelids may also indicate other actions or functions at play. For example, when an individual focuses on a near object, the top eyelid drops. Accordingly detection of this movement may be utilized as an input into an electronic ophthalmic lens with a variable focus optic to correct for a loss in accommodation

associated with presbyopia. Alternately, when an individual attempts to focus on a distant object, he or she may squint. The eyelid motion associated with squinting may be utilized as an input into an electronic ophthalmic lens with a variable focus optic to zoom in on a distant object. In addition, an eyelid position sensor may also be utilized to alert an individual wearing an electronic ophthalmic lens that he or she is in danger of falling asleep. It is also important to note that the sensed data, in addition to or in alternate use may simply be utilized as part of a collection process rather than as a triggering event. For example, the sensed data may be collected, logged and utilized in treating medical conditions. In other words, it should also be appreciated that a device utilizing such a sensor may not change state in a manner visible to the user; rather the device may simply log data. For example, such a sensor could be used to determine if a user has the proper iris response throughout a day or if a problematic medical condition exists.

Referring now to Figure 12, there is illustrated an exemplary lid position sensor system on an eye 1200. The system is incorporated into a contact lens 1202. The top and bottom eyelids are shown, with the top lid having possible locations 1201, 1203, and 1205 in order of increasing closure. The bottom eyelid is also illustrated with levels of closure corresponding to the top lid; namely, locations 1207, 1209 and 1205. When the eyelids are closed, they occupy the same position; namely, 1205. The contact lens 1202 in accordance with the exemplary embodiment comprises a sensor array 1204. This sensor array 1204 includes one or more photosensors. In this exemplary embodiment, the sensor array 1204 comprises twelve (12) photosensors 1206a - 1206l. With the top lid at position 1201 and the bottom lid at position 1207, all photosensors 1206a - 1206l are exposed and receive ambient light, thereby creating a photocurrent which may be detected by an electronic circuit described herein. With the lids partially closed at positions 1203 and 1209, the top and bottom photosensors 1206a and 1206b are covered, receive less light than the other photosensors 1206c – 1206l, and output a correspondingly lower current which may be detected by the electronic circuit. With the lids totally closed in position 1205, all sensors 1206a – 1206l are covered with a

corresponding reduction in current. This exemplary system may be used to detect lid position by sampling each photosensor in the sensor array and using the photocurrent output versus sensor position to determine lid position. It will be appreciated that the photosensors should be placed in suitable locations on the contact lens, for example providing enough sample locations to reliably determine lid position while not obstructing the clear optic zone (roughly the area occupied by a dilated pupil.) This exemplary system may also be used to detect blinks by routinely sampling the sensors and comparing measurements over time. The lid position may be used by a controller (not shown) to initiate a function. For example, eyelids typically droop or drop when one focuses on a near object, as in reading. Thus, the lid position could be used, perhaps in conjunction with other sensors, to detect the desire for near focus in a presbyopic individual as briefly described above.

Figure 13 illustrates an exemplary system in which two eyes 1300 are partially covered with contact lenses 1302. Sensor arrays 1304 are present in both of the contact lenses 1302 to determine lid position, as previously described with respect to Figure 12. In this exemplary embodiment, the contact lenses 1302 each comprise an electronic communication component 1306. Electronic communication component 1306 in each contact lens 1302 permits two-way communication to take place between the contact lenses 1302. The electronic communication components 1306 may comprise radio frequency (RF) transceivers, antennas, interface circuitry for photosensors 1308, and associated or similar electronic components. The communication channel represented by line 1310 may comprise RF transmissions at the appropriate frequency and power with an appropriate data protocol to permit effective communication between the contact lenses 1302. Transmission of data between the two contact lenses 1302 may, for example, verify that both lids have closed in order to detect a true, purposeful blink rather than a wink or involuntary blink. The transmission may also allow a system to determine if both eyelids have closed by a similar amount, for example, that which is associated with a user reading up-close. Data transmission may also take place to an

external device, for example, spectacle glasses, a patch worn on the user's temple, or a smartphone.

Figures 14A and 14B illustrate an exemplary electronic system 1400 in which lid position photosensors, as set forth above, are used to trigger activity in a contact lens 1402 or more specifically, a powered or electronic ophthalmic lens. Figure 14A shows the exemplary electronic system 1400 on the lens 1402, and Figure 14B is an exploded view of the system 1400. Light 1401 is incident onto one or more photosensors 1404 as previously described with respect to Figure 12. These photosensors 1404 may be implemented with photodiodes, cadmium sulfide (CdS) sensors, or other technologies suitable for converting ambient light into current. Depending on the choice of photosensors 1404, amplifiers 1406 or other suitable circuitry may be required to condition the input signals for use by subsequent or downstream circuits. A multiplexer 1408 permits a single analog-to-digital converter 1410 (ADC) to accept inputs from multiple photosensors 1404. The multiplexer 1408 may be placed immediately after the photosensors 1404, before the amplifiers 1406, or may not be used depending on considerations for current consumption, die size, and design complexity. Since multiple photosensors 1404 are needed at various positions on the eye to detect lid position, sharing downstream processing components (for example amplifiers, an analog-to-digital converter, and digital signed processors) may significantly reduce the size needed for the electronic circuitry. The amplifiers 1406 create an output proportional to the input, with gain, and may function as transimpedance amplifiers which convert input current into output voltage. The amplifiers 1406 may amplify a signal to a useable level for the remainder of the system, such as giving the signal enough voltage and power to be acquired by the ADC 1410. For example, the amplifiers 1406 may be necessary to drive subsequent blocks since the output of the photosensors 1404 may be quite small and may be used in low-light environments. Amplifiers 1406 may also be implemented as variable-gain amplifiers, the gain of which may be adjusted by a system controller 1412 to maximize the dynamic range of the system 1400. In addition to providing gain, the amplifiers 1406 may include other analog signal conditioning circuitry, such as

filtering and other circuitry appropriate to the photosensor 1404 and amplifier 1406 output. The amplifiers 1406 may comprise any suitable device for amplifying and conditioning the signal output by the photosensor 1404. For example, the amplifiers 1404 may simply comprise a single operational amplifier or a more complicated circuit comprising one or more operational amplifiers.

As set forth above, the photosensors 1404 and the amplifiers 1406 are configured to detect incident light 1401 at various positions on the eye and convert the input current into a digital signal usable ultimately by the system controller 1412. The system controller 1412 is preferably preprogrammed to sample each photosensor 1404 on the eye to detect lid position and provide an appropriate output signal to an actuator 1414. The system controller 1412 also comprises associated memory. The system controller 1412 may combine recent samples of the photosensors 1404 to preprogrammed patterns correlating to lid open and squinting positions. When the pattern matches that of lid droop associated with near accommodation, for example, the top eyelid drooping, the system controller 1412 may trigger the actuator 1414 to change focus state of a variable power optic associated with the powered contact lens. Recording a user's eyelid patterns under various ambient light and focal distance situations may be required to program the system controller 1412 for reliable detection. The system 1400 may need to differentiate between eyelid position changes, normal changes in ambient light, shadows, and other phenomena. This differentiation may be accomplished through proper selection of the sampling frequency, amplifier gain, and other system parameters, optimization of sensors placement in the contact lens, determination of lid position patterns, recording ambient light, comparing each photosensor to adjacent and all photosensors, and other techniques to discern lid position uniquely.

In this exemplary embodiment, the ADC 1410 may be used to convert a continuous, analog signal output from the amplifiers 1406 through the multiplexer into a sampled, digital signal appropriate for further signal processing. For example, the ADC

1410 may convert an analog signal output from the amplifiers 1406 into a digital signal that may be useable by subsequent or downstream circuits, such as a digital signal processing system or microprocessor 1416. A digital signal processing system or digital signal processor 1416 may be utilized for digital signal processing, including one or more of filtering, processing, detecting, and otherwise manipulating/processing sampled data to permit incident light detection for downstream use. The digital signal processor 1416 may be preprogrammed with various lid patterns. The digital signal processor 1416 also comprises associated memory. The digital signal processor 1416 may be implemented utilizing analog circuitry, digital circuitry, software, and/or preferably a combination thereof. The ADC 1410 along with the associated amplifiers 1406 and digital signal processor 1416 are activated at a suitable rate in agreement with the sampling rate previously described, for example, every one hundred (100) ms.

A power source 1418 supplies power for numerous components comprising the lid position sensor system 1400. The power source 1418 may also be utilized to supply power to other devices on the contact lens. The power may be supplied from a battery, energy harvester, or other suitable means as is known to one of ordinary skill in the art. Essentially, any type of power source 1418 may be utilized to provide reliable power for all other components of the system. A lid position sensor array pattern, processed from analog to digital, may enable activation of the system controller 1412 or a portion of the system controller 1412. Furthermore, the system controller 1412 may control other aspects of a powered contact lens depending on input from the digital signal processor 1408, for example, changing the focus or refractive power of an electronically controlled lens through the actuator 1414.

Referring now to Figure 15 there is illustrated an exemplary output characteristic for three photosensors positioned at three different vertical positions on the contact lens. The output characteristics may represent the current proportional to incident light on each photosensor or may represent a downstream signal, for example digital sampled data values versus time at the output of the ADC (element 1410 in Figure 14).

Total incident light 1502 increases, holds steady, then decreases, for example when walking from a dark room to a bright hallway then back to a dark room. All three photosensors 1504, 1506, and 1508 would output a signal similar to that of the ambient light if the eyelid remained open, illustrated by dotted lines 1501 and 1503 for

5 photosensors 1504 and 1508. In addition to the ambient light level 1502 changing, squinting of the eyelids is indicated by position 1510, different than that of the lid open positions 1512 and 1514. When the lid closes due to squinting, upper photosensor 1504 becomes covered by the upper eyelid and outputs a correspondingly lower level due to obstruction of the photosensor by the eyelid. Despite ambient light 1502 increasing,
10 photosensor 1504 receives less light and outputs a lower signal due to the partially closed eyelid. Similar response is observed with photosensor 1508 which becomes covered during squinting. Middle sensor 1506 is not covered during squinting and thus continues to see the light level increase, with a corresponding increase in output level. While this example illustrates one particular case, it should be apparent how various
15 configurations of sensor position and eyelid movement could be detected.

Figures 16A and 16B illustrate an alternate exemplary detection system 1600 incorporated into a contact lens 1602. Once again Figure 16A shows the system 1600 on the lens 1602 and Figure 16B show an exploded view of the system 1600. In this
20 exemplary embodiment, capacitive touch sensors 1604 are utilized instead of photosensors. Capacitive touch sensors are common in the electronics industry, for example in touch-screen displays. The basic principle is that a variable capacitor 1604 is implemented in a physical manner such that the capacitance varies with proximity or touch, for example, by implementing a grid covered by a dielectric. Sensor conditioners
25 1604 create an output signal proportional to the capacitance, for example, by measuring the change in an oscillator comprising the variable capacitor or by sensing the ratio of the variable capacitor to a fixed capacitor with a fixed-frequency AC signal. The output of the sensor conditioners 1606 may be combined with a multiplexer 1608 to reduce downstream circuitry. In this exemplary embodiment, the necessary signal conditioning
30 circuitry as described above with respect to Figure 14 is omitted for simplicity. A system

controller 1610 receives inputs from the capacitance sensor conditioner 1606 via the multiplexor 1608, for example, by activating each sensor in order and recording the values. It may then compare measured values to pre-programmed patterns and historical samples to determine lid position. It may then activate a function in an actuator 1612, for example, causing a variable-focus lens to change to a closer focal distance. The capacitor touch sensors 1604 may be laid out in a physical pattern similar to that previously described for the photodetectors, but would be optimized for detecting changes in capacitance with lid position. The sensors, and for that matter the whole electronic system, would be encapsulated and insulated from the saline contact lens environment. As the eyelid covers a sensor 1604, the change in capacitance would be detected rather than the change in ambient light previously described.

It is important to note that ADC's and digital signal processing circuitry may be utilized in accordance with the capacitive touch sensors if needed as illustrated with respect to the photosensors of Figure 14B.

In one exemplary embodiment, the electronics and electronic interconnections are made in the peripheral zone of a contact lens rather than in the optic zone. In accordance with an alternate exemplary embodiment, it is important to note that the positioning of the electronics need not be limited to the peripheral zone of the contact lens. All of the electronic components described herein may be fabricated utilizing thin-film technology and/or transparent materials. If these technologies are utilized, the electronic components may be placed in any suitable location as long as they are compatible with the optics.

The activities of the digital signal processing block and system controller (1416 and 1412 in Figure 14B, respectively and system controller 1610 in Figure 16B) depend on the available sensor inputs, the environment, and user reactions. The inputs, reactions, and decision thresholds may be determined from one or more of ophthalmic research, pre-programming, training, and adaptive/learning algorithms. For example,

the general characteristics of eyelid movement may be well-documented in literature, applicable to a broad population of users, and pre-programmed into system controller. However, an individual's deviations from the general expected response may be recorded in a training session or part of an adaptive/learning algorithm which continues to refine the response in operation of the electronic ophthalmic device. In one exemplary embodiment, the user may train the device by activating a handheld fob, which communicates with the device, when the user desires near focus. A learning algorithm in the device may then reference sensor inputs in memory before and after the fob signal to refine internal decision algorithms. This training period could last for one day, after which the device would operate autonomously with only sensor inputs and not require the fob.

An intraocular lens or IOL is a lens that is implanted in the eye and replaces the crystalline lens. It may be utilized for individuals with cataracts or simply to treat various refractive errors. An IOL typically comprises a small plastic lens with plastic side struts called haptics to hold the lens in position within the capsular bag in the eye. Any of the electronics and/or components described herein may be incorporated into IOLs in a manner similar to that of contact lenses.

Although shown and described in what is believed to be the most practical and preferred embodiments, it is apparent that departures from specific designs and methods described and shown will suggest themselves to those skilled in the art and may be used without departing from the spirit and scope of the invention. The present invention is not restricted to the particular constructions described and illustrated, but should be constructed to cohere with all modifications that may fall within the scope of the appended claims.

WHAT IS CLAIMED IS:

1. A powered ophthalmic lens, the powered ophthalmic lens comprising:
a contact lens including an optic zone and a peripheral zone; and
an eyelid position sensor system incorporated into the peripheral zone of the contact lens, the eyelid position sensor system including a sensor array having a plurality of individual sensors to detect eyelid position, a system controller configured to sample each individual sensor in the sensor array to detect eyelid position and provide an output control signal, and at least one actuator configured to receive the output control signal and implement a predetermined function.
2. The powered ophthalmic lens according to Claim 1, wherein the plurality of individual sensors comprise photosensors for detecting light incident on the eye.
3. The powered ophthalmic lens according to Claim 2, wherein the eyelid position sensor system further comprises an amplifier connected to the photosensors, the amplifier being configured to condition signals output from the photosensors for downstream use.
4. The powered ophthalmic lens according to Claim 3, wherein the eyelid position sensor system further comprises a multiplexer configured to receive multiple inputs from the amplifier and output a single signal.
5. The powered ophthalmic lens according to Claim 4, wherein the eyelid position sensor system further comprises an analog-to-digital converter configured to convert the analog signal from the amplifier to a sampled, digital signal for further signal processing.

6. The powered ophthalmic lens according to Claim 5, wherein the eyelid position sensor system further comprises a digital signal processor configured to receive an output from the analog-to-digital converter and perform digital signal processing, including one or more of filtering, processing and detecting sampled data to permit incident light detection for downstream use.

7. The powered ophthalmic lens according to Claim 6, wherein the digital signal processor comprises associated memory.

8. The powered ophthalmic lens according to Claim 1, further comprising a power supply.

9. The powered ophthalmic lens according to Claim 1, wherein the plurality of individual sensors comprise capacitive touch sensors for detecting contact or proximity and outputting a signal indicative thereof.

10. The powered ophthalmic lens according to Claim 9, wherein the sensor system further comprises sensor conditioners that output a signal proportional to capacitance for downstream use.

11. The powered ophthalmic lens according to Claim 10, wherein the eyelid position sensor system further comprise a multiplexer configured to receive multiple inputs from the sensor conductors and output a single signal to the system controller.

12. The powered ophthalmic lens according to Claim 1, wherein the eyelid position sensor system further comprises a communication channel for coordinating action between pairs of powered contact lenses.

13. A powered ophthalmic lens, the powered ophthalmic lens comprising:
a contact lens; and

an eyelid position sensor system incorporated into the contact lens, the eyelid position sensor system including a sensor array having a plurality of individual sensors to detect eyelid position, a system controller configured to sample each individual sensor in the sensor array to detect eyelid position and provide an output control signal, and at least one actuator configured to receive the output control signal and implement a predetermined function.

14. The powered ophthalmic lens according to Claim 13, wherein the plurality of individual sensors comprise photosensors for detecting light incident on the eye.

15. The powered ophthalmic lens according to Claim 14, wherein the eyelid position sensor system further comprises an amplifier connected to the photosensors, the amplifier being configured to condition signals output from the photosensors for downstream use.

16. The powered ophthalmic lens according to Claim 15, wherein the eyelid position sensor system further comprises a multiplexer configured to receive multiple inputs from the amplifier and output a single signal.

17. The powered ophthalmic lens according to Claim 16, wherein the eyelid position sensor system further comprises an analog-to-digital converter configured to convert the analog signal from the amplifier to a sampled, digital signal for further signal processing.

18. The powered ophthalmic lens according to Claim 17, wherein the eyelid position sensor system further comprises a digital signal processor configured to receive an output from the analog-to-digital converter and perform digital signal processing, including one or more of filtering, processing and detecting sampled data to permit incident light detection for downstream use.

19. The powered ophthalmic lens according to Claim 18, wherein the digital signal processor comprises associated memory.

20. The powered ophthalmic lens according to Claim 13, further comprising a power supply.

21. The powered ophthalmic lens according to Claim 13, wherein the plurality of individual sensors comprise capacitive touch sensors for detecting contact or proximity and outputting a signal indicative thereof.

22. The powered ophthalmic lens according to Claim 21, wherein the sensor system further comprises sensor conditioners that output a signal proportional to capacitance for downstream use.

23. The powered ophthalmic lens according to Claim 22, wherein the eyelid position sensor system further comprise a multiplexer configured to receive multiple inputs from the sensor conductors and output a single signal to the system controller.

24. The powered ophthalmic lens according to Claim 13, wherein the eyelid position sensor system further comprises a communication channel for coordinating action between pairs of powered contact lenses.

25. A powered ophthalmic lens, the powered ophthalmic lens comprising:
an intraocular lens; and
an eyelid position sensor system incorporated into the intraocular lens, the eyelid position sensor system including a sensor array having a plurality of individual sensors to detect eyelid position, a system controller configured to sample each individual sensor in the sensor array to detect eyelid position and provide an output control signal, and at least one actuator configured to receive the output control signal and implement a predetermined function.