

HIGH PLUS CENTER TREATMENT ZONE LENS DESIGN AND METHOD FOR PREVENTING AND/OR SLOWING MYOPIA PROGRESSION

CROSS REFERENCE TO RELATED APPLICATION

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This patent application is a continuation-in-part of U.S. Patent Application Serial No. 14,464,182, filed August 20, 2014.

BACKGROUND OF THE INVENTION

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Field of the Invention

The present invention relates to ophthalmic lenses, and more particularly, to contact lenses designed to slow, retard, or prevent myopia progression in the wearer.

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The ophthalmic lenses of the present invention comprise a high plus or high ADD treatment zone, thereby preventing and/or slowing myopia progression.

Discussion of the Related Art

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Common conditions which lead to reduced visual acuity are myopia and hyperopia, for which corrective lenses in the form of spectacles, or rigid or soft contact lenses, are prescribed. The conditions are generally described as the imbalance between the length of the eye and the focus of the optical elements of the eye. Myopic eyes focus in front of the retinal plane and hyperopic eyes focus behind the retinal plane. Myopia typically develops because the axial length of the eye grows to be longer than the focal length of the optical components of the eye, that is, the eye grows too long. Hyperopia typically develops because the axial length of the eye is too short compared with the focal length of the optical components of the eye, that is, the eye does not grow enough.

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Myopia has a high prevalence rate in many regions of the world. Of greatest concern with this condition is its possible progression to high myopia, for example greater than five (5) or six (6) diopters, which dramatically affects one's ability to function without optical aids. High myopia is also associated with an increased risk of retinal disease, cataracts, and glaucoma.

Corrective lenses are used to alter the gross focus of the eye to render a clearer image at the retinal plane, by shifting the focus from in front of the plane to correct myopia, or from behind the plane to correct hyperopia, respectively. However, the corrective approach to the conditions does not address the cause of the condition, but is merely prosthetic or symptomatic.

Most eyes do not have simple myopia or hyperopia, but have myopic astigmatism or hyperopic astigmatism. Astigmatic errors of focus cause the image of a point source of light to form as two mutually perpendicular lines at different focal distances. In the foregoing discussion, the terms myopia and hyperopia are used to include simple myopia or myopic astigmatism and hyperopia and hyperopic astigmatism respectively.

Emmetropia describes the state of clear vision where an object at infinity is in relatively sharp focus with the crystalline lens relaxed. In normal or emmetropic adult eyes, light from both distant and close objects and passing through the central or paraxial region of the aperture or pupil is focused by the crystalline lens inside the eye close to the retinal plane where the inverted image is sensed. It is observed, however, that most normal eyes exhibit positive longitudinal spherical aberration, generally in the region of about +0.50 Diopters (D) for a 5.0 mm aperture, meaning that rays passing through the aperture or pupil at its periphery are focused +0.50 D in front of the retinal plane when the eye is focused to infinity. As used herein the measure D is the dioptric power, defined as the reciprocal of the focal distance of a lens or optical system, in meters.

The spherical aberration of the normal eye is not constant. For example, accommodation (the change in optical power of the eye derived primarily through change to the internal crystalline lens) causes the spherical aberration to change from positive to negative.

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As noted, myopia typically occurs due to excessive axial growth or elongation of the eye. It is now generally accepted, primarily from animal research, that axial eye growth can be influenced by the quality and focus of the retinal image. Experiments performed on a range of different animal species, utilizing a number of different experimental paradigms, have illustrated that altering retinal image quality can lead to consistent and predictable changes in eye growth.

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Furthermore, defocusing the retinal image in both chick and primate animal models, through positive lenses (myopic defocus) or negative lenses (hyperopic defocus), is known to lead to predictable (in terms of both direction and magnitude) changes in eye growth, consistent with the eyes growing to compensate for the imposed defocus. The changes in eye length associated with optical blur have been shown to be modulated by changes in both scleral growth and choroidal thickness. Blur with positive lenses, which leads to myopic blur and decreases scleral growth rate, results in hyperopic refractive errors. Blur with negative lenses, which leads to hyperopic blur and increases scleral growth rate, results in myopic refractive errors. These eye growth changes in response to retinal image defocus have been demonstrated to be largely mediated through local retinal mechanisms, as eye length changes still occur when the optic nerve is damaged, and imposing defocus on local retinal regions has been shown to result in altered eye growth localized to that specific retinal region.

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In humans there is both indirect and direct evidence that supports the notion that retinal image quality can influence eye growth. A variety of different ocular conditions, all of which lead to a disruption in form vision, such as ptosis, congenital cataract, corneal opacity, vitreous hemorrhage and other ocular diseases, have been found to be associated with abnormal eye growth in young humans, which suggests that relatively

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large alterations in retinal image quality do influence eye growth in human subjects. The influence of more subtle retinal image changes on eye growth in humans has also been hypothesized based on optical errors in the human focusing system during near work that may provide a stimulus for eye growth and myopia development in humans.

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One of the risk factors for myopia development is near work. Due to accommodative lag or negative spherical aberration associated with accommodation during such near work, the eye may experience hyperopic blur, which in turn stimulates myopia progression as discussed above. Moreover, the accommodation system is an active adaptive optical system; it constantly reacts to near-objects, as well as optical designs. No matter what optical designs one puts on the eye, when the eye accommodates to near-objects, continuous hyperopic defocus will be present and make the eye myopic. Therefore, one way to design optics to slow the rate of myopia progression is to utilize a high plus signal to the retina through use of high ADD or plus powers.

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U.S. Patent No. 6,045,578 discloses that the addition of positive spherical aberration on the contact lens will reduce or control the progression of myopia. The method includes changing the spherical aberration of an ocular system by a direction and degree related to alter the growth in eye length, in other words emmetropization may be regulated by spherical aberration. In this process, the cornea of a myopic eye is fitted with a lens having increasing dioptric power away from the lens center. Paraxial light rays entering the central portion of the lens are focused on the retina of the eye, producing a clear image of an object. Marginal light rays entering the peripheral portion of the cornea are focused in a plane between the cornea and the retina, and produce positive spherical aberration of the image on the latter. This positive spherical aberration produces a physiological effect on the eye which tends to inhibit growth of the eye, thus mitigating the tendency for the myopic eye to grow longer.

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Although the level of positive spherical aberration and/or plus power required to achieve an optimum slowdown in the myopia progression rate is unclear, researchers in

the field have attempted to use multi-zone devices with regions of positive power of about +1.50 to a maximum of +3.00D ADD in an attempt to slow the progression of myopia. It is important to note that a positive power of up to 4.00 diopters has also been attempted. The approach resulted in treatment results of less than about 50 percent. Treatment efficacy is defined as the relative change of axial length and/or spherical equivalent refraction from baseline for a test group compared to the change of axial length and/or spherical equivalent refraction of a control group over a year or a predetermined time period. There remains a need for a myopia control treatment with efficacy greater than 50 percent and closer to 100 percent. Intuitively adding treatment zones of high plus power would provide greater treatment as the ocular growth response in animals was proportional to the power of the optical stimulus as reported by Wildsoet & Wallman, Vision Research 1995.

However, conventional wisdom in the field of bifocal or multifocal ophthalmic lenses assumes lenses with high plus or high ADD power may have deleterious effects on vision and contrast sensitivity as reported by Ardaya et al, Optometry 2004. Further, Smith et al (US7025460) teaches against going to powers outside the range normally found in bifocal or multifocal lenses for presbyopia. They state "It is important to note that, while the appropriate type of refractive defocus can drive eye growth (or non-growth) leading to myopia (or its regression) in the phenomenon of lens compensation, when the amount of refractive defocus is great, there may be such a large degradation in image quality due to the severe defocus that the optical state may change into the phenomenon of form deprivation and may induce myopia in that way." Further, they teach "that the maximum amount of relative curvature of field before substantial vision degradation occurs, which leads to form deprivation myopia, to be around the spherical equivalent of +3.50D to +4.00D, which represents the upper limit for negative curvature of field for effective treatment of myopia." This belief has discouraged researchers from pursuing high plus treatment zones for myopia control.

To the contrary, applicant's research shows that using a design with a central distance zone and a high plus or high ADD treatment zone having a plus power greater

than about 3.00D reduces visual acuity loss relative to low conventional plus type designs with no significant additional impact on contrast sensitivity. This is also supported in recent work by De Gracia et al, OVS 2013, although they only investigated up to 4.00D of ADD power and did not relate the work to a potential benefit in myopia progression control. This breakthrough enables ophthalmic designs to achieve a meaningful greater than 50 percent slowdown in myopia progression without further negatively impacting visual acuity.

Further, significantly higher plus power relative to the distance power is not expected to lead to reduced accommodation as may occur with a lower ADD power design where a subject might rely to some extent on the ADD power for clear vision during near work activities, as has been observed during the course of our research. This reduced accommodation may lead to hyperopic defocus of rays passing through the distance portion of the device. In the current invention, the subject must accommodate over the distance portion of the lens for near vision correction as objects imaged through the treatment zones of high plus powers are sufficiently out of focus that they cannot be cleared with the accommodation-convergence system.

Another researchers in the field, R. Griffin WO2012/173891, claims to relieve accommodative lag and accommodative stresses that lead to myopia progression through the creation of an artificial pinhole that results in increased depth of focus and depth of field. In their intellectual property, "the eye's accommodation is more relaxed" in contrast to the present invention.

With reference now to FIG. 1, the graph illustrates a device with a design that incorporates a distance zone to correct for distance vision and a peripheral zone of variable plus power. Visual acuity was measured using a four forced choice method with progressively smaller Snellen optotypes. Increasing peripheral plus power to about +2.00D to +3.00D causes an increasing loss of high contrast visual acuity, as typical of multifocal type designs for presbyopes. As the peripheral power continues to increase; however, the relative effect on visual acuity surprisingly improves and plateaus, so that

by above about +4.00D to +5.00D peripheral plus, the visual acuity loss becomes relatively constant. This is of significance for the design of myopia control lenses, since higher plus power is found (with animal models) to have a greater impact on eye growth, as reported in Wildsoet & Wallman, Vision Research 1995.

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However, further optimization of plus power designs is required to optimize image quality. With reference now to FIG. 2, power profiles are illustrated having +5.00D or +10.00D power beyond a 2.25 mm radial location from a center of a lens. Rays passing through these high plus or high ADD power regions form sharp foci in
10 front of the retina. However, due to continued propagation to the retina, these rays form a ring-like defocus blur on the retina.

As shown in the point spread function (PSF) cross section of FIG. 3, rays coming from the +5.00D and +10.00D regions form separate spikes on the retina. Thus, if one
15 looks at a point light source through one of these +5.00D or +10.00D high plus lenses, his/her retina would receive a peak signal surrounded by a ring-like halo. Usually, this is not a problem when one reads letters or resolves fine details of objects because the halo is so dim that the human doesn't perceive it. Nevertheless, this is a problem if a person looks at a black/white edge, a white/black edge, a light/dark edge, a dark/light
20 edge and/or any high contrast edge, as energy from the white/black/light background can leak into the black/white/dark due to the presence of the spike in PSF.

With reference now to FIG. 4, the image cross section for the +5.00D and +10.00D power profiles of FIG. 2 at an entrance pupil size of 6.0 mm are shown by
25 convolving the PSF with a black/white edge in object space. A lens having 0.00D power forms a sharp edge between the black and white (at 0.0 mm location) and thus does not have a halo-like structure. On the other hand, the lenses with +5.00D and +10.00D regions do not have a sharp edge between black and white, thereby resulting in images in which the black background is not completely black, and the white background is not
30 completely white at the 'edge' in the image.

Accordingly, the presence of halo is an inherent property of high plus or high ADD lens designs. The present invention is directed to lenses having high plus power treatment zones that are suitable for the use in treating, controlling, or reducing the progression of myopia while also minimizing a halo effect.

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SUMMARY OF THE INVENTION

The lens design of the present invention overcomes the limitations of the prior art by providing lenses that ensure distance vision correction and have high plus power treatment zones that treat, control, or reduce the progression of myopia while also minimizing a halo effect.

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In accordance with one aspect, the present invention is directed to an ophthalmic lens for at least one of slowing, retarding or preventing myopia progression and for minimizing a halo effect. The ophthalmic lens comprises an optic zone, the optic zone including a center zone configured as a myopia progression treatment zone, the center zone comprising an ADD power of between +0.5 diopters and +20.0 diopters relative to the negative power required to correct myopia, and at least one peripheral zone surrounding the center zone, the at least one peripheral zone comprising a myopia vision correction region with a negative power for myopic vision correction; and an outer zone surrounding the optic zone.

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The ophthalmic lens comprises a center zone with high plus power as a myopic progression treatment zone. High plus power has the same meaning as high ADD power and does not necessarily result in a high positive power in the treatment zone as is the case, say, of vision correction of high hyperopia. Rather it refers to a difference in power between the treatment zone and the myopic vision correction zone that is higher than traditionally used for the reading addition powers classically used in bifocal, multifocal or progressive addition lenses for presbyopia. More specifically, the contact lens comprises an optic zone and an outer zone. The optic zone comprises a center zone and a first peripheral zone. In other embodiments, a different number of zones

may be present as is explained in detail subsequently. In this exemplary embodiment, the center zone has a diameter that ranges from 0.50 mm to 4.00 mm with a power ranging from +5 diopters to +15 diopters. In other embodiments, the power can be lower, for example, +2.5 diopters and higher, for example +20 diopters. Also in this exemplary embodiment, the first peripheral zone has a negative power for myopic vision correction. In other words, the power to correct the individual's refractive error, myopia, resides in the first peripheral zone rather than in the center of the lens. The contact lens may include one or more additional plus powered concentric treatment zones outside of the first peripheral zone. For example, low plus center zone and higher plus peripheral zones or high plus center zone with lower plus peripheral zones. More specifically, the first peripheral zone which has the power to correct the refractive error is surrounded with plus power treatment zones. It is important to note that each of the treatment zones may have the same plus power or different plus powers. The diameter of the first peripheral zone and the one or more additional plus powered concentric treatment zones is selected to provide a balance between adequate vision and myopia control treatment. It will be readily apparent to those skilled in the art that the peripheral zone diameters will be chosen depending on the diameter of the central zone to achieve a balance between obtaining adequate myopia control and vision. For example, in a preferred embodiment, the diameter of the central zone is 1.0 mm, the outer diameter of the first peripheral zone is 2.6 mm, and the outer diameter of the second peripheral zone is 3.6 mm. In that example, there may be additional peripheral zones within the optic zone past 3.6 mm.

The high plus contact lens design of the present invention provides a simple, cost-effective and efficacious means and method for preventing and/or slowing myopia progression which is increasing throughout the world.

BRIEF DESCRIPTION OF THE DRAWINGS

The foregoing and other features and advantages of the invention will be apparent from the following, more particular description of preferred embodiments of the invention, as
5 illustrated in the accompanying drawings.

FIG. 1 illustrates a graph showing changes in visual acuity as plus power is added in a peripheral zone.

10 FIG. 2 illustrates power profiles of two lenses, one having a +5.00D treatment zone and the other having a +10.00D treatment zone.

FIG. 3 illustrates a cross section of the point spread function for the power profiles of FIG. 2 at an entrance pupil size of 6.0 mm.

15 FIG. 4 illustrates an image cross section of the power profiles of FIG. 2.

FIG. 5a illustrates a point spread function for five power profiles.

20 FIG. 5b illustrates the image cross section of the power profiles of FIG. 5a.

FIGS. 6a-c illustrates power profiles of three lenses according to the present invention.

25 FIGS. 7a-c illustrates the image cross section of the power profiles of FIGS. 6a-c, respectively.

FIGS. 8a-c illustrates power profiles of three additional lenses according to the present invention.

FIG. 9 is a diagrammatic representation of an exemplary contact lens in accordance with the present invention.

5 FIG. 10 is a diagrammatic representation of a first alternative exemplary contact lens in accordance with the present invention.

FIG. 11 is a diagrammatic representation of a second alternative exemplary contact lens in accordance with the present invention.

10 FIG. 12 is a graphical representation of the loss in visual acuity versus central zone size (i.e. diameter) over four ADD powers for a 5.5 mm pupil size in accordance with the present invention.

15 FIG. 13 is a graphical representation of the loss in visual acuity versus central zone diameter in a lens with a center plus design having a +10 diopter power for both a 5.5 mm pupil and a 3.5 mm pupil in accordance with the present invention.

20 FIG. 14 is a graphical representation of the size of halo in degrees versus central zone diameter in a lens with a center plus design having a +10 diopter power for both a 5.5 mm pupil and a 3.5 mm pupil in accordance with the present invention.

25 FIG. 15 is a graphical representation of the halo brightness versus central zone diameter in a lens with a center plus design having a +10 diopter power for both a 5.5 mm pupil and a 3.5 mm pupil in accordance with the present invention.

FIGS. 16A – 16D illustrate various exemplary power profiles in accordance with the present invention.

DETAILED DESCRIPTION OF THE INVENTION

In accordance with the present invention, an ophthalmic lens has at least one high plus or high ADD treatment zone surrounding a center zone for treating, preventing, or slowing myopia progression while also minimizing any halo effect at a black/white edge. In accordance with alternate exemplary embodiments, ophthalmic lenses are described with center plus designs and are described with respect to Figure 10 and beyond.

With reference now to FIG. 5a (inset graph), five power profiles are illustrated: 1) a power profile having a +5.00D treatment zone; 2) a power profile having a +10.00D treatment zone; 3) two zig-zag or sawtooth power profiles with periodic power modulation between about +5.00D and about +12D; and 4) a power profile having a gradual power increase from +5.00D to +12.00D.

In the PSF cross section of FIG. 5a (main graph), the two ring spikes of the +5.00D and +10.00D ADD power profiles have a much higher intensity than the other three power profiles, because the latter three designs have continuous power modulation. On the other hand, the latter three designs carry wider ring spikes. The convolution between the spikes with wider width and lower intensity yields a smooth transition of halo intensity between black and white edges, as shown in FIG. 5b (inset graph), as compared to the sharp edges for the +5.00D and +10.00D power profiles, as shown in the main graph of FIG. 5b. As a result of the smooth transition, human vision finds any halo effect for the latter three power profiles less bothersome than the halo effect resulting from the abrupt intensity profiles.

With reference now to FIGS. 6a-6c, the power profiles of three lens designs according to the present invention are illustrated. For each design, the power profile comprises a center zone, which may have a negative focal power to correct existing a myopic distance vision condition (i.e., paraxial power). The diameter of the center zone may be about 3 mm to about 7 mm, for example 4.3 mm. Each lens design also

comprises at least one treatment zone that surrounds the center zone. The at least one treatment zone carries a large amount of high ADD or high plus power relative to the power in the center zone.

5 As illustrated in FIGS. 6a-b, the power profiles rise gradually and continuously from a margin of the center zone (point A) to a point within the at least one treatment zone (point B). In specific embodiments, the location of point B is between 3.0 mm and 4.5 mm from a center of the lens. The at least one treatment zone may remain constant from point B to a margin of an optic zone (point C, for example at 4.5 mm). As
10 illustrated in FIG. 6c, the power profile may zig-zag or oscillate as the power rises from point A to point B and/or point C and does not need to be monotonic. In specific embodiments, the at least one treatment zone may have a dioptric power ranging from about +1D to about +15D.

15 According to the present invention, a gradual and/or periodic change of plus power in the at least one treatment zone mitigates the halo effect because such variations smoothen the intensity profile at sharp black and white edges. The halo intensity profiles of the three lens designs of FIGS. 6a-c are shown in FIGS. 7a-c, respectively. All three designs have a smooth halo intensity profile at the black/white
20 edge.

While lenses of the present invention are designed so that the halo becomes less bothersome to the human eye, it may be difficult to reduce the halo effect when the lens becomes decentered on the eye. When a lens decenters, the ring-like structure in PSF
25 becomes asymmetric, and energy will shift from one side of PSF to another side. As a result, one side of ring-like structure in PSF will have a much higher intensity, and the halo intensity will increase. The halo will become obvious regardless to the halo intensity profile. Hence, the utilized lens geometrical design should preferably result in good lens centration on the eye to further minimize potential for the visual artifacts.

With reference now to FIGS. 8a-c, the power profiles for three additional lens designs according to the present invention are illustrated. These three lens designs have 1) at least one enhanced treatment zone in which power is added within the center zone, and 2) at least one treatment zone. The at least one enhanced treatment zone may vary in diameter from about 0.5 mm to about 1.0 mm. The power magnitude of the at least one enhanced treatment zone may range from about +1D (FIG. 8a) to about +10D (FIGS. 8b-c). The at least one treatment zone have a gradual and/or period change in plus or ADD power as discussed above or may have a stepped increase in plus or ADD power. The power magnitude of the at least one treatment zone may range from about +5D to about +15D (FIGS. 8b-c).

Referring now to FIG. 9, there is illustrated a schematic diagrammatic view of a contact lens 900 in accordance with an embodiment of the present invention. The contact lens 900 comprises an optic zone 902 and an outer zone 904. The optic zone 902 comprises a first, center zone 906 and at least one peripheral zone 908. In specific embodiments, the diameter of the optic zone 902 may be selected to be 8.0 mm, the diameter of the substantially circular first zone 906 may be selected to be 4.0 mm, and the boundary diameters of an annular outer peripheral zone 908 may be 5 mm and 6.5 mm as measured from the geometric center of the lens 900. It is important to note that FIG. 9 only illustrates an exemplary embodiment of the present invention. For example, in this exemplary embodiment, the outer boundary of the at least one peripheral zone 908 does not necessarily coincide with the outer margin of the optic zone 902, whereas in other exemplary embodiments, they may coincide. The outer zone 904 surrounds the optic zone 902 and provides standard contact lens features, including lens positioning and centration. In accordance with one exemplary embodiment, the outer zone 904 may include one or more stabilization mechanisms to reduce lens rotation when on eye.

It is important to note that the various zones in FIG. 9 are illustrated as concentric circles, the zones may comprise any suitable round or non-round shapes such as an elliptical shape.

It is important to note that as the entrance pupil size of the eye varies among subpopulations, in certain exemplary embodiments, the lens design may be customized to achieve both good foveal vision correction and myopic treatment efficacy based on the patient's average pupil size. Moreover, as pupil size correlates with refraction and age for pediatric patients, in certain exemplary embodiments, the lens may be further optimized towards subgroups of the pediatric subpopulation with specific age and/or refraction based upon their pupil sizes. Essentially, the power profiles may be adjusted or tailored to pupil size to achieve an optimal balance between foveal vision correction and minimization of halo effect resulting from a high plus or high ADD treatment zone.

Currently available contact lenses remain a cost effective means for vision correction. The thin plastic lenses fit over the cornea of the eye to correct vision defects, including myopia or nearsightedness, hyperopia or farsightedness, astigmatism, i.e. asphericity in the cornea, and presbyopia, i.e., the loss of the ability of the crystalline lens to accommodate. Contact lenses are available in a variety of forms and are made of a variety of materials to provide different functionality.

Daily wear soft contact lenses are typically made from soft polymer materials combined with water for oxygen permeability. Daily wear soft contact lenses may be daily disposable or extended wear disposable. Daily disposable contact lenses are usually worn for a single day and then thrown away, while extended wear or frequent replacement disposable contact lenses are usually worn for a period of up to thirty days. Colored soft contact lenses use different materials to provide different functionality. For example, a visibility tint contact lens uses a light tint to aid the wearer in locating a dropped contact lens, enhancement tint contact lenses have a translucent tint that is meant to enhance one's natural eye color, the color tint contact lens comprises a darker, opaque tint meant to change one's eye color, and the light filtering tint contact lens functions to enhance certain colors while muting others. Rigid gas permeable hard contact lenses are made from siloxane-containing polymers but are more rigid than soft contact lenses and thus hold their shape and are more durable. Bifocal contact lenses are designed specifically for patients with presbyopia and are available in both soft and

rigid varieties. Toric contact lenses are designed specifically for patients with astigmatism and are also available in both soft and rigid varieties. Combination lenses combining different aspects of the above are also available, for example, hybrid contact lenses.

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It is important to note that the lens designs of the present invention may be incorporated into any number of different contact lenses formed from any number of materials. Specifically, the lens design of the present invention may be utilized in any of the contact lenses described herein, including, daily wear soft contact lenses, rigid gas permeable contact lenses, bifocal contact lenses, toric contact lenses and hybrid
10 contact lenses. In addition, although the invention is described with respect to contact lenses, it is important to note that the concept of the present invention may be utilized in spectacle lenses, intraocular lenses, corneal inlays and onlays.

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In accordance with another exemplary embodiment, an ophthalmic lens comprises a center zone with high plus power as a myopic progression treatment zone. Once again, high plus power has the same meaning as high ADD power and does not necessarily result in a high positive power in the treatment zone as is the case, say, of vision correction of high hyperopia. Rather it refers to a difference in power between
20 the treatment zone and the myopic vision correction zone that is higher than traditionally used for the reading addition powers classically used in bifocal, multifocal or progressive addition lenses for presbyopia. Referring to FIG. 10, there is illustrated a diagrammatic representation of a contact lens 1000 in accordance with this exemplary embodiment. The contact lens 1000 comprises an optic zone 1002 and an outer zone
25 1004. The optic zone 1002 comprises a center zone 1006 and a first peripheral zone 1008. In this exemplary embodiment, the center zone 1006 has a diameter that ranges from 0.50 mm to 4.0 mm with a power ranging from +5 diopters to +15 diopters. In other embodiments, the power can be lower, for example, +2.5 diopters and higher, for example +20 diopters. Also in this exemplary embodiment, the first peripheral zone
30 1008 has a negative power for myopic vision correction. In other words, the power to correct the individual's refractive error, myopia, resides in the first peripheral zone 1008

rather than in the center of the lens. The contact lens 1000 may include an additional plus powered concentric treatment zones 1010 outside of the first peripheral zone 1008. More specifically, the first peripheral zone 1008 which has the power to correct the refractive error is surrounded with plus power treatment zones. It is important to note that each of the treatment zones may have the same plus power or different plus powers. The diameter of the first peripheral zone 1008 and the one or more additional plus powered concentric treatment zones 1010 is selected to provide a balance between adequate vision and myopia control treatment. Additional exemplary zone diameters are illustrated in FIG. 10. It will be readily apparent to those skilled in the art that the peripheral zone diameters will be chosen depending on the diameter of the central zone to achieve a balance between obtaining adequate myopia control and satisfactory vision. For example, in a preferred embodiment, the diameter of the central zone is 1.0 mm, the outer diameter of the first peripheral zone is 4.2 mm, and the outer diameter of the second peripheral zone is 8.5 mm.

Referring to FIG. 11, there is illustrated a diagrammatic representation of a contact lens 1100 in accordance with another exemplary embodiment. The contact lens 1100 comprises an optic zone 1102 and an outer zone 1104. The optic zone 1102 comprises a center zone 1106 and a first peripheral zone 1108. In this exemplary embodiment, the center zone 1106 has a diameter that ranges from 0.50 mm to 4.0 mm with a power ranging from +5 diopters to +15 diopters. In other embodiments, the power may be lower, for example, +2.5 diopters and higher, for example, +20 diopters. Also in this exemplary embodiment, the first peripheral zone 1108 has a negative power for myopic vision correction. In other words, the power to correct the individual's refractive error, myopia, resides in the first peripheral zone 1108 rather than in the center of the lens. The contact lens 1100 may include one or more additional plus powered concentric treatment zones 1110 outside of the first peripheral zone 1108. More specifically, the first peripheral zone 1108 which has the power to correct the refractive error is surrounded with plus power treatment zones. It is important to note that each of the treatment zones may have the same plus power or different plus powers. Contact lens 1100 may include an additional negative power for myopic vision

correction zone 1112. The diameter of the first peripheral zone 1108, the one or more additional plus powered concentric treatment zones 1110, and the additional negative power zone 1112 are selected to provide a balance between adequate vision and myopia control treatment. For this exemplary embodiment, refer to FIG. 11 for the range of diameters for the zones.

Various embodiments may include a center myopia progression treatment zone in combination with peripheral zones that may be utilized for refractive error correction and additional myopia progression treatment zones all within the peripheral region.

Various combinations may be utilized outside of the center zone. Multiple concentric zones for myopic vision correction and treatment with different ADD powers may be added in the peripheral region of the optic zone with the zones so arranged to achieve a balance between myopic control treatment efficacy and adequate vision.

The myopia control efficacy of a multi-zone soft contact lens is believed to be related to several factors, including the power of the treatment zone, the size of the treatment zone relative to the entrance pupil, and the proximity of the treatment zone to the geometric center of the contact lens. The challenge of any myopia control treatment is to deliver a high myopia control effect while maintaining acceptable vision. The design of this exemplary embodiment maximizes the power of the treatment zone and the proximity of the treatment zone to the center of the lens while minimizing the size of the treatment zone relative to the entrance pupil to provide for acceptable vision. In other words, the contact lens of the present invention comprises a small diameter treatment zone of high plus power in the center of the lens. A number of experiments demonstrate the ability to have acceptable vision with these designs and are presented below.

Referring now to FIG. 12, there is illustrated a graphical representation of the loss in visual acuity, VA, in logMAR versus central zone size over four ADD powers for a 5.5 mm pupil size. This VA data was generated by introducing the optical designs to the eye. As may be seen from FIG. 12, minimizing the size of the treatment zone

relative to the entrance pupil yields better results relative to the loss of VA. In addition, the data suggest that once a power of + 5 diopters or greater is utilized, the rays passing through the treatment zones are sufficiently spread upon reaching the retina that loss in visual acuity is minimized.

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FIG. 13 is a graphical representation of the loss in visual acuity versus central zone diameter in a lens with a center plus design having a +10 diopter power for both a 5.5 mm pupil and a 3.5 mm pupil. As illustrated, for a 5.5 mm diameter pupil, VA decreases as the size of the central plus zone increases. For a 5.5 mm diameter pupil, VA is lowered by 0.03 +/- 0.01, 0.05 +/- 0.04 and 0.06 +/- 0.05 logMAR for 1.0, 1.5 and 2.0 mm near zone diameters respectively. For a 3.5 mm diameter pupil, the VA is further decreased to 0.07 +/- 0.03, 0.08 +/- 0.04 and 0.14 +/- 0.01 logMAR compared to the baseline.

FIG. 14 is a graphical representation of the size of halo in degrees versus central diameter for both a 5.5 mm diameter pupil and a 3.5 mm diameter pupil. The halo data of a center plus design having a +10 diopter power was generated by introducing the optical designs to the eye and using purpose built methodologies to measure halo size and brightness. As illustrated, halo was not visible for center plus conditions for a 1.0 mm diameter central plus zone. For a 5.5 mm diameter pupil, the halo was detectable for both 1.5 and 2.0 mm diameter central zones, with halo sizes of 0.40 +/- 0.24 degrees and 0.73 +/- 0.22 degrees respectively. For a 3.5 mm diameter pupil, the halo was only detectable with a 2.0 mm central zone diameter with a halo size of 0.28 +/- 0.05 degrees. FIG. 15 is a graphical representation of the brightness of halo versus central zone diameter for both a 5.5 mm diameter pupil and a 3.5 mm diameter pupil. As illustrated, halo is not visible for center plus designs with a 1.00 mm diameter central plus zone. Halo is not detectable for a 1.5 mm center plus design for a 3.5 mm pupil diameter. For a 5.5 mm diameter pupil, the halo was detectable for 1.5 and 2.0 mm diameter central zones with brightness of 13.5 +/- 2.8 and 16.5 +/- 6.4 gray level respectively. For a 3.5 mm diameter pupil, the halo was only detectable with a 2.0 mm diameter central zone with a brightness of 15.5 +/- 2.8 gray level.

Similar VA and halo experiments may be utilized to allow for the designs of this exemplary embodiment to be optimized for the power, size, and location of the treatment zone(s) to provide acceptable vision.

5 It is important to note that various power profiles may be utilized in the center and one or more peripheral zones or regions of the optic zone. For example, in FIG. 16A, a center zone has a negative power for myopic vision correction, a first peripheral region has a high ADD, and a second peripheral zone has a negative power for myopic vision correction equal to the center zone. In FIG. 16B, the center zone has a high ADD, a
10 first peripheral zone has a negative power for myopic vision correction, a second peripheral zone has a high ADD equal to the center zone and a third peripheral zone has a negative power for myopic vision correction equal to the first peripheral zone. In FIG. 16C, the center zone has a low Add, a first peripheral zone has a negative power for myopic vision correction, a second peripheral zone has a high ADD which is higher
15 than the ADD in the center zone and a third peripheral zone has a negative power for myopic vision correction equal to the first peripheral zone. In FIG 16D, a center zone has a high ADD, a first peripheral zone has a negative power for myopic vision correction, a second peripheral zone has a low ADD and a third peripheral zone has a negative power for myopic vision correction equal to the first peripheral zone. The
20 important thing to understand is that any number of suitable variations may be utilized in accordance with the present invention, including low ADDs may be zero. In FIG 16A through 16D, the y-axis power is relative to the negative power for myopic vision correction as is the case for FIG 2, 6A, 6B, 6C, 8A, 8B, and 8C.

25 Although shown and described is what is believed to be the most practical and preferred embodiments, it is apparent that departures from specific designs and methods described and shown will suggest themselves to those skilled in the art and may be used without departing from the spirit and scope of the invention. The present invention is not restricted to the particular constructions described and illustrated, but
30 should be constructed to cohere with all modifications that may fall within the scope of the appended claims.

WHAT IS CLAIMED IS:

1. An ophthalmic lens for at least one of slowing, retarding or preventing myopia progression and minimizing halo effect, the ophthalmic lens comprising:
an optic zone, the optic zone including a center zone configured as a myopia progression treatment zone, the center zone comprising an ADD power of between +0.5 diopters and +20.0 diopters relative to the negative power required to correct myopia, and at least one peripheral zone surrounding the center zone, the at least one peripheral zone comprising a myopia vision correction region with a negative power for myopic vision correction; and
an outer zone surrounding the optic zone.
2. The ophthalmic lens according to Claim 1, wherein the optic zone comprises one or more additional plus powered concentric myopia progression treatment zones outside of the at least one peripheral zone, the one or more additional plus powered concentric myopia progression treatment zones having an ADD power of between +0.5 diopters and +20.0 diopters.
3. The ophthalmic lens according to Claim 1, wherein the optic zone comprises one or more additional myopic vision correction zones with a negative power for vision correction.
4. The ophthalmic lens according to Claim 1, wherein the ophthalmic lens comprises a contact lens.
5. The ophthalmic lens according to Claim 1, wherein the ophthalmic lens comprises a spectacle lens.
6. The ophthalmic lens according to Claim 1, wherein the ophthalmic lens comprises an intraocular lens, a corneal inlay, or a corneal onlay.

7. The ophthalmic according to Claim 1, further comprising one or more stabilization mechanisms in the outer zone.