METHOD AND APPARATUS FOR PROVIDING VARIATIONS OF A LOWER-LID CONTACT SURFACE AND UNDER-LID SUPPORT STRUCTURES OF A TRANSLATING MULTIFOCAL CONTACT LENS

FIELD OF USE

The invention relates to contact lenses. More specifically, the invention relates to a translating multifocal contact lens comprising a lower-lid contact surface, and optionally an under-lid support structure, wherein, there may be multiple variations of a lower-lid contact surface and multiple techniques to design an under-lid support structure that fall within the present invention.

BACKGROUND

Bifocal lenses are comprised of two or more areas, or zones, with different optical powers, including typically a far-power Optic Zone for distance vision, and a near-power Optic Zone for near or close up vision. The two zones may be subdivided into additional power zones in which case a lens may be called a multifocal lens.

Effective use of a bifocal contact lens requires translation of an ocular system between vision surfaces when an eye changes from gazing at an object at a distance to gazing at a nearby object. Alternatively, there may be a desire to have a translating multifocal contact lens that may have one or more intermediate-power zones in addition to far- and near-power Optic Zones. Such a translating contact lens may have to have an ability to control and optimize the amount of movement of a lens when the pupil translates from distance vision, to intermediate vision, to near vision, or any combination thereof.

While there are many designs for soft translating contact lenses, soft contact lenses have difficulty translating across the surface of an eye when the visual direction of an eye changes from a straight-ahead gaze, to a downward gaze. In one prior art example, there is described a soft bifocal contact lens that has an integrally formed bevel to aid translation of a lens. While other designs may have the capability to translate across the surface of an eye when the visual direction of an eye changes from a straight-ahead gaze, to a downward gaze, but are not very efficient at controlling movement of a lens during an eye's translation to a different visual direction. Another prior art example, describes a soft multifocal contact lens that has an integrally formed ramped ridge zone adjoining an outwardly extending latitudinal ridge that sits

on an eyelid to aid in translation of a lens. The latitudinal ridge portion has a bump at each end, thereby increasing elevation height of the ends of the ridge compared to the elevation height in the middle. Another disadvantage of the prior art is discomfort when worn upon an eye.

Therefore, there is a need for a soft translating multi-focal contact lens that provides various design options and is capable of limiting the amount of translation across the surface of an eye when an eye changes position from one Optic Zone to another while also providing wearers with improved comfort.

SUMMARY

Accordingly, one aspect of this invention provides a translating multifocal contact lens resulting in limited lens translocation relative to the pupil of an eye. The limited translocation may be based upon one or both of vertical stability and rotational stability when using near, intermediate, and distance vision. The lens may include both of a lower-lid contact surface and an under-lid support structure. In some other examples, the lens may include a lower-lid contact surface, and no under-lid support structure. More specifically, a translating multifocal contact lens including multiple variations of a lower-lid contact surface and various techniques that may be implemented to design an under-lid support structure is described. Free-form technology enables many previously unobtainable shapes and forms including non-spherical. The voxel by voxel formation essentially, allows for a great variety of shapes formable on a substrate.

According to a first aspect of the invention there is provided a translating multifocal contact lens. The lens comprising: an anterior surface and a posterior surface wherein said anterior surface and said posterior surface comprise respective arcuate shapes and meet at a lens edge; an optical-power region to provide vision correction for an eye of a user wherein said optical-power region comprises multiple optic zones; and a lower-lid contact surface wherein the lower-lid contact surface is configured to limit the amount of said lens translocation upon the eye of the user when the user changes direction of vision and the user's line of sight moves from at least one optic zone to another said optic zone.

The lens may comprise a Free-form lens formed on a voxel by voxel basis.

The anterior surface may comprise one or both of the lower-lid contact surface and an under-lid support structure.

The lower-lid contact surface may comprise one contiguous, inward extension of the anterior surface portion that extends laterally across said anterior lens surface.

The lower-lid contact surface may be located directly above the adjoining under-lid support structure.

The lower-lid contact surface may be located directly above the adjoining lens edge.

The lower-lid contact surface may comprise a geometric shape defined by one or both of points and lines with at least one curve to define a surface.

The geometric shape may include one or more of a zero slope, a negative slope, and a positive slope.

The lower-lid contact surface may comprise one or more of a blend zone.

The blend zone may comprise a contiguous area blending an anterior portion of the lens to another adjoining said anterior portion of the lens.

The under-lid support structure may adjoin the lower portion of the lower-lid contact surface and extends to a lower said lens edge.

The under-lid support structure may comprise an arcuate anterior surface essentially contoured to the surface of the eye.

The under-lid support structure may comprise a width of 4mm or less, e.g., 3.5, 3, 2.5, 2, 1.5, 1, 0.5mm.

The under-lid support structure may provide for one or both of vertical stability for the lens and rotational stability for the lens.

The under-lid support structure may comprise a uniform thickness or a non-uniform thickness.

The under-lid support structure may be designed based upon a function-driven technique.

The under-lid support structure may be designed based upon a uniform axial thickness technique.

The under-lid support structure may be designed based upon a uniform radial thickness technique.

The under-lid support structure may be designed based upon a minimal energy surface technique.

According to a second aspect of the invention there is provided an apparatus for forming a translating multifocal contact lens, the apparatus comprising: a light source emanating light in a wavelength comprising actinic radiation; a processor in logical communication with a memory wherein said memory having stored therein executable code, executable upon demand to cause

the processor to generate one or more control signals for controlling a digital mirror device to project the actinic radiation through an arcuate substrate to form a translating contact lens described above. The apparatus for forming a translating multifocal contact lens may comprise a digital mirror or digital mirror device (DMD).

According to a third aspect of the invention there is provided a method for forming a translating multifocal contact lens, the method comprising: forming a contact lens comprising an anterior surface and a posterior surface on a voxel by voxel basis, wherein said anterior surface and said posterior surface comprise respective arcuate shapes and meet at a lens edge; forming an optical-p region to provide vision correction for an eye of a user wherein said optical-power region comprises multiple optic zones; and forming a lower-lid contact surface wherein the lower-lid contact surface is configured to limit the amount of said lens translocation upon the eye of the user when the user changes direction of vision and the user's line of sight moves from at least one optic zone to another said optic zone.

BRIEF DESCRIPTIONS OF DRAWINGS

Fig. 1 illustrates method steps that may be used to implement some embodiments of the preset invention.

Fig. 2 illustrates additionally method steps that may be used to implement some embodiments of the present invention.

Fig. 3 illustrates an example of the relationship among absorbance and transmittance with forming and fixing radiation.

Fig. 4 illustrates an example of the lens produced with the invention herein disclosed.

Fig. 5 illustrates apparatus components that may be useful in implementing some embodiments of the present invention comprising Voxel based lithography.

Fig. 6 illustrates exemplary light source apparatus components that may be useful in implementing some embodiments of the present invention.

Fig. 7 illustrates exemplary optical apparatus components that may be useful in implementing some embodiments of the present invention.

Fig. 8 illustrates exemplary digital mirror apparatus components that may be useful in implementing some embodiments of the present invention.

Fig. 9 illustrates additional apparatus components that may be useful in implementing some embodiments of the present invention.

Fig. 10 illustrates an exemplary forming optic that may be useful in implementing some embodiments of the present invention.

Fig. 11 illustrates an exemplary monomer reservoir that may be useful in implementing some embodiments of the present invention.

Fig. 12 illustrates an exemplary material removal apparatus that may be useful in implementing some embodiments of the present invention.

Fig. 13 illustrates the gross motion systems of an exemplary material removal apparatus that may be useful in implementing some embodiments of the present invention.

Fig. 14 illustrates an exemplary stabilization and fixing apparatus that may be useful in implementing some embodiments of the present invention.

Fig. 15 illustrates an exemplary metrology system that may be useful in implementing some embodiments of the present invention.

Fig. 16 illustrates an exemplary hydration and removal system that may be useful in implementing some embodiments of the present invention.

Fig. 17 illustrates an exemplary cross sectional representation of a Lens Precursor.

Figs. 18A-18D illustrate examples of the present invention having a lower-lid contact surface with zero slope adjoining a Lens Edge and anterior surface, and multiple variations of Blend Zones between them.

Figs. 19A-19D illustrate examples of the present invention having a lower-lid contact surface with negative slope adjoining a Lens Edge and anterior surface, and multiple variations of Blend Zones between them.

Figs. 20A-20D illustrate examples of the present invention having a lower-lid contact surface with positive slope adjoining a Lens Edge and anterior surface, and multiple variations of Blend Zones between them.

Figs. 21A-21B illustrate cross-section examples of an under-lid support structure designed via a function-driven technique.

Figs. 22A-22B illustrate cross-section and plan view examples of an under-lid support structure designed via a fixed, axial uniform thickness technique.

Figs. 23A-23B illustrate cross-section and plan view examples of an under-lid support structure designed via a fixed, radial thickness technique.

Figs. 24A-24D illustrate cross-section and plan view examples of an under-lid support structure designed via a MES technique.

Figs. 25A-25D illustrate examples of the present invention having a lower-lid contact surface with a zero slope adjoining an under-lid support structure and anterior surface, and multiple variations of Blend Zones between them.

Figs. 26A-26D illustrate examples of the present invention having a lower-lid contact surface with a negative slope adjoining an under-lid support structure and anterior surface, and multiple variations of Blend Zones between them.

Figs. 27A-27D illustrate examples of the present invention having a lower-lid contact surface with a positive slope adjoining an under-lid support structure and anterior surface, and multiple variations of Blend Zones between them.

Fig. 28 illustrates method steps according to some additional aspect of the present invention.

Fig. 29 illustrates a processor that may be used to implement some embodiments of the present invention.

DETAILED DESCRIPTION

A translating multifocal contact Lens including one or both of a lower-lid contact surface and an under-lid support structure in accordance with a particular patient's eye data is described herein. In a preferred example the lens includes a Free-formed, translating multifocal contact lens including multiple variations of a lower-lid contact surface, and various techniques for designing an under-lid support structure, as is discussed more fully below in relation to the various figures.

In the following sections, detailed descriptions of embodiments of the invention are given. The description of both preferred and alternative embodiments though thorough are examples only, and it is understood to those skilled in the art that variations, modifications and alterations may be apparent. It is therefore to be understood that said examples do not limit the broadness of the aspects of the underlying invention. Method steps described herein are listed in a logical sequence in this discussion. However, this sequence in no way limits the order in which they may be implemented unless specifically stated. In addition, not all of the steps are

required to implement the present invention and additional steps may be included in various embodiments of the present invention.

GLOSSARY

In this description and claims directed to the presented invention, various terms may be used for which the following definitions will apply:

"Blend Zone" as used herein means a contiguous area that blends a portion of a Lens to another adjoining portion of a Lens.

"DMD Show" as used herein, refers to a collection of time based instructional data points that may be used to control activation of mirrors on a DMD, and enable a Lens or Lens Precursor or Lens Precursor Form or Lens Precursor Feature(s) to be fabricated. A DMD Show may have various formats, with (x,y,t), and (r, θ, t) being the most common where, for example "x" and "y" are Cartesian coordinate locations of DMD mirrors, "r" and "θ" are Polar coordinate locations of DMD mirrors, and "t" represents time instructions controlling DMD mirror states. DMD Shows may contain data associated with a regularly or irregularly spaced grid.

"End Point" as used herein, refers to a location that may be specified when implementing one or more of various techniques including one or more of a uniform radial thickness technique, a uniform axial thickness technique, a non-uniform radial thickness technique, a non-uniform axial thickness technique, and a Minimal Energy Surface technique. There may be one or multiple End Points specified on one or both of an anterior surface and a posterior surface, and may be specified by a variety of means known to those skilled in the art. For example, an End Point location may be specified by one or more of a distance from a center of a lens, a distance from a Lens Edge, positions in (x,y,z) Cartesian coordinate space, and positions in (r, theta) polar coordinate space. Additionally, End Point locations may be determined based upon one or more of a patient's eye data, a known averaged patient eye data, and general Lens Design principles.

"Fluent Lens Reactive Media" as used herein means a Reactive Mixture that is flowable in either its native form, reacted form, or partially reacted form and, a portion or all Reactive Media may be formed upon further processing into a part of an ophthalmic lens.

"Free-form" as used herein "free-formed" or "free-form" refers to a surface that is formed by crosslinking of a Reactive Mixture via exposure to actinic radiation on a voxel by voxel basis, with or without a fluent media layer, and is not shaped according to a cast mold, lathe, or laser ablation. Detailed description of Free-form methods and apparatus are disclosed in United States

Patent Application S/N 12/194,981 (published as US 2009-053351-A1) and in United States Patent Application S/N 12/195,132 (published as US 2009-0051059-A1).

"Lens" as used herein "lens" refers to any ophthalmic device that resides in or on the eye. These devices may provide optical correction or may be cosmetic. For example, the term lens may refer to a contact lens, intraocular lens, overlay lens, ocular insert, optical insert or other similar device through which vision is corrected or modified, or through which eye physiology is cosmetically enhanced (e.g. iris color) without impeding vision. Preferred lenses are soft contact lenses are made from silicone elastomers or hydrogels, which include but are not limited to silicone hydrogels, and fluorohydrogels.

"Lens Design" as used herein, refers to form, function or both of a desired Lens, which if fabricated, may provide optical power correction, acceptable Lens fit (e.g., corneal coverage and movement), acceptable Lens rotation stability, etc. Lens Designs may be represented in either a hydrated or un-hydrated state, in Flat or Curved Space, in 2-dimensional or 3-dimensional space, and by a method including but not limited to, geometric drawings, power profile, shape, features, thicknesses etc. Lens Designs may contain data associated with a regularly or irregularly spaced grid.

"Lens Edge" as used herein, refers to a feature to provide a well-defined edge around a perimeter of a Lens Precursor or a Lens that may contain Fluent Lens Reactive Media. A Lens Edge feature may be either continuous around a Lens Precursor or a Lens, or may be present in discrete, non-continuous zones.

"Lens Precursor" as used herein, means a composite object consisting of a Lens Precursor Form and Fluent Lens Reactive Media in contact with a Lens Precursor Form that may be rotationally symmetrical or non-rotationally symmetrical. For example, Fluent Lens Reactive Media may be formed in the course of producing a Lens Precursor Form within a volume of Reactive Mixture. Separating a Lens Precursor Form and Fluent Lens Reactive Media from a volume of Reactive Mixture used to produce a Lens Precursor Form may generate a Lens Precursor. Additionally, a Lens Precursor may be converted to a different entity by either the removal of an amount of Fluent Lens Reactive Media or the conversion of an amount of Fluent Lens Reactive Media into non-fluent incorporated material.

"Lens Precursor Feature", also referred to as "feature", as used herein, refers to a non-fluent substructure of a Lens Precursor Form, and acts as an infrastructure for a Lens Precursor.

Lens Precursor Features may be defined empirically or described mathematically by control parameters (height, width, length, shape, location, etc.,) may be are fabricated via DMD Show instructions. Examples of Lens Precursor Features may include one or more of the following: a Lens Edge feature, a Stabilization Zone feature, a Smart Floor Volumator feature, an Optic Zone feature, a Moat feature, a Drain Channel feature, etc. Lens Precursor Features may be fabricated using Actinic Radiation Voxels and may be incorporated into an ophthalmic Lens upon further processing.

"Minimal Energy Surface" as used herein, or the term "MES", refers to a free-formed surface created by Fluent Lens Reactive Media formed over Lens Precursor Features, which may be in a minimum energy state. Minimal Energy Surfaces may be smooth and continuous surfaces.

"Optic Zone" as used herein, refers to a feature that provides one or both of a desired optical power and aberration correction of a Lens Precursor or ophthalmic Lens, the geometry of which may be directly dependent on a Target File.

"Reactive Mixture" as used herein, may be interchangeably used with "Lens Forming Mixture"; lens-forming monomer; refers to a monomer or prepolymer material which can be cured and/or crosslinked to form an ophthalmic lens or portion of an ophthalmic lens. Various examples can include lens-forming mixtures with one or more additives such as: UV blockers, tints, photoinitiators, or catalysts, and other additives one might desire in an ophthalmic lenses such as, contact or intraocular lenses.

"Start Point" as used herein, refers to a location that may be specified when implementing one or more of various techniques including one or more of a uniform radial thickness technique, a uniform axial thickness technique, a non-uniform radial thickness technique, a non-uniform axial thickness technique, and a Minimal Energy Surface technique. There may be one or multiple Start Points specified on one or both of an anterior surface and a posterior surface, and may be specified by a variety of means known to those skilled in the art. For example, a Start Point location may be specified by one or more of a distance from a center of a lens, a distance from a Lens Edge, positions in (x,y,z) Cartesian coordinate space, and positions in (r, theta) polar coordinate space. Additionally, Start Point locations may be determined based upon one or more of a patient's eye data, a known averaged patient eye data, and general Lens Design principles.

"Target File", as used herein, refers to data that may represent a Lens Design, a Thickness Map, a Lens Precursor design, a Lens Precursor Form design, a Lens Precursor Feature design, or combinations of the above. A Target File may be represented in either a hydrated or un-hydrated state, in Flat or Curved Space, in 2-dimensional or 3-dimensional space, and by methods including but not limited to, geometric drawings, power profile, shape, features, thicknesses etc. Target Files may contain data associated with a regularly or irregularly spaced grid.

"Actinic Radiation" as used herein, refers to radiation that is capable of initiating a chemical reaction.

"Arcuate" as used herein, refers to a curve or bend like a bow.

"Beer's Law" as referred to herein and sometimes referred to as "Beers-Lambert Law" is: $I(x)/I0 = \exp(-\alpha c x)$, wherein $I(x)$ is the intensity as a function of distance x from the irradiated surface, I0 is the incident intensity at the surface, α is the absorption coefficient of the absorbing component, and c is the concentration of the absorbing component.

"Collimate" as used herein means to limit the cone angle of radiation, such as light that proceeds as output from an apparatus receiving radiation as an input; the cone angle may be limited such that proceeding light rays are parallel. Accordingly, a "collimator" includes an apparatus that performs this function and "collimated" describes the effect on radiation.

"DMD" as used herein, a digital micromirror device is a bistable spatial light modulator consisting of an array of movable micromirrors functionally mounted over a CMOS SRAM. Each mirror is independently controlled by loading data into the memory cell below the mirror to steer reflected light, spatially mapping a pixel of video data to a pixel on a display. The data electrostatically controls the mirror's tilt angle in a binary fashion, where the mirror states are either +X degrees (on) or -X degrees (off). For current devices, X can be either 10 degrees or 12 degrees (nominal). Light reflected by the on mirrors then is passed through a projection lens and onto a screen. Light is reflected off to create a dark field, and defines the black-level floor for the image. Images are created by gray-scale modulation between on and off levels at a rate fast enough to be integrated by the observer. The DMD (digital micromirror device) is sometimes DLP projection systems.

"DMD Script" as used herein shall refer to a control protocol for a spatial light modulator and also to the control signals of any system component, such as, for example, a light source or

filter wheel either of which may include a series of command sequences in time. Use of the acronym DMD is not meant to limit the use of this term to any one particular type or size of spatial light modulator.

"Fixing Radiation" as used herein, refers to Actinic Radiation sufficient to one or more of: polymerize and crosslink essentially all Reactive Mixture comprising a Lens Precursor or lens.

"Fluent Lens Reactive Media" as used herein means a Reactive Mixture that is flowable in either its native form, reacted form, or partially reacted form and is formed upon further processing into a part of an ophthalmic lens.

" Gel Point" as used herein shall refer to the point at which a gel or insoluble fraction is first observed. Gel point is the extent of conversion at which the liquid polymerization mixture becomes a solid. Gel point can be determined using a soxhlet experiment: Polymer reaction is stopped at different time points and the resulting polymer is analyzed to determine the weight fraction of residual insoluble polymer. The data can be extrapolated to the point where no gel is present. This point where no gel is present is the gel point. The gel point may also be determined by analyzing the viscosity of the reaction mixture during the reaction. The viscosity can be measured using a parallel plate rheometer, with the reaction mixture between the plates. At least one plate should be transparent to radiation at the wavelength used for polymerization. The point at which the viscosity approaches infinity is the gel point. Gel point occurs at the same degree of conversion for a given polymer system and specified reaction conditions.

"Lens Precursor Form" as used herein, means a non-fluent object with at least one optical quality surface which is consistent with being incorporated upon further processing into an ophthalmic lens.

"Mold" as used herein, refers to a rigid or semi-rigid object that may be used to form lenses from uncured formulations. Some preferred molds include two mold parts forming a front curve mold part and a back curve mold part.

"Radiation Absorbing Component" as used herein, the term "refers to radiation-absorbing component which can be combined in a reactive monomer mix formulation and which can absorb radiation in a specific wavelength range.

Reactive Mixture (also sometimes referred to herein as: Lens Forming Mixture or Reactive Monomer Mixture and with same meaning as "Lens Forming Mixture")

"Release from a mold" as used herein, "release from a mold," means that a lens becomes

either completely separated from the mold, or is only loosely attached so that it can be removed with mild agitation or pushed off with a swab.

"Stereolithographic Lens Precursor" as used herein means a Lens Precursor where the Lens Precursor Form has been formed by use of a stereolithographic technique.

"Substrate" A physical entity upon which other entities are placed or formed.

"Transient Lens Reactive Media" as used herein means a Reactive Mixture that may remain in fluent or non-fluent form on a Lens Precursor Form. However, Transient Lens Reactive Media is significantly removed by one or more of: cleaning, solvating and hydration steps before it becomes incorporated into an ophthalmic lens. Therefore, for clarity, the combination of a Lens Precursor Form and the transient lens Reactive Mixture does not constitute a Lens Precursor.

"Voxel" as used herein "Voxel" or "Actinic Radiation Voxel" is a volume element, representing a value on a regular grid in three dimensional space. A Voxel can be viewed as a three dimensional pixel, however, wherein a pixel represents 2D image data a Voxel includes a third dimension. In addition, wherein Voxels are frequently used in the visualization and analysis of medical and scientific data, in the present invention, a Voxel is used to define the boundaries of an amount of actinic radiation reaching a particular volume of Reactive Mixture, thereby controlling the rate of crosslinking or polymerization of that specific volume of Reactive Mixture. By way of example, Voxels are considered in the present invention as existing in a single layer conformal to a 2-D mold surface wherein the Actinic Radiation may be directed normal to the 2-D surface and in a common axial dimension of each Voxel. As an example, specific volume of Reactive Mixture may be crosslinked or polymerized according to 768×768 Voxels.

"Voxel-based Lens Precursor" as used herein "Voxel-based Lens Precursor" means a Lens Precursor where the Lens Precursor Form has been formed by use of a Voxel-based lithographic technique.

"Xgel" as used herein, Xgel is the extent of chemical conversion of a crosslinkable Reactive Mixture at which the gel fraction becomes greater than zero.

Apparatus

The apparatus disclosed in this invention is generally presented herein in five major subsections, and the first discussion of embodiments of the apparatus will be organized into logical discussions at the subsection level. These subsections are the Voxel-based lithography

optical apparatus, the wicking apparatus, the stabilization and fixing apparatus, the metrology apparatus and the hydration apparatus. Nevertheless, the subsections also function as a whole apparatus and this should be considered in light of the subsection embodiments.

Voxel-Based Lithography optical apparatus

The Voxel-based lithography optical apparatus is the component that uses actinic radiation to create lens forms and Lens Precursors. In the present invention, an apparatus takes highly uniform intensity radiation and controls irradiation onto the surface of a forming optic at numerous discrete points across the forming optic surface, essentially on a Voxel by Voxel basis. This control allows this component to control the degree of reaction that occurs in Reactive Mixture along the light path of a particular Voxel location; ultimately determining the volume of reacted material there and thus, the shape of a Lens Precursor Formed thereon.

The major components of the Voxel-based lithographic optical apparatus are depicted in an exemplary embodiment in Fig. 5. Each component indicated is discussed in detail in a later section. At this point, an exemplary overview is given for the subsection functions.

Referring now to Fig. 5, forming apparatus 500,in this exemplary operation can functionally begin at the light source 520. In such embodiments, the light generated in this source 520 emerges as light in a defined band of wavelengths but with some spatial variation in intensity and direction. Element 530, a spatial intensity controller or collimator, condenses, diffuses and, in some embodiments, collimates light to create a beam of light 540, that is highly uniform in intensity. Further, in some embodiments, the beam 540 impinges on a digital mirror device DMD 510 which divides the beam into pixel elements of intensity each of which can be assigned a digital on or off value. In reality, the mirror at each pixel merely reflects light in one of two paths. The "ON" path, item 550, is the path that leads to photons proceeding toward a reactive chemical media. Conversely, in some embodiments, an "OFF" state includes a light being reflected along a different path that will lie between the paths depicted as items 516 and 517. This "OFF" path directs photons to impinge upon a beam dump 515 which has been carefully crafted to absorb and entrap any photons directed towards it. Referring back to the "on" path 550, light depicted in this path actually includes the potentially many different pixel values that have been set to the "on" value and are spatially directed along the appropriate individual path corresponding to their pixel location. A time averaged intensity of each of the pixel elements along their respective paths 550, can be represented as a spatial intensity profile 560, across the spatial grid defined by the DMD

510. Alternatively, with a constant intensity impinging each mirror, item 560 may represent a spatial time exposure profile.

Continuing, each pixel element in the on state will have photons directed along their path 550. In some embodiments the beam may be focused by a focusing element. By way of example, Fig. 5 500 depicts an embodiment where the light paths 550, are imaged so that they impinge in an essentially vertical manner upon the optic surface of a forming optic 580. The imaged light now proceeds through the forming optic 580, and into a volume of space that contains reactive lens mixture in a reservoir 590. It is the interaction of this light for a given pixel location, that defines an on state Voxel element in the volume in the reservoir 590, and around the forming optic 580. These photons in this volume may be absorbed and precipitate an actinic reaction in the molecule that absorbs it, leading to a polymerization state change of the monomer in this general vicinity.

It is in this general way for one particular embodiment that the Voxel based lithographic optic can be understood to function. Each of these elements in their own right has characteristics and embodiments that describe functional modes of this apparatus. Further understanding of the underlying invention may gain from delving into the individual complexities.

Following now on the basic understanding of the apparatus function presented above, the total system will be discussed as a whole. In some embodiments, Voxel based lithographic systems as a whole are used to generate ophthalmic lenses. (A graphical representation of the wavefront surface of such a formed lens is illustrated in Fig. 4).

In some embodiments, an ambient environment, including temperature and humidity, encompassing apparatus 500 can be controlled. Other embodiments can include environments consistent with a laboratory environment and therefore can vary.

The nature of the ambient gaseous environment can be controlled, for example, through the use of purging nitrogen gas. Purging can be performed to increase or reduce oxygen partial pressure to predetermined levels. Humidity may also be maintained at relatively predetermined levels, such as at relatively lower levels than an office environment.

The level of vibrational energy that is allowed to interact with the individual apparatus components is another environmental parameter that may be controlled in some embodiments. In some embodiments, large massive support structures define a relative low vibrational environment. Other embodiments may include some or all of the Voxel-based lithographic system

500 to be supported upon active vibrational supports. Without limiting the generality of possible solution, it is well known in the art that air bladder support pistons can significantly reduce vibrational transfer into an isolated system. Other standard means of vibrational isolation may as well be consistent with the scope of the invention.

Particulates in the environment of the apparatus may introduce undesirable defect modes of various types including incorporation into the product Lens Precursors and lenses. For example, in the optic path, particulates can modulate the actual intensity of one or more Voxel elements and or affect the function of a particular mirror element. For these reasons, at a minimum, it is entirely within the scope of the invention to provide a means of controlling particulate matter in the environment. One example of an embodiment to achieve this would be the incorporation of high efficiency particulate air (HEPA) filters into the body of the apparatus environment and a means of forcing air through the filters sufficient to establish a laminar flow regime in exposed portions of the apparatus. Nevertheless, any embodiment to significantly limit particulate levels in and around the apparatus is within the intended scope of the invention.

Another aspect of the detailed environmental support for optical apparatus according to the present invention, includes the ambient light and manners to control it. In some embodiments, ambient lighting provides actinic radiation and it is therefore prudent to limit stray sources of photon energy.

Accordingly, in some embodiments, apparatus 500 can be enclosed in opaque materials consistent with the previously discussed environmental needs. A preferred embodiment may employ the use of filtered light sources in the environment of the apparatus, which may be sufficient to avoid exposure of active portions of the apparatus to contaminating environmental lighting.

Referring now to Fig. 6, consider the light source as depicted in a highlighted form 600. Specific aspects of light energy can be considered a fundamental aspect of any lithographic system and in embodiments of this invention which use the Voxel-based lithographic optical apparatus, the nature of the source of light for the system may be important.

In some embodiments it is desirable for a light source 620 to provide light in a narrow spectral band. The components of an exemplary light system 600, provide the means of accomplishing said narrow spectral character. In a preferred embodiment, a light source includes a light emitting diode 620, which exists in an environmental support and enclosure 610. For

exemplary purposes, in some embodiments a light emitting diode source 620 can include the model AccuCure ULM-2-365 light source with controller from Digital Light Lab Inc. (Knoxville, TN USA) This model emits a narrow band of light centered around 365 nm and further having the characteristics of a full width at half maximum breath of approximately 9 nm. Thus, this commercially available light source component already emits light in a desirable narrow band without further apparatus. It may be clear that any LED or other light emitting product with similar characteristics may also be utilized.

Alternatively, wider spectrum light sources, such as, for example carbon arc lamps or Xenon lamps 620 may also be used. In this alternative, a broad band source can be utilized 620. Light emits out of the environmental container 610 and proceeds through a filter wheel 630 deployed on the light source 620. The filter wheel 630, can contain multiple, distinct filters 631, at different operational locations and these filters 631, may, for example, include a band pass filter that will transmit light centered at 365 nm with a full width at half maximum breath of a similar 10 nm performance. In this embodiment, the filter wheel can be actuated by a motorized actuator 610 which can index the filter wheel to different filters; and therefore allow the exemplary Voxel-lithographic system embodiment 500 to operate at multiple selectable wavelengths.

It may be clear that numerous alternative embodiments may easily derive, including in a non-limiting perspective, the fact that the filter 631 may be mounted in a fixed manner proximate to the wide band light source 620 and provide an appropriate embodiment. In another aspect, a multiple wavelength capability of may be derived from an alternative embodiment where the there are multiple LED light sources 620, in the environment 610 that are activated individually for a different wavelength.

More generally, it should be apparent that some embodiments may include various light sources, including, for example, incandescent, laser, light emitting and other analogous products with or without filters of various kinds. Additionally, in some embodiments, light sources can be capable of emitting light in a controlled spectral band can be utilized and are within the scope of this invention.

The light source 600, additionally may have the characteristic of being stable, uniform and relatively intense. In the some preferred embodiments, an AccuCure LED light source 620, outputs intense light and includes an internal monitoring feedback loop to maintain a stable intensity over time periods.

A light source 620, can include means for modulating the intensity in a controlled manner; including modulating the source on and off with a defined duty cycle. Thus, over an integrated period of time, this mode of intensity control will result in selectable time averaged intensity levels. Alternatively, in an additional operational embodiment, the LED source can modulate intensity via a voltage controlled operational mode where the change in intensity occurs for the time independent level of emitted intensity.

For stability of the output of any light source component 620 additional features in the environment of the light source may include additional embodiment definitions. Examples of this aspect could include temperature control means via cooling systems. Other environmental controls may include different embodiment definitions consistent with the intent of this invention.

In a different aspect, the light source apparatus 600, provides an alternative embodiment for intensity modulation. The individual light source 620 may be operated to emit a given intensity and the filter wheel 630 may be actuated by a motorized element 610, to intercept the emitted light with a neutral density filter 631. Thus, the intensity of light provided to the rest of the Voxel-lithographic system 500 will be modulated to a lower intensity. From a generality perspective, it may be noted that the design of the individual light filters 631 may involve numerous degrees of freedom and in their own right include different embodiment aspects. By way of a non-limiting example, a filter may be designed to modulate intensity in a spatially defined manner such that it defines higher intensity along one path through its body than in another path. In a second non-limiting example, a filter wheel may be designed to modulate intensity in a manner such that it is synchronized with operation of the DMD, thereby allowing coordination of pixels and intensities defined by the density values of each filter wheel segment. Combinations of these operational modes provide alternative embodiments, and it should also be clear that any means of controlling light intensity of the characteristics thus described is within the scope of the invention.

Regardless of the embodiment of the light source component 620, and its environment, an embodiment including a filter wheel 630, can allow for an embodiment of an operational mode to shutter in a filter element 631 that acts to completely block irradiation from the rest of the optic system 500. There may be numerous advantages to incorporating such a function including the stability and longevity of downstream optic components. Additionally, in some embodiments, the stability of a light source component 620 may be improved if it is allowed to continuously

operate. A blocking filter 631, may allow for means of performing steps in the rest of the operational system that require the absence of the light from the light source 600. It may be apparent to one skilled in the art that while a particular location of the filter wheel 630, has been described there may be different appropriate locations along the optic path that would include acceptable embodiments within the scope of the invention.

An additional component of a Voxel-based lithography optical apparatus includes a homogenizing and collimating optic. This apparatus is designed to take the light output of the light source 520 and produce output radiation 540 that is of more uniform intensity and is focused upon the DMD 510. From a generalization perspective it may be possible to achieve the intent of the invention in the absence of this componentry, especially if the light source has components of similar intent.

The preferred embodiment is depicted in Fig. 7 700. As mentioned the purpose of this section of the apparatus is to both collimate the light from the light source and also to homogenize that light relative to intensity. It turns out that in the preferred embodiment, the AccuCure 365nm LED light source 620, has attached optical components to perform the collimation of its light output. In a more generalized embodiment, such collimating apparatus would include the first component of this collimation and homogenization component. In the preferred embodiment, however, the light being collimated sufficiently by the light source 620 proceeds into 700 and impinges a set of roughly 1 inch focusing optics 710. These optics are included of off the shelf lens components available for example from CVI Laser, Inc, (Albuquerque, NM USA)

These two lenses 710, focus the source light onto the light pipe 720. This component 720, has the central role of homogenizing the input light, in the process smoothing out nonuniformities in the spatial intensity. The light pipe 720 includes a hexagonal shaped optic pipe made of UV grade acrylic material. While specific details of the embodiment have been described, it should be obvious that any alternative embodiment that provides an optical apparatus for homogenizing the source light spatial uniformity includes solutions anticipated in the scope of the invention.

The homogenized light output from the light pipe 720, is focused by an off the shelf grade optic element 730 again of the type available from CVI Laser Inc. (Albuquerque, NM USA) for example. The focused light now proceeds through an aperture stop 740, on to a set of roughly 2 inch focusing elements 750. Again these focusing elements are standard, off the shelf grade optics as may be available through Thorlabs Inc. (Newton NJ USA), by way of example. The

intent of the focusing optics 750, now is to direct the light to a focal location at the digital mirror device (DMD) 510. This completes the path of light in the illumination section of Voxel-based lithographic system. There may be numerous embodiments that may alter aspects of the collimator and homogenizer components to achieve a similar aim in illuminating the DMD 510 with intense, uniform light of a desired central wavelength and spectral bandwidth, which are within the scope of the invention.

In the preferred embodiment, the illumination system items 520 and 530 impart light,(identified as 820 in Fig. 8 800) onto and just around the active elements comprising a Texas Instruments Digital Mirror Device 510. The DMD used in the preferred embodiment was obtained with a DMD Developer Kit: DMD Discovery 3000 available from DLi (Digital Light Innovations, Austin Texas, USA). The kit contains A DLi DMD Discovery 3000 board with a Texas Instruments DLP^{tm} XGA DMD chip (768 x 1024 mirrors) 0.7" diagonal with UV transmissive window option. Also included is an ALP-3 High Speed light Processing board married to the D3000 board to act as a link from a computer to the D3000. Together these components include 810 in Fig. 8 800 of the imaging system components from this preferred embodiment of the Voxel based lithography system. A detailed description of the TI DLP™ XGA DMD may be obtained from TI as the DMD Discovery™ 3000 Digital Controller (DDC3000) Starter Kit Technical Reference Manual.

The DMD device 810 can function to provide spatial modulation in the intensity of light that exits from the illumination system. The DMD from Texas Instruments performs this function in a digital manner by reflecting light off of the micromirror components that make up a single addressable location in the spatial grid of the active area of the device. Therefore, the intensity of light that gets reflected from the DMD 810 and further down the imaging system 800, per se, is not changed however by controlling the duty cycle of the mirrors into an on state or an off state, the time averaged intensity that is reflected from a single pixel location can be modified.

In other embodiments, a Spatial Light Modulator (SLM) such as those available from Fraunhofer Institut Photonische Microsysteme of Germany can be used to control radiation on a Voxel by Voxel basis and can include the spatial modulation in intensity function 810. The mirror-like surface of the SLM may actually be composed of multiple (i.e. thousands) of tiny moveable mirrors, each mirror with its own storage cell within the integrated circuit. As the image of the desired intensity profile is sent to the SLM, individual mirrors are either flexed or

remain flat (unlike the TI DMD which rotates or tilts the micromirrors). Light reflected off the flexed mirrors is scattered such that it does not pass through and expose the actinically reactive chemical mixture.

Referring now again to Fig. 8, as mentioned above, the active imaging element DMD 810 processes light in a digital manner reflecting it in one of two directions. In the off state, the path of reflection of the light is intended not to ever see the location with the actinically reactive chemical mixture. To ensure, that light directed in the off direction does not ever see this path, part of an imaging system 800 can include a light dump 830. This dump is included of highly absorptive surfaces that absorb significantly any light incident upon them and reflect only into further depths of the dump itself. In the preferred embodiment, as a non-limiting example, these surfaces include absorptive ND glass sheets as that which can be obtained from Hoya Inc. (Tokyo, Japan).

Light that is reflected from mirror elements in the "on" position takes a different path and heads towards focusing elements 840. As with the other optics these roughly 1 inch focusing lenses are off the shelf components that may for example be available from Thorlabs Inc. (Newton NJ USA). These focusing lenses 840 focus the "on" state light emanating from the DMD 810 as an object onto the forming optic where the reaction of light with reactive monomer mixture occurs.

In some embodiments, it is desirable to provide a means of imaging and monitoring the status of the optic path directly, rather than inferring from results on lenses produced. In the preferred embodiment of the Voxel-based lithography optical apparatus, provision is provided for this direct monitoring. Light that would be focused onto the forming optic 580, is intercepted with a mirror 850, that can be switched into and out of the beam path. The light that is so directed is then incident on a photo-detective imaging apparatus 860.

Continuing now to Fig. 9, the components of the forming apparatus 900, impinge the beam on the ultimate target area of the Reactive Mixture. As mentioned above, in some embodiments, this light has been focused onto a normal orientation with the surface of the forming optic 930, itself. In the embodiment illustrated 900, the light may impinge in a roughly vertical manner to the surface of the forming optic 930. In alternative embodiments, a lens can be held in place via a retaining ring or other fastening device, demonstrated as 921, which may maintain the correct orientation of said lens relative to the forming optic 930. From a broad

perspective it should be noted that the invention includes numerous embodiments related to the path light will take on a Voxel by Voxel basis across the optic surface 930.

Continuing with Fig. 9, since the relative orientation of the reservoir and forming optic to the light beam is of importance, mechanism for their interlocked location may be defined in some embodiments as demonstrated by the interaction of items a forming optic retaining member 970,, and the reservoir for containing the reactive monomer mixture 950. The alignment between these two members will also provide for positive control of the centering of the reservoir 950, to the forming optic surface 930. The position control may also be enhanced in some embodiments with the function of spacing ring 951. This spacing likewise will control the volume of reactive monomer mixture that may be added to the reservoir 950.

Fig. 9 also shows an additional embodiment aspect relating to the control of ambient gasses in the neighborhood of the reactive monomer mixture. Since in some embodiments, the presence of oxygen can modify the photochemistry of the monomers and ask as a scavenger of photogenerated free radicals, in some embodiments it needs to be excluded from the gas surrounding the reservoir 950. This is accomplished in Fig. 9 900 by the containment vessel 990. By flowing an inert gas, such as nitrogen, through 960, oxygen may be excluded from the environment. In still another embodiment, the oxygen level may be maintained at a level by controlling its dilution in the gas 960, being flowed through the containment vessel 990. Standard means, through the use of gas mass flow controllers to achieve a constant dilution level of the oxygen in the gas 960 are well known art and include embodiments within the spirit of the invention.

The reservoir 950, which contains the Reactive Mixture, may be filled with an appropriate volume of said Reactive Mixture. In some embodiments, this filling could be performed before the forming optic 930, is positioned relative to the reservoir 950. In other embodiments, the forming optic 930 and the reservoir 950, may be placed inside a containment vessel 990 and subjected to the purging with a gas flow 960. Filtering of the Reactive Mixture prior to use may also be employed. Thereafter, a volume of the Reactive Mixture 945, may be quantitatively filled into the reservoir 950.

There may be numerous means to transfer the Reactive Mixture 945, including hand filling, quantitative fluid transfer by automatic means or filling until a level detector measures the appropriate level of Reactive Mixture 945 in the reservoir 950. From a general perspective it may

be obvious to one skilled in the art, that numerous embodiments to transfer an appropriate amount of Reactive Mixture 945 may be practical, and such techniques are well within the scope of invention.

In embodiments where the level of oxygen is critical to the photoprocessing steps, it may be apparent that oxygen may be present as a dissolved species in the reactive monomer mixture 945. In such an embodiment, means to establish the oxygen concentration in the reactive monomer mixture 945 are required. Some embodiments to accomplish this function include allowing the mixture to dwell in the gaseous environment through which the purge gas 960, is flowing. Alternative embodiments may involve vacuum purging of the dissolved gasses in a supply of the monomer mixture and reconstituting a desired amount of oxygen during a dispensing of the mixture through membrane exchange of gas with the liquid to be dispensed. Within the scope of the invention, it should be apparent that any means to establish the needed dissolved gas at an appropriate concentration is acceptable. Furthermore, in a more general sense, other materials may act as appropriate inhibitors in the presence or absence of the dissolved oxygen. From an even more general perspective, embodiments that include apparatus to establish and maintain an appropriate level of inhibitor are anticipated in the scope of the invention.

Referring now again to Fig. 10, an exemplary shape of a forming optic and its holding and locating apparatus 1000 is illustrated. The structure that holds the forming optic can include flat glass disk 1040. The forming optic can be located and fastened by means of an optically consistent adhesive 1020 using an assembly jig to ensure alignment between the disk and the forming optic. The disk's flat surface provides positive orientation in the vertical direction, while a locating notch 1030 and other flat surfaces not illustrated can allow for radial and horizontal positional control.

Referring now to Fig. 11, the disk 1000, mates with the reservoir system 1100. The flat surfaces sit upon three mating surfaces 1130. Some embodiments may additionally include a spring loaded locating pin 1120 which positively mates and locates to item 1030. Two static locating pins (not illustrated) engage two other flat surfaces on the forming optic assembly and the combination acts to kinematically locate the forming optic assembly, in all degrees of freedom, thus ensuring a repeatable and stable means of locating the forming optic in the optical light path. In some embodiments, a reservoir for containment of the reactive monomer 1110 can also be included. From a more general perspective, there are numerous embodiments, consistent with the

inventive art disclosed herein, that may be obvious to one skilled in the art for ways to center a forming optic, to locate such optic in proximity to a reservoir which will contain Reactive Mixture and to locate one or more such functions in an ambient controlled environment.

The forming optic 1010 is at least partially transmissive to a desired spectrum of actinic radiation. Accordingly, in various embodiments, forming optic 1010, may include, by way of example, one or more of: quartz, plastic, glass, or other material transmissive of light wavelengths operative to cure a RMM used. It may further be noted that the shape of the forming optic 1010 includes one of the surfaces 1011 with characteristics to be imparted into a lens or Lens Precursor, formed along the surface 1011 via polymerization resulting from the forming actinic radiation that passes through the forming optic 1010. Numerous shape embodiments may include the inventive art herein.

Within the various embodiments that may be employed for the design and characteristics of a forming optic 1010, individual examples of said pieces may have unique aspects related, for example, to its stock material, manufacturing, history of usage and/or other causes. These aspects may or may not interact with the overall function of the Voxel lithographic system 500, creating unique optical offsets for the Voxel by Voxel intensity profile required to achieve an end product aim. Therefore, some embodiments may employ means to condition forming optics 1010, maintain them and track them. By reason of example, one embodiment may be to encode an identification mark in machine readable format on the flat surface of a forming optic piece 1040. Additional embodiments could include, for example, the attachment of an RF identification device along with said identification mark for machine readability. There may be numerous other embodiments to identify individual forming optic pieces 1040, that may include the intent of this invention.

The output product of the Voxel-based lithography optical equipment 500 may include numerous embodiments. In one embodiment, as shown at 900 a reactive product 940 will form on the surface of the forming optic 930 while still residing in the residual reactive chemical mixture 945. The action of removing the forming optic 930 with reactive product 940, from the chemical mixture 945 may include additional embodiments of the apparatus. In some such embodiments, the forming optic 930 and adhered reactive product 940 may be raised out of the chemical mixture 945 under the action of robotic automation for example.

In some embodiments, an article of manufacture that results from the process discussed may be an entity called a Lens Precursor. The Lens Precursor can be adhered to the forming optic upon formation. A schematic representation 1700 is presented of what may be included in a precursor without the substrate or forming optic that the Lens Precursor may be adhered to. This rough representation illustrates, however, the key features of a Lens Precursor. The reactive product has a solid component, referred to as a Lens Precursor Form, now identified as 1740. In this embodiment, the attached face (without forming optic illustrated) is depicted with an optical surface as 1750. The Lens Precursor Form 1740, will now have a surface 1730 that has been defined by the operation of the Voxel-based lithographic system 500. Adhered to this surface 1730, is a Fluent Lens Reactive Mixture 1745. In such embodiments, media 1745 will remain on the forming optic, wherein they may be exposed to additional processing such as described herein.

Flowable Material Removal Apparatus

The Lens Precursor 1700 which in some embodiments has been produced by a previously described Voxel-based lithography optical system 500, defines a novel entity. A Flowable Material Removal Apparatus (sometimes referred to as a Wicking apparatus) is one set of apparatus which can act upon a Lens Precursor 1700, and is described in detail hereafter.

Referring now to Fig. 12 1200, a schematic representation of some aspects of an embodiment of a flowable chemical removal apparatus is demonstrated. The Lens Precursor is now demonstrated attached to a forming optic 1250, and an alignment plate 1260 attach thereon. The combination is demonstrated as an embodiment where the Lens Precursor's surface is facing downwards. The Fluent Lens Reactive Mixture 1240, will move under a variety of forces including that of gravity. A wicking capillary 1210, is positioned in close proximity to the Fluent Lens Reactive Mixture 1240, around and in the fluent chemical that has pooled at a low point along the lens surface. In a preferred embodiment the wicking capillary may include a polymer wicking model made from a Safecrit, Model HP8U Untreated Plastic Microhematocrit tube. By way of alternative example, the capillary may also include glass, metal or other material consistent with the physical and chemical/materials requirements of fluent chemical removal.

The fluent chemical 1240, is drawn into the capillary 1210, and forms a volume 1241 that is drawn away from the Lens Precursor. In one embodiment, the process may repeat a number of

times. After processing, the Lens Precursor 1200 remains with a reduced amount of Fluent Lens Reactive Mixture adhered to the Lens Precursor Form 1750.

Various aspects of the Fluent Lens Reactive Mixture may be affected by this processing; including for example, that less viscous components in the Fluent Lens Reactive Mixture may be separated and removed. It should be apparent to those skilled in the art that there are many different embodiment options related to how the chemical removal process may be performed, all consistent with the scope of this invention.

In general, embodiment options may include numerous physical designs to draw away chemical from the surface. An example of a different embodiment may be the actuation of a vacuum system component 1220 to assist in drawing away the Fluent Lens Reactive Mixture 1240. By way of non-limiting example, another embodiment may be included of redundant copies of the capillary apparatus 1210, deployed with their points mimicking the shape of the forming optic surface 1250. Additionally, the chemical removal could be performed with a high surface area material, like sponge, or nanoscale materials with high surface area, as an example. Restating a concept described previously, an alternative embodiment may include controlling the rate of withdrawal of a Lens Precursor on a forming optic 930, from the Reactive Mixture 945. The surface tension forces, in this embodiment may include a form of chemical removal, with similarity to a capillary wicking step; and result in the reduction of the amount of Fluent Lens Reactive Mixture 1710 remaining when the Lens Precursor results. From a generality perspective, the numerous embodiments of apparatus that could perform the function of removal of portions of the Fluent Lens Reactive Mixture 1240 include art within the scope of the invention.

The vacuum system component 1220, in the preferred embodiment, has an alternative function to that previously defined. In the processing of multiple Lens Precursors, the chemical removal apparatus 1200 will perform chemical removal numerous times. The vacuum system component 1220, may be used to clean and evacuate the capillary apparatus 1210. A different embodiment may include a cleansing solvent being flowed through the capillary apparatus 1210, in conjunction with the vacuum system component 1220.

Generally the embodiments 1200 depicted in Fig. 12 illustrate how a chemical removal system could function, and it focuses in detail and in a close up view, on the components involved. By comparison, Fig. 13, depicts a more global view of some embodiments of a

chemical removal system 1300 embodiment to aid in the description both of the equipment employed in a preferred embodiment and some alterations. Fig. 13 1300 includes a capillary removal component 1305 and a Lens Precursor mounted on a forming optic and forming optic plate 1306 in a similar configuration and with the Lens Precursor pointing directly down.

Referring now again to Fig. 13, it may be apparent that the placement of the wicking capillary 1306 may in alternate embodiments be located at a position off of the center of the forming optic Lens Precursor 1305, center point. Item 1330 indicates a single dimension, of a xy translation table, where the adjustment is used to offset the capillary to forming optic center alignment. By way of example, the 1330 is depicted in a preferred embodiment manual vernier adjustment form. However, it may be clear to one skilled in the art that the adjustment may be performed by automation comprising stepping motors for example; and more generally, various levels of escalating sophistication in automation equipment for the location of the XY translation table would be anticipated within this invention. From an even higher level of generalization, and to simplify the following discussion, it may be assumed that any movement capability on the apparatus may have similar freedom in embodiment possibilities.

Item 1320, a forming optic holding apparatus, includes an apparatus to flexibly hold a forming optic in a desired firm location. The forming optic piece, as depicted as 1000 in previous discussion may employ similar location schemes as when located in the Voxel-based lithographic apparatus 500 in this embodiment. Alternative embodiments may enable the transfer of the forming optic holding apparatus 1000 under automated means. It should be apparent that numerous alternatives in manners of holding the forming optic and locking it into an appropriate location in a flowable chemical removal apparatus include consistent aspects of the current invention.

The discussion thus far has generally depicted embodiments with the axis of the forming optic located such that it is perpendicular to a horizontal plane and in the direction of gravitational forces. Alternative embodiments may allow a rotation of the axis at some angle about this perpendicular orientation. Item 1350 includes an adjustment means to alter the angle the forming optic axis makes with gravity. The fundamental effect of such a change would be that the fluent matter 1710 on the Lens Precursor will tend to pool at a location off of the center of the forming optic center. In some embodiments there may be advantages to drawing off fluent media at a location off center.

A number of indicated items in Fig. 13 relate to the location in a vertical manner of a capillary wicking apparatus 1306 to the fluent media on the Lens Precursor. For example 1340 may include a gross or rough adjustment of this dimension by moving the stage affixed to the wicking capillary 1306 along the vertical axis. Additionally 1345, includes a fine level adjustment for the same movement possibility. It is equivalently possible to adjust the forming optic mounting stage 1310 relative to the capillary wicking apparatus 1306 along the same axis. Item 1370 includes a fine adjustment apparatus for this purpose.

For the purpose of moving the wicking capillary into different orientations 1360 includes a rotary motion device. For example, such an embodiment may allow for simplified and automated capability for changing out the wicking device 1306.

As mentioned there may be numerous embodiments which relate to the automation of movements among the various components of the fluent chemical removal apparatus 1300. In addition, however, it is entirely within the scope of the invention for alternative embodiments to include optical measurements for controlling the process of removing chemical. Further alternative embodiments for such monitoring may include, for example, liquid level sensors of various types. By way of generalization, it may be obvious to one skilled in the art that the process of controllably removing in part a fluent chemical mixture from a solid support may require numerous sensing and metrology apparatus.

The spirit of the embodiments relating to apparatus for fluent lens reactive chemical removal discussed thus far includes methods and apparatus for the removal of a portion of the chemical 1710 from the surface of the Lens Precursor Form 1730. It may be apparent to one skilled in the art, that chemical cleaning steps may include embodiments with more aggressive cleaning options. Through use of industry standard cleansing techniques, the fluent lens reactive chemical 1710, may be removed in part or near entirety. By definition, apparatus with such cleansing action would convert the Lens Precursor 1700 into a different form. However, in some embodiments, it may be possible to reconstitute a Lens Precursor after said cleansing technique by applying a Reactive Mixture back upon the Lens Precursor Form's surface 1730, such as, for example via deposition, spraying, ink jetting or wicking.

Other embodiments of chemical removal may not use equipment external to a Lens Precursor Form 1740. Alternatively, since the shape of the Lens Precursor Form 1740, may be defined by numerous embodiments, there are designs of a Lens Precursor Form that may include

topographical depressions or channels (Item 440 in Fig. 4 400 includes some exemplary embodiments of such features and is discussed in other sections herein) in certain locations of the Lens Precursor Form 1740. By guiding the Fluent Lens Reactive Mixture 1710 into the channels a reduction in the amount of the Fluent Lens Reactive Mixture 1710 "On" the Lens Precursor Form 1740 may be obtained and may include said alternative embodiment of chemical removal. In general, it may be apparent that in embodiments of this type, the actual shape of the topographic relief features to function in this manner may vary and be generated into a free form surface.

Stabilization and Fixing Apparatus

The Lens Precursor 1700 includes a basis for additional embodiments of apparatus for the customized formation of an ophthalmic lens. The fluent layer of the Lens Precursor, shown in the depiction of one embodiment as layer 1710 provides novel manners to form an optical quality ophthalmic lens surface. When a Lens Precursor is placed upright, the fluent media may move over time. Under certain conditions, for example length of time, the fluent layer may spread under both gravity and surface forces to achieve a stable entity. The surface of the stabilized Fluent Lens Reactive Mixture 1710, can be represented by 1720. Under certain embodiments, a resulting surface 1720, may include an optically superior surface when compared to the surface 1730 of the Lens Precursor Form 1740. Numerous apparatus may provide the functional ability to stabilize the Fluent Lens Reactive Mixture 1710.

Proceeding now to Fig. 14, a stabilizing apparatus 1400 in a preferred embodiment is depicted. One aspect allows the flowing system to be isolated from movements or vibrational energy. This is accomplished in 1400 with component 1450. A relatively massive table 1450 can be supported upon a vibration isolation system 1440. As the force of gravity is also employed in such embodiments, it may be preferred for the massive table 1450 to have a flat surface that is level. A Lens Precursor 1410 can be attached to a forming optic holder 1430 which may be attached with a holding apparatus 1451. In some embodiments, automated timing equipment may be used to control a minimum amount of time for the fluent media to achieve a relatively stable state.

In some embodiments, the apparatus used for stabilization includes attached components allowing for the exposure of the Lens Precursor to an actinic irradiation step for the purpose of

fixing the Lens Precursor 1700 into a formed ophthalmic lens. In some embodiments, fixing radiation causes photochemical reactions to occur only in the Fluent Lens Reactive Mixture 1710. In alternative embodiments, other parts of a Lens Precursor, such as, for example, a Lens Precursor Form 1740, may undergo one or more chemical changes under the fixing radiation. Other embodiments that constitute variations based on the nature of the materials comprising the Lens Precursor may be obvious to an expert as consistent under the current invention.

In 1400, the source of fixing radiation is identified as 1460. By way of example, a similar light source to that previously discussed in the context of the Voxel – lithography optical system 520 may be employed. For example, in some embodiments, an AccuCure ULM-2-420 light source with controller from Digital Light Lab Inc. (Knoxville, TN USA) 1460 may constitute an acceptable source of the fixing radiation 1461. After the appropriate parameters are performed for stabilization, the controller for the fixing light source 1460 is switched to an on position exposing the Lens Precursor and surroundings to the fixing radiation 1461, and forming an ophthalmic lens of one embodiment form. From a general perspective, there may be numerous embodiments relating to the stabilizing or otherwise moving the Fluent Lens Reactive Mixture across the Lens Precursor Form 1730 surface and then in some manner irradiating with fixing radiation.

By way of example, some alternative embodiments for processing in the fixing apparatus may include a Lens Precursor Form where fluent material may have been washed off in a washing system. As this Lens Precursor Form in a fixed form may include a lens of certain characteristics in its own right, it is within the scope of the invention to anticipate embodiments that involve the use of the fixing apparatus in a manner that does not require the stabilization apparatus per se. In a more general sense, the invention may anticipate numerous embodiments of materials and forms where the fixing apparatus may fix materials that do not require a previous flowing of a fluent material on the surface to be fixed. By way of example, a Lens Precursor Form that has been formed with the Voxel-based lithographic optical system and has Fluent Lens Reactive Mixture 1710 washed off may still include an embodiment where the fixing apparatus is capable of fixing the Lens Precursor into a lens.

One set of embodiments includes alternative manners to cause the movement of the Fluent Lens Reactive Mixture 1710. By way of example, in some embodiments, agitating a Lens Precursor surface including Fluent Lens Reactive Mixture 1710 may enable the movement of the Fluent Lens Reactive Mixture 1710. Additionally, for example, it may be desirable in some

embodiments to spin a Lens Precursor around a central axis in a spin coating manner common to film processing.

Still other embodiments may include minimizing gravitational force experienced by the Fluent Lens Reactive Mixture 1710 by way of dropping the Lens Precursor 1410 in a controlled manner over a certain distance. Additional embodiments may alter the effect of gravity by changing the level of the surface 1450 upon which the Lens Precursor 1410, forming optic 1420, and holder 1430, are rested. With a different surface level, the forces on the Fluent Lens Reactive Mixture 1710 in the center optic region may vary and cause movement.

In another aspect, some embodiments may include chemical or physical changes to the Fluent Lens Reactive Mixture 1710. By way of example, an alternative embodiment may include the introduction of a solvent material in and around the fluent reactive chemical in such a manner to change its fluent nature. Additionally, said added material may effect the surface energy properties of components in the Lens Precursor system 1700. The properties of the fluent reactive chemical 1710 may be partially altered through the use of the fixing irradiation 1461, to alter the fluent nature in a manner that is distinct from fixing. Numerous alternative embodiments of a general nature relating to altering properties of the fluent chemical system may be anticipated by the nature of this invention.

At a significantly fundamental level, the nature of the reactive chemical mixture 945 may interact with the various embodiments of apparatus to enable different results. It should be apparent that the nature of the stabilization and fixing apparatus 1400, and variation in embodiments that derive from changing the fundamental chemical components in the reactive chemical mixture include embodiments within the scope of the invention. By way of example, this could include for example changes in the wavelength employed for fixing radiation and may introduce apparatus embodiments that have flexibility in said wavelength of fixation radiation.

As the materials of the Lens Precursor may include part of a formed lens, it may be obvious to one skilled in the art that the environmental controls in and around the stabilization and fixing apparatus include important embodiment aspects. For example, control of particulate matter with, for example, HEPA filtrated air flow may include one embodiment of environmental control. As the fluent media is still sensitive to actinic radiation, controls over stray light entering the environment include additional embodiment options. As well, humidity and other gaseous contaminants may effect lens quality and control over these environmental conditions may

include alternative embodiments. The numerous aspects of environmental control that may be apparent to one skilled in the arts include art within the scope of this invention.

The product of treating a Lens Precursor of some embodiment with the stabilization and fixation apparatus may include devices that are similar to or forms of ophthalmic lenses. In many senses this material has characteristics that directly relate to a final, hydrated ophthalmic lens. However, many embodiments after lens stabilization and fixation create an entity, still on the forming optic and holder 1430, that in the non-hydrated form may be subject to various forms of metrology.

Metrology Apparatus

Continuing to Fig. 15, a representation of an embodiment of a metrology apparatus capable of measuring optical and material characteristics is displayed. It may be obvious that metrology may be possible with both "dry" lenses, as would be the result following processing with the aforementioned fixation apparatus1400; and with hydrated lenses. This embodiment, however, focuses on metrology of dry lenses which desirably are still affixed to the forming optic. Referring to Fig. 15, the dry lens 1520, is still affixed to the forming optic 1530 and its appropriate holding components 1540. For an example, this holding component 1540, is affixed to a pair of mounts 1550 and 1560, that together enable controlled rotational movement of the lens about a central axis.

In some embodiments, the interaction of laser light 1515, from a laser displacement sensor 1510 such as one manufactured by Keyence (Osaka, Japan) model LT-9030, with the surface of the lens sample 1520 occurs as the sample 1520 forming optic 1530 and holding clamp 1540 rotate axially. A rotary servomotor 1570, drives a rotary bearing kinematic stage upon which the sample assembly sits. For stability of the rotation, the center of mass of the lens sample assembly is set, in some embodiments, as close to the center point as possible. As the stage rotates, the laser displacement sensor 1510, measures displacement of multiple points along axial rings of the surface of the lens 1520. After the stage rotates a full turn, the displacement sensor 1510 is moved azimuthally. Each movement creates a new circular profile around the surface of the lens. The process in this embodiment repeats until the entire lens surface has been profiled. By measuring a particular forming optic 1530 without the lens sample 1520, the surface location of the forming optic may be obtained in an equivalent spherical notation format. Subtracting this

result from the result with the lens upon the optic results in a thickness mapping of the lens product. Again, unique identification of a forming optic in an electronic format, via an attached RFID or by some other means, may include another embodiment form for the apparatus.

In some embodiments of this type, a free vibrational displacement of the sample surface 1520 relative to the sensor 1510 can include a significant error on the displacement measurement obtained by the system. Therefore, vibrational damping and isolation may be included. Accordingly, in some embodiments a massive supporting table 1580 sitting upon vibrational isolation mounts 1590 can be utilized to minimize vibrational effects. Some embodiments may be less sensitive to vibrational noise than others; however, generally speaking various methods of minimizing vibrational energy transfer modes into the environment around the various forms of detectors and the sample locating apparatus include embodiments within the scope of the invention.

Other embodiments may employ different measurement systems, in some cases in addition to the first described laser displacement sensor, to extract lens characteristics. By way of non-limiting example, a Shack-Hartmann Wavefront Sensor available from Thorlabs Inc (Newton, NJ, USA), may also be used in some embodiments to determine thickness of the formed lens body.

From a general perspective, there may be a significant diversity in metrology devices that are anticipated within the scope of this invention, including in part and for example, techniques to characterize the refractive index, radiation absorption, and density. Aspects relating to environmental controls may also be anticipated including for example, particle detection. These various techniques may be located in the same environment and location as the exemplary metrology device 1500, or in alternative embodiments may include additional locations within or external to the generalized system environment.

Collection, storage and communication of metrology and logistical data relating to particular samples and components used in the production of particular samples include a general embodiment principle of the invention. These various data may be useful in establishing feedback loops for control of lens characteristics. In an exemplary and preferred embodiment, the output from the laser displacement sensor based metrology apparatus 1500 for a lens sample 1520 is recorded and stored in a computing system. The individual forming optic piece, in one embodiment 1530, may have had the similar laser displacement metrology performed on it before

being used in the production of said sample 1520. Through use of the data computing system the displacement data may be processed in some manner to generate a representation of the thickness of the lens sample thus produced.

Within the computing system a desired model for the lens sample, useful in providing starting parameter set points for the various components in the lens fabrication system, may be compared to the manipulation of the displacement data for the sample,1520, and forming optic 1530. In some embodiments, various location points in a model may be mapped or correlated back to the individual components of the imaging system; in the preferred embodiment, a particular Voxel element in the Voxel-based lithography optic system. Via adjustment of the parameters for that Voxel, a next lens or Lens Precursor sample may be produced with adjusted performance compared to the previous sample. Within the numerous embodiments of metrology and the various calculational algorithms and apparatus, there should be a clarity to one skilled in the art, that many alternative embodiments of obtaining, processing, modeling, feeding back, and communicating of data include elements within the scope of this invention.

In some embodiments, metrology data of a particular system relating to the thickness of a produced lens sample 1520 may be enhanced via the use of alignment features designed into the profile of a Lens Precursor Form 1720. In the exemplary Fig. 4, 400, thickness metrology obtained in a manner similar to that described above was obtained. Other discussions of this 400 will be made elsewhere in this disclosure; but for use of understanding an alignment embodiment, the 440 may be considered. Item 440 may include a relatively deep profile recess in the surface of a lens sample 1520. The design of such a feature may be useful in orienting numerous processing steps in the apparatus. In one embodiment, the signal related to 400 may be extracted or recognized by an algorithm or manipulation of the metrology data. Such an extraction may be useful in locating portions of the various apparatus that are in proximity to or provide processing upon a location relative to the alignment feature 440. It may be apparent to one skilled in the art that numerous different embodiments of alignment features including the use of marking materials and designs of profile features among others are possible and include art within the scope of this invention.

Some alternative embodiments use of metrology data produced by a metrology system 1500 may utilize this data for diagnostic and control purposes for the entire ophthalmic lens production system or its various apparatus, therein. By way of non-limiting example, storage of

the above mentioned measurement of a forming optic 1530, may result in a history of such measurements. Through alternative computation and algorithmic processing, the characteristics of the surface could be compared over time and changes in those characteristics, of either an abrupt or steady manner might be used to flag a need for diagnostic intervention of some kind. One example, in the many possible causes of such a signal change, might include that a forming optic has received a surface scratch of some kind on its surface. In additional embodiments, statistical based process control algorithms could be used to both establish acceptable limits on metrology results obtained and to flag in an automated sense a valid change in measurement. Still additional embodiments may provide means for automation within the system to react to these flags in an automated means. However, from a general perspective, the invention scope anticipates these and numerous other embodiments of using metrology data from, for example, a system 1500, to diagnose and control the overall system.

The embodiments for the metrology apparatus discussed thus far may have generally pertained to metrology on a "dry" lens sample 1520 or its forming optic 1530. From a more general perspective, however, similar or additional metrology embodiments may derive from measuring characteristics of other forms in the total system. By way of non-limiting example, the "dry" lens may in some embodiments continue processing and become hydrated. Metrology on such a newly defined sample 1520, may include an example of the more general embodiment discussion. A further example may include performing metrology on a Lens Precursor sample 1700. Thus, in a general sense, there are numerous embodiments that are anticipated in the scope of the invention to perform metrology on the various forms of material used in processing or in comprising a product in an ophthalmic lens production system of this kind.

Hydration and Removal Apparatus

Another subsection of the apparatus for the production of an ophthalmic lens includes the steps of removing a lens or Lens Precursor from its forming optic, cleansing it and hydrating it. In some embodiments, these steps may be performed essentially simultaneously. Proceeding to Fig. 16 1600 an embodiment of apparatus to perform these steps, referred to as an hydration apparatus for simplicity, is depicted. The apparatus is included of a vessel for the containment of the hydration fluid 1610, A fluid bath 1620, that a lens 1630, and forming optic holder 1640 are immersed in and a thermal control unit 1650, to maintain the bath at a constant temperature.

In a preferred embodiment, the fluid bath 1620, is included of deionized (DI) water into which a surfactant has been added. There are numerous embodiments for this bath that are practiced in the art and are consistent with the scope of this invention. In an alternate embodiment, the fluid bath 1620, may be included of a mixture of an organic alcohol, sometimes in a mixture with deionized water and a surfactant. Therefore, some embodiments of the vessel 1610, may be included of materials that are consistent with containing a volume of water or organic alcohols and also transmitting thermal energy between a temperature control unit 1650 and the fluid bath 1620. From a perspective of generality, there may be numerous alternative embodiments, comprising materials of vessels, designs of vessels and means of filling and emptying vessels that fall within the scope of hydrating and cleansing a lens and include embodiments of this inventive art.

In some embodiments, the temperature of the bath is elevated to speed the hydration, cleansing and removal operation. In one such embodiment, the temperature may be maintained by the presence of a hot plate with internal sensing apparatus 1650. More advanced embodiments may include alternative manners to heat the fluid including alternative irradiative and conductive materials and apparatus. And, additional embodiments may include different manners to monitor the bath temperature and control it within a temperature zone. A still further and more advanced embodiment could include the ability to vary or program the temperature of the fluid bath in time. It may be obvious to one skilled in the art that numerous embodiments exist to control a hydration bath's temperature that include embodiments within the scope of this invention.

As the exposure of the lens 1630, and forming optic 1640 to the fluid bath proceeds and the lens becomes hydrated, in some embodiments the lens body will swell and eventually detach from the forming optic 1640. Therefore some embodiments may include means of catching the detached lens for assembly into appropriate storage and packaging means. Further embodiments may include, locating and picking the detached lens from the fluid bath media 1620. Alternatively, embodiments may provide the ability to strain said fluid bath media 1620 during a drain process to isolate a lens from the fluid. From a general perspective, numerous manners of localizing a lens and handling it into a storage means include consistent embodiments within the scope of this invention.

However, as referred to above, a lens in a swelled form may include optical characteristics that most match the performance of the lens while the lens is worn by a patient. Therefore, in

some embodiments, one or more metrology steps may be performed on the swelled lens. Such embodiments may include similar aspects of feedback, control and diagnostics as has been discussed with other metrology steps, and still additional embodiments may be apparent to an expert that derive from the swelling of the lens in the hydration apparatus.

These subsections include the five major subsections in this invention of an apparatus for formation of an ophthalmic lens. In a preferred embodiment, each has its own embodiment to define the apparatus. However, it may be clear that as each subsection of apparatus may contain numerous alternative embodiments even at a higher level there are alternatives that may exist that either have a different organization of the subsections or alternatively may have one or more subsection omitted and still include an embodiment under the scope of the invention.

Methods

The methodology disclosed in this invention essentially may include five major subsections, and therefore, the discussion of some embodiments of the methods will be organized into logical discussions at the subsection level. The subsections are the methodology concerning production of voxel-based lithographic Lens Precursors, a more generalized methodology of production of Lens Precursors, the various methodology of processing Lens Precursors, the post processing of lenses and Lens Precursors, and the methodology of metrology and feedback amongst the various sections. It should be noted that the following steps and description of methodology are exemplary and are not meant to limit the scope of invention as otherwise presented or set forth in the claims attached hereto.

There are embodiments of methodology which include all subsections or a subset thereof as well, accordingly, the order and inclusion of one or more method steps described does not limit the invention. Referring to Fig. 1, sub-sectional blocks of methodology 100 are identified, and include: a voxel-based lithography methodology 110; alternative forming methodology 120; Lens Precursor processing methodology 130; post processing methodology 140; and metrology and feedback methodology 150. In Fig. 1, two entities are identified in the oval shaped features; they are the Lens Precursor, item 160; and the ophthalmic lens as item 170. The arrows with a single flow may include the general direction that some embodiments may take, and the arrows with two heads on them depict that some or all of, materials, data and information can flow from the various methodology sections to and from the core measurement and feedback section.

Voxel-based lithography methodologies.

The methods of producing Lens Precursors from the voxel-based lithography apparatus include numerous embodiments related to the numerous apparatus embodiments as well as numerous methods to use these apparatus embodiments in the processing of Lens Precursors. Referring to Fig. 1, item 110, the voxel-based lithography methods, there is a beginning step demonstrated as box 115 that may include the initial step in making a lens from this system. Desired lens parameters may be input into an algorithmic calculation. In some embodiments these parameters may have been obtained by measuring optical aberrations on an ophthalmic patient's optical surfaces. These measurements can be turned into the required wavefront characteristics for the lens to be made to. In other embodiments there may be theoretical lens wavefront characteristics that may be input into the algorithm to determine lens production parameters. It may be obvious to one skilled into the arts that there may be numerous method embodiments related to the initial step of defining the desired output lens characteristics.

Continuing with item 115, an algorithm takes the above-mentioned input parameters, and in some embodiments correlates the parameters to previously produced lenses. A series of "frames" may now be determined for the exposure "movie" or script that will be communicated to the spatial light modulator. It may be obvious that there may be a multitude of embodiments related to the methodology that defines the algorithmic treatment of the required parameters that are inputted to an algorithm.

In a like way, there may be numerous methodologies that can be used to convert an algorithmic output for a particular voxel element into the planned light reflection profile in time that would include the "DMD" script. By way of example, the total intensity value desired by the algorithm may be delivered to a voxel location at the reactive mixture as a series of time steps where the input intensity of the light illumination systems is reflected during the entire time. The integrated intensity of these full "on" steps may then be supplemented by another time step where a partial value is written to the mirror element and thus the mirror has a duty cycle "On" level less then full on, for the remaining time steps that will be exposed to the reactive mixture as a whole, this particular voxel element could then be "off" for the remaining duration. An alternative methodology may include, taking the average value of intensity for the number of steps or "frames" that will be delivered and using that value to set the bulk of the frame values that are

sent to the DMD. It may be clear to one in the art, that the generality of spatial light modulators discussed in the previous apparatus discussion, as well, have methodology embodiments to correlate with the intent of creating this intensity and time exposure control.

While the above described methods are given examples relating to modulating a fixed intensity applied to the spatial illumination device through the action of the spatial illumination device, more advanced methodologies may derive if the intensity from the light source is modulated either at the source or in the optic system with light filtration. Further embodiments may derive from the combination of intensity control both in the illumination system components and in the spatial illumination modulator. Still further embodiments may derive from the control of the wavelength of illumination.

The method of forming the "DMD" script, which from a general sense should be considered to relate to control signals to any spatial light modulator of any size and also to the control signals of any system component, as for example the light source, filter wheel and the like, may therefore, in general include creating a series of programmed command sequences in time. It may be obvious to one skilled in the art, that there are numerous embodiments relating to the method of creating a control signal program that encompass the many embodiments of the details of the actinic radiation, of the details of the optic system employed and of the details of materials comprising the reactive monomer mixture.

It may be noticed that the details of the "DMD" script and the algorithms may have relationship to results obtained after processing. The feedback of critical parameters will be discussed later, and such detailed discussion is thus deferred. Nevertheless, in terms of the method of creation of a DMD script as shown in box 115, the double headed arrows pointing to and from the voxel based lithography methodology and feedback and metrology methodology refer in part to a role in this information exchange in the methods to create a DMD script.

Another input into the methodology of forming the Lens Precursors, is included by the various methods in formulating and preparing a reactive mixture for the system. In Fig. 1, item 111 is a box representation of the various methodologies included in the reactive mixture. It may be apparent to one skilled in the art that the apparatus embodiments discussed as within the scope of this invention, include a high degree of flexibility as to the type of and makeup of the components within the reactive mixture and it is anticipated as part of the invention, that an abundance of embodiments of the reactive mixture element include the scope of the invention.

Without loss of generality, for example, the chemical constituents acting as monomer units in the reactive mixture may include chemicals that are photoreactive to light in the ultraviolet spectrum, as has been described in some of the embodiments. However, these monomer molecules could likewise be chosen so as to photoreactively absorb radiation in the visible spectrum. Components within the system may likewise be tailored for consistency to another portion of the electromagnetic spectrum. Thus, it may be understood, that the materials methodology relating to this invention may include molecules sensitive to actinic radiation across a large portion of the electromagnetic spectrum.

In some embodiments, the monomer mixture is in reality a mixture of one or more actinically reactive monomer types that is also mixed with other chemical constituents. By reason of non-limiting example, other chemicals may be included as absorbing compounds. Such an additive to the monomer mixture may be, for example, important in embodiments that operate the voxel-based lithography in such a manner that the intensity of the actinic radiation along the path defined by a voxel element may be modeled by the Beer-Lambert-Bouguer Law. This component may largely define the thickness sensitivity of the formation process within the voxel element. It may be obvious to one skilled in the art that an abundant amount of embodiments may include art within the scope of this invention for adding a component to the monomer mixture that absorbs light within a relevant spectral region.

In other embodiments, the absorbing component of the monomer mixture may include additional complexity to that just discussed. For example, it may be within the scope of this invention for a method defining the absorber component to be included of multiple molecules that absorb light in differing manners. Additional embodiments may derive from absorber elements comprised of molecules that have multiple, relevant, bands of absorption themselves. Still further embodiments of methodology may include adding components to the monomer mixture that have a combined monomer and absorber role. This combined role in turn may in some embodiments also allow for a continued absorbance role even after a monomer undergoes chemical reaction. And, the opposite case may include embodiments to the method, where chemicals are added which have the property of altered absorbance as actinic reactions occur. From a general perspective, it may be clear that many embodiments for the methodology of comprising a reactive monomer mixture with a constituent to absorb radiation at one or more relevant spectral bands may be within the scope of the invention.

Additional embodiments may derive if addition of an inhibitor component is included into the method of preparing a monomer mixture. In this sense, an inhibitor compound would have a role in reacting with a chemical product that has formed in the reactive monomer mixture. In some embodiments, absorption of actinic radiation may generate one or more free radical chemical species. An inhibitor may act in reacting with the free radical species, and thereby, end a path of polymerizing reactions. One effect of such an embodiment would be to limit the duration of a photochemical polymerization reaction, or in other ways limit the distance that a polymerization reaction may occur away from the original photoabsorption initiator event. It may be apparent that some embodiments of the addition of inhibitor to the monomer mixture, therefore, may have relevance on the spatial resolution that a collection of photons in a voxel element will ultimately reflect in the spatial localization of the reactions that they initiate. In general, the action of the inhibitor may include numerous embodiments relevant to the art.

The types of chemical species or components of the reactive mixture that may act in an inhibitory manner includes numerous other embodiments of the art. As with the absorber, it is within the scope of the invention for an inhibitor to have dual roles, in inhibiting multiple polymerization pathways. Furthermore, the inhibitor may include a portion of a monomer molecule itself. And, in other manners of generality, the inhibitor may itself have a thermal or photoreactive sensitivity. Still other embodiments may derive from the nature of the inhibitor in its pure chemical state; as it may include a dissolved form in the mixture but exhibit gaseous, liquid or solid characteristics in its pure form.

The method of preparing a monomer mixture may have additional embodiments with respect to the addition of an initiator component. The initiator may include a photoabsorptive component that in absorbing a photon generates a chemical species that precipitates a polymerization reaction. The initiator may include a molecule that absorbs significantly in a particular band. Further embodiments may occur with initiator molecules that are photoabsorptive in multiple relevant bands for the apparatus. Its absorption may include a relatively broad band of relevant frequencies as well. Still further embodiments are possible if the initiator component of the monomer mixture derives from chemical initiator reactivity residing one or more of the monomer molecule types in the monomer mixture as well. Within the scope of the invention, it may be obvious to one skilled in the arts that numerous alternative embodiments

may include the methodology of comprising a monomer mixture with a component that acts as an initiator.

In some embodiments, the role of these described additives includes functionality towards the method for formation of an ophthalmic lens. In an example embodiment the monomer mixture used was Etafilcon A, a reactive monomer mixture having general use in the production of ophthalmic lenses. Referring again to Fig. 3, Etafilcon A includes a monomer component that under polymerization will form solids or gels. Etafilcon A also includes an absorber molecule, Norbloc, which absorbs UV radiation in a band comprising the lower wavelengths in item 300 and depicted for example as item 310. Furthermore, Etafilcon A also includes a component that acts as an initiator, and its absorbance is represented by item 340. In the mixture, the presence of dissolved gaseous oxygen includes an inhibitor role. Thus the methodology for forming a reactive monomer mixture in this embodiment includes both the formulation of a mixture of solid and or liquid components and further includes controlling a level of dissolved oxygen. The description of this embodiment is exemplary, and, therefore it is not meant to limit the scope of invention.

It may be apparent that other embodiments of the method to form the reactive monomer mixture in this invention may derive by control of physical aspects of the monomer mixture. In some embodiments, this may involve the addition of solvents or diluents to alter the viscosity of the mixture. Further embodiments may derive from other methods that result in altered viscosity of the mixture.

In the methodology of the preparation of the monomer mixture, additional embodiments may be defined from treatments performed on the nascent mixture. By way of non-limiting example, the mixture may be subjected to an evacuated environment which may result in the desorption of certain dissolved gaseous species. In another embodiment, the monomer mixture may be treated by exposing the bulk mixture to an exposure of actinic radiation, thus altering the degree and population distribution of multimeric components in the mixture before it is used in a subsequent actinic processing step. It may be obvious to one skilled in the arts that numerous additional embodiments may be possible for the purpose of treating a monomer mixture to result in an altered characteristic; the resulting mixture being useful in the further purpose of producing ophthalmic Lens Precursors and lenses.

Moving along the arrow in Fig. 1, to box 112, the methods for dosing and deposition of the reactive monomer mixture are of relevance. In some embodiments, an amount of the reactive mixture may be equilibrated to have a desired concentration of dissolved oxygen. In some embodiments, the equilibration may be accomplished by storing a vessel containing a significant amount of monomer mixture in an enclosure where the ambient includes the desired amount of oxygen to equilibrate to the desired concentration when dissolved. Additional embodiment may include automated equipment that may exchange the correct amount of oxygen into flowing reactive mixture via membrane technology. It may be obvious to one skilled in the art, that there may be numerous manners to alter or dose the reactive mixture to a desired level of incorporated gas consistent with the scope of the invention.

In some embodiments, a volume of the dosed reactive monomer mixture may now be transferred in a manual means into the reservoir comprising the vessel to contain the mixture in the proximity of the forming optic surface. Other embodiments may include automated mechanisms to fill the reservoir with the reactive monomer mixture. Still further embodiments of the invention may include filling disposable vessels that may be used when needed for the lens forming process. The invention scope includes using a methodology of some kind to fill the reservoir in proximity of the forming optic surface with at least an amount of reactive monomer mixture that is greater than the amount of material which will include a formed lens after all processing.

It may be apparent to one skilled in the arts that with the description of the various apparatus embodiments, material embodiments of the reactive monomer mixture, physical embodiments of the nature of the actinic radiation, and control formalism embodiments of the script and the apparatus it includes, one may now describe some of the embodiments that will form the output of the voxel-based lithography methodology. Moving in the process flow diagram, Fig. 1, item 116 indicates the forming methods that will use these various embodiments. It may be apparent to one skilled in the art that alternative embodiments for each of the components mentioned above may exist and that description of the methods pertaining to certain such embodiments do not limit the scope of the invention herein.

It may be useful to consider some of the methodology of item 116 at a microscopic scale. Consider, by way of non limiting example, an overall forming method where a monomer mixture includes an absorbing element such that there is a significant absorptive reduction upon the

intensity with the depth that the imaged actinic radiation has passed through; as may in some embodiments be modeled with a Beer's law formalism. And, for example consider the embodiment depicted in Fig. 3, where the wavelength of the actinic irradiation directed upon a particular voxel element is such that it is in the actively absorbed wavelength region for the initiator included into the reactive mixture and is in a rapidly changing absorption region for the absorber. Also consider, by way of non-limiting example that the monomer mixture includes an inhibitor. For easy reference and description, for this discussion this combination of methodology may be called Example 3. Although this is presented by way of enabling embodiment, it is not meant to limit the scope of the invention and other models may be used.

In one embodiment of Example 3, the inhibitor may be found in a significant concentration in the monomer mixture. At a microscopic level, this example embodiment may have the characteristic that the incident actinic irradiation defines a very limited local region around itself where chemical reaction initiated by the actinic radiation in a particular element will occur at a rate that exceeds the ability of the highly concentrated inhibitor to inhibit its furtherance. Because of the fact that some spatial light modulator systems will have a portion of their surface between each individual modulating element as "dead" space, not reflecting the light in the same manner as the modulating element, it may be apparent that in this embodiment, the resulting material that is formed upon the forming optic surface may take the form of isolated voxel-based columnar elements, that in the extreme may not connect with each other.

By way of continued non limiting examples of embodiments of Example 3, the inhibitor concentration may be found in a somewhat lower concentration and in this embodiment may, for example, be in a concentration where the spatial propagation for a given set of actinic illumination parameters is just far enough so that each of the voxel elements will define actinic activity that proceeds to overlap any border between voxel elements. In such a case on a microscopic basis, the individual columnar elements may tend to blend into each other for illumination conditions where neighboring voxels define significant intensity conditions. In some embodiments, the optical imaging system may be run in a mode where it is de-focused as another method embodiment to drive the individual columnar elements to blend together. In still further embodiments, a vibrational or wobble movement of the forming lens optic and holder in space may drive a similar effect where the voxel elements will overlap each other forming a continuous form piece.

It may be useful to continue describing the effects of the forming methodology at a microscopic basis in the depth dimension of the voxel element. It may be apparent, from the condition of Example 3, that a particular voxel element's "DMD script" may define an integrated intensity or exposure time which causes reaction to occur into the depth of the voxel element away from the forming optic surface. At some particular exemplary depth, this condition may include an intensity driven reaction condition in the monomer mixture where the degree of reaction defines a gel point. At depths that are less then this depth the reaction product may have formed a three dimensional aspect; however at depths greater than this depth, the reaction product may not have reached the gel point and may still include a mixture of components that is more viscous that the surrounding nascent reactive monomer mixture due to some level of monomer reaction that has occurred. In this embodiment, as may be clear, there was sufficient volume or the nascent reactive mixture to at least include these two regions; that is the regions where the reaction has occurred to a higher degree than the gel point, and the region where material includes a non-gelled layer which may be a mixture of partially reacted and unreacted monomer mixture. Under some embodiments, some of this layer may include what is called fluent lens reactive media. At a microscopic level it is being formed within the volume space of the reactive mixture.

In other embodiments, the "DMD script" may be useful to define local design elements into the voxel defined layer that has reacted past the gel point. This entity may be considered a Lens Precursor Form in some embodiments. By way of a non-limiting example, consider the effect of embedding an essentially linear feature into the DMD Script which is a number of voxel elements wide and many voxel elements in length and has the property of low integrated intensity for all voxel elements it includes. Using the embodiments discussed for Example 3, by way of non-limiting example, it may be envisioned that such a linear feature would be defined physically into the Lens Precursor Form. At the microscopic scale, neighboring voxel elements may include intensity to define their thickness in the Lens Precursor Form at some significant level. At the first neighboring voxel element of the linear feature, the form thickness will drop resulting in a profile feature related to the linear feature defined in the DMD script.

By way of example, referring to item 400 in Fig. 4, a representation of the thickness of a lens formed with an entire embodiment of this invention is presented. In this example, the lens thickness shows some features that have the characteristic of the linear feature thus described. Item 440, for example is a linear feature that extends for many voxel elements across a lens. It

may be obvious by inference, that the aspects of the invention include many different embodiments of shapes and profile features that may be defined in addition to the optical surface definitions of the lenses. Amongst, the numerous embodiments possible, by way of example there may be alignment features, like for example the embodiment intent of the feature 440. Additional embodiments may include profile features that define drain channels, linear feature extending along an essentially radial path toward the edge of the Lens Precursor Form; wells or bottomed holes in various shapes and sizes; abrupt steps up or down compared to the neighboring average topology; and plateaus or essentially flat features across a subset of the lens definition region. These examples are but a few of the numerous embodiments that may be apparent to one skilled in the art related to the forming step methodology.

Proceeding to step 117 of Fig. 1, in some embodiments the methodology relating to the removal of the material, resulting from step 116, away from the environment of the reactive monomer mixture is described. In some embodiments, one method for this removal may include the process of raising a forming optic with its holding piece and with the Lens Precursor Form from the reservoir of reactive monomer mixture. In other embodiments, the reservoir may be lowered away from the forming optic with the attached Lens Precursor Form. Still further embodiments may derive from automating either the lowering or raising step with equipment capable of controlling the rate of such removal with some precision. In alternative embodiments the reservoir of reactive monomer mixture may be drained in some manner resulting in separation of the forming optic with attached Lens Precursor Form from the reactive monomer mixture. From a general perspective it may be obvious to one skilled in the art that there are numerous embodiments which include step 117, of removing the product of step 116 from the reactive monomer mixture; these embodiments comprising art within the scope of this invention.

In Fig. 1, the products and intermediate products are indicated in an oval shaped pattern. Thus, the Lens Precursor 160 in some embodiments includes a device entity. For purposes of understanding other sections with discussion of methodology, a review of the aspects of a Lens Precursor is warranted. The Lens Precursor 1700 may be included of two layers; the Lens Precursor Form 1740 and the fluent lens reactive media, item 1710. These layers correspond in some embodiments to the previous discussion of the methodology of forming. In some embodiments the Lens Precursor Form is the material that has been defined by the voxel based lithographic system and has reacted past the gel point. It may have the various structural

embodiments discussed previously. In Fig. 17, the embodiment is portrayed where the voxel columns will have overlapped with each other during the forming methodology.

The fluent lens reactive media 1710 in some embodiments is the layer that is formed by the voxel based lithographic process that is deeper than the point at which the gel point has occurred in the reactive media. When the forming optic and reacted material is removed from the reactive monomer mixture, there may be a viscous material that adheres to the surface of the Lens Precursor Form. In the inventive art herein, this fluent film may in some embodiments be further processed with methods to be described. This combination of a Lens Precursor Form and the fluent material on it that becomes after further processing part of the lens is what makes up a Lens Precursor. It may be apparent that in some embodiments, the Lens Precursor assumes a unique structure. It has a component that includes a three-dimensional shape, however, because of the fluent nature of the adsorbed reactive media, the entity does not have a fixed three-dimensional form. It may be obvious to one skilled in the art that the scope of this invention includes all the various embodiments of form that the methods of forming, item 116, include as well as the different embodiments related to the methods of removing the forming optic from the reactive monomer mixture and their effect on the nature of the fluent lens reactive media.

In some embodiments, item 131, includes the embodiment of methodology to remove portions of the fluent lens reactive media from the Lens Precursor. As may be apparent from the previous sections on the apparatus comprising some embodiments to perform this methodology, there are a number of method embodiments possible for this purpose. By way of non-limiting example, the fluent lens reactive media may be removed by capillary action. In some embodiments, the methodology may include a dwelling step to allow some of the fluent lens reactive media to pool together before the step of capillary action is performed. In still further embodiments, the lens surface may be positioned so that its surface axis is angled relative to the direction of gravity. It may be obvious that numerous embodiments relating to methods to remove fluent lens reactive media with a capillary based apparatus may be possible and include art within the scope of this invention.

In other embodiments, the methodology to remove fluent lens reactive media may include alternative apparatus to the capillary wicking equipment. For example, a method comprising using an absorptive surface to remove the fluent media may include some embodiments. Additional embodiments may relate to methods using apparatus with may capillary points rather

than the one described in detail. Still further embodiments may include methods to spin process the Lens Precursor to remove the fluent material. Any of the numerous methods to use an apparatus to remove some of the fluent material, as may be obvious to one skilled in the arts may include aspects within the scope of this invention.

A different type of embodiment to remove material from the top surface of the Lens Precursor may include the method of defining relief features into the lens body for this purpose. In these types of embodiments, features such as the drain channels mentioned in a previous section may be designed for the purpose of creating a location to enable the relatively low viscosity fluent media to flow out of thereby creating below grade space for the relatively higher viscosity to flow into.. In further embodiments, the use of spinning of the lens body may also include embodiments to remove lens material in conjunction with designing relief features for the material to flow into. It may be obvious to one skilled in the arts that embodiments comprising the various embodiments of different relief surface design also include art within the scope of this invention.

In some embodiments, it may be possible to bypass the removal of fluent lens reactive media and continue to further processing steps. In Fig. 1, this aspect may be portrayed by the dotted line arrow running from element 160 around box 131.

The next step shown in the embodiments that include the methods of forming an ophthalmic lens may be illustrated in Fig. 1 box is item 132, stabilization. In some embodiments, this novel methodology includes the manner of processing that enables the fluent lens reactive media to flow under various forces to find a stable, perhaps low energy, state along the surface of the Lens Precursor Form. At a microscopic level, it may be evident, that a surface of a precursor form may locally have some level of roughness to it. Numerous aspects of the forming embodiments may determine the nature of this roughness, for example of one such case, the effect of the inhibitor to relatively abruptly stop reaction in the vicinity that it starts. The surface forces of the fluent media, frictional and diffusion forces, the force of gravity and other applied forces combine in many embodiments to create a smooth covering that has flowed over the topography. In the methodology that determines these forces there are numerous embodiment possibilities within the scope of the invention.

In one embodiment, the Lens Precursor may be configured to allow the fluent lens reactive media to flow under the force of gravity. The method to perform this may include the movement

of the Lens Precursor into different orientations to aid in flow. Alternative embodiments may include the opposite strategy by maintaining the Lens Precursor in a fixed state with as little movement as practical. Still further alternative embodiments may include subjecting the fluent material to the forces related to spinning the Lens Precursor around an axis. In some embodiments, this spinning may be performed around an axis centered in the middle of the Lens Precursor. In alternative embodiments, said spinning may include rotating the Lens Precursor around an external axis point while either facing the top of the Lens Precursor towards or away from the axis point or at the myriad possible orientations between such. In still other embodiments the Lens Precursor may be processed in a free fall environment to minimize the effect of gravity. It may be apparent to one skilled in the arts that there may be numerous methods related to the application of fluent forces to the Lens Precursor during a stabilization method.

In other embodiments, the fluent nature of the fluent media may be altered by methodology. In some embodiments, the viscosity of the fluent media may be altered by means of dilution or solvation. Alternative embodiments may include evaporating some of the diluent to increase viscosity. An exposure to some level of actinic radiation may include still further methods to alter said fluent films viscosity. There may be numerous embodiments relating to altering the viscosity of the fluent media.

In other embodiments, the surface energy related forces on the fluent lens reactive media may be altered by methodology. In some embodiments this may include the addition of surfactants to the nascent reactive monomer mixture. In alternative embodiments additives or chemical reactants may be added to the Lens Precursor for the purpose of altering the surface energy.

The design of the Lens Precursor Form may include methods to create different flow conditions of the fluent lens reactive media. Channels, as a non-limiting example, may include a means to draw fluent lens reactive media away from a region of the Lens Precursor. In alternative embodiments, design methods relating to abrupt profile change may include methodology for providing altered stabilized states. To an expert in the art, it may be apparent that the may be numerous methods in design of the Lens Precursor that include art within the scope of the invention.

From a general perspective, these various embodiment types should not limit the generality of methods to create a fully stabilized or partially stabilized or unstabilized nature of the fluent lens reactive media in the methodology comprising stabilization. Combinations of the various embodiments for example may be obvious, to an expert in the arts, additional embodiments for said methodology.

After a methodology of stabilization has been performed the fluent material may in some embodiments be subjected to a next methodology type indicated as item 133, fixation, to convert it into a non-fluent state. In some embodiments, the nature of the actinic radiation applied during the fixing method may include alternatives. The spectral band or bands applied may be an example of one type of methodology embodiment. Alternative embodiments may include the intensity of the radiation applied. In alternative embodiments, the application of various aspects of the fixation irradiation may include time dependency. By way of non-limiting example, an initial wavelength band may include a first step that then is changed to a different band. The universe of embodiments that may be obvious to one skilled in the art for the method of defining the light conditions are within the scope of this invention.

In some embodiments of item 133, the fixation method may include different paths that the irradiation may take. In an example of type of embodiment, the irradiation may occur on the front surface of the Lens Precursor; or alternatively through the back surface. Still other embodiments may derive from multiple sources of irradiation, some perhaps with different light characteristics to create different effects of the actinic radiation in the Lens Precursor entities. Still further embodiments may derive from the fixation method comprising other energy forms than radiation. By way of generality, the numerous methods that may include a fixation step are within the scope of the invention.

In some embodiments, after fixation has occurred, the processing of the Lens Precursor 130, has been completed. This completed product may, in some embodiments, be processed further. This product type includes a good example of the type of art indicated in block 120 of Fig. 1, alternative forming of a precursor. By way of non-limiting example, if the product of the fixation were introduced back into the voxel based lithography methodology a second layer of processing may occur. This multipass aspect introduces many embodiment methodology options.

In some embodiments, the complex Lens Precursor that may be formed from multiple passes which may include by way of non-limiting example, a first step where an ophthalmic lens

surface is defined and a second step where profile features are added to the surface. Other complex embodiments of the methodology may include, for example, a first pass through the voxel based lithography system with conditions, as some of the previous examples described, that make for isolated voxel columns along the Lens Precursor Form. A second voxel based lithography step may then include filling in the features between voxel columns with a material of a different characteristic. Continuing a third pass through the system may then define an ophthalmic lens. It may be obvious that the generalization to methodology of multiple passes through the system, each of which may have the abundant different embodiment possibilities discussed, may include a great many different embodiments all within the scope of the invention.

In some other embodiments, the Lens Precursor may be formed by applying a fluent reactive media onto a Lens Precursor Form. For example, the Lens Precursor Formed by way of the voxel-based lithography methods may be subjected to a washing system as an extreme method of removal of the fluent lens reactive media. A Lens Precursor Form will derive from the washing method. In some embodiments, this Lens Precursor Form may next be subjected to a method of adding a next fluent lens reactive media to its surface. The methodology of adding the next fluent media to the surface, in some embodiments may include dipping and removal of the Lens Precursor in methods similar to the embodiments described in item 117. The resulting Lens Precursor may now have a different distribution of monomer and multimeric molecules, or in some embodiments may include different polymer chemistry than that used to form the Lens Precursor Form. It may be apparent to one skilled in the art that numerous embodiments comprising the methodology to apply fluent lens media onto a variety of Lens Precursor Form embodiments includes art within the scope of this invention.

In an alternative set of embodiments, the Lens Precursor Form may be formed by other means than voxel-based lithography. In a first, non-limiting example, various embodiments may be possible by using stereolithography as the basis for forming the Lens Precursor Form. In some embodiments, this stereolithographically formed Lens Precursor Form may have fluent lens reactive media from a removal methodology as in 117, but other embodiments may include adding a fluent lens reactive media to the stereolithographically formed base. Alternative embodiments may be possible by using a masked based lithography process to determining the Lens Precursor Form and then using it in the methods mentioned. Still further embodiments may include the use of a Lens Precursor Form that is formed by a standard cast molding process

common in the manufacture of ophthalmic lenses, and then forming a Lens Precursor in the methods mentioned. It may be apparent that the numerous embodiments that form a Lens Precursor Form may include methods for forming a Lens Precursor.

After a Lens Precursor is formed by one of the various method embodiments and then processed by a method embodiment it may in some embodiments form an ophthalmic lens as a result. In some embodiments, the lens will now still be found upon the surface of the forming optic. In most embodiments it as well will need to be cleaned and hydrated to form a product form of ophthalmic lens. In methods that are generally standard to the art, the lens and in some embodiments its attached form may be immersed in a bath of aqueous solution. In some embodiments this bath will be heated to a temperature between 60 degrees and 95 degrees centigrade to aid in the method of immersion. Said immersion methods will in some embodiments, cleanse the lens body and hydrate it. In the process of hydration, the lens will swell and in some embodiments release from the support that it is adjoined to. It may be apparent that within the scope of the invention there may be means of coordinating the processing so that the same support and chemical handling structures may include embodiments for the hydration method as well. It should be noted that preceding steps and description of methodology are exemplary and are not meant to limit the scope of invention.

The resulting product after release in many embodiments includes the formed ophthalmic lens of the invention. It may be obvious that other steps upon this product are useful in the production of an acceptable product ophthalmic lens. The methodology in some embodiments may include standard art for isolating the hydrated lens, packaging it and then subjecting it to a sterilization process, item 142. It may be obvious to one skilled in the arts that the order that these steps include relative to each other and also relative to prior steps may include different embodiments consistent with the invention.

The various embodiments of ophthalmic lens, item 170, resulting from the apparatus and methods described herein include another dimension of the art in this invention. It may be clear to one skilled in the arts that the product of Lens Precursor may have unique forms to it. First the lens at some level is a composite of two hardened layers. One of these, the Lens Precursor Form, is in some embodiments formed by the actions of the voxel-based lithography apparatus and methods. This Lens Precursor Form may have numerous embodiments, some examples of which may be apparent from the previous discussions of methodology.

For example, with some method embodiments, the form may include a set of relatively isolated columnar voxel elements each with a different extension determined by the voxel lithography process. In other embodiments, the Lens Precursor Form may include a completely interconnected set of voxel based columns of material. It may be obvious to one skilled in the arts, that there are numerous embodiments relating to the actual composition of the monomer mixture. Furthermore, as previously mentioned in the context of methodology, the Lens Precursor Form may be formed by various other techniques than voxel based lithography, including but not limited to stereolithography, mask based lithography and machining. There are embodiments where the voxel based lithographic form has profile features designed with the voxel based technique; these include but are not limited to linear features, curvilinear features, wells, feature in partial height of the lens or in full height, abrupt changes in topology, plateaus and channels.

Still further, more complex embodiments may derive from the multiple pass aspect of the invention. A Lens Precursor Form, by way of non-limiting example, may be the composite of a first pass through a voxel based lithography step which defines a spherical type profile in the surface with abrupt features in its perimeter. A second pass may define customized ophthalmic parameters into the visibly active portion of the lens. By way of generalization it may be clear that there are abundant embodiments comprising multiple passes through the voxel based lithographic apparatus and methods. Variations may include different means to form the first pass, including the alternative lithography options discussed and, for example, a molded ophthalmic lens. This first lens type material includes a Lens Precursor when it is acted upon in a second pass, and ultimately may define a new lens embodiment.

The nature of the second component of a Lens Precursor, the fluent lens reactive media, in some embodiments, when incorporated into the lens defines novelty in the lens embodiment. When processed with the methodology and apparatus discussed for some embodiments, item 130, these embodiments may include a second distinguishable layer which has a smooth surface. The combination of the numerous embodiments of Lens Precursor Form and the various embodiments of fluent lens reactive media may include novel embodiments of an ophthalmic lens.

Formation of an ophthalmic lens may be enhanced via metrology and feedback 150. Some embodiments may include a straight processing methodology flow from box 116 through to item 170. However, superior embodiments may derive from using methods of metrology to drive

controls of the parameters of the various methods employed. In Fig. 1, these feedback mechanisms and flow of information are indicated schematically by the double headed arrows flowing to and from item 150. It may be apparent to one skilled in the arts that numerous metrology embodiments may include art within the scope of this invention.

Proceeding to Fig. 2, an exemplary embodiment of a metrology and feedback loop methodology related to the thickness and optical performance of a lens embodiment formed by the voxel based lithographic methods is depicted. In some embodiments, there may be a feedback loop that functions as depicted in item 200, starting with item 205 representing the input of desired lens parameters from an external source. For exemplary purposes, the model of the lens surface may come from an ocular measurement device applied to a patient's eye. In other embodiments, theoretical input parameters may include the methodology of step 205. These inputs will be processed in some methodology to align them with the input requirements of the voxel based lithography 210. The various apparatus and method embodiments will receive this input and, in some embodiments, with an algorithmic method convert them to useable parameters in the voxel based lithography system 211.

Proceeding further in Fig. 2, a Lens Precursor is made in the voxel based lithography system as shown in item 220. It may subsequently be processed with the Lens Precursor processing methodology 230 resulting in a "dry" form of an ophthalmic lens 240. This dry ophthalmic lens may now be measured in a metrology step 250. For exemplary purposes, this step may include use of a laser displacement sensor. Again by example, the surface topology result from this measurement may in some embodiments appear as is shown in Fig. 4, item 400. Algorithms may process this data, as depicted in items 251 and 252 to compare the result to what would be expected if the lens matched the input parameters from step 205. In some embodiments, differences from the input parameters may be processed and correspond with a need to change the parameters used to process the lens in the voxel based lithography system 211. This feedback loop of data and parametric information is depicted in the feedback loop of item 253. The data may also be processed and correspond to parameter changes desired in the Lens Precursor processing methodology 252. Feedback of desired changes to parameters in this system 252 is depicted by the feedback loop 254. It may be apparent that the various computational and control methodology may be performed on various data processing equipment including but not limited to mainframes, personal computers, industrial computers and other similar computational

environments. It should be noted that the steps shown in Fig. 2 and the description of related methodology are exemplary and are not meant to limit the scope of invention.

The results of the metrology step 250, and the various processing of the data 251 and 252, in some embodiments may include the ability to decide whether the produced lens 240, is within a set of acceptable limits around the input parameters of item 205. A decision on this lens is then shown in item 251 where the lens may be discarded for another lens to be produced with altered parameters. Alternatively, the lens may be within acceptable limits and therefore proceed onto step 260 for processing in the post processing methodology and apparatus embodiments. After the lens is then swelled and released it may be subjected to another metrology methodology as shown in item 270. In some embodiments, the result of this metrology could have similar feedback embodiments as has been indicated for step 250 in this embodiment. After an ophthalmic lens product is realized 280, the processing flow may join the flow where the dry lens was rejected. Thereafter it is possible for the entire flow to loop back to step 205 in a step indicated by the condition return step of 290. It may be apparent to one skilled in the arts that there are numerous modifications, additions and alternatives in performing a metrology step on the various products of this invention and then devising a feedback loop that incorporates the measured results and adjusts the system parameters.

In some slightly different embodiments, an additional type of measurement may gauge the quality aspects of the lens for global equipment feedback. As a non-limiting example, a particulate detection scheme may be deployed in some embodiments to measure the presence of such defects in the produced Lens Precursor. If such a measurement gave a result flagging a particulate issue, there could be a feedback loop that might in some embodiments involve feedback to an operator of the apparatus and methodology to remedy the issue flagged. It may be obvious to one skilled in the art that numerous metrology embodiments may include art within the scope of this invention where a measurement result is feedback to an operator.

In still further embodiments, the use of logistic data may include an element of a feedback loop. As mentioned in discussions of the apparatus of the invention, in some embodiments key components of the apparatus may have identification. This component identification may be tracked, in some cases, by an automation apparatus. The feedback may include, for example, that a particular component has been used for a particular aspect that includes its useful life. The feedback may in some embodiments be made to an operator, or include automated responses of

the system. In still further embodiments that use component identification, results of the previous metrology embodiments, where thickness results effect parameters of the system, the unique identification of a component, as for example the forming optic piece, may allow for individual tailoring of otherwise global parameters to that particular component. It may be obvious to one skilled in the art that the invention described herein includes numerous embodiments of various forms to obtain logistic and metrologic data, to process that data by various algorithmic means and by various data processing equipment, to discriminate that data from input lens requirements and to provide means to feedback that data to the system itself or to operators external to the system; all of which are considered within the scope of this invention.

A patient's eye measurement data may be obtained utilizing various types of clinical vision equipment and may be used to influence parameters such as, for example, size, shape, amount, and location of physical features that may be included a translating multifocal ophthalmic lens. Physical features included in a lens may be functionally important to aid in lens comfort and fit when upon an eye. Additionally, physical features may be functionally important to aid in one or both of vertical stability and rotational stability by limiting movement of a lens when a pupil's line of sight moves from one Optic Zone to another Optic Zone. A lens according to an aspect of the invention may include one or both of a lower-lid contact surface and an under-lid support structure.

In one aspect of the present invention, a lower-lid contact surface may include a contiguous, inward extension of an anterior surface portion that extends laterally across an entire anterior lens surface thereby, providing a shelf-like structure that may rest on a lower eyelid. A lower-lid contact surface may be located directly above an adjoining under-lid support structure. Furthermore, a lower-lid contact surface may take form in a variety of geometric shapes defined by one or both of points and lines with at least one curve to define a surface. Accordingly, a lower-lid contact surface may be contoured to an exact shape of a patient's lower eyelid that may provide for one or more of a better fit, wearer comfort, vertical stability, rotational stability, and limiting an amount of lens translocation when a wearer changes line of sight from one Optic Zone to another.

Furthermore, a lower-lid contact surface may be designed including a variety of different geometric shapes and Blend Zones. A Blend Zone may comprise a contiguous area blending a portion of a lens to another adjoining portion of a lens. For example, a lower-lid contact surface

may adjoin other features of a lens wherein, there may be no Blend Zones present, or there may be one or both of one or multiple of a top Blend Zone and a bottom Blend Zone present. Examples of lenses that are manufactured using the apparatuses and methods described herein are now described.

Referring now to Figs. 18A-20D, examples of multiple variations and Blend Zones (2008, 2010) of a lower-lid contact surface adjoining a Lens Edge, and an anterior surface are illustrated. For example, a Top Blend Zone 2008 may adjoin a superior anterior portion 2002 with the a lower-lid contact surface 2006 and a Bottom Blend Zone may adjoin a Lens Edge 2004 and a lower-lid contact surface 2006. A translating multifocal lens may include a lower-lid contact surface wherein, an under-lid support structure may not be present. For example, Blend Zones may blend into one or both of a superior anterior portion 2002 of a lens 2000, and a Lens Edge 2004 (shown in Figs. 18A-20D). In some examples, a lower-lid contact surface 2006 may include one or more of a zero slope 2006 Figs. 18A-18D, a negative slope 2012 Figs. 19A-19D, and a positive slope 2014 Figs. 20A-20D.

In another aspect of the present invention, an under-lid support structure may begin underneath and adjoin a bottom portion of a lower-lid contact surface, and extend to a lower Lens Edge. In preferred examples, an under-lid support structure may have a width (w) of 4mm or less, preferably a width of 2.1mm. Accordingly, an under-lid support structure may include an arcuate anterior surface essentially contoured to a surface of an eye. An under-lid support structure may be contoured to a patient's eye that may provide for a larger surface area and may allow a lens to more readily wrap around a cornea. Additionally, such an under-lid support structure may aid in one or more of improved wearer comfort, vertical stability, and rotational stability for a lens when upon an eye. An under-lid support structure may be designed based upon various techniques, for example, including one or more of a function-driven technique, a uniform axial thickness technique, a uniform radial thickness technique, and a Minimal Energy Surface (MES) technique. Furthermore, an under-lid support structure may occur across multiple cross-sections of a lens. As illustrated, an under-lid support structure may also include one or more concave or convex curved portions.

Referring now to Figs. 21A and 21B, these illustrate cross-section examples of an under-lid support structure 2400, designed via a function-driven technique. Fig. 21A illustrates an example of how a curved portion may be described and calculated via a function-driven

technique such as, a geometric equation of $(y-b)^2+ (x-a)^2 = R^2$ that represents curvature 2404 between a Start Point 2401 and End Point 2402 to design an under-lid support structure 2400 wherein, (a,b) represents the center of a circle and "R" represents the radius of a circle. Fig. 21B illustrates an example of how a curved portion 2406 may be described and calculated a function-driven technique such as, a trigonometric equation of $y=A\sin(n\cdot x) + B\cos(m\cdot x) +C$ that represents curvature between a Start Point 2401 and End Point 2402 to design an under-lid support structure 2400.

More generally, a function-driven technique may utilize equations that relate y as an f(x) to design an under-lid support structure 2400. Accordingly, there may be multiple geometric shapes and variations of an under-lid support structure 2400 that fall within the scope of the present invention. For example, a function-driven technique may be implemented via defining functions based upon a patient's eye data. Furthermore, implementation of a function-driven technique may result in either uniform thickness or non-uniform thickness variations of an under-lid support structure 2400.

Referring now to Figs. 22A and 22B, Fig. 22A illustrates a cross-section of a lens illustrating an under-lid support structure 2500 designed via a uniform axial thickness technique. Fig. 22B illustrates a plan view of a lens depicting a boundary 2504 of an under-lid support structure 2500 defined by multiple Start Points 2501 and End Points 2501 wherein, every axial lens thickness value 2503 is identical. A uniform axial thickness technique may describe a curved portion of an under-lid support structure via specifying one or more of a Start Point 2501 location, an End Point 2502 location, and a desired axial lens thickness 2503 relative to either one of a posterior surface 2506 and an anterior surface 2505.

Accordingly, one or more of a Start Point location 2501, an End Point 2502 location, and a desired axial thickness 2503 may be specified based upon a patient's eye data. Furthermore, combinations of Start Points 2501 and End Points 2502 may define a boundary 2504 including multiple axial lens thickness values 2503 each being identical to a desired axial lens thickness 2503 (as shown in Fig. 22) thereby, resulting in a design of an under-lid support structure 2500 including a uniform axial thickness.

Referring now to Figs. 23A and 23B, Fig. 23A illustrates a cross-section view of an under-lid support structure 2600 designed via a uniform radial thickness technique. Fig. 23B illustrates a plan view of a lens depicting a boundary 2604 of an under-lid support structure 2600

defined by multiple Start Points 2601 and End Points 2602 wherein, every radial lens thickness value 2603 is identical. A uniform radial thickness technique may describe a curved portion of an under-lid support structure via specifying one or more of a Start Point 2601 location, an End Point 2602 location, and a desired radial thickness 2603 relative to one or both of a posterior surface 2606 and an anterior surface 2605. In some preferred examples, one or more of a Start Point 2601 location, an End Point 2602 location, and a desired radial thickness 2603 may be relative to a posterior surface 2606 that usually includes a shorter arc length, as opposed to an anterior surface 2605 that may often result in non-continuous, misleading thickness profiles.

Accordingly, one or more of a Start Point 2601 location, an End Point 2602 location, and a desired radial thickness 2603 may be specified based upon a patient's eye data. Furthermore, combinations of Start Points 2601 and End Points 2602 may define a boundary 2604 including multiple radial lens thickness values 2603 each being identical to a desired radial lens thickness 2603 (as shown in Fig. 23B) thereby, resulting in a design of an under-lid support structure including a uniform radial thickness.

Referring now to Figs. 24A-24D, Figs. 24A-24C illustrate a cross-section view of various examples an under-lid support structure 2700 designed via a MES technique, whereby curved portions of an under-lid support structure 2700 may be designed by free flowing liquid, called Fluent Lens Reactive Media (FLRM) 2701. Fig. 24D illustrates a plan view of a lens depicting an under-lid support structure 2700 designed via a MES technique. For example, when utilizing a MES technique a FLRM 2701 may be used to form an under-lid support structure 2700, as opposed to using a gel included in a Lens Precursor Feature. For example, the under-lid support structure 2700 may follow the contour of the lens as in Figure 24A, the under-lid support structure 2700 may be concave as in Figure 24B or the under-lid support structure 2700 may be convex as in Figure 24C.

Accordingly, a FLRM 7201 may occur in a natural energy state and may "bridge" between two or more Lens Precursor Features 2700. In preferred examples, FLRM 2701 may bridge between two Lens Precursor Features to design an under-lid support structure 2700. Furthermore, for example, a Lens Precursor comprising gel features including both a Lens Edge 2703 and a lower-lid contact surface 2702, may allow design of an under-lid support structure 2700 to occur subsequent to, a FLRM 2701 bridging a gap between a Lens Edge 2703 and a lower-lid contact surface 2702 (as shown in Figs. 24A-24D).

In some other implementations, specified parameters of an under-lid support structure 2700 may be based upon a patient's eye data. Additionally, one or both of shape and thickness of an under-lid support structure 2700 may be dependent on one or more of volume of a FLRM 2701 available; heights, locations, shapes, and extents of gel features of a Lens Precursor; material properties of a FLRM 2701, and a gel; and operating conditions. Accordingly, one or both of shape and thickness of an under-lid support structure 2700 may be one or more of axially uniformly thick, radially uniformly thick, and non-uniformly thick.

In yet another aspect of this present invention, a lower-lid contact surface may adjoin an under-lid support structure of a lens 2105. Referring now to Figs. 25A-27D, illustrate examples of multiple variations and Blend Zones of a lower-lid contact surface 2101, 2106, 2108 adjoining an under-lid support structure 2102, and an anterior surface 2100. A translating multifocal lens may include a lower-lid contact surface, and an under-lid support structure. In some other examples, Blend Zones (Top Blend Zone 2103, Bottom Blend Zone 2104) may blend into one or both of a superior anterior portion 2100 of a lens 2105 and an under-lid support structure 2102 (shown in Figs. 25A-27D). In some additional examples, a lower-lid contact surface may include one or more of a zero slope 2101 Figs. 25A-25D, a negative slope 2106 Figs. 26A-26D, and a positive slope 2108 Figs. 27A-27D.

Alternatively, in some additional aspects of the present invention, referring now to Figure 28, illustrates method steps that may be implemented to form a translating multifocal contact lens. Patient data may be used to implement formation of a translating multifocal contact lens. In one example, eye data may be obtained from various ocular measurement devices such as topographers, wavefront devices, microscopes, video cameras, etc., and the data subsequently stored. In another example, an eye may be examined in various lighting conditions, such as: low, intermediate, and bright lighting conditions, in which any data obtained, may be stored.

Different types of eye data obtained may include, for example, eye shape; lower-lid position relative to an upper-lid, a pupil, and a limbus; pupil, and limbus size, shape, and location at near viewing, intermediate viewing, and distance viewing; and lower-lid radius of curvature, and distance from pupil center. In one example, data obtained from a patient's eye may influence features of a lens such as, a shape of a Lens; shape, size, location, and amount of Stabilization Zones present; shape, size, location, and amount of Optic Zones present; and shape, size, and location of a lower-lid contact surface, and an under-lid support structure of a Lens.

At 2200, a patient's eye measurement data may be input. At 2201, once received, a patient's eye measurement data may be converted by algorithms into usable lens parameters. At 2202, lens parameters may be utilized to define lens features included in a lens. At 2203, a Lens Design may be generated based upon specified lens parameters and lens features. For exemplary purposes, a Lens Design of a lens surface may be based upon parameter data acquired from one or more ocular measurement devices applied to a patient's eye. For example, size, shape, and location of an optical-power region of a Lens Design may be determined by a patient's pupil movement in various gaze directions. In some other examples, shape and location of a lower-lid contact surface may be governed by a patient's lower-lid position and movement. At 2204, a Free-form lens may be created based upon a generated Lens Design.

Referring now to Fig. 29, illustrates a controller 2300 that may be used to implement aspects of the present invention, such as, for example, the aforementioned method steps. A processor unit 2301, which may include one or more processors, coupled to a communication device 2302 configured to communicate via a communication network. The communication device 2302 may be used to communicate, for example, with one or more controller apparatus or manufacturing equipment components. For example, the apparatus illustrated in Figures 5 to 15.

A processor 2301 may also be used in communication with a storage device 2303. A storage device 2303 may comprise any appropriate information storage device, including combinations of magnetic storage devices (*e.g.*, magnetic tape and hard disk drives), optical storage devices, and/or semiconductor memory devices such as Random Access Memory (RAM) devices and Read Only Memory (ROM) devices. The storage device 2303 may have stored therein executable instructions, which when executed on the processor 2301 cause the apparatus described herein to perform the methods described herein. The executable instructions may include a DMD script described herein.

A storage device 2303 may store an executable software program 2204 for controlling a processor 2301. A processor 2301 performs instructions of a software program 2304, and thereby operates in accordance with the present invention such as, for example, the aforementioned method steps. For example, a processor 2301 may receive information descriptive of a patient's eye data. A storage device 2303 may also store ophthalmic related data

in one or more databases 2305 and 2306. A database may include customized Lens Design data, metrology data, and defined lens parameter data for specific Lens Designs.

A non-exhaustive list of aspects of the invention are set out in the following numbered clauses:

1. An apparatus for forming a translating multifocal contact lens, the apparatus comprising:

a light source emanating light in a wavelength comprising actinic radiation;

a processor in logical communication with a memory wherein said memory stores executable code, executable upon demand to cause the processor to generate one or more control signals for controlling the digital mirror device to project the actinic radiation through an arcuate substrate to:

form a contact lens comprising an anterior surface and a posterior surface on a voxel by voxel basis, wherein said anterior surface and said posterior surface comprise respective arcuate shapes and meet at a Lens Edge;

form an optical-power region to provide vision correction for an eye of a user wherein said optical-power region comprises multiple Optic Zones; and

form a lower-lid contact surface wherein the lower-lid contact surface limits the amount of said lens translocation upon the eye of the user when the user changes direction of vision and the user's line of sight moves from at least one Optic Zone to another said Optic Zone.

2. The apparatus of Clause 1 wherein the translating multifocal contact lens comprises a Free-form lens.

3. The apparatus of Clause 1 wherein the anterior surface comprises one or both of the lower-lid contact surface and an under-lid support structure.

4. The apparatus of Clause 1 wherein the lower-lid contact surface comprises a contiguous, inward extension of the anterior surface portion that extends laterally across said anterior lens surface.

5. The apparatus of Clause 4 wherein the lower-lid contact surface is located directly above the adjoining under-lid support structure.

6. The apparatus of Clause 4 wherein the lower-lid contact surface is located directly above the adjoining Lens Edge.

7. The apparatus of Clause 1 wherein the lower-lid contact surface comprises a geometric shape defined by one or both of points and lines with at least one curve to define a surface.
8. The apparatus of Clause 7 wherein the geometric shape includes one or more of a zero slope, a negative slope, and a positive slope.
9. The apparatus of Clause 4 wherein the lower-lid contact surface may comprise one or more of a Blend Zone.
10. The apparatus of Clause 9 wherein the Blend Zone comprises a contiguous area blending an anterior portion of the lens to another adjoining said anterior portion of the lens.
11. The apparatus of Clause 3 wherein the under-lid support structure adjoins the lower portion of the lower-lid contact surface and extends to a lower said Lens Edge.
12. The apparatus of Clause 11 wherein the under-lid support structure comprises an arcuate anterior essentially contoured to the surface of the eye.
13. The method of Clause11 wherein the under-lid support structure comprises a width of 4mm or less.
14. The apparatus of Clause 11 wherein the under-lid support structure provides for one or both of vertical stability for the Lens and rotational stability for the Lens.
15. The apparatus of Clause 11 wherein the under-lid support structure comprises a uniform thickness.
16. The apparatus of Clause 11 wherein the under-lid support structure comprises a non-uniform thickness.
17. The apparatus of Clause 11 wherein the under-lid support structure may be designed based upon a function-driven technique.
18. The apparatus of Clause 11 wherein the under-lid support structure may be designed based upon a uniform axial thickness technique.
19. The apparatus of Clause 11 wherein the under-lid support structure may be designed based upon a uniform radial thickness technique.
20. The apparatus of Clause 11 wherein the under-lid support structure may be designed based upon a Minimal Energy Surface technique.
21. A translating multifocal contact lens comprising:

an anterior surface and a posterior surface on a voxel by voxel basis wherein said anterior surface and said posterior surface comprise respective arcuate shapes and meet at a Lens Edge;

an optical-power region to provide vision correction for an eye of a user wherein said optical-power region comprises multiple Optic Zones; and

a lower-lid contact surface wherein the lower-lid contact surface limits the amount of said Lens translocation upon the eye of the user when the user changes direction of vision and the user's line of sight moves from at least one Optic Zone to another said Optic Zone.

22. The translating contact lens of Clause 21 wherein the lens comprises a Free-form lens formed on a voxel by voxel basis.

23. The translating contact lens of Clause 21 wherein the anterior surface comprises one or both of the lower-lid contact surface and an under-lid support structure.

24. The translating contact lens of Clause 21 wherein the lower-lid contact surface comprises one contiguous, inward extension of the anterior surface portion that extends laterally across said anterior Lens surface.

25. The translating contact lens of Clause 24 wherein the lower-lid contact surface is located directly above the adjoining under-lid support structure.

26. The translating contact lens of Clause 24 wherein the lower-lid contact surface is located directly above the adjoining Lens Edge.

27. The translating contact lens of Clause 24 wherein the lower-lid contact surface comprises a geometric shape defined by one or both of points and lines with at least one curve to define a surface.

28. The translating contact lens of Clause 27 wherein the geometric shape includes one or more of a zero slope, a negative slope, and a positive slope.

29. The translating contact lens of Clause 24 wherein the lower-lid contact surface may comprise one or more of a Blend Zone.

30. The translating contact lens of Clause 29 wherein the Blend Zone comprises a contiguous area blending an anterior portion of the lens to another adjoining said anterior portion of the lens.

31. The translating contact lens of Clause 23 wherein the under-lid support structure adjoins the lower portion of the lower-lid contact surface and extends to a lower said Lens Edge.

32. The translating contact lens of Clause 31 wherein the under-lid support structure comprises an arcuate anterior surface essentially contoured to the surface of the eye.
33. The translating contact lens of Clause 31 wherein the under-lid support structure comprises a width of 4mm or less.
34. The translating contact lens of Clause 31 wherein the under-lid support structure provides for one or both of vertical stability for the Lens and rotational stability for the Lens.
35. The translating contact lens of Clause 31 wherein the under-lid support structure comprises a uniform thickness.
36. The translating contact lens of Clause 31 wherein the under-lid support structure comprises a non-uniform thickness.
37. The translating contact lens of Clause 31 wherein the under-lid support structure may be designed based upon a function-driven technique.
38. The translating contact lens of Clause 31 wherein the under-lid support structure may be designed based upon a uniform axial thickness technique.
39. The translating contact lens of Clause 31 wherein the under-lid support structure may be designed based upon a uniform radial thickness technique.
40. The translating contact lens of Clause 31 wherein the under-lid support structure may be designed based upon a Minimal Energy Surface technique.

Conclusion

The description above and as further defined by the claims below, provides for a Free-form translating multifocal contacts lens wherein, a lens may include multiple variations of a lower-lid contact surface. In some examples, a lens may additionally include an under-lid support structure that may be designed based upon one or more various techniques.

CLAIMS

1. A translating multifocal contact lens comprising:

an anterior surface and a posterior surface on a voxel by voxel basis wherein said anterior surface and said posterior surface comprise respective arcuate shapes and meet at a Lens Edge;

an optical-power region to provide vision correction for an eye of a user wherein said optical-power region comprises multiple Optic Zones;

a lower-lid contact surface wherein the lower-lid contact surface limits the amount of said Lens translocation upon the eye of the user when the user changes direction of vision and the user's line of sight moves from at least one Optic Zone to another said Optic Zone; and

an under-lid contact support structure adjoining the lower portion of the lower-lid contact surface and extending to said Lens Edge, the under-lid support structure having an arcuate anterior surface including a concave portion and a convex portion.

2. The translating contact lens of Claim 1 wherein the lens comprises a Free-form lens formed on a voxel by voxel basis.
3. The translating contact lens of Claim 1 wherein the lower-lid contact surface comprises one contiguous, surface portion that extends laterally across said anterior Lens surface.
4. The translating contact lens of Claim 1 wherein the under-lid support structure provides for one or both of vertical stability for the Lens and rotational stability for the Lens.
5. The translating contact lens of Claim 1 wherein the anterior surface of the under-lid support structure is described by a function-driven technique.
6. The translating contact lens of claim 5, wherein said function driven technique is a sinusoidal function between a Start Point and an End Point of the under-lid support structure.