

CONTACT LENSES WITH STABILIZATION FEATURES

BACKGROUND OF THE INVENTION

- Correction of certain optical defects can be accomplished by imparting non-spherical corrective aspects to one or more surfaces of a contact lens such as cylindrical, bifocal, or multifocal characteristics. These lenses must generally be maintained at a specific orientation while on the eye to be effective. Maintenance of the on-eye orientation of a lens typically is accomplished by altering the mechanical characteristics of the lens. Prism stabilization including decentering of the lens' front surface relative to the back surface, thickening of the inferior lens periphery, forming depressions or elevations on the lens' surface, and truncating the lens edge are examples of stabilization approaches. Additionally, dynamic stabilization has been used in which the lens is stabilized by the use of thin zones, or areas in which the thickness of the lens' periphery is reduced. Typically, the thin zones are located at two regions that are symmetric about either the vertical or horizontal axis of the lens from the vantage point of its on-eye placement.
- Evaluating lens design involves making judgments concerning the performance of the lens on-eye and then optimizing the design if necessary and possible. This process is typically done by clinically evaluating the test design in patients. However, this process is time consuming and expensive because it requires a significant number of patients to be tested since patient to patient variability must be accounted for.
- There is a continuing need for improving the stabilization of certain contact lenses.

SUMMARY OF THE INVENTION

The invention is a contact lens designed with improved stabilization relative to a nominal stabilized design.

- In another aspect of the invention, a method for stabilizing contact lenses incorporates a lens design with a nominal set of stabilization zone parameters, evaluating the on-eye performance of the lens design, calculating a merit function based on this performance, and optimizing the stabilization zone parameters by applying the merit function. This process may be performed

iteratively via a virtual model (e.g., software based) that simulates the effects of eye mechanics such as blinking and adjusts the stabilization scheme accordingly.

In yet another aspect of the invention, contact lenses are stabilized according to a scheme in which the moment of momentum of torques acting on the lens on-eye are balanced.

- 5 In yet another aspect of the invention, contact lenses are stabilized by the formation of one or more zones having a different thickness than the remainder of the lens and in which these zones are located on the lenses such that the moment of momentum of torques acting on the lens when the lens is on-eye will be balanced.

- 10 In yet another aspect of the invention a contact lens has a stabilization zone with the bulk of its length lying beneath the horizontal axis of the lens.

In yet another aspect of the invention a contact lens has a stabilization zone having a differing rate of change of slope (from its peak) in one direction relative to the other.

In yet another aspect of the invention a contact lens has a different in height profile above the horizontal axis than it does below the horizontal axis.

15 **BRIEF DESCRIPTION OF THE DRAWINGS**

FIG. 1 is a front or object view of a stabilized contact lens.

FIGS. 2A-C -are schematic representations of an eye with an inserted lens that
identify the axis of rotation and various torques acting at the lens.

FIG. 3 is a flowchart showing a stabilization optimization process according to the invention.

- 20 FIGS. 4A-C is a-front view of a stabilized lens with stabilization zones and thickness graphs corresponding to example 1.

FIGS. 5A-C is a front view of a stabilized lens with stabilization zones and thickness graphs corresponding to example 2.

- 25 FIGS. 6A-C is a front view of a stabilized lens with stabilization zones and thickness graphs corresponding to example 3.

FIGS. 7A-C is a front view of a stabilized lens with stabilization zones and thickness graphs corresponding to example 4.

FIG. 8 is a graph showing rotation speed measurements.

5 DETAILED DESCRIPTION

Contact lenses of this invention have designs that optimize stabilization based on balancing various forces that act on the lenses. This involves the application of a design process that balances torques operating on the eye, components of the eye, and ultimately the stabilized lens that is placed on the eye. Preferably, improved stabilization is attained by starting the
10 improvement process with a nominal design that includes stabilization elements. For example, a lens design that has two stabilization zones that are symmetric about both the horizontal and vertical axes running through the center is a convenient reference from which to optimize stabilization of the lens according the inventive methods. By “stabilization zone” is meant an area of the peripheral zone of the lens which has thickness values larger than the average
15 thickness of the remaining areas of the peripheral zone. By “peripheral zone” is meant the area of the lens surface circumferentially surrounding the optic zone of the lens, and extending up to but not including the edge of the lens. Another stabilization design that is a useful starting point is described in US Patent Publication 20050237482 which is incorporated herein by reference but any stabilization design can be used as the nominal design that is then optimized according to
20 this invention. The stabilization design improvement process can also incorporate testing the improvement with the eye model described below, evaluating the results of the testing, and continuing iteratively with the improvement process until a desirable level of stabilization is achieved.

FIG. 1 depicts the front, or object side, surface of a stabilized lens. Lens 10 has an optical zone
25 11. The lens' periphery surrounds optic zone 11. Two thick regions 12 are located in the periphery and are stabilization zones.

The model that is preferably used in the process to produce the new designs incorporates various factors and assumptions that simulate the mechanical operation and their effects on lens stability. Preferably, this model is reduced to software using standard programming and coding techniques

according to well-known programming techniques. In broad overview, the model is used in the process for designing stabilized lenses by simulating the application of the forces described below in a prescribed number of blinks of the eye. The degree to which the lens rotates and decenters is determined accordingly. The design is then altered in a way that is directed to bringing rotation and/or centration to more desirable levels. It is then subjected to the model again to determine translation upon blinking after the pre-determined number of blinks. The alteration of the design is accomplished by the application of merit functions described in more detail below.

The model assumes that the eye preferably consists of at least two spherical surface parts representing the cornea and the sclera and that the origin of the x-y-z coordinate axes is in the center of the sphere representing the cornea. More complex surfaces such as aspheric surfaces may also be used. The base shape of the lens consists of spherical surface parts but the base curve radius of the lens is allowed to change from the center of the lens towards the edge. More than one base curve may be used to describe the back surface. It is assumed that a lens positioned on the eye assumes the same shape as that of the eye. The thickness distribution of the lens need not necessarily be rotationally symmetric and indeed is not symmetric according to some preferred embodiments of the inventive lenses. Thick zones at the edge of the lens may be used to control the position and orientation behavior of the lens. A uniform thin film of liquid (tear film) exists between the lens and the eye, with a typical thickness of 5 μm . This tear film is referred to as the post-lens tear film. At the lens edge the thickness of the liquid film between the lens and eye is much smaller and is referred to as the mucin tear film. A uniform thin film of liquid (also, tear film) with a typical thickness of 5.0 μm exists between the lens and the lower and upper eyelids and these are referred to as the pre-lens tear films. The boundaries of both the lower and the upper eyelids lie in planes having unit normal vectors in the x-y plane. Hence, the projections of these boundaries on the plane perpendicular to the z-axis are straight lines. This assumption is also made during the motion of the eyelids. The upper eyelid exerts a uniform pressure on the contact lens. This uniform pressure is exerted on the whole area of the contact lens covered by the upper eyelid or on a part of this area near the boundary of the upper eyelid with uniform width (measured in the direction perpendicular to the plane through the curve describing the edge of the eyelid). The lower eyelid exerts a uniform pressure on the contact

lens. This pressure is exerted on the whole area of the contact lens covered by the lower eyelid. The pressure exerted by the eyelids on the contact lens contributes to the torque acting at the lens through a non-uniform thickness distribution (thick zone) of the contact lens, especially near the edge. The effect of this pressure on the torques acting at the contact lens is referred to as the
 5 melon seed effect. Viscous friction exists in the post-lens tear film if the lens moves with respect to the eye. Viscous friction also exists in the mucin tear film between lens edge and the eye if the lens moves with respect to the eye. Additionally, viscous friction exists in the pre-lens tear film if the lens moves and/or the eyelids move. Strains and stresses in the lens occur due to the deformation of the lens. These strains and stresses result in an elastic energy content of the lens.
 10 As the lens moves with respect to the eye and the deformation of the lens changes, the elastic energy content changes. The lens tends toward a position at which the elastic energy content is minimal.

The parameters describing the geometry of the eye (cornea and sclera), base shape of the lens and the motion of the eyelids the eyelids are shown in Fig. 2. The motion of the lens follows
 15 from the balance of moment of momentum acting at the lens. Inertial effects are neglected. Then the sum of all moments acting at the lens is zero. Hence,

$$\begin{aligned}\vec{0} = & \vec{M}_{l,cor} + \vec{M}_{l,muc} + \vec{M}_{l,low} + \vec{M}_{l,upp} + \vec{M}_{l,Ulow} + \vec{M}_{l,Uupf} \\ & + \vec{M}_{l,Vupp} + \vec{M}_{ms,low} + \vec{M}_{ms,upp} + \vec{M}_{elast} + \vec{M}_{grav}\end{aligned}$$

20 The first 4 moments are resisting torques and are linearly dependent on the lens motion. The remaining torques are driving torques. This balance of moment of momentum results in a non-linear first order differential equation for the position β of the lens

$$A(\bar{\beta}, t) \frac{d\bar{\beta}}{dt} = \vec{M}_{total}^{driving}(\bar{\beta}, t)$$

This equation is solved with a fourth order Runge-Kutta integration scheme. The positions of points on the contact lens follow from a rotation around the rotation vector $\beta(t)$. The rotation matrix $R(t)$ transforming the old position of points to the current position follows from Rodrigues's formula

$$\begin{aligned}\vec{x}_{new} &= \vec{x}_{old} + \sin\beta(\vec{n} \times \vec{x}_{old}) + (1 - \cos\beta)(\vec{n} \times (\vec{n} \times \vec{x}_{old})) \\ \vec{x}_{new} &= R(t)\vec{x}_{old}\end{aligned}$$

$$\text{where } \vec{n} = \frac{\vec{\beta}}{|\vec{\beta}|} \text{ and } \beta = |\vec{\beta}|.$$

In the numerical integration method a time-discretization is used. Then the motion of the lens can be seen as a number of subsequent rotations, hence at the next time step t_{n+1} the rotation matrix is

$$R_{n+1} = R_{\Delta t} R_n$$

where $R_{\Delta t}$ is the rotation during the time step Δt .

The rotation matrix is decomposed into a rotation R_α and a decentration R_θ of the lens

$$R(t) = R_\theta(t) R_\alpha(t)$$

The rotation of the lens is a rotation around the centerline of the lens. The decentration is a rotation around a line in the (x, y) plane. Hence, the position of the lens is seen as a rotation $\bar{\alpha}$ of the lens around its centerline followed by a decentration $\bar{\theta}$.

In a preferred method of the invention, merit functions (MFs) based on these relationships are fashioned to adjust and thereby improve stabilization schemes of nominal designs. These merit functions are defined based on lens on-eye performance requirements. In a preferred embodiment the merit functions are defined but not limited to: a) lens rotation and centration performance (Equation 1), b) lens stability around a resting position (Equation 2), or c) Lens rotation and centration performance and stability around resting position (Equation 3).

$$MF_1 = \sqrt{W_R \left(\frac{Rot}{R_{REF}} \right)^2 + W_C \left(\frac{Cent}{C_{REF}} \right)^2}$$

(Equation 1)

By lens rotation is meant the angular movement of the lens around its z-axis occurring during and in between blinks. Rotation may be clockwise or counter clockwise depending on the initial position of the lens on the eye or the lens behavior when modeled on the eye.

By lens centration is meant the distance between the lens geometric center and the corneal apex. Centration is recorded in an x-y coordinate system in the plane of the corneal apex.

By lens stability is meant the amount of maximum lens movement in the horizontal direction (x axis) and the vertical direction (y axis) and amount of lens rotation during the blink period. Lens stability is preferably recorded with no lens misorientation and decentration after the lens reaches its final position.

5

Using Equation 1 as exemplary of the purpose and application of the merit function, Rot and Cent respectively describes lens performance in rotation and centration of the lens design to be optimized. R_{REF} and C_{REF} are variables describing the lens performance in rotation and centration of the initial lens design. W_R and W_C are two weighting factors allowing the adjustment of the contribution of one factor relative to the other and can take values between 0 and 1. When applied, as exemplified below, these functions are best solved numerically. The weighting factors are applied so that components of interest are given appropriate consideration. They may be equal or one component may be of more interest than another. Thus, for example, if one is more concerned with optimizing rotation than centration they would select a W_R that is greater than W_C . A stabilized design is improved when its merit function is decreased relative to the design that preceded it under this construct. Further, it is optimized when the merit function is minimized in such a case. Of course, one lens design may be preferable to another for reasons other than stabilization so an improved stabilization may still be undertaken according to the invention without necessarily optimizing the stabilization aspect of the design.

10

15

20

$$MF_2 = \sqrt{W_X \left(\frac{X_{Range}}{X_{REF}} \right)^2 + W_Y \left(\frac{Y_{Range}}{Y_{REF}} \right)^2 + W_\theta \left(\frac{\theta_{Range}}{\theta_{REF}} \right)^2} \quad (\text{Equation 2})$$

25

In Equation 2, X_{Range} , Y_{Range} and θ_{Range} describe lens performance in stability in horizontal direction, vertical direction and rotation of the lens design to be optimized,

X_{REF} , Y_{REF} and θ_{REF} the lens performance in stability in horizontal direction, vertical direction and rotation of the initial lens design, and W_X , W_Y and W_θ the weighting factors allowing the adjustment of the contribution of the factors relative to each others.

$$MF_3 = \sqrt{W_R \left(\frac{Rot}{R_{REF}} \right)^2 + W_C \left(\frac{Cent}{C_{REF}} \right)^2 + W_S \left(\frac{Stab}{S_{REF}} \right)^2}$$

(Equation 3)

In Equation 3 Rot, Cent and Stab describe lens performance in rotation, centration and stability of the lens design to be optimized, R_{REF} , C_{REF} and S_{REF} the lens performance in rotation, centration and stability of the initial lens design, and R_{REF} , C_{REF} and S_{REF} the weighting factors allowing the adjustment of the contribution of the factors relative to each others.

In another embodiment merit functions include wearing comfort and can also include stabilization zone volume, stabilization zone surface area, soft contact lens wearer awareness to stabilization zone or any other relevant criteria.

In further preferred embodiments the merit functions are defined from the following parameters in the same fashion as those set forth above:

- 20 - Rotation performance:
 - Surface area below the rotation curve response
 - Time to reach resting position in rotation within +/- 5.0 degrees
 - Initial rotation speed
- Centration performance:
 - 25 - Surface area below the centration curve response

- Time to reach resting position in centration
- First time to reach the final resting position
- Centration speed
- Stability performance:
 - Magnitude of movement in horizontal direction
 - Magnitude of movement in vertical direction
 - Magnitude of rotation
 - Duration of horizontal movement
 - Duration of vertical movement
 - Duration of rotation.
- Wearing comfort:
 - Volume of material in excess for building stabilization zone
 - Surface area covered by stabilization zone
 - Lens wearer awareness to stabilization zone

There is no limitation in the type of stabilization that can be produced by the method.

Stabilization zones can be of the following type:

- Symmetrical with respect to X and Y axis
- Symmetrical with respect to X or Y-axis
- Asymmetric with respect to both X and Y axis
- Constant radial distance
- Variable radial distance

Various stabilization zone parameters may be evaluated during the optimization, including without limitation the following: zone length, peak thickness location, ramp angles on either side of the peak, circumferential tilt of the zone, and zone width. The optimization parameters can also include lens diameter, base curve, thickness, optic zone diameter, peripheral zone width, material properties, other parameters describing lens features.

In a preferred embodiment of the invention, two types of improvement approaches are disclosed. In the first, a full optimization is conducted in which the model of on-eye behavior with a given iteration of the stabilization adjustment induced by the MF requires several blink cycles until the lens reaches its resting position. In another embodiment, the design is improved during a
5 predetermined number of blink cycles. Three blink cycles are generally the least that will be effective in providing meaningful stabilization improvements. In either case, the process is conducted iteratively with the application of the MF to a nominal design. In the case in which three blink cycles are used, an initial blink orients the lens at an angle α from the horizontal, intermediate blink where the lens is oriented at an angle β from the horizontal, and final blink
10 where the lens is positioned at the resting location. In the most preferred embodiment the angle α is set to 45 degrees and the angle β is set to 22 degrees (but both angles are not limited to these values). In another embodiment the optimization process is a combination of both approaches where a reduced number of blink cycles is preliminary used to reach an intermediate solution then several blink cycles are used to validate that the optimization has been conducted to an
15 acceptable degree.

Fig. 3 shows a flow chart of this improvement process. The initial stabilization zones design can be either a pre-existing design or a new design. Stabilization zone parameters from these designs are determined. These parameters are obtained from calculating the design performance when
20 the parameters are modified around their initial values. Parameters that give the most variations in the lens performance are preferably selected for the optimization process. In step 1, stabilization zone parameters are selected for consideration. These can include, for example, magnitude of the stabilization zone (Z_0), peak location along 0-180 deg. meridians (r_0), peak location angularly around the 0-180 deg. meridian (θ_0), slope above and below the peak location,
25 the angular length of the stabilization zone (σ_0), stabilization zones rotated around the peak location, and width of the stabilization zone (σ_R) among many others.

In step 2, the lens is defined mathematically in terms of the stabilization zones parameters to arrive at an initial or nominal design. There is no limitation in the type of mathematic function
30 describing the stabilization zones. Stabilization zones can also be described using computer

Weight	W_R	W_C	W_x	W_y	W_z	generated software such as CAD
Example 1	1.00	1.00	0.50	0.50	1.70	
Example 2	1.00	1.00	0.50	0.50	1.70	
Example 3	1.00	1.00	0.50	0.50	1.70	
Example 4	1.00	1.00	0.50	0.50	1.70	
Performance indicator	R_{REF}	C_{REF}	X_{range}	Y_{range}	θ_{range}	
Example1	505.110	1.100	1.03	2.65	1.88	
Example2	218.91	0.416	1.02	2.67	0.52	
Example3	277.22	0.356	1.03	2.68	0.67	
Example4	349.32	0.780	1.02	2.67	0.55	
	Merit functions		% Improvement			
	Equ. (1)	Equ. (2)	Equ. (1)	Equ. (2)		
Example1	1.414	1.643	N/A	N/A		
Example2	0.575	1.062	59.32	35.35		
Example3	0.637	1.106	54.96	32.68		
Example4	0.990	1.070	29.97	34.88		

- 5 applications. The mathematically described design (with defined parameters) is entered into the eye model in Step 3 and rotation, centration, and stability data is generated as shown in Table 1). This data can then be used to modify one or more of the stabilization parameters in optional step 4.

10

15

20 Table 1. Performance indicators obtained from designs of examples 1, 2, 3, and 4 applied to the merit functions defined by equations (1) and (2).

The stabilization zones are modified either by reshaping, scaling, rotating, shifting, or using any other techniques to modify the current design. In steps 5a-5d the modified stabilization parameters are again run through the eye model to generate rotation, centration, and stability data for each of now modified designs. In each case of corresponding steps 6a-6d merit functions are created and applied to each new design to generate new rotation, centration, and stability data in steps 7 and 8 as the lens is maneuvered (preferably through rotation). Again, in each iteration merit functions are calculated in step 9 and checked to see if they are decreasing in step 10. A decrease is an improvement over the previous iteration. If the merit function did not decrease then a stabilization parameter can then be modified again in optional step 11 and the resulting modified lens design is then put back into the selection and data generation steps 7 and 8. If the merit function did decrease it shows an improvement in stabilization and the lens design is determined to be the final design (step 12) or other zones are again improved in optional step 13. The invention may find its greatest utility in toric and multifocal lenses. Additionally, the designs may be useful in lenses customized to a specific individual's corneal topography, lenses incorporating high order wave-front aberration correction, or both. Preferably, the invention is used to stabilize toric lenses or toric multifocal lenses as, for example, disclosed in U.S. Pat. Nos. 5,652,638, 5,805,260 and 6,183,082 which are incorporated herein by reference in their entireties.

As yet another alternative, the lenses of the invention may incorporate correction for higher order ocular aberrations, corneal topographic data, or both. Examples of such lenses are found in U.S. Pat. Nos. 6,305,802 and 6,554,425 incorporated herein by reference in their entireties.

The lenses of the invention may be made from any suitable lens forming materials for manufacturing ophthalmic lenses including, without limitation, spectacle, contact, and intraocular lenses. Illustrative materials for formation of soft contact lenses include, without limitation silicone elastomers, silicone-containing macromers including, without limitation, those disclosed in U.S. Pat. Nos. 5,371,147, 5,314,960, and 5,057,578 incorporated in their entireties herein by reference, hydrogels, silicone-containing hydrogels, and the like and combinations thereof. More preferably, the surface is a siloxane, or contains a siloxane functionality, including, without limitation, polydimethyl siloxane macromers, methacryloxypropyl polyalkyl siloxanes,

and mixtures thereof, silicone hydrogel or a hydrogel, such as etafilcon A.

Curing of the lens material may be carried out by any convenient method. For example, the material may be deposited within a mold and cured by thermal, irradiation, chemical,
5 electromagnetic radiation curing and the like and combinations thereof. Preferably, for contact lens embodiments, molding is carried out using ultraviolet light or using the full spectrum of visible light. More specifically, the precise conditions suitable for curing the lens material will depend on the material selected and the lens to be formed. Suitable processes are disclosed in U.S. Pat. No. 5,540,410 incorporated herein in its entirety by reference.

10 The contact lenses of the invention may be produced by any convenient method. One such method uses an OPTOFORM.TM. lathe with a VARIFORM.TM. attachment to produce mold inserts. The mold inserts in turn are used to form molds. Subsequently, a suitable liquid resin is placed between the molds followed by compression and curing of the resin to form the lenses of
15 the invention. One ordinarily skilled in the art will recognize that any number of known methods may be used to produce the lenses of the invention.

The invention will now be further described with respect to the following non-limiting examples.

20 **Example 1**

A contact lens having a known design for correcting the vision of astigmatic patients is shown in Figure 6. It was designed using conventional lens design software with the following input design parameters:

Sphere power: -3.00D

25 Cylinder Power: -0.75D

Cylinder Axis: 180 deg

Lens diameter: 14.50mm

Front optical zone diameter of 8.50mm

Back optical zone diameter of 11.35mm

30 Lens base curve: 8.50mm

Center Thickness: 0.08mm

Eye model parameters used are listed in Table 2A and 2B.

The stabilization zone is an extra thick zone added to the thickness profile of that lens. The initial stabilization zone is constructed using a combination of normalized Gauss functions describing the radial and angular changes in thickness. The mathematical expression describing the Sag of the stabilization zone in polar coordinates is:

$$Z(R, \theta) = Z_0 \cdot \text{Exp} \left(-0.5 \cdot \left(\frac{r - r_0}{\sigma_R} \right)^2 \right) \cdot \text{Exp} \left(-0.5 \cdot \left(\frac{\theta - \theta_0}{\sigma_\theta} \right)^2 \right)$$

Where Z_0 is the maximum magnitude of the stabilization zone, r_0 and θ_0 the radial and angular location of the peak, and σ_R and σ_θ are parameters controlling the profile of the thickness change in the radial and angular directions.

The change in slope along the radial and angular direction is obtained using log-normal Gauss distributions. The equation becomes:

$$Z(R, \theta) = Z_0 \cdot \text{Exp} \left(-0.5 \cdot \left(\frac{\text{Log}(r) - r_0}{\sigma_R} \right)^2 \right) \cdot \text{Exp} \left(-0.5 \cdot \left(\frac{\text{Log}(\theta) - \theta_0}{\sigma_\theta} \right)^2 \right)$$

The design parameters controlling the stabilization zones are:

Change in magnitude of the stabilization zone (Z_0).

Peak location changes along 0-180 deg. meridians (r_0).

Peak location changes angularly around the 0-180 deg. meridian (θ_0).

Slope changes above and below the peak location.

Change of the angular length of the stabilization zone (σ_θ).

Stabilization zones rotated around the peak location.

Change in width of the stabilization zone (σ_R) along the 0-180 deg. meridian.

The values from which the initial stabilization zone were built were:

$$Z_0 = 0.25\text{mm}$$

$$r_0 = 5.75\text{mm}$$

$$\sigma_R = 0.50\text{mm}$$

$$\theta_0 = 180 \text{ degrees and } 0 \text{ degrees for left and right stabilization zones, respectively}$$

5 $\sigma_\theta = 25.0 \text{ degrees}$

The stabilization zone was then added to the original lens thickness profile. The final maximum lens thickness was 0.38mm. A graphic illustration of the profile is shown in Fig. 4.

Stabilization zones are symmetric about both horizontal and vertical axes with slopes that uniformly descend from peak height

5

Tear film	Aqueous layer viscosity	8.30E-04	[Pa.s]
	Mucin layer viscosity	1.50E-03	[Pa.s]
	Mucin layer thickness	3.50E-07	[m]
	Pre-lens tear film thickness	5.00E-06	[m]
	Post-lens tear film thickness	5.00E-06	[m]

10

Eye geometry	Cornea Radius	7.95E-03	[m]
	Sclera Radius	1.15E-02	[m]
	Visible Cornea Radius	5.82E-03	[m]
	File (eye geometry)		[mm]

Lens properties	Lens base curve radii	8.50E-03	[m]
	Lens transition radii	5.50E-03	[m]
	File (lens back geometry)		[mm]
	Contact angle edge	-5.00	[degree]
	Contact area lens edge	2.40E-05	[m2]
	Density of lens material	1000	[Kg/m3]
	Young's modulus	280000	[N/m2]
	Poisson's ratio	0.48	[-]
	File (lens normal thickness profile)		[mm]

15

Eyelid geometry and blink properties	Lower eyelid lateral displacement	4.00E-03	[m]
	Upper eyelid lateral displacement	3.50E-03	[m]
	Time to complete downward motion upper eyelid	0.082	[s]
	Time to complete blink	0.258	[s]
	Time between two blinks	3	[s]
	Eyelid pressure	200	[N/m2]
	Lower eyelid position at start of blink	6.35E-03	[m]
	Upper eyelid position at start of blink	4.70E-03	[m]
	Width pressure band at upper eyelid edge	5.00E-04	[m]
	Angle upper eyelid at start of blink	-4.47	[degree]
	Angle lower eyelid at start of blink	-2.07	[degree]
	Eye velocity	2	---

Gaze direction	Eye gaze (choice in predefined transient gaze direction)	0	---
	Amplitude gaze	20	[degree]
	Frequency gaze	2.78	[Hz]

Initial position	Initial rotation angle lens	0.00	[degree]
	Initial decentration in X-direction	0.00	[m]
	Initial decentration in Y-direction	0.00	[m]

Gravity	Gravity	9.80	[m/s2]
---------	---------	------	--------

20

Simulation parameters	Number of cycles that has to be simulated	5	---
	Number of time steps in [0, Tdownblink] (If <0 then specified time step is used)	-400	---
	Specified time step	0.005	[second]
	Lens discretization in radial direction	20	---
	Lens discretization in circumferential direction	90	---

Table 2A. Initial parameters provided to the eye model.

Eye velocity				
1	Velocity eyelid constant			
2	Velocity eyelid matching human eye velocity			
Eye gaze (choice in predefined transient gaze direction)				
0	No change in gaze direction			
1	Horizontal motion			
2	Vertical motion			
3	Circular motion (counter clockwise)			
4	Circular motion (clockwise)			
5	Constant gaze in horizontal direction			
6	Constant gaze in vertical direction			

Table 2B. Initial parameters provided to the eye model.

- 10 The contact lens rotation and centration characteristics were determined using the eye model described above with initial parameters provided in Table 2. Rotation of the lens steadily decreased from about 45 deg to less than 10 degrees as the number of blinks modeled went from 0 to 20. Over the course of blinks 1-20, centration remained relatively steady from about .06 mm to just over .08 mm. The resulting value of the merit function defined by equation 1 applied on
- 15 the prior art lens was 1.414 with $W_R = W_C = 1.0$. This example shows the rotation, centration and stability achieved by the lens of these parameters where maintenance of the on-eye orientation is achieved using depressions or elevations on the periphery of the front surface.

Example 2:

- 20 A new stabilization zone was designed using the eye model and optimization method described above and the initial design described in Example 1. The merit function was defined using
- Surface area below the response in rotation.
 - Surface area below the response in centration.
 - Identical weight for rotation and centration, $W_R = W_C = 1.0$.

25

The values from which the initial stabilization zone were built were:

- $Z_0 = 0.25\text{mm}$
- $r_0 = 5.75\text{mm}$
- $\sigma_R = 0.50\text{mm}$
- 5 - $\theta_0 = 180$ degrees and 0 degrees for left and right stabilization zones, respectively
- $\sigma_\theta = 25.0$ degrees

The stabilization zone was then added to the original lens thickness profile.

- 10 The stabilization zone was rotated around the peak location until the lens performance characteristics represented a significant improvement over the initial design. The rotation was obtained by applying a coordinate transformation (rotation around the peak location) on the original stabilization zone coordinates:

$$15 \quad (x, y) = \begin{bmatrix} \cos(\alpha) & \sin(\alpha) \\ \sin(\alpha) & \cos(\alpha) \end{bmatrix} (x_0, y_0)$$

Where (X_0, Y_0) were the original coordinates and (x, y) were the new coordinates, and α the angle of rotation.

- 20 An improved stabilization design was obtained in which the final orientation of the stabilization zone was 10.0 degrees off from the vertical with the upper portion of the stabilization oriented toward the center of the lens as shown in Fig. 5. Additionally, stabilization zones are not symmetric about the horizontal axis. In this case, the bulk of the long dimension of each zone lies above the horizontal axis. The final value of the merit function was 0.58 . Improvement on the merit function was of the order of 59% . Rotation declined sharply relative to the initial
- 25 stabilization design. Beginning at blink 4 less than 30 degrees rotation were seen with no rotation from blink 12 onward compared to about 40 - 25 degrees of rotation seen in the initial

design over the same range of blinks.. Centration remained steady with less than 0.04 mm on blink 1 and less than 0.03 thereafter in the improved design relative to 0.06 to greater than 0.08 for the initial design over the same number of blink cycles. This example shows improved rotation, centration and stability as compared with the lens of Example 1.

5

Example 3:

A new stabilization zone was designed using the eye model and optimization method described above and the initial design described in Example 1. The merit function was defined using

- Surface area below the response in rotation.
- Surface area below the response in centration.
- Identical weight for rotation and centration, $W_R = W_C = 1.0$.

The values from which the initial stabilization zone were built were:

- $Z_0 = 0.25\text{mm}$
- $r_0 = 5.75\text{mm}$
- $\sigma_R = 0.50\text{mm}$
- $\theta_0 = 180$ degrees and 0 degrees for left and right stabilization zones, respectively
- $\sigma_\theta = 25.0$ degrees

The stabilization zone was added to the original lens thickness profile.

An improved stabilization design was obtained in which the final orientation of the stabilization zone was such that the peak location of the stabilization zone was changed angularly around the 0-180 deg. meridian from the geometrical center of the lens as shown in Fig. 6. Stabilization zones are no longer symmetric about the horizontal axis and the rate of change of the slope of those zones differs in direction away from the 0-180 meridian. The final value of the merit function was 0.64. Improvement on the merit function was of the order of 55%. Rotation declined sharply relative to the initial stabilization design. Beginning at blink 4 less than 30 degrees rotation were seen with about 10 degrees of rotation seen at blink 10 and no rotation from blink 16 onward compared to about 40-30-15 degrees of rotation seen in the initial design

over the same range of blinks.. Centration was less than 0.06 mm on blink 1 and less than 0.04 at blink 4. Thereafter it dropped sharply, being less than .02 at 8 blinks and zero at blink 16 relative to greater than 0.06 to greater than 0.07 and greater than 0.08 for the initial design over the same number of blink cycles. This example shows improved rotation, centration and stability as compared with the lens of Example 1.

Example 4:

A new stabilization zone was designed using the eye model and optimization method described above and the initial design described in Example 1. The merit function was defined using

- Surface area below the response in rotation.
- Surface area below the response in centration.
- Weight for rotation $W_R = 0.84$, weight for centration $W_C = 1.14$.

The values from which the initial stabilization zone were built were:

- $Z_0 = 0.25\text{mm}$
- $r_0 = 5.75\text{mm}$
- $\sigma_R = 0.50\text{mm}$
- $\theta_0 = 1.954$
- $\sigma_\theta = 0.14$

The stabilization zone was added to the original lens thickness profile. The stabilization zone was adjusted to change the slope around the peak location. Peak locations remain on the 0-180 degrees meridian as shown in Fig. 7. Stabilization zones are not symmetric about the horizontal axis and the rate of change of the slope of those zones differs in direction away from peak height. This is accentuated in this case with a much more gradual decline in slope toward the bottom portion of the lens. Slope changes were obtained using a log-normal Gauss distribution function for describing angularly the thickness change. The final value of the merit function was 0.86. Improvement on the merit function was of the order of 30%. Rotation declined moderately

relative to the initial stabilization design. Beginning at blink 6 less than 30 degrees rotation were seen with about 10 degrees of rotation seen at blink 12 and no rotation from blink 16 onward compared to about 38-30-15 degrees of rotation seen in the initial design over the same range of blinks.. Centration was less than 0.08 mm on blink 1 and less than 0.07 at blink 4. Thereafter it
5 dropped sharply, being less than .05 at 8 blinks and 0.04 at blink 16 relative to 0.06 to greater than 0.07 and 0.08 for the initial design over the same number of blink cycles. This example shows improved rotation, centration and stability as compared with the lens of Example 1.

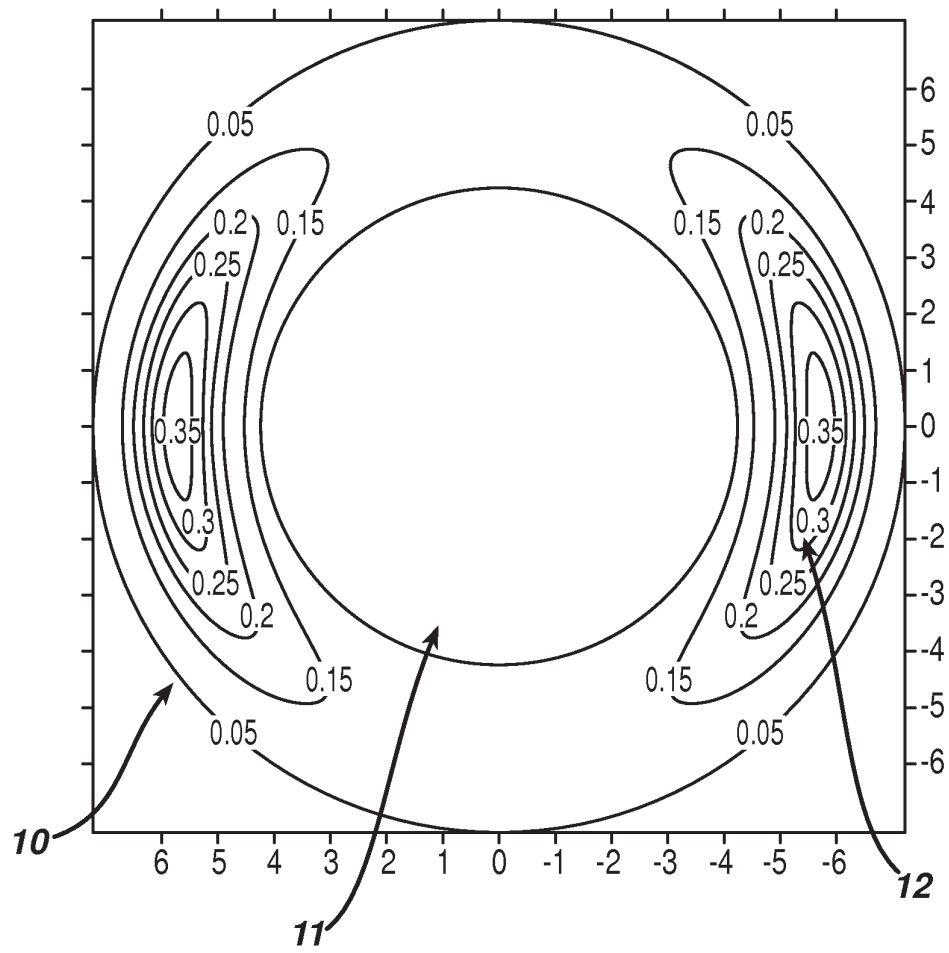
Figure 8 summarizes the rotation speed versus lens orientation on eye for the example 1, 2, 3,
10 and 4. The initial design described in example 1 has an average rotation speed of about -0.55°/sec. in the 45°-0° miss-orientation range, while designs given in examples 2, 3 and 4 have an average rotation speed above -0.70°/sec. within the same miss-orientation range. Example 2 and 4 have higher rotation speed for miss-orientations below 15°. Both designs are more adequate for lenses requiring single orientation on eye such as soft contact lenses designed for
15 high order aberration correction. These designs might require different fitting method requiring special fiducials on the front surface to help the patient for lens insertion. As the lens orientation on eye is unique due to the asymmetry of the stabilization and because of the markings on the front surface, the orientation of the lens during insertion should be very close to the final orientation of the lens after it reaches its resting position. High rotation speed for small miss-
20 orientation at insertion will provide faster full vision correction. Those designs also present better centration performance over the design of example 3. Lens centration gets stable over a smaller number of blinks.

Claims

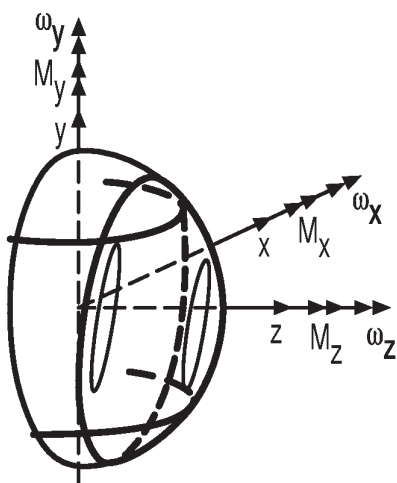
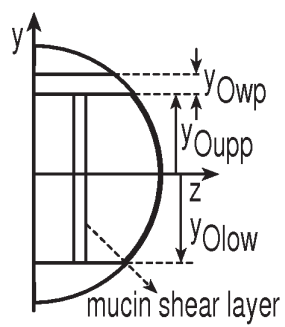
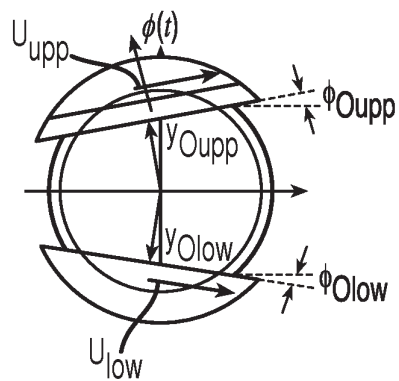
We claim:

- 5 1. A contact lens designed with improved stabilization relative to a nominal stabilized design wherein the moments of momentum are balanced.
2. The contact lens of claim 1 wherein a stabilization zone has the bulk of its length lying beneath the horizontal axis of the lens.
- 10 3. The contact lens of claim 1 wherein a stabilization zone has a differing rate of change of slope (from its peak) in one direction relative to the other
4. The contact lens of claim 1 wherein a stabilization zone has a different height profile
15 above the horizontal axis than it does below the horizontal axis
5. The contact lens of claim 1 wherein the distance from the lens center to a point along the contour of maximum thickness of a stabilization zone is different from the distance from the lens center to another point along the contour of maximum thickness of the same
20 stabilization zone.
6. The contact lens of claim 1 wherein the distance from the lens edge along a meridian to a point along the contour of maximum thickness of a stabilization zone is not the same as the distance from the lens edge along a meridian to another point along the contour of
25 maximum thickness of the same stabilization zone

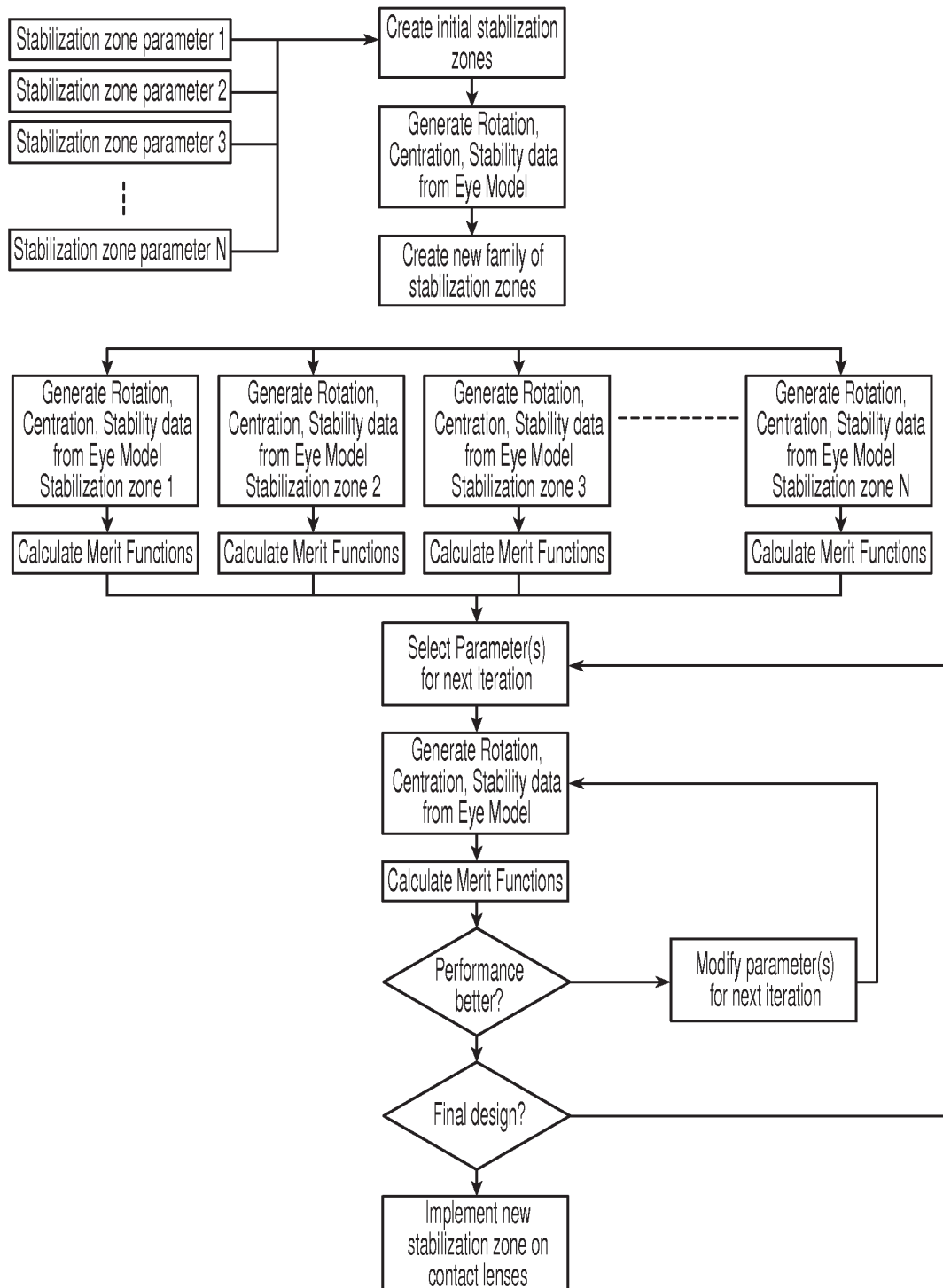
1/12

FIG. 1

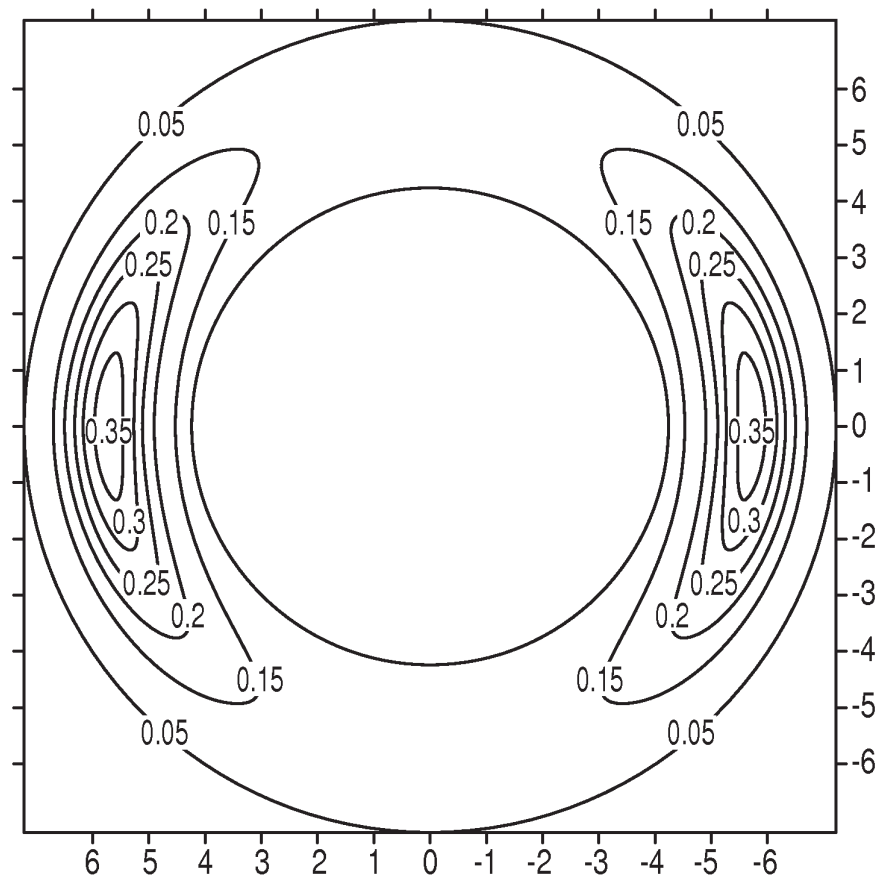
2/12

FIG. 2A**FIG. 2B****FIG. 2C**

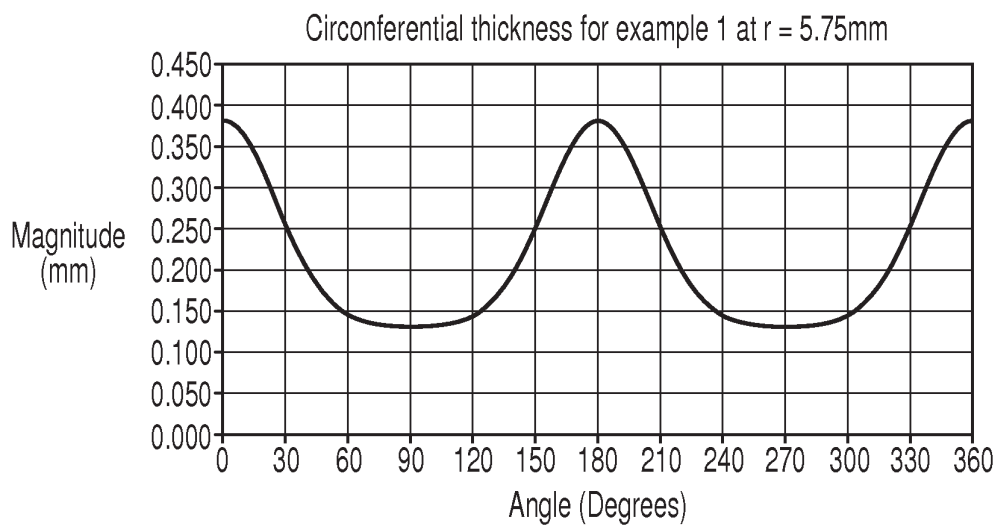
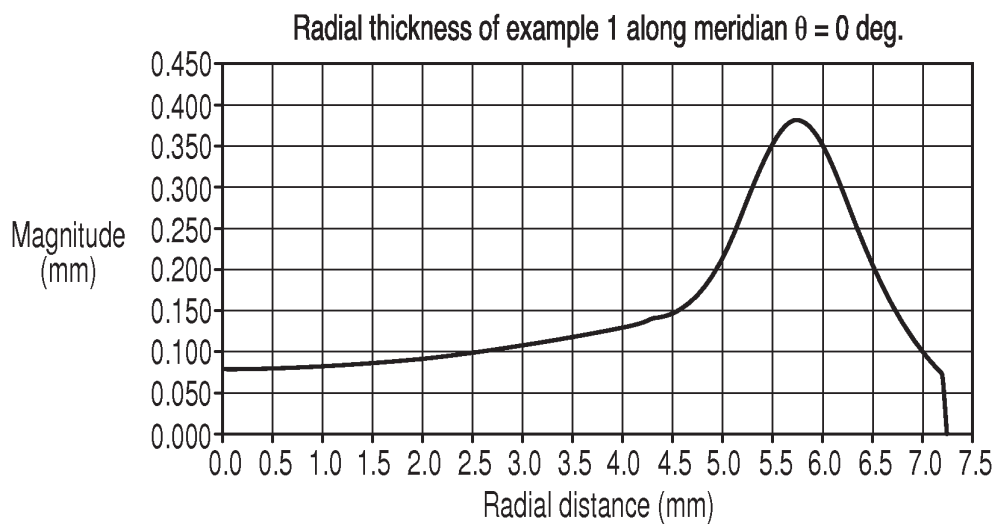
3/12

FIG. 3

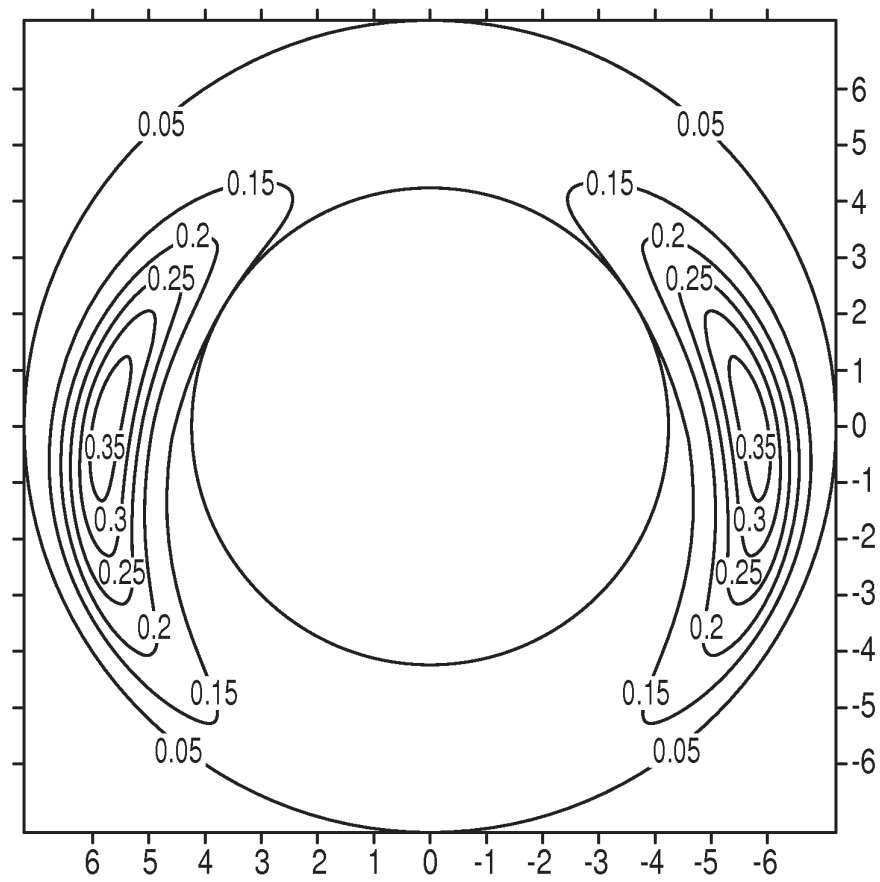
4/12

FIG. 4A

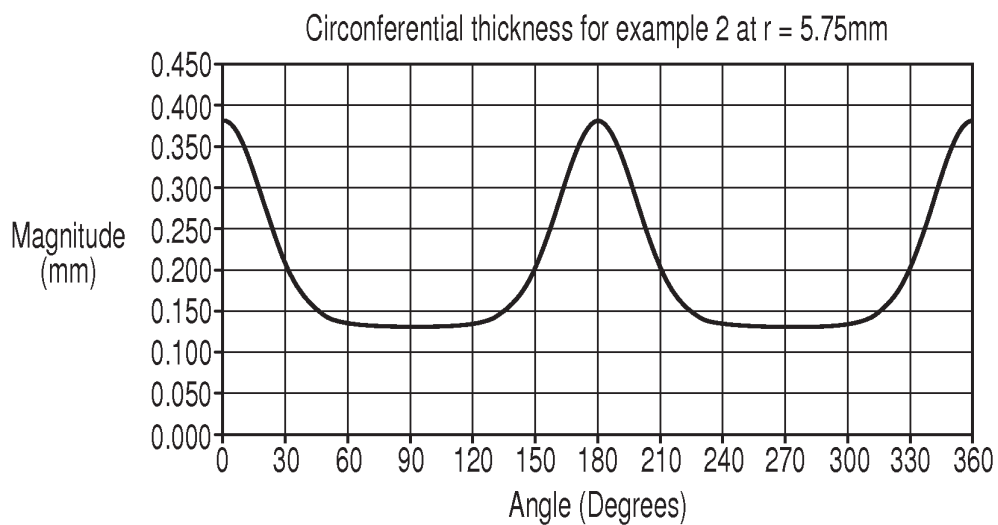
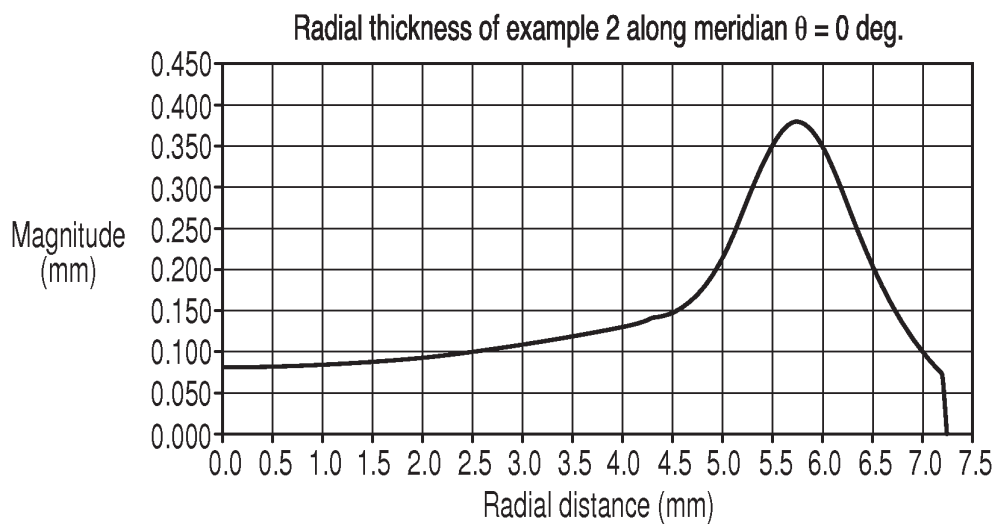
5/12

FIG. 4B**FIG. 4C**

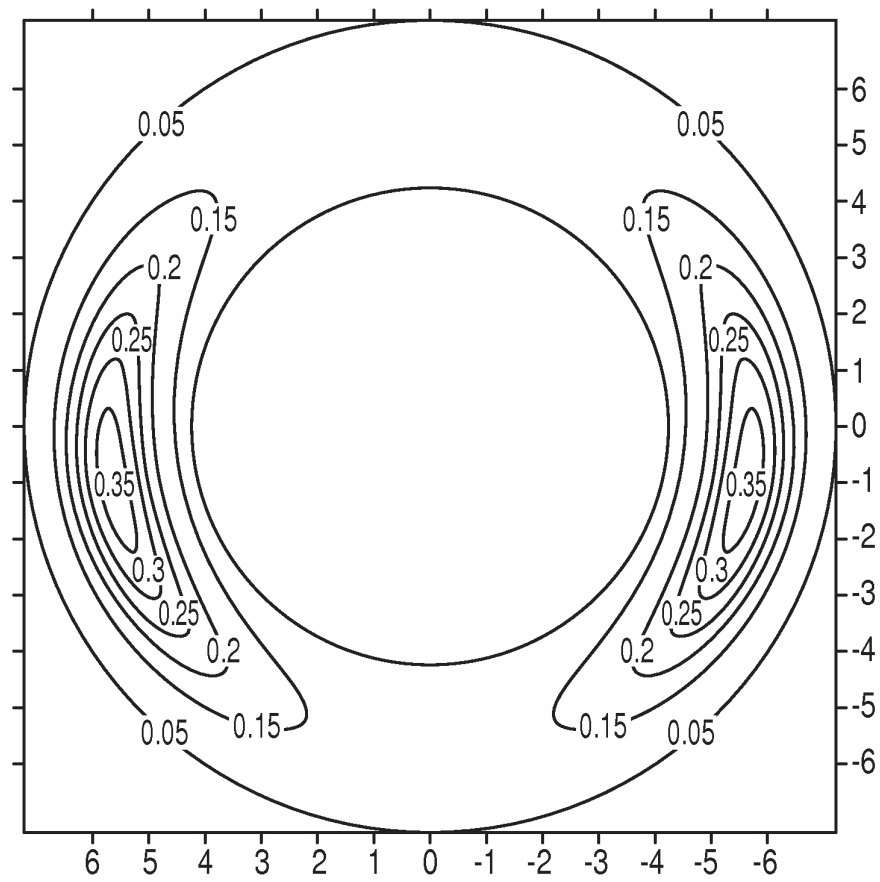
6/12

FIG. 5A

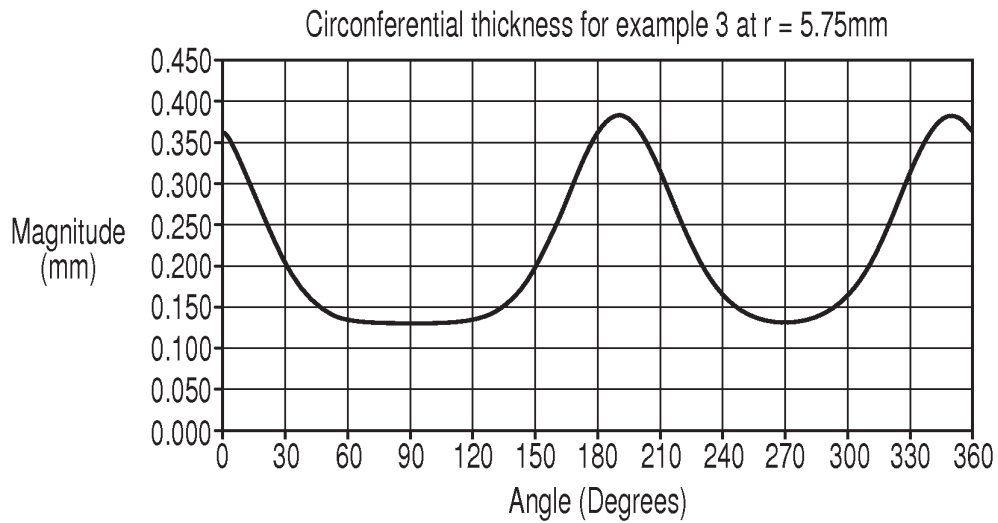
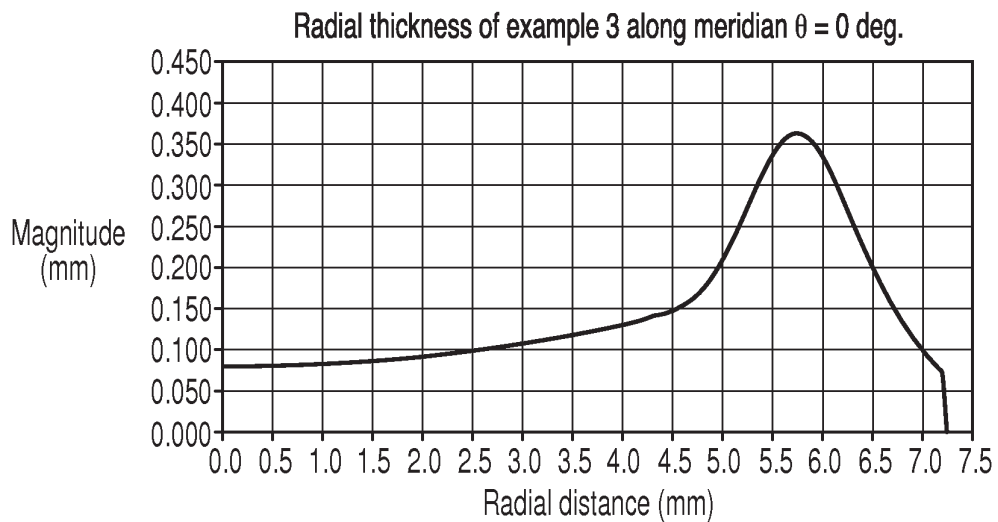
7/12

FIG. 5B**FIG. 5C**

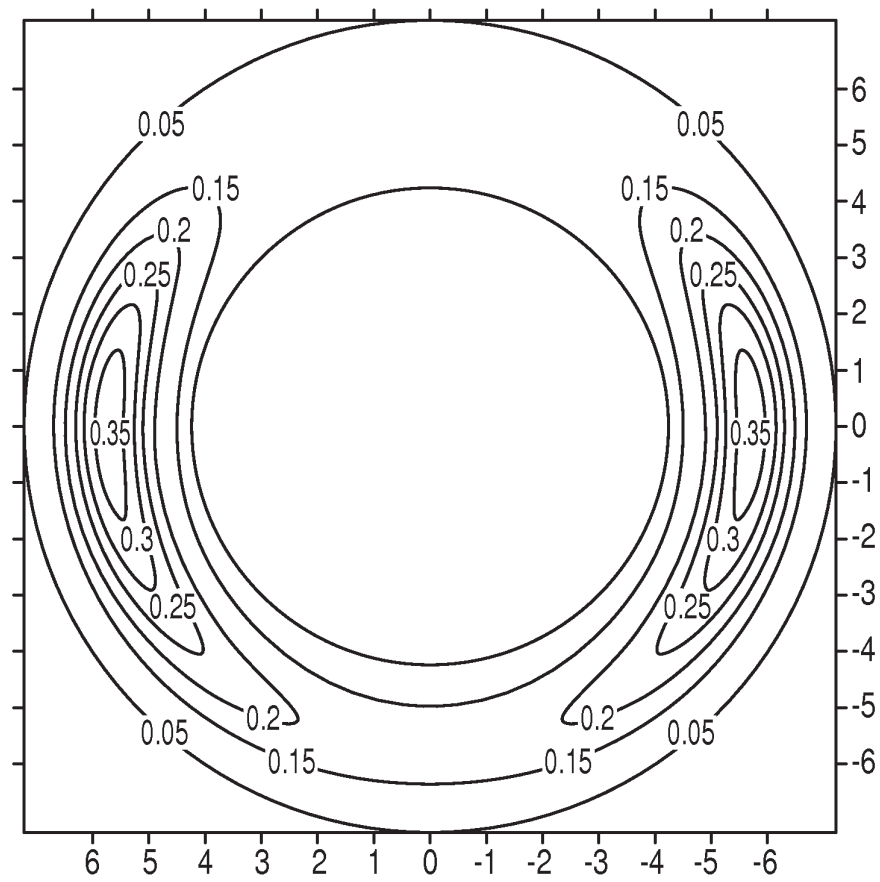
8/12

FIG. 6A

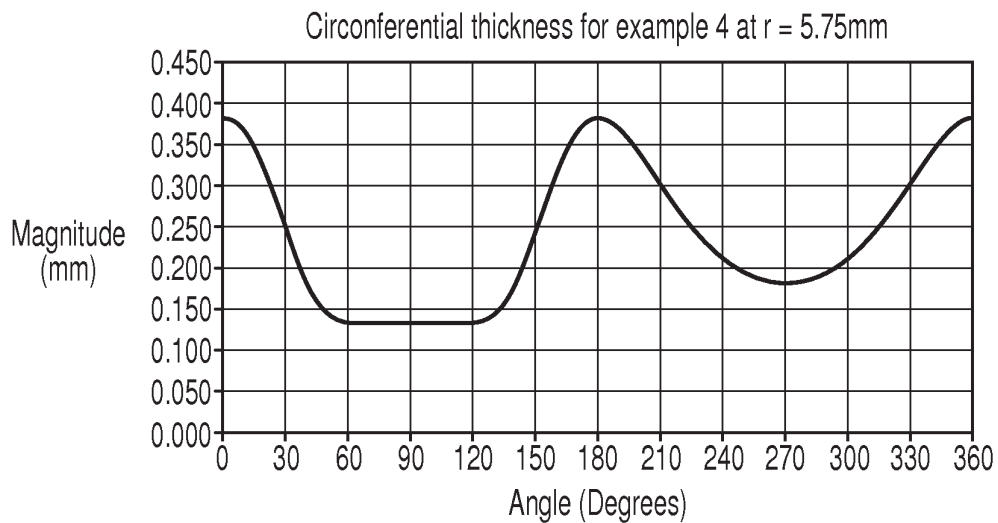
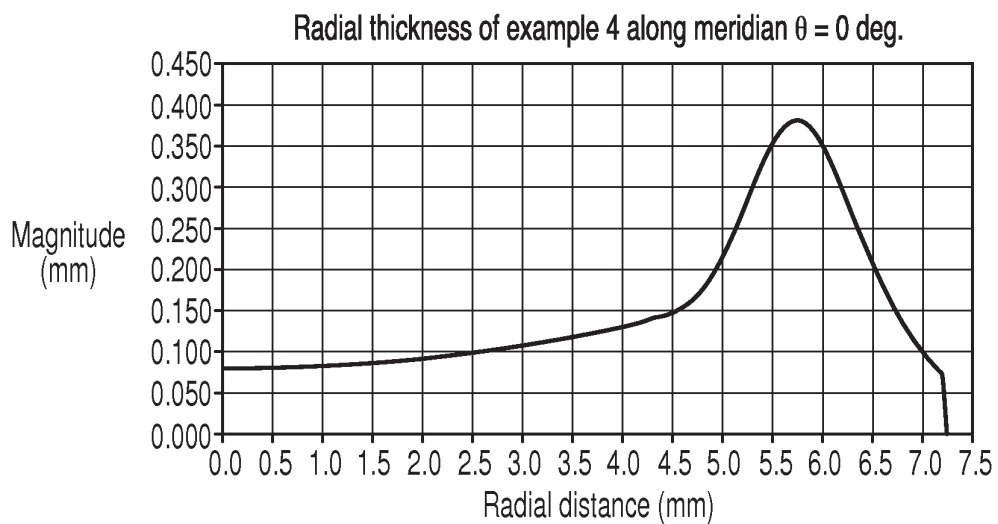
9/12

FIG. 6B**FIG. 6C**

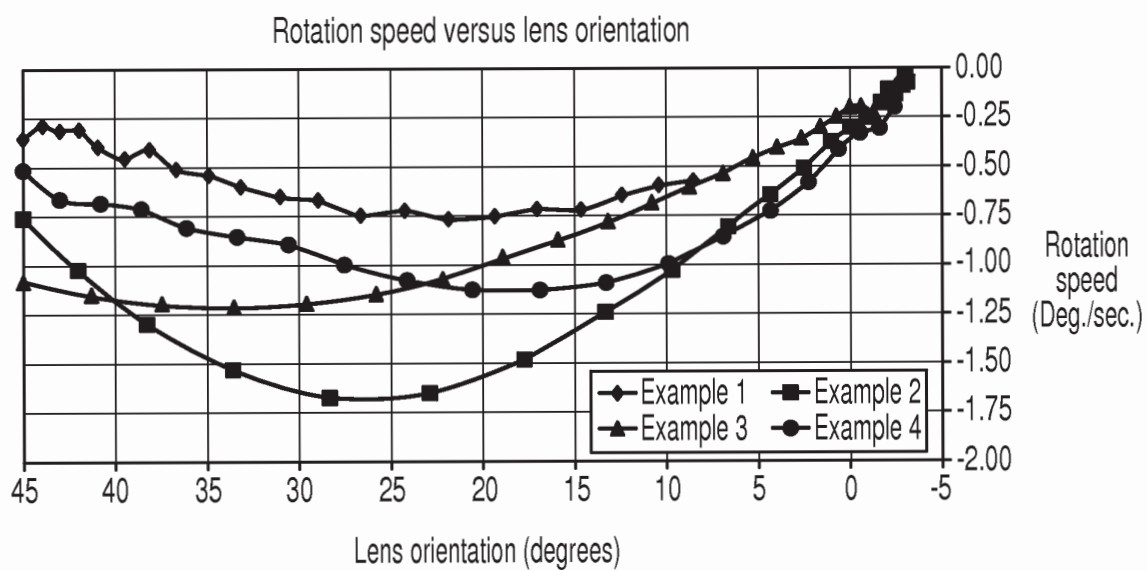
10/12

FIG. 7A

11/12

FIG. 7B**FIG. 7C**

12/12

FIG. 8

INTERNATIONAL SEARCH REPORT

International application No

PCT/US2010/060987

A. CLASSIFICATION OF SUBJECT MATTER

INV. G02C7/04
ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
G02C

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EP0-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2009/225273 A1 (CLUTTERBUCK TIMOTHY A [US] ET AL) 10 September 2009 (2009-09-10) paragraph [0018] figures 1, 3, 4, 7 -----	1-6
X	EP 0 866 354 A1 (ESSILOR INT [FR]) 23 September 1998 (1998-09-23) page 2, line 3 - line 7 page 4, line 14 - line 18 page 5, line 55 - page 6, line 6 figures 1-8 -----	1-6
X	US 2005/041202 A1 (JUBIN PHILIPPE F [US] ET AL) 24 February 2005 (2005-02-24) cited in the application paragraphs [0001], [0004], [0013], [0015], [0038] figures 1, 2 ----- -/-	1,2,5,6

☒ Further documents are listed in the continuation of Box C.☒ See patent family annex.

* Special categories of cited documents :

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier document but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"&" document member of the same patent family

Date of the actual completion of the international search

21 March 2011

Date of mailing of the international search report

31/03/2011

Name and mailing address of the ISA/

European Patent Office, P.B. 5818 Patentlaan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040,
Fax: (+31-70) 340-3016

Authorized officer

Vazquez Martinez, D

INTERNATIONAL SEARCH REPORT

International application No

PCT/US2010/060987

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO 2004/010204 A1 (JOHNSON & JOHNSON VISION CARE [US]) 29 January 2004 (2004-01-29) page 5, line 7 - line 22 figure 2 -----	1,2,5,6
A	WO 01/75509 A1 (OCULAR SCIENCES INC [US]) 11 October 2001 (2001-10-11) page 15, line 10 - line 29 figure 3 -----	1
A	GRANT R: "Mechanics of Toric Soft lens Stabilization", JOURNAL OF THE BRITISH CONTACT LENS ASSOCIATION, ELSEVIER, NL, vol. 9, no. Supplement 1, 1 January 1986 (1986-01-01), pages 44-47, XP007917345, ISSN: 0141-7037, DOI: DOI::10.1016/S0141-7037(86)80023-4 [retrieved on 2006-09-20] page 44 - page 45 page 46, column 1, line 30 - line 32 -----	1

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No

PCT/US2010/060987

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2009225273	A1	10-09-2009	AR 070855 A1 12-05-2010
			AU 2009221955 A1 11-09-2009
			CA 2716910 A1 11-09-2009
			CN 101960358 A 26-01-2011
			EP 2250528 A2 17-11-2010
			KR 20100121532 A 17-11-2010
			WO 2009111545 A2 11-09-2009
EP 0866354	A1	23-09-1998	CA 2230181 A1 17-09-1998
			FR 2760853 A1 18-09-1998
			NO 981151 A 18-09-1998
			US 5912719 A 15-06-1999
US 2005041202	A1	24-02-2005	AR 045390 A1 26-10-2005
			AU 2004267683 A1 03-03-2005
			BR PI0413692 A 24-10-2006
			CA 2536147 A1 03-03-2005
			CN 1871540 A 29-11-2006
			EP 1656582 A1 17-05-2006
			JP 2007503017 T 15-02-2007
			KR 20060061842 A 08-06-2006
			SG 130199 A1 20-03-2007
			US 2005237482 A1 27-10-2005
			WO 2005019907 A1 03-03-2005
WO 2004010204	A1	29-01-2004	AU 2002319593 A1 09-02-2004
			BR 0215812 A 26-04-2005
			CA 2492840 A1 29-01-2004
			CN 1639613 A 13-07-2005
			EP 1525508 A1 27-04-2005
			JP 4263172 B2 13-05-2009
			JP 2005534058 T 10-11-2005
WO 0175509	A1	11-10-2001	AT 358289 T 15-04-2007
			AU 4784701 A 15-10-2001
			BR 0109734 A 04-02-2003
			CA 2404554 A1 11-10-2001
			CN 1432139 A 23-07-2003
			DE 06019325 T1 09-08-2007
			DE 60127547 T2 27-12-2007
			EP 1281099 A1 05-02-2003
			ES 2280354 T3 16-09-2007
			HK 1051406 A1 10-08-2007
			HK 1088667 A1 09-04-2010
			JP 2004506925 T 04-03-2004
			KR 20090081428 A 28-07-2009
WO 0175509	A1		MX PA02009327 A 26-03-2004
			US 2009009712 A1 08-01-2009
			US 2002149742 A1 17-10-2002
			US 6467903 B1 22-10-2002