

Cross references to related applications

The present application claims the benefit of priority to and incorporates by reference herein the entirety of each of: European patent application no. 2016245.7, filed on 6 April 2020; United States patent application no. 16/889667, filed on 1 June 2020; United States patent application no. 17/065992, filed on 8 October 2020; United States provisional patent application no. 63/111592, filed on 9 November 2020; and United States patent application no. 17/122025, filed on 15 December 2020.

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Field

The present invention relates to cell lysis systems and methods. The present invention more particularly relates to cell lysis systems and methods which use ultrasonic waves to lyse cells.

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Background

Polymerase Chain Reaction (PCR) is a process that uses the two matching strands in DNA to amplify a targeted DNA sequence from a small number of samples to billions of copies for analysis.

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An initial step of the PCR process involves cell lysis to break or rupture the lipid bilayer of cells in a sample in order to provide a gateway through which a cell's components, including DNA and/or RNA, may be extracted. Cell lysis is typically performed either chemically or electromechanically, or a combination of both.

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The cell lysis process extracts components from the cells in a liquid solution. The solution is then filtered to separate the nucleic acids (DNA/RNA) from other cell components. The extracted DNA/RNA can then be amplified and analysed in the remaining steps of the PCR process.

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5 A conventional PCR apparatus performs cell lysis on a sample when the sample is input into the PCR apparatus. The components performing the cell lysis process are typically integrated within the PCR apparatus. The problem with a conventional PCR apparatus of this kind is that the apparatus is typically expensive and cumbersome. Moreover, the integrated components which
10 perform the cell lysis are typically restricted for use only within the same PCR apparatus.

Standalone cell lysis devices have been proposed previously but these standalone devices can suffer from reduced efficiency and performance
15 compared with the cell lysis functionality of a complete PCR apparatus.

Thus, a need exists in the art for improved cell lysis systems and methods which seek to address at least some of the problems described herein.

20 **Summary**

According to some arrangements, there is provided a cell lysis system comprising: a driver apparatus which incorporates: a plurality of driver output terminals which provide an electrical connection between the driver apparatus and a cell lysis device to drive an ultrasonic transducer within the cell lysis
25 device; an AC driver which generates an AC drive signal at a predetermined frequency and outputs the AC drive signal at the driver output terminals to drive the ultrasonic transducer within the cell lysis device; an active power monitoring arrangement which monitors the active power used by the ultrasonic transducer when the ultrasonic transducer is driven by the AC drive signal, wherein the
30 active power monitoring arrangement provides a monitoring signal which is indicative of an active power used by the ultrasonic transducer; a processor which controls the AC driver and receives the monitoring signal from the active power monitoring arrangement; and a memory storing instructions which, when executed by the processor, cause the processor to:

35 A. control the AC driver to output an AC drive signal to the ultrasonic transducer at a predetermined sweep frequency;

- 5 B. calculate the active power being used by the ultrasonic transducer based on the monitoring signal;
- C. control the AC driver to modulate the AC drive signal to maximise the active power being used by the ultrasonic transducer;
- 10 D. store a record in the memory of the maximum active power used by the ultrasonic transducer and the sweep frequency of the AC drive signal;
- E. repeat steps A-D for a predetermined number of iterations with the sweep frequency incrementing with each iteration such that, after the predetermined number of iterations has occurred, the sweep frequency has been incremented from a start sweep frequency to an end sweep frequency;
- 15 F. identify from the records stored in the memory the optimum frequency for the AC drive signal which is the sweep frequency of the AC drive signal at which a maximum active power is used by the ultrasonic transducer; and
- 20 G. control the AC driver to output an AC drive signal to the ultrasonic transducer at the optimum frequency.
- 25 In some arrangements, the active power monitoring arrangement comprises: a current sensing arrangement which senses a drive current of the AC drive signal driving the ultrasonic transducer, wherein the active power monitoring arrangement provides a monitoring signal which is indicative of the sensed drive current.
- 30 In some arrangements, the memory stores instructions which, when executed by the processor, cause the processor to: repeat steps A-D with the sweep frequency being incremented from a start sweep frequency of 2800kHz to an end sweep frequency of 3200kHz.

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- 5 In some arrangements, the memory stores instructions which, when executed by the processor, cause the processor to: in step G, control the AC driver to output an AC drive signal to the ultrasonic transducer at frequency which is shifted by between 1-10% of the optimum frequency.
- 10 In some arrangements, the AC driver modulates the AC drive signal by pulse width modulation to maximise the active power being used by the ultrasonic transducer.

- In some arrangements, the memory stores instructions which, when executed
- 15 by the processor, cause the processor to: control the AC driver to alternately output an AC drive signal to the ultrasonic transducer at the optimum frequency for a first predetermined length of time and to not output an AC drive signal to the ultrasonic transducer for a second predetermined length of time.
- 20 In some arrangements, the memory stores instructions which, when executed by the processor, cause the processor to: alternately output the AC drive signal and to not output the AC drive signal according to an operating mode selected from:

Operating mode	First predetermined length of time (seconds)	Second predetermined length of time (seconds)
1	4	2
2	3	2
3	2	2
4	1	2
5	1	1
6	2	1
7	3	1
8	4	1
9	4	3
10	3	3
11	2	3
12	1	3

5 In some arrangements, the system further comprises: a cell lysis device which is releasably attached to the driver apparatus, the cell lysis device comprising: a housing; a plurality of electrical terminals which are connected electrically to the plurality of driver output terminals; a sonication chamber provided within the housing, the sonication chamber being at least partly filled with an ultrasonic
10 wave transfer medium, wherein the housing comprises an opening which is configured to receive a sample container such that a part of the sample container projects into the ultrasonic wave transfer medium; an ultrasonic transducer which generates ultrasonic waves in the ultrasonic wave transfer medium within the sonication chamber, wherein the ultrasonic waves are
15 transferred by the ultrasonic wave transfer medium from the ultrasonic transducer to the sample container to lyse cells when cells are contained within the sample container.

In some arrangements, the driver apparatus comprises a first interference fit
20 attachment and the cell lysis device comprises a second interference fit attachment, and wherein the first interference fit attachment releasably attaches to the second interference fit attachment to releasably attach the cell lysis device to the driver apparatus.

25 According to some arrangements, there is provided a cell lysis device comprising: a housing; a sonication chamber provided within the housing, the sonication chamber being at least partly filled with an ultrasonic wave transfer medium, wherein the housing comprises an opening which is configured to receive a sample container such that a part of the sample container projects
30 into the ultrasonic wave transfer medium; an ultrasonic transducer which generates ultrasonic waves in the ultrasonic wave transfer medium within the sonication chamber, wherein the ultrasonic waves are transferred by the ultrasonic wave transfer medium from the ultrasonic transducer to the sample container to lyse cells when cells are contained within the sample container.

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- 5 In some arrangements, the ultrasonic transducer is at least partly of a compound comprising lead, zirconium and titanium.

In some arrangements, the ultrasonic transducer is a circular disc shape and has a diameter of 16mm and a thickness of 0.7mm.

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In some arrangements, the ultrasonic transducer comprises a first electrode and a second electrode which are provided on opposing sides of the ultrasonic transducer, wherein the first electrode and the second electrode comprise silver and the capacitance between the first electrode and the second electrode is

15 800pF to 1300pF.

In some arrangements, the first electrode is at least partly covered with a glass coating.

- 20 In some arrangements, the ultrasonic transducer is carried by a transducer holder which is of silicone rubber.

In some arrangements, the ultrasonic wave transfer medium comprises vegetable glycerine.

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In some arrangements, the sample container is a microcentrifuge tube.

- According to some arrangements, there is provided a method of lysing cells in a sample, the method comprising: placing a liquid sample containing cells to be lysed in a sample container; positioning the sample container through an opening in a housing of a cell lysis device such that a part of the sample container projects into an ultrasonic wave transfer medium provided in a sonication chamber within the housing; and attaching the cell lysis device to a driver apparatus, the driver apparatus incorporating: an AC driver which generates an AC drive signal at a predetermined frequency and outputs the AC drive signal at the driver output terminals to drive an ultrasonic transducer
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- 5 within the cell lysis device; an active power monitoring arrangement which monitors the active power used by the ultrasonic transducer when the ultrasonic transducer is driven by the AC drive signal, wherein the active power monitoring arrangement provides a monitoring signal which is indicative of an active power used by the ultrasonic transducer, wherein the method further
- 10 comprises:
- A. controlling, by a processor, the AC driver to output an AC drive signal to the ultrasonic transducer at a predetermined sweep frequency;
 - B. calculating, by the processor, the active power being used by the ultrasonic transducer based on the monitoring signal;
 - 15 C. controlling, by the processor, the AC driver to modulate the AC drive signal to maximise the active power being used by the ultrasonic transducer;
 - D. storing a record in a memory of the maximum active power used by the ultrasonic transducer and the sweep frequency of the AC drive signal;
 - 20 E. repeating steps A-D for a predetermined number of iterations with the sweep frequency incrementing with each iteration such that, after the predetermined number of iterations has occurred, the sweep frequency has been incremented from a start sweep frequency to an end sweep frequency;
 - 25 F. identifying, by the processor, from the records stored in the memory the optimum frequency for the AC drive signal which is the sweep frequency of the AC drive signal at which a maximum active power is used by the ultrasonic transducer; and
 - 30 G. controlling, by the processor, the AC driver to output an AC drive signal to the ultrasonic transducer at the optimum frequency.

In some arrangements, the method further comprises: repeating steps A-D with the sweep frequency being incremented from a start sweep frequency of

35 2800kHz to an end sweep frequency of 3200kHz.

- 5 In some arrangements, the method further comprises: controlling, by the processor, the AC driver to alternately output an AC drive signal to the ultrasonic transducer at the optimum frequency for a first predetermined length of time and to not output an AC drive signal to the ultrasonic transducer for a second predetermined length of time.

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Brief description of the drawings

So that the present invention may be more readily understood, embodiments of the present invention will now be described, by way of example, with reference to the accompanying drawings, in which:

- 15 Figure 1 is a diagrammatic perspective view of a system of some arrangements;
Figure 2 is a diagrammatic perspective view of a cell lysis device of some arrangements;
Figure 3 is a cross-sectional view of the cell lysis device of Figure 2;
20 Figure 4 is a diagrammatic perspective view of a driver apparatus of some arrangements;
Figure 5 is a cross-sectional view of the driver apparatus of Figure 4;
Figure 6 is a diagram showing a piezoelectric transducer modelled as an RLC circuit;
25 Figure 7 is a graph showing the change in impedance with increase in frequency in an RLC circuit;
Figure 8 is a graph showing how a piezoelectric transducer acts as a capacitor or an inductor; and
Figure 9 is a table showing the timings of operating modes of a system of some
30 arrangements.

Detailed description

- Aspects of the present disclosure are best understood from the following detailed description when read with the accompanying figures. It is noted that,
35 in accordance with the standard practice in the industry, various features are

5 not drawn to scale. In fact, the dimensions of the various features may be arbitrarily increased or reduced for clarity of discussion.

The following disclosure provides many different embodiments, or examples, for implementing different features of the provided subject matter. Specific
10 examples of components, concentrations, applications and arrangements are described below to simplify the present disclosure. These are, of course, merely examples and are not intended to be limiting. For example, the attachment of a first feature and a second feature in the description that follows may include embodiments in which the first feature and the second feature are
15 attached in direct contact, and may also include embodiments in which additional features may be positioned between the first feature and the second feature, such that the first feature and the second feature may not be in direct contact. In addition, the present disclosure may repeat reference numerals and/or letters in the various examples. This repetition is for the purpose of
20 simplicity and clarity and does not in itself dictate a relationship between the various embodiments and/or configurations discussed.

The following disclosure describes representative arrangements or examples. Each example may be considered to be an embodiment and any reference to
25 an “arrangement” or an “example” may be changed to “embodiment” in the present disclosure.

Referring initially to Figure 1 of the accompanying drawings, a cell lysis system 1 of some arrangements comprises a driver apparatus 2 and a cell lysis device
30 3. The driver apparatus 2 comprises a first interference fit attachment 4 which releasably attaches to a second interference fit attachment 5 provided on the cell lysis device 3. The interference fit attachments 4, 5 allow the cell lysis device 3 to be releasably attached to the driver apparatus 2 when the cell lysis device 3 is placed onto the driver apparatus 2 as indicated generally by arrow 6
35 in Figure 1.

5 The components of the cell lysis system 1 are described below, starting with the cell lysis device 3.

Referring to Figures 2 and 3 of the accompanying drawings, the cell lysis device 3 of some arrangements comprises a housing 7. In this arrangement,
10 the housing 7 is generally cylindrical with a side wall 8, a generally circular cover 9 at one end and a generally circular base 10 at the other end. In this arrangement, the cell lysis device 3 is a disposable, single-use capsule.

A sonication chamber 11 is provided within the housing 7. The sonication
15 chamber 11 is at least partly filled with an ultrasonic wave transfer medium (not shown). In some arrangements, the sonication chamber 11 is pre-filled with the ultrasonic wave transfer medium. In other arrangements, the sonication chamber 11 is filled with an ultrasonic wave transfer medium when the cell lysis device is being prepared for use.

20 In some arrangements, the ultrasonic wave transfer medium is a liquid which has a higher acoustic impedance than water. In some arrangements, the ultrasonic wave transfer medium is vegetable glycerine since vegetable glycerine has a higher acoustic impedance than water.

25 The cell lysis device 3 comprises an ultrasonic transducer 12. An upper surface 13 of the ultrasonic transducer 12 faces towards the sonication chamber 11 so that ultrasonic waves generated by the ultrasonic transducer 12 are directed towards the sonication chamber 11.

30 In some arrangements, the ultrasonic transducer 12 is a circular disc shape. In this arrangement, the ultrasonic transducer 12 has a diameter of approximately 16mm and a thickness of approximately 0.7mm. In this arrangement, the ultrasonic transducer 12 is polarized to generate vibrations in the thickness
35 mode.

5 In this arrangement, the ultrasonic transducer 12 is carried by a transducer holder 14 in the form of a ring which at least partly surrounds the ultrasonic transducer 12. In this arrangement, the transducer holder 14 is of silicone rubber. Apart from holding the ultrasonic transducer 12 in place, the transducer holder 14 also ensures minimal damping of the vibration of the ultrasonic
10 transducer 12. In addition, the transducer holder 14 minimises the risk of the liquid ultrasonic wave transfer medium from leaking out from the base 10 of the cell lysis device 3.

In some arrangements, the ultrasonic transducer 12 is at least partly of a
15 compound comprising lead, zirconium and titanium. The compound of the ultrasonic transducer 12 is selected to provide the ultrasonic transducer 12 with the properties for it to oscillate at a frequency of 2.8MHz to 3.2MHz. This frequency range is the preferred frequency range for the ultrasonic transducer 12 to produce ultrasonic waves which lyse or rupture cells.

20 In some arrangements, the ultrasonic transducer 12 comprises a first electrode on the upper side 13 and a second electrode on a lower side 15 which is on the opposing side of the ultrasonic transducer 12. In some arrangements, the first electrode and the second electrode comprise silver, for instance in the form of
25 silver stamp paint. In some arrangements, the capacitance between the first electrode and the second electrode is 800pF to 1300pF.

In some arrangements, the first electrode on the upper side 13 of the ultrasonic transducer 12 is at least partly covered with a glass coating. The glass coating
30 minimizes or prevents possible contamination of the ultrasonic wave transfer medium by the material of the first electrode. The glass coating also minimizes or prevents erosion of the silver of the first electrode, for instance due to cavitation bubble collapse caused by ultrasonic waves travelling through the ultrasonic wave transfer medium when the cell lysis device 3 is in use.

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5 The first and second electrodes of the ultrasonic transducer 12 are connected electrically to respective first and second electrical terminals 16, 17 which are provided at the lower surface of the base 10 of the cell lysis device 3.

A plurality of projections 18, 19 (only two of which are visible in Figure 2)
10 extend outwardly from the side of the base 10 of the cell lysis device 3. The projections 18, 19 are part of the second interference fit attachment 5 of the cell lysis device 3. In other arrangement, the second interference fit attachment 5 comprises only one projection and in further arrangements, the second interference fit attachment 5 comprises more than 2 projections.

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The cover 9 is provided at the opposite end of the cell lysis device 3 to the base 10. The cover 9 provides a generally planar circular surface and is formed integrally with the side wall 8 of the housing 7. In this arrangement, a bevelled edge 19 is provided around the circumference of the cover 9 at the intersection
20 between the cover 9 and the side wall 8.

An opening 20 is provided in the cover 9. In this arrangement, the opening 20 is a generally circular aperture which is provided at the centre of the cover 9. In other arrangements, the opening 20 may be a different shape and may be
25 provided in a different portion of the cover 9.

In this arrangement, a cylindrical collar 21 is aligned with the opening 20 and extends from the opening 20 into the sonication chamber 11. The opening 20 and the collar 21 are configured to receive a sample container 22 such that a
30 part of the sample container 22 projects into the ultrasonic wave transfer medium within the sonication chamber 11.

In some arrangement, the sample container 22 is a microcentrifuge tube. In some arrangement, the sample container 22 is an Eppendorf Tube®. In some
35 arrangements, the sample container 22 is a microcentrifuge tube or Eppendorf Tube® which holds a liquid volume of 0.5ml, 1.5ml or 2ml.

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The sample container 22 comprises a conical first portion 23 which is joined to a cylindrical body portion 24. A distal end of the body portion 24 is provided with a sample container aperture 24 through which a sample may be introduced into the sample container 22. A cap 25 is moveably mounted to the
10 body portion 24, with the cap 25 being configured to seal the aperture 24 to retain a sample within the sample container 22.

The sample container 22 closes and seals the opening 20 when the sample container 22 is inserted into the opening 20. The housing 7 of the cell lysis
15 device 3 is thus sealed to retain the ultrasonic wave transfer medium within the housing 7. In some arrangements, the sonication chamber 11 is initially empty and the sonication chamber 11 is filled with the ultrasonic wave transfer medium shortly before the sample container 22 is inserted into the opening 20.

20 Referring now to Figures 4 and 5 of the accompanying drawings, the driver apparatus 2 comprises a housing 26 which houses electrical components of the driver apparatus 2. In this arrangement, the driver apparatus 2 is a portable, stand-alone apparatus.

25 The housing 26 comprises a main housing 27 and a base protrusion 28. The main housing 27 comprises an internal chamber 29 which receives a battery 30 and at least part of a printed circuit board (PCB) 31. The PCB 31 carries the electronic components which provide the driver functionality of the driver apparatus 2.

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In this arrangement, the battery 30 is rechargeable. In some arrangements, the battery 30 is a lithium polymer (LiPo) battery. In some arrangements, the capacity of the battery 30 provides sufficient power to enable the driver apparatus 2 to operate for at least 24 hours. In this arrangement, the driver
35 apparatus 2 comprises a charging connection (not shown) which is configured to receive power from an external power source to charge the battery 30.

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In some arrangements, the battery 30 is omitted and the driver apparatus 2 is instead provided with a power input connection to receive power from an external power source. In some arrangements, the external power source is a power adapter which converts a mains voltage to an appropriate voltage (e.g.
10 5-12V) to power the driver apparatus 2.

The base protrusion 28 is, in this embodiment, of reduced thickness compared with the housing 26. The base protrusion 28 is provided with a recess 32 which is configured to receive the base 10 of the cell lysis device 3. In this
15 arrangement, the recess 32 is generally circular. The recess 32 is provided with indentations 33, 34 which are positioned above a generally circular channel 35 to form the first interference fit attachment 4 of the driver apparatus 2. The indentations 33, 34 are positioned to align with the projections 18, 19 on the cell lysis device 3. In other embodiments, there may be a different number
20 of indentations which match a different number of projections on the cell lysis device 3.

Two driver output terminals 36, 37 are provided at the base of the recess 32. In this arrangement, one of the driver output terminals 36 is provided centrally
25 within the recess 32 and the other driver output terminal 37 is provided adjacent the side of the recess 32. In this arrangement, each of the driver output terminals 36, 37 is a spring contact probe which protrudes upwardly from the base of the recess 32. The driver output terminals 36, 37 are positioned to engage and form an electrical connection with the first and
30 second electrical terminals 16, 17 which are provided at the lower surface of the base 10 of the cell lysis device 3 when the cell lysis device 3 is attached to the driver apparatus 2. In some arrangements, the driver output terminals 36, 37 and/or the electrical terminals 16, 17 are of a brass material which is plated with a first 3µm thick layer of nickel and a second 0.05µm thick layer of gold.

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- 5 In some arrangements, the driver output terminals 36, 37 extend through the base of the recess 32 to the PCB 31 where the driver output terminals 36, 37 are soldered to form an electrical connection with the PCB 31 and the electronic components provided on the PCB 31.
- 10 In this arrangement, the cell lysis device 3 is releasably attached to the driver apparatus 2 by placing the base 10 of the cell lysis device 3 into the recess 32 with the protrusions 18, 19 passing through the indentations 33, 34 until the protrusions 18, 19 are aligned with the channel 35. The cell lysis device 3 is then rotated with the protrusions 18, 19 within the channel 35. The protrusions
- 15 18, 19 are then retained within the channel 35 to provide an interference fit attachment which releasably attaches the cell lysis device 3 to the driver apparatus 2.

The interference fit attachments 4, 5 enable a user to releasably attach the cell

20 lysis device 3 to the driver apparatus 2 by pushing and turning the cell lysis device 3 to lock the cell lysis device 3 to the driver apparatus. This process is then performed in reverse to remove the cell lysis device 3 from the driver apparatus 2 after the lysing process has finished.

- 25 As the cell lysis device 3 is pushed into the recess 32, the driver output terminals 36, 37 deform resiliently and align with the electrical terminals 16, 17 on the cell lysis device 3. The resiliently deformed driver output terminals 36, 37 press against the electrical terminals 16, 17 to form an electrical connection. When the cell lysis device 3 is releasably attached to the driver apparatus 2 in
- 30 this way, the cell lysis device 3 is able to be driven by the driver apparatus 2 to lyse cells within the cell lysis device 3.

An AC driver 38 is provided on the PCB 31. The AC driver 38 generates an AC drive signal at a predetermined frequency and outputs the AC drive signal at

35 the driver output terminals 36, 37 to drive the ultrasonic transducer 12 within the cell lysis device 3. In some arrangements, the AC driver 38 comprises a H-

5 bridge circuit. In some arrangements, the H-bridge circuit comprises four MOSFETs which are connected to convert a direct current into an alternating current at high frequency (e.g. a frequency in the range 2.8MHz to 3.2MHz).

An active power monitoring arrangement 39 is provided on the PCB 31. The
10 active power monitoring arrangement 39 monitors the active power used by the ultrasonic transducer 12 when the ultrasonic transducer 12 is driven by the AC drive signal. The active power monitoring arrangement 39 provides a monitoring signal which is indicative of an active power used by the ultrasonic transducer 12. In some arrangements, the active power monitoring
15 arrangement 39 comprises a current sensing arrangement which senses a drive current of the AC drive signal driving the ultrasonic transducer 12 and provides a monitoring signal which is indicative of the sensed drive current.

The PCB 31 is provided with a processor 40 which controls the AC driver 38
20 and receives the monitoring signal from the active power monitoring arrangement 39. The PCB 31 is also provided with a memory 41 storing executable instructions for execution by the processor 40.

In some arrangements, the driver apparatus 2 comprises a frequency controller
25 which is configured to control the frequency at which the ultrasonic transducer 12 operates. The frequency controller is implemented in the executable code stored in the memory 41 which, when executed by the processor 40, cause the processor 40 to perform at least one function of the frequency controller.

30 The memory 41 stores executable instructions which, when executed by the processor, cause the processor to control the ultrasonic transducer 12 to oscillate at a plurality of frequencies within a predetermined sweep frequency range and to select a drive frequency for the ultrasonic transducer 12 which is between a first predetermined frequency and a second predetermined
35 frequency for lysing cells within the sample container 22.

- 5 In some arrangements, the frequency will be determined by the type of cells that are being lysed as some cells may require different frequencies due to their physical characteristics (size, shape, presence of cell wall, etc.).

There is an optimum frequency or frequency range for lysing cells. The
10 optimum frequency or frequency range will depend on at least the following four parameters:

1. Transducer Manufacturing Processes

In some arrangements, the ultrasonic transducer 12 comprises a piezoelectric
15 ceramic. The piezoelectric ceramic is manufactured by mixing compounds to make a ceramic dough and this mixing process may not be consistent throughout production. This inconsistency can give rise to a range of different resonant frequencies of the cured piezoelectric ceramic.

20 If the resonant frequency of the piezoelectric ceramic does not correspond to the required frequency of operation, the process of lysing cells is not optimal. Even a slight offset in the resonant frequency of the piezoelectric ceramic is enough to impact the lysing process, meaning that the system will not function optimally.

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2. Load on transducer

During operation, any changes in the load on the ultrasonic transducer 12 will inhibit the overall displacement of the oscillation of the ultrasonic transducer 12. To achieve optimal displacement of the oscillation of the ultrasonic transducer
30 12, the drive frequency must be adjusted to provide adequate power for maximum displacement.

The types of loads that can affect the efficiency of the ultrasonic transducer 12 can include the amount of liquid on the transducer (i.e. the amount of liquid
35 within the sonication chamber 11).

5 **3. Temperature**

Ultrasonic oscillations of the ultrasonic transducer 12 are partially damped by its assembly in the driver apparatus 2. This dampening of the oscillations can cause a rise in local temperatures on and around the ultrasonic transducer 12.

10 An increase in temperature affects the oscillation of the ultrasonic transducer 12 due to changes in the molecular behaviour of the ultrasonic transducer 12. An increase in the temperature means more energy to the molecules of the ceramic, which temporarily affects its crystalline structure. Although the effect is reversed as the temperature reduces, a modulation in supplied frequency is
15 required to maintain optimal oscillation.

An increase in temperature also reduces the viscosity of the solution within the sonication chamber 11, which may require an alteration to the drive frequency to optimise lysis of cells within the sonication chamber 11.

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4. Distance to Power Source

The oscillation frequency of the ultrasonic transducer 12 can change depending on the wire-lengths between the ultrasonic transducer 12 and the AC driver 38. The frequency of the electronic circuit is inversely proportional to the distance
25 between the ultrasonic transducer 49 and the controller 23.

Although the distance parameter is primarily fixed in this arrangement, it can vary during the manufacturing process of the system 1. Therefore, it is desirable to modify the drive frequency of the ultrasonic transducer 12 to
30 compensate for the variations and optimise the efficiency of the system.

A piezoelectric transducer can be modelled as an RLC circuit in an electronic circuit, as shown in Figure 6. The four parameters described above may be modelled as alterations to the overall inductance, capacitance, and/or
35 resistance of the RLC circuit, changing the resonance frequency range supplied to the transducer. As the frequency of the circuit increases to around

- 5 the resonance point of the transducer, the log Impedance of the overall circuit dips to a minimum and then rises to a maximum before settling to a median range.

Figure 7 shows a graph explaining the change in overall impedance with
10 increase in frequency in an RLC circuit. Figure 8 shows how a piezoelectric transducer acts as a capacitor in a first capacitive region at frequencies below a first predetermined frequency f_s and in a second capacitive region at frequencies above a second predetermined frequency f_p . The piezoelectric transducer acts as an inductor in an inductive region at frequencies between
15 the first and second predetermined frequencies f_s , f_p . In order to maintain optimal oscillation of the transducer and hence maximum efficiency, the current flowing through the transducer must be maintained at a frequency within the inductive region.

- 20 The driver apparatus 2 of some arrangements is configured to maintain the frequency of oscillation of the piezoelectric transducer 12 within the inductive region, in order to maximise the efficiency of the lysis of cells.

The driver apparatus 2 is configured to perform a sweep operation in which the
25 frequency controller drives the transducer at frequencies which track progressively across a predetermined sweep frequency range. In other words, the driver apparatus 2 drives the transducer at a plurality of different frequencies across the predetermined sweep frequency range. For instance at frequencies which increment by a predetermined frequency from one end of the
30 sweep frequency range to the other end of the sweep frequency range.

As will be described in more detail below, the driver apparatus 2 of some arrangements determines the active power being used by the ultrasonic transducer 12 by monitoring the current flowing through the transducer 12.

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- 5 Ultrasonic (piezoelectric) transducer mechanical deformation is linked to the AC Voltage amplitude that is applied to it, and in order to guarantee optimal functioning and delivery of the system, the maximum deformation must be supplied to the ultrasonic transducer all the time. By Pulse Width Modulation (PWM) of the AC voltage applied to the ultrasonic transducer, the mechanical
- 10 amplitude of the vibration remains the same. In some arrangements, the system actively adjusts the duty cycle of the AC voltage waveform to maximise deformation of the ultrasonic transducer in order to guarantee optimal functioning and delivery of the system.
- 15 One approach involves modifying the AC voltage applied to the ultrasonic transducer via the use of a Digital to Analog Converter (DAC). The energy transmitted to the ultrasonic transducer would be reduced but so would the mechanical deformation which as a result does not produce maximum deformation. The RMS voltage applied to the ultrasonic transducer would be
- 20 the same with effective Duty Cycle modulation as with Voltage modulation, but the active power transferred to the ultrasonic transducer would degrade. Indeed, given the formula below:

Active Power displayed to the ultrasonic transducer being:

25
$$Pa = \frac{2\sqrt{2}}{\pi} Irms * Vrms * \cos\varphi,$$

Where

φ is the shift in phase between current and voltage

I_{rms} is the root mean square Current

V_{rms} is the root mean square Voltage.

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When considering the first harmonic, I_{rms} is a function of the real voltage amplitude applied to the ultrasonic transducer, as the pulse width modulation alters the duration of voltage supplied to the ultrasonic transducer, controlling I_{rms} .

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- 5 In this arrangement, the memory 41 stores instructions which, when executed by the processor 40, cause the processor 40 to:
- A. control the AC driver 38 to output an AC drive signal to the ultrasonic transducer 12 at a predetermined sweep frequency;
 - B. calculate the active power being used by the ultrasonic transducer 12
 - 10 based on the monitoring signal;
 - C. control the AC driver 38 to modulate the AC drive signal to maximise the active power being used by the ultrasonic transducer 12;
 - D. store a record in the memory 41 of the maximum active power used by the ultrasonic transducer 12 and the sweep frequency of the AC drive signal;
 - 15 E. repeat steps A-D for a predetermined number of iterations with the sweep frequency incrementing with each iteration such that, after the predetermined number of iterations has occurred, the sweep frequency has been incremented from a start sweep frequency to an end sweep frequency;
 - F. identify from the records stored in the memory 41 the optimum
 - 20 frequency for the AC drive signal which is the sweep frequency of the AC drive signal at which a maximum active power is used by the ultrasonic transducer 12; and
 - G. control the AC driver 38 to output an AC drive signal to the ultrasonic transducer 12 at the optimum frequency.

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In some arrangements, the start sweep frequency is 2800kHz and the end sweep frequency is 3200kHz. In other arrangements, the start sweep frequency and the end sweep frequency are lower and upper frequencies of a frequency range within the range of 2800kHz to 3200kHz.

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In some arrangements, the processor 40 controls the AC driver 38 to output an AC drive signal to the ultrasonic transducer 12 at frequency which is shifted by between 1-10% of the optimum frequency. In these arrangements, the frequency shift is used to prolong the life of the ultrasonic transducer 12 by

35 minimising potential damage caused to the ultrasonic transducer 12 when the

5 ultrasonic transducer 12 is driven continuously at the optimum drive frequency
which produces maximum displacement.

In some arrangements, the AC driver 38 modulates the AC drive signal by
pulse width modulation to maximise the active power being used by the
10 ultrasonic transducer 12.

In some arrangements, the processor 40 controls the AC driver 38 to
alternately output an AC drive signal to the ultrasonic transducer 12 at the
optimum frequency for a first predetermined length of time and to not output an
15 AC drive signal to the ultrasonic transducer 12 for a second predetermined
length of time. This alternate activation and deactivation of the ultrasonic
transducer 12 has been found to optimise the process of lysing cells in a
sample within the cell lysis device 3.

20 In some embodiments, in order to ensure optimal operation of the ultrasonic
transducer 12, the driver apparatus 2 operates in a recursive mode. When the
driver apparatus 2 operates in the recursive mode, the driver apparatus 2 runs
the sweep of frequencies in steps A-D periodically during the operation of the
system.

25 In some arrangements, the driver apparatus 2 activates automatically to start
the lysing process when the cell lysis device 3 is attached to the driver
apparatus 2. In some arrangements, the driver apparatus 2 stops the lysing
process automatically after a predetermined length of time. Once the lysing
30 process has finished, the cell lysis device 3 is removed from the driver
apparatus 3.

In some arrangements, the processor 40 controls the AC driver 38 to
alternately output the AC drive signal and to not output the AC drive signal
35 according to an operating mode. The timings of twelve operating modes of

5 some arrangements are shown in the table in Figure 9 of the accompanying drawings.

In some arrangements, the driver apparatus 2 activates automatically when the cell lysis device 3 is attached to the driver apparatus 2. In other arrangements,
10 the driver apparatus 2 is provided with a switch or other control device to enable a user to activate and deactivate the driver apparatus 2.

Once the system has been activated and has performed the lysing process for a predetermined duration, the cell lysis device 3 is separated from the driver
15 apparatus 2. The liquid within the cell lysis device 3, which now contains lysed cells, is removed for use in another process, such as a PCR process. The cell lysis device 3 may then be discarded.

While the arrangements described above comprise one recess 32 and one set
20 of driver output terminals 36, 37, other arrangements comprise a plurality of recesses and a plurality of sets of output terminals. In these other arrangements, the driver apparatus 2 can be used simultaneously with a plurality of cell lysis devices. In these arrangements, the driver apparatus 2 controls each of the plurality of cell lysis devices to perform cell lysis individually.

25 The foregoing outlines features of several examples or embodiments so that those of ordinary skill in the art may better understand various aspects of the present disclosure. Those of ordinary skill in the art should appreciate that they may readily use the present disclosure as a basis for designing or modifying
30 other processes and structures for carrying out the same purposes and/or achieving the same advantages of various examples or embodiments introduced herein. Those of ordinary skill in the art should also realise that such equivalent constructions do not depart from the spirit and scope of the present disclosure, and that they may make various changes, substitutions,
35 and alterations herein without departing from the spirit and scope of the present disclosure.

5

Although the subject matter has been described in language specific to structural features or methodological acts, it is to be understood that the subject matter of the appended claims is not necessarily limited to the specific features or acts described above. Rather, the specific features and acts described
10 above are disclosed as example forms of implementing at least some of the claims.

Various operations of examples or embodiments are provided herein. The order in which some or all of the operations are described should not be
15 construed to imply that these operations are necessarily order dependent. Alternative ordering will be appreciated having the benefit of this description. Further, it will be understood that not all operations are necessarily present in each embodiment provided herein. Also, it will be understood that not all operations are necessary in some examples or embodiments.

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Moreover, "exemplary" is used herein to mean serving as an example, instance, illustration, etc., and not necessarily as advantageous. As used in this application, "or" is intended to mean an inclusive "or" rather than an exclusive "or". In addition, "a" and "an" as used in this application and the
25 appended claims are generally be construed to mean "one or more" unless specified otherwise or clear from context to be directed to a singular form. Also, at least one of A and B and/or the like generally means A or B or both A and B. Furthermore, to the extent that "includes", "having", "has", "with", or variants thereof are used, such terms are intended to be inclusive in a manner
30 similar to the term "comprising". Also, unless specified otherwise, "first," "second," or the like are not intended to imply a temporal aspect, a spatial aspect, an ordering, etc. Rather, such terms are merely used as identifiers, names, etc. for features, elements, items, etc. For example, a first element and a second element generally correspond to element A and element B or two
35 different or two identical elements or the same element.

5 Also, although the disclosure has been shown and described with respect to one or more implementations, equivalent alterations and modifications will occur to others of ordinary skill in the art based upon a reading and understanding of this specification and the annexed drawings. The disclosure comprises all such modifications and alterations and is limited only by the
10 scope of the following claims. In particular regard to the various functions performed by the above described features (e.g., elements, resources, etc.), the terms used to describe such features are intended to correspond, unless otherwise indicated, to any features which performs the specified function of the described features (e.g., that is functionally equivalent), even though not
15 structurally equivalent to the disclosed structure. In addition, while a particular feature of the disclosure may have been disclosed with respect to only one of several implementations, such feature may be combined with one or more other features of the other implementations as may be desired and advantageous for any given or particular application.

20

Examples or embodiments of the subject matter and the functional operations described herein can be implemented in digital electronic circuitry, or in computer software, firmware, or hardware, including the structures disclosed in this specification and their structural equivalents, or in combinations of one or
25 more of them.

Some examples or embodiments are implemented using one or more modules of computer program instructions encoded on a computer-readable medium for execution by, or to control the operation of, a data processing apparatus. The
30 computer-readable medium can be a manufactured product, such as hard drive in a computer system or an embedded system. The computer-readable medium can be acquired separately and later encoded with the one or more modules of computer program instructions, such as by delivery of the one or more modules of computer program instructions over a wired or wireless
35 network. The computer-readable medium can be a machine-readable storage

5 device, a machine-readable storage substrate, a memory device, or a combination of one or more of them.

The terms “computing device” and “data processing apparatus” encompass all apparatus, devices, and machines for processing data, including by way of
10 example a programmable processor, a computer, or multiple processors or computers. The apparatus can include, in addition to hardware, code that creates an execution environment for the computer program in question, e.g., code that constitutes processor firmware, a protocol stack, a database management system, an operating system, a runtime environment, or a
15 combination of one or more of them. In addition, the apparatus can employ various different computing model infrastructures, such as web services, distributed computing and grid computing infrastructures.

The processes and logic flows described in this specification can be performed
20 by one or more programmable processors executing one or more computer programs to perform functions by operating on input data and generating output.

Processors suitable for the execution of a computer program include, by way of
25 example, both general and special purpose microprocessors, and any one or more processors of any kind of digital computer. Generally, a processor will receive instructions and data from a read-only memory or a random access memory or both. The essential elements of a computer are a processor for performing instructions and one or more memory devices for storing
30 instructions and data. Generally, a computer will also include, or be operatively coupled to receive data from or transfer data to, or both, one or more mass storage devices for storing data, e.g., magnetic, magneto-optical disks, or optical disks. However, a computer need not have such devices. Devices suitable for storing computer program instructions and data include all forms of
35 non-volatile memory, media and memory devices.

- 5 In the present specification "comprise" means "includes or consists of" and "comprising" means "including or consisting of".

The features disclosed in the foregoing description, or the following claims, or the accompanying drawings, expressed in their specific forms or in terms of a
10 means for performing the disclosed function, or a method or process for attaining the disclosed result, as appropriate, may, separately, or in any combination of such features, be utilised for realising the invention in diverse forms thereof.

15

5 CLAIMS

1. A cell lysis device comprising:
a housing comprising:
an opening configured to receive a sample container such that
10 when the sample container is received by the opening the opening is
closed by the sample container to seal the housing; and
an interference fit attachment configured to releasably attach to a
further interference fit attachment of a driver apparatus to releasably
attach the housing to the driver apparatus, wherein the cell lysis device
15 further comprises:
a sonication chamber provided within the housing, the sonication
chamber being at least partly filled with an ultrasonic wave transfer medium,
wherein when the opening receives a sample container a part of the sample
container projects into the ultrasonic wave transfer medium; and
20 an ultrasonic transducer which generates ultrasonic waves in the
ultrasonic wave transfer medium within the sonication chamber, wherein the
ultrasonic waves are transferred by the ultrasonic wave transfer medium from
the ultrasonic transducer to the sample container to lyse cells when cells are
contained within the sample container.
25
2. The device of claim 1, wherein the interference fit attachment comprises
at least one projection extending outwardly from the side of a base of the cell
lysis device.
- 30 3. The device of claim 1 or claim 2, wherein the ultrasonic transducer is at
least partly of a compound comprising lead, zirconium and titanium.
4. The device of any one of the preceding claims, wherein the ultrasonic
transducer is configured to oscillate at a frequency of 2.8MHz to 3.2MHz.

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- 5 5. The device of any one of the preceding claims, wherein the ultrasonic transducer is a circular disc shape and has a diameter of 16mm and a thickness of 0.7mm.
- 10 6. The device of any one of the preceding claims, wherein the ultrasonic transducer comprises a first electrode and a second electrode which are provided on opposing sides of the ultrasonic transducer, wherein the first electrode and the second electrode comprise silver and the capacitance between the first electrode and the second electrode is 800pF to 1300pF.
- 15 7. The device of claim 6, wherein the first electrode is at least partly covered with a glass coating.
8. The device of any one of the preceding claims, wherein the ultrasonic transducer is carried by a transducer holder which is of silicone rubber.
- 20 9. The device of claim 8, wherein the transducer holder is in the form of a ring which at least partly surrounds the ultrasonic transducer.
10. The device of any one of the preceding claims, wherein the ultrasonic wave transfer medium is of a higher acoustic impedance than water.
- 25 11. The device of any one of the preceding claims, wherein the ultrasonic wave transfer medium comprises vegetable glycerine.
12. A system comprising:
30 the cell lysis device (3) of any one of the preceding claims; and
a sample container (22), wherein the sample container is received by the opening and the opening (20) is closed by the sample container to seal the housing.
- 35 13. The system of claim 12, wherein the sample container is a microcentrifuge tube.