

ARRANGING INTERACTION AND BACK PRESSURE CHAMBERS FOR MICROFLUIDIZATION

This application claims the benefit of US provisional patent application 61/283,548 filed December 3rd 2009, the complete contents of which are incorporated herein by reference for all purposes.

TECHNICAL FIELD

- 5 This invention is in the field of manufacturing oil-in-water emulsion adjuvants for vaccines by microfluidization.

BACKGROUND ART

10 The vaccine adjuvant known as 'MF59' [1-3] is a submicron oil-in-water emulsion of squalene, polysorbate 80 (also known as Tween 80), and sorbitan trioleate (also known as Span 85). It may also include citrate ions *e.g.* 10mM sodium citrate buffer. The composition of the emulsion by volume can be about 5% squalene, about 0.5% Tween 80 and about 0.5% Span 85. The adjuvant and its production are described in more detail in Chapter 10 of reference 4, chapter 12 of reference 5 and chapter 19 of reference 6.

15 As described in reference 7, MF59 is manufactured on a commercial scale by dispersing Span 85 in the squalene phase and Tween 80 in the aqueous phase, followed by high-speed mixing to form a coarse emulsion. This coarse emulsion is then passed repeatedly through a microfluidizer to produce an emulsion having a uniform oil droplet size. As described in reference 6, the microfluidized emulsion is then filtered through a 0.22 μm membrane in order to remove any large oil droplets, and the mean droplet size of the resulting emulsion remains unchanged for at least 3 years at 4°C. The
20 squalene content of the final emulsion can be measured as described in reference 8.

Oil-in-water emulsions contain oil droplets. The larger oil droplets contained in these emulsions may act as nucleation sites for aggregation, leading to emulsion degradation during storage.

It is an object of the invention to provide further and improved methods for the production of microfluidized oil-in-water emulsions (such as MF59), in particular methods that are suitable for use
25 on a commercial scale and which provide improved microfluidization to provide emulsions with fewer large particles.

DISCLOSURE OF THE INVENTION

The invention provides a method for the manufacture of an oil-in-water emulsion comprising: passing a first emulsion having a first average oil droplet size through a microfluidization device to
30 form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size. The microfluidization device comprises an interaction chamber which comprises a plurality of Z-type channels and an auxiliary processing module comprising at least one channel, wherein the auxiliary processing module is positioned downstream of the interaction chamber.

The first emulsion may be introduced into the interaction chamber at a first pressure and the second
35 emulsion can exit the auxiliary processing module at a second pressure which is lower than the first

pressure. In one embodiment, between 80 and 95 % of the pressure difference between the first and the second pressures is dropped across the interaction chamber and 5 to 20 % of the pressure difference between the first and the second pressures is dropped across the auxiliary processing module.

5 The present invention also provides a method for the manufacture of an oil-in-water emulsion comprising the step of passing a first emulsion having a first average oil droplet size through a microfluidization device to form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size. The microfluidization device comprises an interaction chamber comprising a plurality of channels and an auxiliary processing module comprising a
10 plurality of channels.

The first emulsion may either (i) be introduced into the interaction chamber at a first pressure and the second emulsion can exit the auxiliary processing module at a second pressure which is lower than the first pressure; or the first emulsion may (ii) be introduced into the auxiliary processing module at a first pressure and the second emulsion can exit the interaction chamber at a second pressure which
15 is lower than the first pressure. In one embodiment, between 80 and 95 % of the pressure difference between the first and the second pressures is dropped across the interaction chamber and 5 to 20 % of the pressure difference between the first and the second pressures is dropped across the auxiliary processing module.

As described in more detail below, the first emulsion may have an average oil droplet size of 5000nm
20 or less *e.g.* an average size between 300nm and 800nm. The number of oil droplets in the first emulsion with a size $>1.2 \mu\text{m}$ may be 5×10^{11} /ml or less, as described below. Oil droplets with a size $>1.2 \mu\text{m}$ are disadvantageous as they can cause instability of the emulsion due to agglomeration and coalescence of droplets [14].

After formation, the first emulsion may then be subjected to at least one pass of microfluidization to
25 form the second emulsion having a reduced average oil droplet size. As described below, the average oil droplet size of the second emulsion is 500 nm or less. The number of oil droplets in the second emulsion having a size $>1.2 \mu\text{m}$ may be 5×10^{10} /ml or less, as described below. To achieve these characteristics it may be necessary to pass the emulsion components through the microfluidization device a plurality of times, *e.g.* 2, 3, 4, 5, 6, 7 times.

30 The second emulsion may then be filtered, *e.g.* through a hydrophilic polyethersulfone membrane, to give an oil-in-water emulsion that may be suitable for use as a vaccine adjuvant. The average oil droplet size of the oil-in-water emulsion produced after filtration may be 220 nm or less, *e.g.* between 135-175 nm, between 145-165 nm, or about 155 nm. The number of oil droplets having a size $>1.2 \mu\text{m}$ present in the oil-in-water emulsion produced after filtration may be 5×10^8 /ml or less,
35 *e.g.* 5×10^7 /ml or less, 5×10^6 /ml or less, 2×10^6 /ml or less or 5×10^5 /ml or less.

The final oil-in-water emulsion formed after filtration may have at least 10^2 times fewer oil droplets having a size $>1.2\text{ }\mu\text{m}$ in comparison to the first emulsion, and ideally at least 10^3 times fewer (*e.g.* 10^4 times fewer).

In some embodiments, more than one cycle of steps (i) and (ii) is used prior to step (iii). Similarly, multiple repeats of individual steps (i) and (ii) may be used.

In general, the method is performed between 20-60°C, and ideally at $40\pm 5^\circ\text{C}$. Although the first and second emulsion components may be relatively stable even at higher temperatures, thermal breakdown of some components can still occur and so lower temperatures are preferred.

Emulsion components

The average oil droplet size (*i.e.* the number average diameter of the emulsion's oil droplets) may be measured using a dynamic light scattering technique, as described in reference 13. An example of a dynamic light scattering measurement machine is the Nicomp 380 Submicron Particle Size Analyzer (from Particle Sizing Systems).

The number of particles having a size $>1.2\text{ }\mu\text{m}$ may be measured using a particle counter such as the Accusizer™ 770 (from Particle Sizing Systems).

Methods of the invention are used for the manufacture of oil-in-water emulsions. These emulsions include three core ingredients: an oil; an aqueous component; and a surfactant.

Because the emulsions are intended for pharmaceutical use then the oil will typically be biodegradable (metabolisable) and biocompatible.

The oil used may comprise squalene, a shark liver oil which is a branched, unsaturated terpenoid ($\text{C}_{30}\text{H}_{50}$; $[(\text{CH}_3)_2\text{C}=\text{CHCH}_2\text{CH}_2\text{C}(\text{CH}_3)]_2=\text{CHCH}_2-$; 2,6,10,15,19,23-hexamethyl-2,6,10,14,18,22-tetracosahexaene; CAS RN 7683-64-9). Squalene is particularly preferred for use in the present invention.

The oil of the present invention may comprise a mixture (or combination) of oils *e.g.* comprising squalene and at least one further oil.

Rather than (or on addition to) using squalene an emulsion can comprise oil(s) including those from, for example, an animal (such as fish) or a vegetable source. Sources for vegetable oils include nuts, seeds and grains. Peanut oil, soybean oil, coconut oil, and olive oil, the most commonly available, exemplify the nut oils. Jojoba oil can be used *e.g.* obtained from the jojoba bean. Seed oils include safflower oil, cottonseed oil, sunflower seed oil, sesame seed oil and the like. In the grain group, corn oil is the most readily available, but the oil of other cereal grains such as wheat, oats, rye, rice, teff, triticale and the like may also be used. 6-10 carbon fatty acid esters of glycerol and 1,2-propanediol, while not occurring naturally in seed oils, may be prepared by hydrolysis, separation and esterification of the appropriate materials starting from the nut and seed oils. Fats and oils from mammalian milk are metabolizable and so may be used. The procedures for separation, purification,

saponification and other means necessary for obtaining pure oils from animal sources are well known in the art.

Most fish contain metabolizable oils which may be readily recovered. For example, cod liver oil, shark liver oils, and whale oil such as spermaceti exemplify several of the fish oils which may be used herein. A number of branched chain oils are synthesized biochemically in 5-carbon isoprene units and are generally referred to as terpenoids. Squalane, the saturated analog to squalene, can also be used. Fish oils, including squalene and squalane, are readily available from commercial sources or may be obtained by methods known in the art.

Other useful oils are the tocopherols, particularly in combination with squalene. Where the oil phase of an emulsion includes a tocopherol, any of the α , β , γ , δ , ϵ or ξ tocopherols can be used, but α -tocopherols are preferred. D- α -tocopherol and DL- α -tocopherol can both be used. A preferred α -tocopherol is DL- α -tocopherol. The tocopherol can take several forms *e.g.* different salts and/or isomers. Salts include organic salts, such as succinate, acetate, nicotinate, *etc.* If a salt of this tocopherol is to be used, the preferred salt is the succinate. An oil combination comprising squalene and a tocopherol (*e.g.* DL- α -tocopherol) can be used.

The aqueous component can be plain water (*e.g.* w.f.i.) or can include further components *e.g.* solutes. For instance, it may include salts to form a buffer *e.g.* citrate or phosphate salts, such as sodium salts. Typical buffers include: a phosphate buffer; a Tris buffer; a borate buffer; a succinate buffer; a histidine buffer; or a citrate buffer. Buffers will typically be included in the 5-20mM range.

The surfactant is preferably biodegradable (metabolisable) and biocompatible. Surfactants can be classified by their 'HLB' (hydrophile/lipophile balance), where a HLB in the range 1-10 generally means that the surfactant is more soluble in oil than in water, and a HLB in the range 10-20 are more soluble in water than in oil. Emulsions preferably comprise at least one surfactant that has a HLB of at least 10 *e.g.* at least 15, or preferably at least 16.

The invention can be used with surfactants including, but not limited to: the polyoxyethylene sorbitan esters surfactants (commonly referred to as the Tweens), especially polysorbate 20 and polysorbate 80; copolymers of ethylene oxide (EO), propylene oxide (PO), and/or butylene oxide (BO), sold under the DOWFAX™ tradename, such as linear EO/PO block copolymers; octoxynols, which can vary in the number of repeating ethoxy (oxy-1,2-ethanediyl) groups, with octoxynol-9 (Triton X-100, or t-octylphenoxypolyethoxyethanol) being of particular interest; (octylphenoxy)polyethoxyethanol (IGEPAL CA-630/NP-40); phospholipids such as phosphatidylcholine (lecithin); polyoxyethylene fatty ethers derived from lauryl, cetyl, stearyl and oleyl alcohols (known as Brij surfactants), such as triethyleneglycol monolauryl ether (Brij 30); polyoxyethylene-9-lauryl ether; and sorbitan esters (commonly known as the SPANs), such as sorbitan trioleate (Span 85) and sorbitan monolaurate. Preferred surfactants for including in the emulsion are polysorbate 80 (Tween 80; polyoxyethylene sorbitan monooleate), Span 85 (sorbitan trioleate), lecithin and Triton X-100.

Mixtures of surfactants can be included in the emulsion *e.g.* Tween 80/Span 85 mixtures, or Tween 80/Triton-X100 mixtures. A combination of a polyoxyethylene sorbitan ester such as polyoxyethylene sorbitan monooleate (Tween 80) and an octoxynol such as t-octylphenoxy-polyethoxyethanol (Triton X-100) is also suitable. Another useful combination comprises laureth 9
 5 plus a polyoxyethylene sorbitan ester and/or an octoxynol. Useful mixtures can comprise a surfactant with a HLB value in the range of 10-20 (*e.g.* Tween 80, with a HLB of 15.0) and a surfactant with a HLB value in the range of 1-10 (*e.g.* Span 85, with a HLB of 1.8).

Formation of the first emulsion

Before the microfluidization step, emulsion components may be mixed to form a first emulsion.

- 10 Oil droplets in the first emulsion may have an average size of 5000 nm or less *e.g.* 4000 nm or less, 3000nm or less, 2000nm or less, 1200nm or less, 1000nm or less, *e.g.* an average size between 800 and 1200 nm or between 300nm and 800nm.

In the first emulsion the number of oil droplets with a size $>1.2 \mu\text{m}$ may be 5×10^{11} /ml or less, *e.g.* 5×10^{10} /ml or less or 5×10^9 /ml or less.

- 15 The first emulsion may then be microfluidised to form a second emulsion having a lower average oil droplet size than the first emulsion and/or fewer oil droplets with size $>1.2 \mu\text{m}$.

The average oil droplet size of the first emulsion can be achieved by mixing the first emulsion's components in a homogenizer. For instance, as shown in Figure 1, they can be combined in a mixing vessel (12) and then the combined components can be introduced (13) into a mechanical
 20 homogenizer, such as a rotor-stator homogenizer (1).

Homogenizers can operate in a vertical and/or horizontal manner. For convenience in a commercial setting, in-line homogenizers are preferred.

- The components are introduced into a rotor-stator homogenizer and meet a rapidly rotating rotor containing slots or holes. The components are centrifugally thrown outwards in a pump like fashion
 25 and pass through the slots/holes. In some embodiments the homogenizer includes multiple combinations of rotors and stators *e.g.* a concentric arrangement of comb-teeth rings, as shown by features (3) & (4); (5) & (6) and (7) & (8) in Figure 1 and by Figure 2. The rotors in useful large-scale homogenizers may have comb-teeth rings on the edge of a horizontally oriented multi-bladed impeller (*e.g.* feature (9) in Figure 1) aligned in close tolerance to matching teeth in a static liner. The
 30 first emulsion forms via a combination of turbulence, cavitation and mechanical shearing occurring within the gap between rotor and stator. The components are usefully introduced in a direction parallel to the rotor's axis.

- An important performance parameter in rotor-stator homogenizers is the tip speed of the rotor (peripheral velocity). This parameter is a function both of rotation speed and of rotor diameter. A tip
 35 speed of at least 10 ms^{-1} is useful, and ideally quicker *e.g.* $\geq 20 \text{ ms}^{-1}$, $\geq 30 \text{ ms}^{-1}$, $\geq 40 \text{ ms}^{-1}$, *etc.* A tip speed of 40 ms^{-1} can be readily achieved at 10,000 rpm with a small homogenizer or at lower rotation

speeds (e.g. 2,000 rpm) with a larger homogenizer. Suitable high-shear homogenizers are commercially available.

For commercial-scale manufacture the homogenizer should ideally have a flow rate of at least 300 L/hr e.g. ≥ 400 L/hr, ≥ 500 L/hr, ≥ 600 L/hr, ≥ 700 L/hr, ≥ 800 L/hr, ≥ 900 L/hr, ≥ 1000 L/hr, ≥ 2000 L/hr, ≥ 5000 L/hr, or even ≥ 10000 L/hr. Suitable high-capacity homogenizers are commercially available.

A preferred homogenizer provides a shear rate of between 3×10^5 and 1×10^6 s⁻¹, e.g. between 3×10^5 and 7×10^5 s⁻¹, between 4×10^5 and 6×10^5 s⁻¹, e.g. about 5×10^5 s⁻¹.

Although rotor-stator homogenizers generate relatively little heat during operation, the homogenizer may be cooled during use. Ideally, the temperature of the first emulsion is maintained below 60°C during homogenization, e.g. below 45°C.

In some embodiments the first emulsion components may be homogenized multiple times (e.g. 2, 3, 4, 5, 6, 7, 8, 9, 10, 20, 30, 40, 50 or more times). To avoid the need for a long string of containers and homogenizers the emulsion components can instead be circulated (e.g. as shown by feature (11) in Figure 1). In particular, the first emulsion may be formed by circulating the first emulsion components through a homogenizer a plurality of times (e.g. 2, 3, 4, 5, 6, 7, 8, 9, 10, 20, 30, 40, 50, 100 *etc* times). However, too many cycles may be undesirable as it can produce re-coalescence as described in reference 14. Thus the size of oil droplets may be monitored if homogenizer circulation is used to check that a desired droplet size is reached and/or that re-coalescence is not occurring.

Circulation through the homogenizer is advantageous because it can reduce the average size of the oil droplets in the first emulsion. Circulation is also advantageous because it can reduce the number of oil droplets having a size >1.2 μm in the first emulsion. These reductions in average droplet size and number of droplets >1.2 μm in the first emulsion can provide advantages in downstream process(es). In particular, circulation of the first emulsion components through the homogenizer can lead to an improved microfluidization process which may then result in a reduced number of oil droplets having a size >1.2 μm in the second emulsion, *i.e.* after microfluidization. This improvement in the second emulsion parameters can provide improved filtration performance. Improved filtration performance may lead to less content losses during filtration, e.g. losses of squalene, Tween 80 and Span 85 when the oil-in-water emulsion is MF59.

Two particular types of circulation are referred to herein as "type I" and "type II". Type I circulation is illustrated in Figure 5, whereas type II circulation is illustrated in Figure 6.

The circulation of the first emulsion components may comprise a type I circulation of transferring the first emulsion components between a first premix container and a homogenizer. The first premix container may be from 50 to 500 L in size, e.g. 100 to 400 L, 100 to 300 L, 200 to 300 L, 250 L or 280 L. The first premix container may be manufactured from stainless steel. The type I circulation may be continued for 10 to 60 minutes, e.g. 10 to 40 minutes or 20 minutes.

The circulation of the first emulsion components may comprise a type II circulation of transferring the first emulsion components from a first premix container, through a first homogenizer to a second premix container (optionally having the same properties as the first premix container), and then through a second homogenizer. The second homogenizer will usually be the same as the first homogenizer, but in some arrangements the first and second homogenizers are different. Following the pass of the first emulsion components through the second homogenizer, the first emulsion components may be transferred back to the first premix container, for example if the type II circulation process is to be repeated. Thus the emulsion components may travel in a figure of eight route between the first and second premix containers via a single homogenizer (see Figure 6). Type II circulation may be carried out a single time or a plurality of times, *e.g.* 2, 3, 4, 5 *etc* times.

Type II circulation is advantageous, compared to type I circulation, because it can help to ensure that all of the components of the first emulsion pass through the homogenizer. Emptying of the first premix container means that the complete emulsion contents have passed through the homogenizer, into the second premix container. Similarly, the contents of the second premix container can be emptied, again ensuring that they all pass through the homogenizer. Thus the type II arrangement can conveniently ensure that all of the emulsion components are homogenized at least twice, which can reduce both the average size of the oil droplets and the number of oil droplets having a size $>1.2\ \mu\text{m}$ in the first emulsion. An ideal type II circulation thus involves emptying the first premix container and passing substantially all of its contents through the homogenizer into the second premix container, followed by emptying the second premix container and re-passing substantially all of its contents through the homogenizer back into the first premix container. Thus all particles pass through the homogenizer at least twice, whereas this is difficult to achieve with type I circulation.

In some embodiments a combination of type I and type II circulations is used, and this combination can provide a first emulsion with good characteristics. In particular, this combination can greatly reduce of the number of oil droplets having a size $>1.2\ \mu\text{m}$ in the first emulsion. This combination can comprise any order of type I and II circulation, *e.g.*, type I followed by type II, type II followed by type I, type I followed by type II followed by type I again *etc*. In one embodiment, the combination comprises 20 minutes of type I circulation followed by a single type II circulation, *i.e.* transferring the circulated first emulsion components from a first premix container, through a first homogenizer to a second premix container, and then through a second homogenizer once.

The first and second premix containers may be held under an inert gas, *e.g.* nitrogen, *e.g.* at up to 0.5 bar. This can prevent the emulsion components from oxidizing, which is particularly advantageous if one of the emulsion components is squalene. This can provide an increase in the stability of the emulsion.

As mentioned above, the initial input for the homogenizer may be a non-homogenized mixture of the first emulsion components. This mixture may be prepared by mixing the individual first emulsion components individually but, in some embodiments, multiple components can be combined prior to

this mixing. For instance, if the emulsion includes a surfactant with a HLB below 10 then this surfactant may be combined with an oil prior to mixing. Similarly, if the emulsion includes a surfactant with a HLB above 10 then this surfactant may be combined with an aqueous component prior to mixing. Buffer salts may be combined with an aqueous component prior to mixing, or may be added separately.

Methods of the invention may be used at large scale. Thus a method may involve preparing a first emulsion whose volume is greater than 1 liter *e.g.* ≥ 5 liters, ≥ 10 liters, ≥ 20 liters, ≥ 50 liters, ≥ 100 liters, ≥ 250 liters, *etc.*

After its formation, the first emulsion may be microfluidized, or may be stored to await microfluidization.

In some embodiments, in particular those where multiple cycles of steps (i) and (ii) are used, the input for the homogenizer will be the output of a microfluidizer, such that the first emulsion is microfluidized and then again subjected to homogenization.

Microfluidization

After its formation the first emulsion is microfluidized in order to reduce its average oil droplet size and/or to reduce the number of oil droplets having a size of $>1.2 \mu\text{m}$.

Microfluidization instruments reduce average oil droplet size by propelling streams of input components through geometrically fixed channels at high pressure and high velocity. The pressure at the entrance to the interaction chamber (also called the "first pressure") may be substantially constant (*i.e.* $\pm 15\%$; *e.g.* $\pm 10\%$, $\pm 5\%$, $\pm 2\%$) for at least 85% of the time during which components are fed into the microfluidizer, *e.g.* at least 87%, at least 90%, at least 95%, at least 99% or 100% of the time during which the emulsion is fed into the microfluidizer.

In one embodiment, the first pressure is 1300 bar $\pm 15\%$ (18 kPSI $\pm 15\%$), *i.e.* between 1100 bar and 1500 bar (between 15 kPSI and 21 kPSI) for 85% of the time during which the emulsion is fed into the microfluidizer. Two suitable pressure profiles are shown in Figure 3. In Figure 3A the pressure is substantially constant for at least 85% of the time, whereas in Figure 3B the pressure continuously remains substantially constant.

A microfluidization apparatus typically comprises at least one intensifier pump (preferably two pumps, which may be synchronous) and an interaction chamber. The intensifier pump, which is ideally electric-hydraulic driven, provides high pressure (*i.e.* the first pressure) to force an emulsion into and through the interaction chamber. The synchronous nature of the intensifier pumps may be used to provide the substantially constant pressure of the emulsion discussed above, which means that the emulsion droplets are all exposed to substantially the same level of shear forces during microfluidization.

One advantage of the use of a substantially constant pressure is that it can reduce fatigue failures in the microfluidization device, which may lead to longer life of the device. A further advantage of the use of a substantially constant pressure is that the parameters of the second emulsion can be improved. In particular, the number of oil droplets having a size $>1.2\ \mu\text{m}$ present in the second emulsion can be reduced. Furthermore, the average oil droplet size of the second emulsion can be reduced when a substantially constant pressure is used. The reduction in the average oil droplet size and in the number of oil droplets having a size $>1.2\ \mu\text{m}$ in the second emulsion may provide improved filtration performance. Improved filtration performance may lead to less content losses during filtration, *e.g.* losses of squalene, Tween 80 and Span 85 when the emulsion is MF59.

The interaction chamber may contain a plurality, *e.g.* 2, 3, 4, 5, 6, 7, 8, 9, 10 *etc.*, of fixed geometry channels into which the emulsion passes. The emulsion enters the interaction chamber through an input line which may have a diameter of between 200 to 250 μm . The emulsion divides into streams as it enters the interaction chamber and, under high pressure, accelerates to high velocity. As it passes through the channels, forces produced by the high pressure may act to reduce the emulsion's oil droplet size and reduce the number of oil droplets having a size $>1.2\ \mu\text{m}$. These forces can include: shear forces, through deformation of the emulsion stream occurring from contact with channel walls; impact forces, through collisions occurring when high velocity emulsion streams collide with each other; and cavitation forces, through formation and collapse of cavities within the stream. The interaction chamber usually includes no moving parts. It may include ceramic (*e.g.* alumina) or diamond (*e.g.* polycrystalline diamond) channel surfaces. Other surfaces may be made of stainless steel.

The fixed geometry of the plurality of channels in the interaction chamber may be "Y" type geometry or "Z" type geometry.

In a Y-type geometry interaction chamber a single input emulsion stream is split into first and second emulsion streams, which are then recombined into a single output emulsion stream. Prior to recombination, each of the first and second emulsion streams may independently be split into a first and second plurality (*e.g.* 2, 3, 4, 5, 6, 7, 8, 9, 10 *etc.*) of sub-streams. When the emulsion streams are recombined, the first and second emulsion streams (or their sub-streams) are ideally flowing in substantially opposite directions (*e.g.* the first and second emulsion streams, or their sub-streams, are flowing in substantially the same plane ($\pm 20^\circ$) and the flow direction of the first emulsion stream is $180 \pm 20^\circ$ different from the flow direction of the second emulsion stream). The forces produced when the emulsion streams are recombined may act to reduce the emulsion's oil droplet size and reduce the number of oil droplets having a size $>1.2\ \mu\text{m}$.

In a Z-type geometry interaction chamber the emulsion stream passes around a plurality (*e.g.* 2, 3, 4, 5, 6, 7, 8, 9, 10 *etc.*) of substantially right angled corners (*i.e.* $90 \pm 20^\circ$). Figure 4 illustrates an interaction chamber with Z-type geometry and two right-angled corners in the direction of flow. During its passage around the corners, an input emulsion stream may be split into a plurality (*e.g.* 2,

3, 4, 5, 6, 7, 8, 9, 10 *etc.*) of sub-streams and then recombined into a single output emulsion stream (*e.g.* as shown in Figure 4, with four sub-streams (32)). The split and then recombination (31) may occur at any point between input and output. The forces produced when the emulsion contacts the channel walls as it passes around the corners may act to reduce the emulsion's oil droplet size and
5 reduce the number of oil droplets having a size $>1.2\ \mu\text{m}$. An example of a Z-type interaction chamber is the E230Z interaction chamber from Microfluidics.

In one embodiment, the emulsion stream passes around two substantially right angled corners. At the point when the input emulsion stream passes around the first substantially right angled corner, it is split into five sub-streams. At the point when the sub-streams pass around the second substantially
10 right angled corner, they are recombined into a single output emulsion stream.

In the prior art it has been usual to use Y-type interaction chambers for oil-in-water emulsions like those of the present invention. However, we have discovered that it is advantageous to use a Z-type channel geometry interaction chamber for oil-in-water emulsions because this can lead to a greater reduction in the number of oil droplets having a size of $>1.2\ \mu\text{m}$ present in the second emulsion
15 compared to a Y-type geometry interaction chamber. The reduction in number of oil droplets having a size $>1.2\ \mu\text{m}$ in the second emulsion can provide improved filtration performance. Improved filtration performance may lead to less content losses during filtration, *e.g.* losses of squalene, Tween 80 and Span 85 when the emulsion is MF59.

A preferred microfluidization apparatus operates at a pressure between 170 bar and 2750 bar (approximately 2500 psi to 40000 psi) *e.g.* at about 345 bar, about 690 bar, about 1380 bar, about
20 2070 bar, *etc.*

A preferred microfluidization apparatus operates at a flow rate of up to 20 L/min *e.g.* up to 14 L/min, up to 7 L/min, up to 3.5 L/min, *etc.*

A preferred microfluidization apparatus has an interaction chamber that provides a shear rate in
25 excess of $1 \times 10^6\ \text{s}^{-1}$ *e.g.* $\geq 2.5 \times 10^6\ \text{s}^{-1}$, $\geq 5 \times 10^6\ \text{s}^{-1}$, $\geq 10^7\ \text{s}^{-1}$, *etc.*

A microfluidization apparatus can include multiple interaction chambers that are used in parallel *e.g.* 2, 3, 4, 5 or more, but it is more useful to include a single interaction chamber.

The microfluidization device may comprise an auxiliary processing module (APM; also known in microfluidizers as a back pressure chamber – these terms are used interchangeably herein)
30 comprising at least one channel. The APM contributes to the reduction in the average size of the oil droplets in the emulsion being passed through the microfluidization device, although the majority of the reduction occurs in the interaction chamber. As mentioned above, the emulsion components are introduced to the interaction chamber by the intensifier pump(s) under a first pressure. The emulsion components generally exit the APM at a second pressure which is lower than the first pressure (*e.g.*
35 atmospheric pressure). In general, between 80 and 95% of the pressure difference between the first and the second pressures is dropped across the interaction chamber (*e.g.* from P_1 to P_2 in Figure 4)

and 5 to 20% of the pressure difference between the first and the second pressures is dropped across the auxiliary processing module, *e.g.* the interaction chamber may provide approximately 90% of the pressure drop while the APM may provide approximately 10% of the pressure drop. If the pressure dropped across the interaction chamber and the pressure dropped across the auxiliary processing module do not account for the whole of the pressure difference between the first and the second pressure, this can be due to a finite pressure drop across the connectors between the interaction chamber and the auxiliary processing module.

The APM usually includes no moving parts. It may include ceramic (*e.g.* alumina) or diamond (*e.g.* polycrystalline diamond) channel surfaces. Other surfaces may be made of stainless steel.

The APM is generally positioned downstream of the interaction chamber and may also be positioned sequential to the interaction chamber. In the prior art, APMs are generally positioned downstream of interaction chambers comprising Y-type channels to suppress cavitation and thereby increase the flowrate in the Y-type chamber by up to 30%. Furthermore, in the prior art APMs are generally positioned upstream of interaction chambers comprising Z-type channels to reduce the size of large agglomerates. In the latter case, the APM only decreases the flowrate in the Z-type chambers by up to 3%. However, it has been found that positioning the APM downstream of an interaction chamber comprising a plurality of Z-type channels is advantageous in the present invention because it can lead to a greater reduction in average oil droplet size and a greater reduction in the number of oil droplets having a size of $>1.2\ \mu\text{m}$ present in the second emulsion. As discussed above, the reduction in number of oil droplets having a size $>1.2\ \mu\text{m}$ in the second emulsion may provide improved filtration performance. Improved filtration performance may lead to less content losses during filtration, *e.g.* losses of squalene, Tween 80 and Span 85 when the oil-in-water emulsion is MF59. A further advantage of this positioning of a Z-type interaction chamber and a downstream APM is that it can lead to a slower pressure decrease after the interaction chamber. The slower pressure decrease may lead to an increase in product stability because there is less gas enclosed in the emulsion.

An APM contains at least one fixed geometry channel into which the emulsion passes. The APM may contain a plurality *e.g.* 2, 3, 4, 5, 6, 7, 8, 9, 10 *etc.*, of fixed geometry channels into which the emulsion passes. The channel or channels of the APM may be linear or non-linear. Suitable non-linear channels are of "Z" type geometry or "Y" type geometry, which are the same as those described above for the interaction chamber. In one embodiment, the channel, or channels, of the APM are of Z-type geometry. A plurality of Z-type channels divides the emulsion into streams as it enters the APM.

In contrast to the manufacturer's recommendations, the use of an APM comprising a plurality of fixed geometry channels is advantageous compared to a single fixed geometry channel APM because it can lead to a greater reduction in the number of oil droplets having a size $>1.2\ \mu\text{m}$ present in the second emulsion. As discussed above, the reduction in the number of oil droplets having a size $>1.2\ \mu\text{m}$ in the second emulsion can provide improved filtration performance. Improved filtration

performance may lead to less content losses during filtration, *e.g.* losses of squalene, Tween 80 and Span 85 when the oil-in-water emulsion is MF59.

A microfluidization apparatus generates heat during operation, which can raise an emulsion's temperature by 15-20°C relative to the first emulsion. Advantageously, therefore, the microfluidized emulsion is cooled as soon as possible. The temperature of the second emulsion may be maintained below 60°C, *e.g.* below 45°C. Thus an interaction chamber's output and/or an APM's output may feed into a cooling mechanism, such as a heat exchanger or cooling coil. The distance between the output and the cooling mechanism should be kept as short as possible to shorten the overall time by reducing cooling delays. In one embodiment, the distance between the output of the microfluidizer and the cooling mechanism is between 20-30cm. A cooling mechanism is particularly useful when an emulsion is subjected to multiple microfluidization steps, to prevent over-heating of the emulsion.

The result of microfluidization is an oil-in-water emulsion, the second emulsion, in which the average size of the oil droplets is 500 nm or less. This average size is particularly useful as it facilitates filter sterilization of the emulsion. Emulsions in which at least 80% by number of the oil droplets have an average size of 500 nm or less, *e.g.* 400 nm or less, 300 nm or less, 200 nm or less or 165 nm or less, are particularly useful. Furthermore, the number of oil droplets in the second emulsion having a size >1.2 µm is 5×10^{10} /ml or less, *e.g.* 5×10^9 /ml or less, 5×10^8 /ml or less or 2×10^8 /ml or less.

The initial input for the microfluidization may be the first emulsion. In some embodiments, however, the microfluidized emulsion is subjected to microfluidization again, such that multiple rounds of microfluidization occur. In particular, the second emulsion may be formed by circulating the second emulsion components through a microfluidization device a plurality of times, *e.g.* 2, 3, 4, 5, 6, 7, 8, 9, 10 *etc* times. The second emulsion may be formed by circulating the second emulsion components through a microfluidization device 4 to 7 times.

The circulation of the second emulsion components may comprise a type I circulation of transferring the second emulsion components between a first emulsion container (optionally having the same properties as the first premix container) and the microfluidization device.

The circulation of the second emulsion components may comprise a type II circulation of transferring the second emulsion components from a first emulsion container, through a first microfluidization device to a second emulsion container (optionally having the same properties as the first premix container), and then through a second microfluidization device.

The second microfluidization device may be the same as the first microfluidization device. Alternatively, the second microfluidization device may be different to the first microfluidization device.

The first emulsion container may be the same as the first premix container. Alternatively, the first emulsion container may be the same as the second premix container.

The second emulsion container may be the same as the first premix container. Alternatively, the second emulsion container may be the same as the second premix container.

The first emulsion container may be the same as the first premix container and the second emulsion container may be the same as the second premix container. Alternatively, the first emulsion container may be the same as the second premix container and the second emulsion container may be the same as the first premix container.

As an alternative, the first and second emulsion containers may be different to the first and second premix containers.

Following the pass of the second emulsion components through the second microfluidization device, the second emulsion components may be transferred back to the first emulsion container, for example if the type II circulation process is to be repeated. Type II circulation may be carried out a single time or a plurality of times, *e.g.* 2, 3, 4, 5 *etc* times.

Type II circulation is advantageous as it ensures that all the second emulsion components have passed through the microfluidization device at least 2 times, which reduces the average size of the oil droplets and the number of oil droplets having a size $>1.2\ \mu\text{m}$ in the second emulsion.

A combination of type I circulation and type II circulation may be used during microfluidization. This combination can comprise any order of type I and II circulation, *e.g.*, type I followed by type II, type II followed by type I, type I followed by type II followed by type I again *etc*.

The first and second emulsion containers may be held under an inert gas, *e.g.* up to 0.5 bar of nitrogen. This prevents the emulsion components oxidizing, which is particularly advantageous if one of the emulsion components is squalene. This leads to an increase in the stability of the emulsion.

Methods of the invention may be used at large scale. Thus a method may involve microfluidizing a volume greater than 1 liter *e.g.* ≥ 5 liters, ≥ 10 liters, ≥ 20 liters, ≥ 50 liters, ≥ 100 liters, ≥ 250 liters, *etc*.

Filtration

After microfluidization, the second emulsion is filtered. This filtration removes any large oil droplets that have survived the homogenization and microfluidization procedures. Although small in number terms, these oil droplets can be large in volume terms and they can act as nucleation sites for aggregation, leading to emulsion degradation during storage. Moreover, this filtration step can achieve filter sterilization.

The particular filtration membrane suitable for filter sterilization depends on the fluid characteristics of the second emulsion and the degree of filtration required. A filter's characteristics can affect its suitability for filtration of the microfluidized emulsion. For example, its pore size and surface characteristics can be important, particularly when filtering a squalene-based emulsion.

The pore size of membranes used with the invention should permit passage of the desired droplets while retaining the unwanted droplets. For example, it should retain droplets that have a size of $\geq 1\mu\text{m}$ while permitting passage of droplets $< 200\text{nm}$. A $0.2\mu\text{m}$ or $0.22\mu\text{m}$ filter is ideal, and can also achieve filter sterilization.

- 5 The emulsion may be prefiltered *e.g.* through a $0.45\mu\text{m}$ filter. The prefiltration and filtration can be achieved in one step by the use of known double-layer filters that include a first membrane layer with larger pores and a second membrane layer with smaller pores. Double-layer filters are particularly useful with the invention. The first layer ideally has a pore size $> 0.3\mu\text{m}$, such as between $0.3\text{--}2\mu\text{m}$ or between $0.3\text{--}1\mu\text{m}$, or between $0.4\text{--}0.8\mu\text{m}$, or between $0.5\text{--}0.7\mu\text{m}$. A pore size of $\leq 0.75\mu\text{m}$ in the first
- 10 layer is preferred. Thus the first layer may have a pore size of $0.6\mu\text{m}$ or $0.45\mu\text{m}$, for example. The second layer ideally has a pore size which is less than 75% of (and ideally less than half of) the first layer's pore size, such as between 25-70% or between 25-49% of the first layer's pore size *e.g.* between 30-45%, such as 1/3 or 4/9, of the first layer's pore size. Thus the second layer may have a pore size $< 0.3\mu\text{m}$, such as between $0.15\text{--}0.28\mu\text{m}$ or between $0.18\text{--}0.24\mu\text{m}$ *e.g.* a $0.2\mu\text{m}$ or
- 15 $0.22\mu\text{m}$ pore size second layer. In one example, the first membrane layer with larger pores provides a $0.45\mu\text{m}$ filter, while the second membrane layer with smaller pores provides a $0.22\mu\text{m}$ filter.

The filtration membrane and/or the prefiltration membrane may be asymmetric. An asymmetric membrane is one in which the pore size varies from one side of the membrane to the other *e.g.* in which the pore size is larger at the entrance face than at the exit face. One side of the asymmetric

20 membrane may be referred to as the "coarse pored surface", while the other side of the asymmetric membrane may be referred to as the "fine pored surface". In a double-layer filter, one or (ideally) both layers may be asymmetric.

The filtration membrane may be porous or homogeneous. A homogeneous membrane is usually a dense film ranging from 10 to 200 μm . A porous membrane has a porous structure. In one

25 embodiment, the filtration membrane is porous. In a double-layer filter, both layers may be porous, both layers may be homogenous, or there may be one porous and one homogenous layer. A preferred double-layer filter is one in which both layers are porous.

In one embodiment, the second emulsion is prefiltered through an asymmetric, hydrophilic porous membrane and then filtered through another asymmetric hydrophilic porous membrane having

30 smaller pores than the prefiltration membrane. This can use a double-layer filter.

The filter membrane(s) may be autoclaved prior to use to ensure that it is sterile.

Filtration membranes are typically made of polymeric support materials such as PTFE (poly-tetrafluoro-ethylene), PES (polyethersulfone), PVP (polyvinyl pyrrolidone), PVDF (polyvinylidene fluoride), nylons (polyamides), PP (polypropylene), celluloses (including cellulose esters), PEEK

35 (polyetheretherketone), nitrocellulose, *etc.* These have varying characteristics, with some supports being intrinsically hydrophobic (*e.g.* PTFE) and others being intrinsically hydrophilic (*e.g.* cellulose

acetates). However, these intrinsic characteristics can be modified by treating the membrane surface. For instance, it is known to prepare hydrophilized or hydrophobized membranes by treating them with other materials (such as other polymers, graphite, silicone, *etc.*) to coat the membrane surface *e.g.* see section 2.1 of reference 15. In a double-layer filter the two membranes can be made of
5 different materials or (ideally) of the same material.

An ideal filter for use with the invention has a hydrophilic surface, in contrast to the teaching of references 9-12 that hydrophobic (polysulfone) filters should be used. Filters with hydrophilic surfaces can be formed from hydrophilic materials, or by hydrophilization of hydrophobic materials, and a preferred filter for use with the invention is a hydrophilic polyethersulfone membrane. Several
10 different methods are known to transform hydrophobic PES membranes into hydrophilic PES membranes. Often it is achieved by coating the membrane with a hydrophilic polymer. To provide permanent attachment of the hydrophilic polymer to the PES a hydrophilic coating layer is usually subjected either to a cross-linking reaction or to grafting. Reference 15 discloses a process for modifying the surface properties of a hydrophobic polymer having functionalizable chain ends,
15 comprising contacting the polymer with a solution of a linker moiety to form a covalent link, and then contacting the reacted hydrophobic polymer with a solution of a modifying agent. Reference 16 discloses a method of PES membrane hydrophilization by direct membrane coating, involving pre-wetting with alcohol, and then soaking in an aqueous solution containing a hydrophilic monomer, a polyfunctional monomer (cross-linker) and a polymerization initiator. The monomer and
20 cross-linker are then polymerized using thermal- or UV-initiated polymerization to form a coating of cross-linked hydrophilic polymer on the membrane surface. Similarly, references 17 and 18 disclose coating a PES membrane by soaking it in an aqueous solution of hydrophilic polymer (polyalkylene oxide) and at least one polyfunctional monomer (cross-linker), and then polymerizing a monomer to provide a non-extractable hydrophilic coating. Reference 19 describes the hydrophilization of PES
25 membrane by a grafting reaction in which a PES membrane is submitted to low-temperature helium plasma treatment followed by grafting of hydrophilic monomer N-vinyl-2-pyrrolidone (NVP) onto the membrane surface. Further such processes are disclosed in references 20 to 26.

In methods that do not rely on coating, PES can be dissolved in a solvent, blended with a soluble hydrophilic additive, and then the blended solution is used for casting a hydrophilic membrane *e.g.*
30 by precipitation or by initiating co-polymerization. Such methods are disclosed in references 27 to 33. For example, reference 33 discloses a method of preparing a hydrophilic charge-modified membrane that has low membrane extractables and allows fast recovery of ultrapure water resistivity, having a cross-linked inter-penetrating polymer network structure formed making a polymer solution of a blend of PES, PVP, polyethyleneimine, and aliphatic diglycidyl ether, forming a thin film of the
35 solution, and precipitating the film as a membrane. A similar process is disclosed in reference 34.

Hybrid approaches can be used, in which hydrophilic additives are present during membrane formation and are also added later as a coating *e.g.* see reference 35.

Hydrophilization of PES membrane can also be achieved by treatment with low temperature plasmas. Reference 36 describes hydrophilic modification of PES membrane by treatment with low temperature CO₂-plasma.

Hydrophilization of PES membrane can also be achieved by oxidation, as described in reference 37.

- 5 This method involves pre-wetting a hydrophobic PES membrane in a liquid having a low surface tension, exposing the wet PES membrane to an aqueous solution of oxidizer, and then heating.

Phase inversion can also be used, as described in reference 38.

- 10 An ideal hydrophilic PES membrane can be obtained by treatment of PES (hydrophobic) with PVP (hydrophilic). Treatment with PEG (hydrophilic) instead of PVP has been found to give a hydrophilized PES membrane that is easily fouled (particularly when using a squalene-containing emulsion) and also disadvantageously releases formaldehyde during autoclaving.

A preferred double-layer filter has a first hydrophilic PES membrane and a second hydrophilic PES membrane.

- 15 Known hydrophilic membranes include Bioassure (from Cuno); EverLUX™ polyethersulfone; STyLUX™ polyethersulfone (both from Meissner); Millex GV, Millex HP, Millipak 60, Millipak 200 and Durapore CVGL01TP3 membranes (from Millipore); Fluorodyne™ EX EDF Membrane, Supor™ EAV; Supor™ EBV, Supor™ EKV (all from Pall); Sartopore™ (from Sartorius); Sterlitech's hydrophilic PES membrane; and Wolftechnik's WFPES PES membrane.

- 20 During filtration, the emulsion may be maintained at a temperature of 40°C or less, *e.g.* 30°C or less, to facilitate successful sterile filtration. Some emulsions may not pass through a sterile filter when they are at a temperature of greater than 40°C.

- 25 It is advantageous to carry out the filtration step within 24 hours, *e.g.* within 18 hours, within 12 hours, within 6 hours, within 2 hours, within 30 minutes, of producing the second emulsion because after this time it may not be possible to pass the second emulsion through the sterile filter without clogging the filter, as discussed in reference 39.

Methods of the invention may be used at large scale. Thus a method may involve filtering a volume greater than 1 liter *e.g.* ≥5 liters, ≥10 liters, ≥20 liters, ≥50 liters, ≥100 liters, ≥250 liters, *etc.*

The final emulsion

- 30 The result of microfluidization and filtration is an oil-in-water emulsion in which the average size of the oil droplets may be less than 220 nm, *e.g.* 155 ± 20 nm, 155 ± 10 nm or 155 ± 5 nm, and in which the number of oil droplets having a size >1.2 μm may be 5 × 10⁸ /ml or less, *e.g.* 5 × 10⁷ /ml or less, 5 × 10⁶ /ml or less, 2 × 10⁶ /ml or less or 5 × 10⁵ /ml or less.

The average oil droplet size of emulsions described herein (including the first and second emulsions) is generally not less than 50 nm.

Methods of the invention may be used at large scale. Thus a method may involve preparing a final emulsion with a volume greater than 1 liter *e.g.* ≥ 5 liters, ≥ 10 liters, ≥ 20 liters, ≥ 50 liters, ≥ 100 liters, ≥ 250 liters, *etc.*

Once the oil-in-water emulsion has been formed, it may be transferred into sterile glass bottles. The glass bottles may be 5 L, 8 L, or 10 L in size. Alternatively, the oil-in-water may be transferred into a sterile flexible bag (flex bag). The flex bag may be 50 L, 100 L or 250 L in size. In addition, the flex bag may be fitted with one or more sterile connectors to connect the flex bag to the system. The use of a flex bag with a sterile connectors is advantageous compared to glass bottles because the flex bag is larger than the glass bottles meaning that it may not be necessary to change the flex bag to store all the emulsion manufactured in a single batch. This can provide a sterile closed system for the manufacture of the emulsion which may reduce the chance of impurities being present in the final emulsion. This can be particularly important if the final emulsion is used for pharmaceutical purposes, *e.g.* if the final emulsion is the MF59 adjuvant.

Preferred amounts of oil (% by volume) in the final emulsion are between 2-20% *e.g.* about 10%. A squalene content of about 5% or about 10% is particularly useful. A squalene content (w/v) of between 30-50mg/ml is useful *e.g.* between 35-45mg/ml, 36-42mg/ml, 38-40mg/ml, *etc.*

Preferred amounts of surfactants (% by weight) in the final emulsion are: polyoxyethylene sorbitan esters (such as Tween 80) 0.02 to 2%, in particular about 0.5% or about 1%; sorbitan esters (such as Span 85) 0.02 to 2%, in particular about 0.5% or about 1%; octyl- or nonylphenoxy polyoxyethanols (such as Triton X-100) 0.001 to 0.1%, in particular 0.005 to 0.02%; polyoxyethylene ethers (such as laureth 9) 0.1 to 20%, preferably 0.1 to 10% and in particular 0.1 to 1% or about 0.5%. A polysorbate 80 content (w/v) of between 4-6mg/ml is useful *e.g.* between 4.1-5.3mg/ml. A sorbitan trioleate content (w/v) of between 4-6mg/ml is useful *e.g.* between 4.1-5.3mg/ml.

The process is particularly useful for preparing any of the following oil-in-water emulsions:

- An emulsion comprising squalene, polysorbate 80 (Tween 80), and sorbitan trioleate (Span 85). The composition of the emulsion by volume can be about 5% squalene, about 0.5% polysorbate 80 and about 0.5% sorbitan trioleate. In weight terms, these amounts become 4.3% squalene, 0.5% polysorbate 80 and 0.48% sorbitan trioleate. This adjuvant is known as 'MF59'. The MF59 emulsion advantageously includes citrate ions *e.g.* 10mM sodium citrate buffer.
- Emulsions comprising squalene, an α -tocopherol (ideally DL- α -tocopherol), and polysorbate 80. These emulsions may have (by weight) from 2 to 10% squalene, from 2 to 10% α -tocopherol and from 0.3 to 3% polysorbate 80 *e.g.* 4.3% squalene, 4.7% α -tocopherol, 1.9% polysorbate 80. The weight ratio of squalene:tocopherol is preferably ≤ 1 (*e.g.* 0.90) as this provides a more stable emulsion. Squalene and polysorbate 80 may be present volume ratio of about 5:2, or at a weight ratio of about 11:5. One such emulsion can be made by dissolving

polysorbate 80 in PBS to give a 2% solution, then mixing 90ml of this solution with a mixture of (5g of DL- α -tocopherol and 5ml squalene), then microfluidizing the mixture. The resulting emulsion may have submicron oil droplets *e.g.* with a size between 100 and 250nm, preferably about 180nm.

- 5 • An emulsion of squalene, a tocopherol, and a Triton detergent (*e.g.* Triton X-100). The emulsion may also include a 3-O-deacylated monophosphoryl lipid A ('3d-MPL'). The emulsion may contain a phosphate buffer.
- An emulsion comprising squalene, a polysorbate (*e.g.* polysorbate 80), a Triton detergent (*e.g.* Triton X-100) and a tocopherol (*e.g.* an α -tocopherol succinate). The emulsion may include
10 these three components at a mass ratio of about 75:11:10 (*e.g.* 750 μ g/ml polysorbate 80, 110 μ g/ml Triton X-100 and 100 μ g/ml α -tocopherol succinate), and these concentrations should include any contribution of these components from antigens. The emulsion may also include a 3d-MPL. The emulsion may also include a saponin, such as QS21. The aqueous phase may contain a phosphate buffer.
- 15 • An emulsion comprising squalene, an aqueous solvent, a polyoxyethylene alkyl ether hydrophilic nonionic surfactant (*e.g.* polyoxyethylene (12) cetostearyl ether) and a hydrophobic nonionic surfactant (*e.g.* a sorbitan ester or mannide ester, such as sorbitan monoleate or 'Span 80'). The emulsion is preferably thermoreversible and/or has at least 90% of the oil droplets (by volume) with a size less than 200 nm [40]. The emulsion may also
20 include one or more of: alditol; a cryoprotective agent (*e.g.* a sugar, such as dodecylmaltoside and/or sucrose); and/or an alkylpolyglycoside. It may also include a TLR4 agonist, such as one whose chemical structure does not include a sugar ring [41]. Such emulsions may be lyophilized.

The compositions of these emulsions, expressed above in percentage terms, may be modified by
25 dilution or concentration (*e.g.* by an integer, such as 2 or 3 or by a fraction, such as 2/3 or 3/4), in which their ratios stay the same. For instance, a 2-fold concentrated MF59 would have about 10% squalene, about 1% polysorbate 80 and about 1% sorbitan trioleate. Concentrated forms can be diluted (*e.g.* with an antigen solution) to give a desired final concentration of emulsion.

Emulsions of the invention are ideally stored at between 2°C and 8°C. They should not be frozen.
30 They should ideally be kept out of direct light. In particular, squalene-containing emulsions and vaccines of the invention should be protected to avoid photochemical breakdown of squalene. If emulsions of the invention are stored then this is preferably in an inert atmosphere *e.g.* N₂ or argon.

Vaccines

Although it is possible to administer oil-in-water emulsion adjuvants on their own to patients (*e.g.* to
35 provide an adjuvant effect for an antigen that has been separately administered to the patient), it is more usual to admix the adjuvant with an antigen prior to administration, to form an immunogenic

composition *e.g.* a vaccine. Mixing of emulsion and antigen may take place extemporaneously, at the time of use, or can take place during vaccine manufacture, prior to filling. The methods of the invention can be applied in both situations.

Thus a method of the invention may include a further process step of admixing the emulsion with an antigen component. As an alternative, it may include a further step of packaging the adjuvant into a kit as a kit component together with an antigen component.

Overall, therefore, the invention can be used when preparing mixed vaccines or when preparing kits including antigen and adjuvant ready for mixing. Where mixing takes place during manufacture then the volumes of bulk antigen and emulsion that are mixed will typically be greater than 1 liter *e.g.* ≥ 5 liters, ≥ 10 liters, ≥ 20 liters, ≥ 50 liters, ≥ 100 liters, ≥ 250 liters, *etc.* Where mixing takes place at the point of use then the volumes that are mixed will typically be smaller than 1 milliliter *e.g.* ≤ 0.6 ml, ≤ 0.5 ml, ≤ 0.4 ml, ≤ 0.3 ml, ≤ 0.2 ml, *etc.* In both cases it is usual for substantially equal volumes of emulsion and antigen solution to be mixed *i.e.* substantially 1:1 (*e.g.* between 1.1:1 and 1:1.1, preferably between 1.05:1 and 1:1.05, and more preferably between 1.025:1 and 1:1.025). In some embodiments, however, an excess of emulsion or an excess of antigen may be used [42]. Where an excess volume of one component is used, the excess will generally be at least 1.5:1 *e.g.* $\geq 2:1$, $\geq 2.5:1$, $\geq 3:1$, $\geq 4:1$, $\geq 5:1$, *etc.*

Where antigen and adjuvant are presented as separate components within a kit, they are physically separate from each other within the kit, and this separation can be achieved in various ways. For instance, the components may be in separate containers, such as vials. The contents of two vials can then be mixed when needed *e.g.* by removing the contents of one vial and adding them to the other vial, or by separately removing the contents of both vials and mixing them in a third container.

In another arrangement, one of the kit components is in a syringe and the other is in a container such as a vial. The syringe can be used (*e.g.* with a needle) to insert its contents into the vial for mixing, and the mixture can then be withdrawn into the syringe. The mixed contents of the syringe can then be administered to a patient, typically through a new sterile needle. Packing one component in a syringe eliminates the need for using a separate syringe for patient administration.

In another preferred arrangement, the two kit components are held together but separately in the same syringe *e.g.* a dual-chamber syringe, such as those disclosed in references 43-50 *etc.* When the syringe is actuated (*e.g.* during administration to a patient) then the contents of the two chambers are mixed. This arrangement avoids the need for a separate mixing step at time of use.

The contents of the various kit components will generally all be in liquid form. In some arrangements, a component (typically the antigen component rather than the emulsion component) is in dry form (*e.g.* in a lyophilized form), with the other component being in liquid form. The two components can be mixed in order to reactivate the dry component and give a liquid composition for administration to a patient. A lyophilized component will typically be located within a vial rather

than a syringe. Dried components may include stabilizers such as lactose, sucrose or mannitol, as well as mixtures thereof *e.g.* lactose/sucrose mixtures, sucrose/mannitol mixtures, *etc.* One possible arrangement uses a liquid emulsion component in a pre-filled syringe and a lyophilized antigen component in a vial.

- 5 If vaccines contain components in addition to emulsion and antigen then these further components may be included in one these two kit components, or may be part of a third kit component.

Suitable containers for mixed vaccines of the invention, or for individual kit components, include vials and disposable syringes. These containers should be sterile.

- Where a composition/component is located in a vial, the vial is preferably made of a glass or plastic material. The vial is preferably sterilized before the composition is added to it. To avoid problems with latex-sensitive patients, vials are preferably sealed with a latex-free stopper, and the absence of latex in all packaging material is preferred. In one embodiment, a vial has a butyl rubber stopper. The vial may include a single dose of vaccine/component, or it may include more than one dose (a 'multidose' vial) *e.g.* 10 doses. In one embodiment, a vial includes 10 x 0.25 ml doses of emulsion.
- 15 Preferred vials are made of colorless glass.

- A vial can have a cap (*e.g.* a Luer lock) adapted such that a pre-filled syringe can be inserted into the cap, the contents of the syringe can be expelled into the vial (*e.g.* to reconstitute lyophilized material therein), and the contents of the vial can be removed back into the syringe. After removal of the syringe from the vial, a needle can then be attached and the composition can be administered to a patient. The cap is preferably located inside a seal or cover, such that the seal or cover has to be removed before the cap can be accessed.
- 20

- Where a composition/component is packaged into a syringe, the syringe will not normally have a needle attached to it, although a separate needle may be supplied with the syringe for assembly and use. Safety needles are preferred. 1-inch 23-gauge, 1-inch 25-gauge and 5/8-inch 25-gauge needles are typical. Syringes may be provided with peel-off labels on which the lot number, influenza season and expiration date of the contents may be printed, to facilitate record keeping. The plunger in the syringe preferably has a stopper to prevent the plunger from being accidentally removed during aspiration. The syringes may have a latex rubber cap and/or plunger. Disposable syringes contain a single dose of vaccine. The syringe will generally have a tip cap to seal the tip prior to attachment of a needle, and the tip cap is preferably made of a butyl rubber. If the syringe and needle are packaged separately then the needle is preferably fitted with a butyl rubber shield.
- 25
- 30

- The emulsion may be diluted with a buffer prior to packaging into a vial or a syringe. Typical buffers include: a phosphate buffer; a Tris buffer; a borate buffer; a succinate buffer; a histidine buffer; or a citrate buffer. Dilution can reduce the concentration of the adjuvant's components while retaining their relative proportions *e.g.* to provide a "half-strength" adjuvant.
- 35

Containers may be marked to show a half-dose volume *e.g.* to facilitate delivery to children. For instance, a syringe containing a 0.5ml dose may have a mark showing a 0.25ml volume.

Where a glass container (*e.g.* a syringe or a vial) is used, then it is preferred to use a container made from a borosilicate glass rather than from a soda lime glass.

5 Various antigens can be used with oil-in-water emulsions, including but not limited to: viral antigens, such as viral surface proteins; bacterial antigens, such as protein and/or saccharide antigens; fungal antigens; parasite antigens; and tumor antigens. The invention is particularly useful for vaccines against influenza virus, HIV, hookworm, hepatitis B virus, herpes simplex virus, rabies, respiratory syncytial virus, cytomegalovirus, *Staphylococcus aureus*, chlamydia, SARS coronavirus, varicella
10 zoster virus, *Streptococcus pneumoniae*, *Neisseria meningitidis*, *Mycobacterium tuberculosis*, *Bacillus anthracis*, Epstein Barr virus, human papillomavirus, *etc.* For example:

- Influenza virus antigens. These may take the form of a live virus or an inactivated virus. Where an inactivated virus is used, the vaccine may comprise whole virion, split virion, or purified surface antigens (including hemagglutinin and, usually, also including neuraminidase).
15 Influenza antigens can also be presented in the form of virosomes. The antigens may have any hemagglutinin subtype, selected from H1, H2, H3, H4, H5, H6, H7, H8, H9, H10, H11, H12, H13, H14, H15 and/or H16. Vaccine may include antigen(s) from one or more (*e.g.* 1, 2, 3, 4 or more) influenza virus strains, including influenza A virus and/or influenza B virus, *e.g.* a monovalent A/H5N1 or A/H1N1 vaccine, or a trivalent A/H1N1 + A/H3N2 + B vaccine. The
20 influenza virus may be a reassortant strain, and may have been obtained by reverse genetics techniques [*e.g.* 51-55]. Thus the virus may include one or more RNA segments from a A/PR/8/34 virus (typically 6 segments from A/PR/8/34, with the HA and N segments being from a vaccine strain, *i.e.* a 6:2 reassortant). The viruses used as the source of the antigens can be grown either on eggs (*e.g.* embryonated hen eggs) or on cell culture. Where cell culture is
25 used, the cell substrate will typically be a mammalian cell line, such as MDCK; CHO; 293T; BHK; Vero; MRC-5; PER.C6; WI-38; *etc.* Preferred mammalian cell lines for growing influenza viruses include: MDCK cells [56-59], derived from Madin Darby canine kidney; Vero cells [60-62], derived from African green monkey kidney; or PER.C6 cells [63], derived from human embryonic retinoblasts. Where virus has been grown on a mammalian cell line
30 then the composition will advantageously be free from egg proteins (*e.g.* ovalbumin and ovomucoid) and from chicken DNA, thereby reducing allergenicity. Unit doses of vaccine are typically standardized by reference to hemagglutinin (HA) content, typically measured by SRID. Existing vaccines typically contain about 15µg of HA per strain, although lower doses can be used, particularly when using an adjuvant. Fractional doses such as ½ (*i.e.* 7.5µg HA
35 per strain), ¼ and ⅛ have been used [64,65], as have higher doses (*e.g.* 3x or 9x doses [66,67]). Thus vaccines may include between 0.1 and 150µg of HA per influenza strain, preferably between 0.1 and 50µg *e.g.* 0.1-20µg, 0.1-15µg, 0.1-10µg, 0.1-7.5µg, 0.5-5µg, *etc.*

Particular doses include *e.g.* about 15, about 10, about 7.5, about 5, about 3.8, about 3.75, about 1.9, about 1.5, *etc.* per strain.

- Human immunodeficiency virus, including HIV-1 and HIV-2. The antigen will typically be an envelope antigen.
- 5 • Hepatitis B virus surface antigens. This antigen is preferably obtained by recombinant DNA methods *e.g.* after expression in a *Saccharomyces cerevisiae* yeast. Unlike native viral HBsAg, the recombinant yeast-expressed antigen is non-glycosylated. It can be in the form of substantially-spherical particles (average diameter of about 20nm), including a lipid matrix comprising phospholipids. Unlike native HBsAg particles, the yeast-expressed particles may include phosphatidylinositol. The HBsAg may be from any of subtypes ayw1, ayw2, ayw3, 10 ayw4, ayr, adw2, adw4, adr- and adr+.
- Hookworm, particularly as seen in canines (*Ancylostoma caninum*). This antigen may be recombinant Ac-MTP-1 (astacin-like metalloprotease) and/or an aspartic hemoglobinase (Ac-APR-1), which may be expressed in a baculovirus/insect cell system as a secreted protein 15 [68,69].
- Herpes simplex virus antigens (HSV). A preferred HSV antigen for use with the invention is membrane glycoprotein gD. It is preferred to use gD from a HSV-2 strain ('gD2' antigen). The composition can use a form of gD in which the C-terminal membrane anchor region has been deleted [70] *e.g.* a truncated gD comprising amino acids 1-306 of the natural protein with the 20 addition of a paralog and glutamine at the C-terminus. This form of the protein includes the signal peptide which is cleaved to yield a mature 283 amino acid protein. Deletion of the anchor allows the protein to be prepared in soluble form.
- Human papillomavirus antigens (HPV). Preferred HPV antigens for use with the invention are L1 capsid proteins, which can assemble to form structures known as virus-like particles 25 (VLPs). The VLPs can be produced by recombinant expression of L1 in yeast cells (*e.g.* in *S.cerevisiae*) or in insect cells (*e.g.* in *Spodoptera* cells, such as *S.frugiperda*, or in *Drosophila* cells). For yeast cells, plasmid vectors can carry the L1 gene(s); for insect cells, baculovirus vectors can carry the L1 gene(s). More preferably, the composition includes L1 VLPs from both HPV-16 and HPV-18 strains. This bivalent combination has been shown to be highly effective [71]. In addition to HPV-16 and HPV-18 strains, it is also possible to include L1 30 VLPs from HPV-6 and HPV-11 strains. The use of oncogenic HPV strains is also possible. A vaccine may include between 20-60µg/ml (*e.g.* about 40µg/ml) of L1 per HPV strain.
- Anthrax antigens. Anthrax is caused by *Bacillus anthracis*. Suitable *B.anthraxis* antigens include A-components (lethal factor (LF) and edema factor (EF)), both of which can share a common B-component known as protective antigen (PA). The antigens may optionally be 35 detoxified. Further details can be found in references [72 to 74].

- *S.aureus* antigens. A variety of *S.aureus* antigens are known. Suitable antigens include capsular saccharides (e.g. from a type 5 and/or type 8 strain) and proteins (e.g. IsdB, Hla, etc.). Capsular saccharide antigens are ideally conjugated to a carrier protein.
- 5 • *S.pneumoniae* antigens. A variety of *S.pneumoniae* antigens are known. Suitable antigens include capsular saccharides (e.g. from one or more of serotypes 1, 4, 5, 6B, 7F, 9V, 14, 18C, 19F, and/or 23F) and proteins (e.g. pneumolysin, detoxified pneumolysin, polyhistidine triad protein D (PhtD), etc.). Capsular saccharide antigens are ideally conjugated to a carrier protein.
- 10 • Cancer antigens. A variety of tumour-specific antigens are known. The invention may be used with antigens that elicit an immunotherapeutic response against lung cancer, melanoma, breast cancer, prostate cancer, etc.

A solution of the antigen will normally be mixed with the emulsion e.g. at a 1:1 volume ratio. This mixing can either be performed by a vaccine manufacturer, prior to filling, or can be performed at the point of use, by a healthcare worker.

Pharmaceutical compositions

- 15 Compositions made using the methods of the invention are pharmaceutically acceptable. They may include components in addition to the emulsion and the optional antigen.

The composition may include a preservative such as thiomersal or 2-phenoxyethanol. It is preferred, however, that the vaccine should be substantially free from (i.e. less than 5µg/ml) mercurial material e.g. thiomersal-free [75,76]. Vaccines and components containing no mercury are more preferred.

- 20 The pH of a composition will generally be between 5.0 and 8.1, and more typically between 6.0 and 8.0 e.g. between 6.5 and 7.5. A process of the invention may therefore include a step of adjusting the pH of the vaccine prior to packaging.

- 25 The composition is preferably sterile. The composition is preferably non-pyrogenic e.g. containing <1 EU (endotoxin unit, a standard measure) per dose, and preferably <0.1 EU per dose. The composition is preferably gluten free.

The composition may include material for a single immunization, or may include material for multiple immunizations (i.e. a 'multidose' kit). The inclusion of a preservative is preferred in multidose arrangements.

- 30 Vaccines are typically administered in a dosage volume of about 0.5ml, although a half dose (i.e. about 0.25ml) may be administered to children.

Methods of treatment, and administration of the vaccine

The invention provides kits and compositions prepared using the methods of the invention. The compositions prepared according to the methods of the invention are suitable for administration to

human patients, and the invention provides a method of raising an immune response in a patient, comprising the step of administering such a composition to the patient.

The invention also provides these kits and compositions for use as medicaments.

The invention also provides the use of: (i) an aqueous preparation of an antigen; and (ii) an oil-in-water emulsion prepared according to the invention, in the manufacture of a medicament for raising an immune response in a patient.

The immune response raised by these methods and uses will generally include an antibody response, preferably a protective antibody response.

The compositions can be administered in various ways. The most preferred immunization route is by intramuscular injection (*e.g.* into the arm or leg), but other available routes include subcutaneous injection, intranasal [77-79], oral [80], intradermal [81,82], transcutaneous, transdermal [83], *etc.*

Vaccines prepared according to the invention may be used to treat both children and adults. The patient may be less than 1 year old, 1-5 years old, 5-15 years old, 15-55 years old, or at least 55 years old. The patient may be elderly (*e.g.* ≥ 50 years old, preferably ≥ 65 years), the young (*e.g.* ≤ 5 years old), hospitalized patients, healthcare workers, armed service and military personnel, pregnant women, the chronically ill, immunodeficient patients, and people travelling abroad. The vaccines are not suitable solely for these groups, however, and may be used more generally in a population.

Vaccines of the invention may be administered to patients at substantially the same time as (*e.g.* during the same medical consultation or visit to a healthcare professional) other vaccines.

Intermediate processes

The invention also provides a method for the manufacture of an oil-in-water emulsion, comprising microfluidization of a first emulsion to form a second emulsion and then filtration of the second emulsion. The first emulsion has the characteristics described above.

The invention also provides a method for the manufacture of an oil-in-water emulsion, comprising filtration of a second emulsion, *i.e.* a microfluidized emulsion. The microfluidised emulsion has the characteristics described above.

The invention also provides a method for the manufacture of a vaccine, comprising combining an emulsion with an antigen, where the emulsion has the characteristics described above.

Specific embodiments

Specific embodiments of the present invention include:

- A method for the manufacture of a oil-in-water emulsion comprising squalene, comprising steps of (i) formation of a first emulsion having a first average oil droplet size; (ii) microfluidization of the first emulsion to form a second emulsion having a second average oil

droplet size which is less than the first average oil droplet size; and (iii) filtration of the second emulsion using a hydrophilic membrane.

- A method for the manufacture of a oil-in-water emulsion, comprising steps of (i) formation of a first emulsion having a first average oil droplet size of 5000 nm or less; (ii) microfluidization of the first emulsion to form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size; and (iii) filtration of the second emulsion using a hydrophilic membrane.
- A method for the manufacture of a oil-in-water emulsion, comprising steps of (i) formation of a first emulsion having a first average oil droplet size; (ii) microfluidization of the first emulsion to form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size; and (iii) filtration of the second emulsion using a hydrophilic polyethersulfone membrane.
- A method for the manufacture of an oil-in-water emulsion comprising squalene, the method comprising the step of (i) formation of a first emulsion having a first average oil droplet size using a homogenizer, wherein the first emulsion is formed by circulating the first emulsion components through a homogenizer a plurality of times.
- A method for the manufacture of an oil-in-water emulsion comprising squalene, the method comprising the step of (b) microfluidization of a first emulsion having a first average oil droplet size to form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size, wherein the second emulsion is formed by circulating the second emulsion components by transferring the second emulsion components from a first emulsion container, through a first microfluidization device to a second emulsion container, and then through a second microfluidization device, wherein the first and second microfluidization devices are the same.
- A method for the manufacture of an oil-in-water emulsion comprising: passing a first emulsion having a first average oil droplet size through a microfluidization device to form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size; wherein the microfluidization device comprises an interaction chamber which comprises a plurality of Z-type channels and an auxiliary processing module comprising at least one channel; wherein the auxiliary processing module is positioned downstream of the interaction chamber.
- A method for the manufacture of an oil-in-water emulsion comprising the step of passing a first emulsion having a first average oil droplet size through a microfluidization device to form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size; wherein the microfluidization device comprises an interaction chamber and an auxiliary processing module comprising a plurality of channels.

- A method for the manufacture of an oil-in-water emulsion comprising the step of passing a first emulsion having a first average oil droplet size through a microfluidization device to form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size, wherein the microfluidization device comprises an interaction chamber and wherein the pressure of the emulsion components at the entrance to the interaction chamber is substantially constant for at least 85% of the time during which the emulsion is fed into the microfluidizer.
- A method for the manufacture of a oil-in-water emulsion, comprising the step of formation of a first emulsion having a first average oil droplet size, wherein formation of the first emulsion is carried out under an inert gas, *e.g.* nitrogen, *e.g.* at a pressure of up to 0.5 bar.
- A method for the manufacture of a oil-in-water emulsion, comprising the step of passing a first emulsion having a first average oil droplet size through a microfluidization device to form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size, wherein formation of the second emulsion is carried out under an inert gas, *e.g.* nitrogen, *e.g.* at a pressure of up to 0.5 bar.
- A method for the manufacture of a oil-in-water emulsion, comprising steps of (i) formation of a first emulsion having a first average oil droplet size; (ii) microfluidization of the first emulsion to form a second emulsion having a second average oil droplet size which is less than the first average oil droplet size; (iii) filtration of the second emulsion; (iv) transfer of the oil-in-water emulsion into a sterile flex bag.

General

The term “comprising” encompasses “including” as well as “consisting” *e.g.* a composition “comprising” X may consist exclusively of X or may include something additional *e.g.* X + Y.

The word “substantially” does not exclude “completely” *e.g.* a composition which is “substantially free” from Y may be completely free from Y. Where necessary, the word “substantially” may be omitted from the definition of the invention.

The term “about” in relation to a numerical value *x* is optional and means, for example, $x \pm 10\%$.

Unless specifically stated, a process comprising a step of mixing two or more components does not require any specific order of mixing. Thus components can be mixed in any order. Where there are three components then two components can be combined with each other, and then the combination may be combined with the third component, *etc.*

Where animal (and particularly bovine) materials are used in the culture of cells, they should be obtained from sources that are free from transmissible spongiform encephalopathies (TSEs), and in particular free from bovine spongiform encephalopathy (BSE). Overall, it is preferred to culture cells in the total absence of animal-derived materials.

BRIEF DESCRIPTION OF DRAWINGS

Figure 1 shows a specific example of a homogenizer that can be used to form a first emulsion.

Figure 2 shows detail of a rotor and stator that can be used in such a homogenizer.

Figure 3 shows two pressure profiles for a synchronous intensifier pump mode.

5 Figure 4 shows a Z-type channel interaction chamber.

Figure 5 shows a type I circulation, whereas Figure 6 shows a type II circulation. Containers are labeled as "C" whereas a homogenizer is labeled as "H". Direction and order of fluid movements are shown. In Figure 6 the homogenizer has two input arrows and two output arrows but in reality the homogenizer has a single input channel and a single output channel.

10 **MODES FOR CARRYING OUT THE INVENTION**

A first emulsion comprising squalene, polysorbate 80, sorbitan trioleate and sodium citrate buffer was prepared by homogenization. The first emulsion was homogenized until it had an average oil droplet size of 1200 nm or less and a number of oil droplets having a size $>1.2 \mu\text{m}$ of 5×10^9 /ml or less.

15 The first emulsion was then subject to microfluidization to form a second emulsion. The microfluidization device comprised two synchronous intensifier pumps providing a substantially constant pressure of approximately 700 bar (*i.e.* approximately 10000 psi). The emulsion was passed through the microfluidization device five times. The emulsion was maintained at a temperature of $40 \pm 5^\circ\text{C}$ during microfluidization through the use of a cooling mechanism.

20 Four test runs were carried out. In the first pair of test runs a single channel auxiliary processing module (APM) was positioned upstream of an 8 channel, Z-type interaction chamber (IXC), as recommended by the manufacturer, and the flowrate of the emulsion in the microfluidizer device was 10.2 L/min. In the second pair of test runs, a multi-channel APM was positioned downstream of an 8 channel, Z-type IXC and the flowrate of the emulsion in the microfluidizer device was 11.6 L/min. Both runs were conducted at large scale (250 liters). The results of the four test runs are in Table 1:

25

Order	APM-IXC		IXC-APM	
Run number	1	2	3	4
Average oil droplet size after 1 pass	249	220.9	200.8	200.3
No. of oil droplets with a size $> 1.2\mu\text{m}$ after 2 passes	180.7×10^6	175.4×10^6	54.3×10^6	62.1×10^6
Average oil droplet size after 1 pass	230	224.9	170.9	167.5
No. of oil droplets with a size $> 1.2\mu\text{m}$ after 2 passes	170.2×10^6	139.6×10^6	43.0×10^6	42.8×10^6
Average oil droplet size	218	221.5	166.8	156.7

after 3 passes				
No. of oil droplets with a size > 1.2µm after 3 passes	166.7 x 10 ⁶	164.3 x 10 ⁶	36.7 x 10 ⁶	42.5 x 10 ⁶
Average oil droplet size after 4 passes	215	222.6	154.3	156.8
No. of oil droplets with a size > 1.2µm after 4 passes	127.6 x 10 ⁶	115.6 x 10 ⁶	35.9 x 10 ⁶	43.2 x 10 ⁶

Table 1

As shown in Table 1, the test runs in which the APM was positioned downstream of the IXC produced emulsions with a smaller average particle size and fewer particles with a size > 1.2µm. Moreover, the IXC-APM order reached a particle diameter of ≤200nm after 1 pass whereas this size had not been reached even after 4 passes with the APM-IXC order. Therefore, the positioning of the APM downstream of the Z-type IXC was shown to be advantageous for large-scale manufacture.

It will be understood that the invention has been described by way of example only and modifications may be made whilst remaining within the scope and spirit of the invention.

REFERENCES

- [1] WO90/14837.
- [2] Podda & Del Giudice (2003) *Expert Rev Vaccines* 2:197-203.
- [3] Podda (2001) *Vaccine* 19: 2673-2680.
- [4] *Vaccine Design: The Subunit and Adjuvant Approach* (eds. Powell & Newman) Plenum Press 1995 (ISBN 0-306-44867-X).
- [5] *Vaccine Adjuvants: Preparation Methods and Research Protocols* (Volume 42 of *Methods in Molecular Medicine* series). ISBN: 1-59259-083-7. Ed. O'Hagan.
- [6] *New Generation Vaccines* (eds. Levine *et al.*). 3rd edition, 2004. ISBN 0-8247-4071-8.
- [7] O'Hagan (2007) *Expert Rev Vaccines* 6(5):699-710.
- [8] EP-B-2029170
- [9] Baudner *et al.* (2009) *Pharm Res.* 26(6):1477-85.
- [10] Dupuis *et al.* (1999) *Vaccine* 18:434-9.
- [11] Dupuis *et al.* (2001) *Eur J Immunol* 31:2910-8.
- [12] Burke *et al.* (1994) *J Infect Dis* 170:1110-9.
- [13] *Light Scattering from Polymer Solutions and Nanoparticle Dispersions* (W. Scharl), 2007. ISBN: 978-3-540-71950-2.
- [14] Jafari *et al* (2008) *Food Hydrocolloids* 22:1191-1202
- [15] WO90/04609.
- [16] US-4,618,533
- [17] US-6,193,077
- [18] US-6,495,050
- [19] Chen *et al.* (1999) *Journal of Applied Polymer Science*, 72:1699-1711.
- [20] US-4,413,074
- [21] US-4,432,875

- [22] US-4,340,482
- [23] US-4,473,474
- [24] US-4,473,475
- [25] US-4,673,504
- [26] EP-A-0221046.
- [27] US-4,943,374
- [28] US-6,071,406
- [29] US-4,705,753
- [30] US-5,178,765
- [31] US-6,495,043
- [32] US-6,039,872
- [33] US-5,277,812
- [34] US-5,531,893.
- [35] US-4,964,990
- [36] Wavhal & Fisher (2002) *Journal of Polymer Science Part B: Polymer Physics* 40:2473-88.
- [37] WO2006/044463.
- [38] Espinoza-Gómez *et al.* (2003) *Revista de la Sociedad Química de México* 47:53-57.
- [39] Lidgate *et al* (1992) *Pharmaceutical Research* 9(7):860-863.
- [40] US-2007/0014805.
- [41] WO2007/080308.
- [42] WO2007/052155.
- [43] WO2005/089837.
- [44] US 6,692,468.
- [45] WO00/07647.
- [46] WO99/17820.
- [47] US 5,971,953.
- [48] US 4,060,082.
- [49] EP-A-0520618.
- [50] WO98/01174.
- [51] Hoffmann *et al.* (2002) *Vaccine* 20:3165-3170.
- [52] Subbarao *et al.* (2003) *Virology* 305:192-200.
- [53] Liu *et al.* (2003) *Virology* 314:580-590.
- [54] Ozaki *et al.* (2004) *J. Virol.* 78:1851-1857.
- [55] Webby *et al.* (2004) *Lancet* 363:1099-1103.
- [56] WO97/37000.
- [57] Brands *et al.* (1999) *Dev Biol Stand* 98:93-100.
- [58] Halperin *et al.* (2002) *Vaccine* 20:1240-7.
- [59] Tree *et al.* (2001) *Vaccine* 19:3444-50.
- [60] Kistner *et al.* (1998) *Vaccine* 16:960-8.
- [61] Kistner *et al.* (1999) *Dev Biol Stand* 98:101-110.
- [62] Bruhl *et al.* (2000) *Vaccine* 19:1149-58.
- [63] Pau *et al.* (2001) *Vaccine* 19:2716-21.
- [64] WO01/22992.
- [65] Hehme *et al.* (2004) *Virus Res.* 103(1-2):163-71.
- [66] Treanor *et al.* (1996) *J Infect Dis* 173:1467-70.
- [67] Keitel *et al.* (1996) *Clin Diagn Lab Immunol* 3:507-10.

- [68] Williamson *et al.* (2006) *Infection and Immunity* 74: 961-7.
- [69] Loukas *et al.* (2005) *PLoS Med* 2(10): e295.
- [70] EP-A-0139417.
- [71] Harper *et al.* (2004) *Lancet* 364(9447):1757-65.
- [72] *J Toxicol Clin Toxicol* (2001) 39:85-100.
- [73] Demicheli *et al.* (1998) *Vaccine* 16:880-884.
- [74] Stepanov *et al.* (1996) *J Biotechnol* 44:155-160.
- [75] Banzhoff (2000) *Immunology Letters* 71:91-96.
- [76] WO02/097072.
- [77] Greenbaum *et al.* (2004) *Vaccine* 22:2566-77.
- [78] Zurbriggen *et al.* (2003) *Expert Rev Vaccines* 2:295-304.
- [79] Piascik (2003) *J Am Pharm Assoc (Wash DC)*. 43:728-30.
- [80] Mann *et al.* (2004) *Vaccine* 22:2425-9.
- [81] Halperin *et al.* (1979) *Am J Public Health* 69:1247-50.
- [82] Herbert *et al.* (1979) *J Infect Dis* 140:234-8.
- [83] Chen *et al.* (2003) *Vaccine* 21:2830-6.

CLAIMS

1. A microfluidization apparatus comprising an interaction chamber comprising at least one intensifier pump, and a back pressure chamber, wherein the interaction chamber contains a plurality of fixed geometry channels and wherein the back pressure chamber is located downstream of the interaction chamber.
2. The apparatus of claim 1, wherein the channels in the interaction chamber include a plurality of substantially right-angled corners.
3. The apparatus of claim 2, wherein the channels in the interaction chamber include two substantially right-angled corners.
4. The apparatus of any preceding claim, wherein the fixed geometry of the channels in the interaction chamber is Z-type geometry.
5. The apparatus of any preceding claim, wherein the back pressure chamber comprises at least one fixed geometry channel.
6. The apparatus of claim 5, wherein the back pressure chamber comprises a plurality of fixed geometry channels.
7. The apparatus of any preceding claim, wherein the interaction chamber provides a shear rate in excess of $1 \times 10^6 \text{ s}^{-1}$.