

**CRYSTALLINE FORM OF (2S)-(-)-N-(6-CHLORO-2,3-DIHYDRO-
BENZO[1,4]DIOXIN-2-YLMETHYL)-SULFAMIDE**

FIELD OF THE INVENTION

[0001] The present invention relates to mechanisms for the attaching a reusable cable and housing containing a biosensor for magnetic field based localization to a conductive and adhesive patch assembly having at an electrode used for electrical and mechanical contact with the body surface of a patient. More particularly, the invention relates to a patch and cable attachment mechanism optimized for use in an electrophysiology mapping and ablation system using both biosensors and electrodes for magnetic and impedance or current based localization and mapping of medical devices in the human body.

BACKGROUND OF THE INVENTION

[0002] Many abnormal medical conditions in humans and other mammals have been associated with disease and other aberrations along the lining or walls that define several different body spaces. In order to treat such abnormal conditions of the body spaces, medical device technologies adapted for delivering various therapies to the body spaces using the least invasive means possible.

[0003] As used herein, the term "body space," including derivatives thereof, is intended to mean any cavity within the body which is defined at least in part by a tissue wall. For example, the cardiac chambers, the uterus, the regions of the gastrointestinal tract, and the arterial or venous vessels are all considered illustrative examples of body spaces within the intended meaning.

[0004] The term "vessel," including derivatives thereof, is herein intended to mean any body space which is circumscribed along a length by a tubular tissue wall and which terminates at each of two ends in at least one opening that communicates externally of the body space. For example, the large and small intestines, the vas deferens, the trachea, and the fallopian tubes are all illustrative

examples of vessels within the intended meaning. Blood vessels are also herein considered vessels, including regions of the vascular tree between their branch points. More particularly, the pulmonary veins are vessels within the intended meaning, including the region of the pulmonary veins between the branched portions of their ostia along a left ventricle wall, although the wall tissue defining the ostia typically presents uniquely tapered luminal shapes.

[0005] One means of treating body spaces in a minimally invasive manner is through the use of catheters to reach internal organs and vessels within a body space. Electrode or electrophysiology (EP) catheters have been in common use in medical practice for many years. They are used to stimulate and map electrical activity in the heart and to ablate sites of aberrant electrical activity. In use, the electrode catheter is inserted into a major vein or artery, e.g., the femoral artery, and then guided into the chamber of the heart that is of concern in order to perform mapping and ablation procedures. It is important to know and be able to map the location of the tip or other portions of such electrode catheters within the vessels or other locations in the body space.

[0006] U.S. Pat. Nos. 5,391,199, 5,443,489, 6,788,967 and 6,690,963 to Ben-Haim, whose disclosures are incorporated herein by reference, describe systems wherein the coordinates of an intrabody probe are determined using one or more field sensors, such as a Hall effect device, coils, or other antennae carried on the probe. Such systems are used for generating three-dimensional location information regarding a medical probe or catheter. Preferably, a sensor coil is placed in the catheter and generates signals in response to externally applied magnetic fields. The magnetic fields are generated by three radiator coils, fixed to an external reference frame in known, mutually spaced locations. The amplitudes of the signals generated in response to each of the radiator coil fields are detected and used to compute the location of the sensor coil. Each radiator coil is preferably driven by driver circuitry to generate a field at a known frequency, distinct from that of other radiator coils, so that the signals generated by the

sensor coil may be separated by frequency into components corresponding to the different radiator coils.

[0007] In United States Patent Application No. 2007/0016007 filed by Govari and incorporated herein by reference, a hybrid position sensing system includes a probe adapted to be introduced into a body cavity of a subject. The probe includes a biosensor having a magnetic field transducer and at least one probe electrodes. A control unit is configured to measure position coordinates of the probe using the magnetic field transducer of the biosensor. The control unit also measures an impedance between the at least one probe electrodes and one or more points on a body surface of the subject. Using the measured position coordinates, the control unit calibrates the measured impedance.

[0008] Thus, in such a hybrid magnetic and impedance based systems, a biosensor and electrode must be placed at multiple points on the body surface of the patient. Because the biosensors and the electrical cabling connecting them to the EP mapping system are relatively expensive, it is ideal that the biosensors and the associated cable be reusable. The portion attached to the skin is preferably disposable, therefore, a disposable patch is necessary for affixing the reusable biosensor and possibly a portion of the electrode to the skin of the patient.

[0009] Existing patches comprises one or more stainless steel studs, foam and a conductive adhesive gel that is in contact with the skin of the patient. The matching patch cable in existing systems primarily comprise one or more matching stainless steel snaps into which the studs of the patch mate, a biosensor and the associated electrical cable all housed in an epoxy shell. Existing biosensor cable and patch mechanisms are radiopaque, i.e., the stainless steel snaps and studs appear on fluoroscopy. When multiple snaps are used which is often the case in order to provide a secure and non-rotating connection between the patch and the sensor cable, the multiple snaps do not allow the patch to take

the shape of the body. Also, the patches are often large and conflict with other patches used on the body for ECG, defibrillators, intra-cardiac echograms, etc.

[0010] Prior art mechanisms do not provide an adequate solution. For example, U.S. Patent No. 3,606,881, relates to a disposable patch having a metallic terminal with an enlarged head which permits a squeeze activated clip to be secured around the metallic terminal. U.S. Patent No. 3,829,826 provides a mechanical mechanism for attaching to the standard male metallic snap of the standard ECG patch.

[0011] U.S. Patent No. 4,490,005 relates to a patch in which the central stud is a metal coated non-metallic substrate and which permits rotation of the sensor cable while reducing the effect of rotation on the metal to metal connection. U.S. Patent No. 4,635,642 relates to a disposable pad in which a conductive, preferably, silver coated metallic stud is inserted in order to make electrical conduct with a gel matrix that is in contact with the skin of the patient.

[0012] A similar conductively coated electrically conductive plastic is provided in U.S. Patent No. 5,499,628 as an eyelet that is press fit into a terminal made of a resilient nonmetallic composition such as polypropylene blended with carbon fiber.

[0013] U.S. Patent No. 5,615,674 relates to a clamping contact connection for contacting a fetal scalp probe.

[0014] U.S. Patent No. 5,782,761 relates to a molded electrode one-piece and two-piece constructions for a molded electrode made of a conductive material such as a carbon-filled plastic.

[0015] U.S. Patent No. 6,650,922 relates to an electrode element made of an electrode made of a biodegradable material that is also electro conductive.

[0016] U.S. Patent No. 6,780,065 relates to a device for electrical connection of the power lead to an electrode for use on the skin.

[0017] U. S. Patent No 7,226,299 relates to a circular electrical connector that engages the socket of a female connector that may include a locking device having resilient prongs.

[0018] Design Patent 240,166 relates to a medical electrode with a rectangular cube portion.

[0019] U.S. Patent Application Publication No. 2006/0167354 relates to a system for connecting an electrode to a conductive cable.

[0020] U.S. Patent Application Publication No. 2006/0149146 relates to a device having an electrode for contact with the patient and a pressure sensor.

[0021] U.S. Patent No. 5,978,693 relates to an electrode having a deformation sensor such as a strain gauge.

[0022] It is an object of the present invention to provide a patch that is generally not visible under fluoroscopy.

[0023] It is a further object of the present invention that the patch be capable of being smaller than currently used patches so as to minimize the amount of space used on the skin of the patient and reduce potential conflict with other patches.

[0024] Additionally, it is an object of the present invention to provide a patch and sensor cable that will not rotate as would previous designs utilizing a single snap.

[0025] Furthermore, it is an object of the present invention to have a patch and sensor cable attachment mechanism that is easy to attach.

[0026] Additionally, it is an object of the present invention to have a patch and sensor cable design that could be used for ECG or other instrument systems.

[0027] Finally, it is an object of the present invention to have a patch and sensor cable attachment mechanism that enables repeated reuse of the biosensor and sensor cable without any degradation in performance.

SUMMARY OF THE INVENTION

[0028] The present invention generally relates to a patch and sensor assembly for use in an electrophysiology mapping and ablation system. More specifically, the present invention relates to a patch and sensor assembly in which a magnetic-based biosensor is housed in a reusable portion that connects to the mapping and localization system whereas at least a portion of the electrode is in a disposable patch assembly.

[0029] More specifically the present invention discloses a patch and sensor assembly for use in a device mapping system used to map the location of a device within the body of a patient comprising a reusable portion and a disposable portion. The reusable portion includes a magnetic-based biosensor for providing location information about the location of the device within the body of the patient to the device mapping system, a housing adapted to house the biosensor and a first electrical lead for communicating an electrical signal from the biosensor to the device mapping system. The disposable portion comprises an adhesive hydrogel layer for adhering the electrode to the body of the patient, an electrode layer disposed on the adhesive hydrogel layer, a foam layer disposed on a portion of the electrode layer, a second electrical lead for communicating an electrical signal from the electrode layer to the device mapping system and an

engagement element adapted to detachably receive at least a portion of the housing of the reusable portion.

[0030] In a preferred embodiment the sensor engagement element adapted to detachably receive at least a portion of the housing of the reusable portion wherein the engagement element comprises a first engagement element for engaging an indentation in the top portion of the housing of the reusable portion and a second engagement element for engaging an indentation in the proximal end of the bottom portion of said housing.

[0031] The electrode layer comprises carbon composite, preferably carbon fibers in polyvinyl chloride (PVC) coated on at least one dimension with a metallic material such as silver chloride. Preferably, an additional layer of silver is disposed on the silver chloride.

[0032] The disposable portion of the patch and sensor assembly further includes a second foam layer disposed on the first foam layer and comprising at least one indentation adapted to receive the first electrical lead. The second electrical lead comprises a plurality of wires having a distal end and a proximal end and the distal ends of the plurality of wires are arrayed in a fan and positioned between the electrode layer and the foam layer.

[0033] The first foam layer is comprised of polyethylene foam with a medical grade acrylic pressure sensitive adhesive on the patient facing side. The first foam layer has an opening for receiving a portion of the sensor engagement element.

[0034] The reusable portion of the patch and sensor assembly further comprises a strain relief element for reducing mechanical strain on the connection between the biosensor and the sensor cable.

[0035] The sensor engagement element may be made of a polycarbonate, preferably Lexan® polycarbonate.

[0036] The disposable portion of the patch and sensor assembly further includes a release liner on which the hydrogel layer is disposed. The release liner is preferably made of polyethylene terephthalate (PET) with a silicone coating on the side facing the hydrogel layer.

[0037] The electrical leads of the disposable patch assembly and the reusable sensor assembly are connected to a device mapping and localization system such as the Carto® system.

BRIEF DESCRIPTION OF THE DRAWINGS

[0038] FIG. 1 is a planar view of the top of the patch and sensor cable assembly in accordance with a first embodiment of the present invention.

[0039] FIG. 2 is a partial cross-sectional view of the patch and sensor cable assembly of FIG. 1 through line A-A.

[0040] FIG. 3 is a perspective view of the strain relief element for use in patch and sensor cable assembly of FIG. 1.

[0041] FIG. 4 is a perspective view of a second embodiment of a patch and sensor cable connector in accordance with the present invention.

[0042] FIG. 5 is a planar view of the top of a further embodiment of a patch and sensor cable assembly in accordance with the present invention.

[0043] FIG. 6 is a cross-sectional view of the embodiment of the patch and sensor cable assembly of FIG. 5.

[0044] FIG. 7 is a planar view of another embodiment of the disposable portion of a patch and sensor cable assembly in accordance with the present invention.

[0045] FIG. 8 is an exploded view of the embodiment of the disposable portion of the patch and sensor cable assembly of FIG. 7.

[0046] FIG. 9 is a cross-sectional view of the embodiment of the disposable portion of the patch and sensor cable assembly of FIG. 7 through line L-L.

[0047] FIG. 10 is a planar top view of the reusable sensor cable assembly for use in the embodiment of patch assembly of FIG. 7

[0048] FIG. 11 is a cross-sectional view of the reusable sensor cable assembly through line A-A of FIG. 10.

DETAILED DESCRIPTION OF THE INVENTION

[0049] Referring to the drawings, FIG. 1 depicts a planar view of an embodiment of the patch and sensor cable assembly in accordance with the present invention. As shown in FIG. 1, the patch and sensor assembly **100** comprises two major components: a patch assembly **110** and a sensor cable assembly **130**. Sensor cable assembly **130** comprises a sensor housing **122** that is adapted to connect to the patch assembly **110** and a sensor cable **124**. In FIG. 1 the connection between the sensor housing **122** and patch assembly **110** is a snap-fit based on the engagement of ridge **123** of sensor housing **122** and the lip of engagement element **114** of patch assembly **110**. Patch assembly **110** comprises a foam disk **112** having a plurality of indentations **113** adapted to receive the sensor cable **124**. The patch assembly in FIG. 1 is shown with three such indentations enabling a user to attach the sensor cable assembly in one of three positions even after the disposable patch assembly has been placed on the patient. One or more such

indentations 113 may be used with the upper limit constrained by the ability of the remaining engagement element 114 to securely engage the ridge 123 of sensor housing 122. Engagement element 114 contains indentations that match those in foam disk 112. The foam used to form foam disk 112 may be any suitable material such as thermofoam, any elastomers like rubber, santoprene, polyurethane etc. and is preferably thermofoam.

[0050] FIG. 2 depicts a partial cross-section of the patch and sensor assembly of FIG. 1 taken through line A-A. Foam disk 112 rests on a carbon film disk 116 coated with a layer of silver chloride on both sides. Carbon film disk 116 is approximately 0.5 mm in thickness and the layer of silver chloride is approximately 0.1 mm in thickness. Other thicknesses of carbon film disk 116 and silver chloride coating may be used without departing from the spirit of the invention. On the patient facing side of carbon film disk 116 is a hydrogel layer 117. Hydrogel layer 117 is comprised of a conductive gel medium, which also has adhesive properties to the skin, preferably a hydrogel being a mix of Silver/Silver Chloride with water based compound and is approximately 1mm mm in thickness.

[0051] Foam disk 112, carbon film disk 116 and the hydrogel layer 117 generally have approximately the same diameter which should be large enough to provide a secure attachment to the body surface of the patient and is preferably between 4 cm and 16 cm. The only other component of patch assembly 110 is the engagement element 114. Patch assembly 110 comprises only low-cost components in order to increase the disposability of the patch assembly in this embodiment.

[0052] The other component of the patch and sensor assembly 100 depicted in FIGS. 1 and 2 is the reusable sensor cable assembly 130. The reusable sensor cable assembly 130 comprises the aforementioned sensor housing 122. Sensor housing 122 is a two-piece design in which upper housing portion 122a is design

to fit together with lower housing portion 122b. Lower housing portion **122b** contains the ridge **123** that engages engagement element **114** of the patch assembly although this ridge could be disposed on the upper housing portion without departing from the spirit of the present invention. Sensor housing **122** is comprised of a polymer such as ABS, nylon, polypropylene or other suitable polymer known in the art and is preferably made from polypropylene. Sensor housing **122** could be comprised of more than two parts without departing from the spirit of the invention.

[0053] Sensor cable assembly **130** further comprises the sensor cable **124** which comprises a conductive ACL cable made of a conductive and flexible material, preferably 28 gauge braided copper wire, three twisted pair conductors for the biosensor has along with two Kevlar fibers for added strength inside a polymeric outer sheath. One wire in sensor cable **124** is welded or bonded using a conductive epoxy to biosensor **126**.

[0054] Sensor cable assembly **130** further comprises active current location (ACL) disk **134** which may be made of a suitably conductive material and is preferably a generally circular carbon disk coated with silver chloride. Gold or platinum may also be used instead of silver chloride for the coating and the carbon disk could be replaced with a polymer such as ABS or polycarbonate with or without carbon fibers embedded therein. ACL cable **136** is attached to ACL sensor **134** using a suitable conductive epoxy, preferably any epoxy preferably embedded silver particles. In use, current flowing through the patient is conducted through the hydrogel layer **117**, carbon film disk **116** to ACL sensor **134** and through ACL cable **136** to the localization and mapping system that uses the ACL information to perform localization and mapping functions in accordance with United States Patent Application No. 2007/0016007 filed by Govari and incorporated herein by reference or other such similar system.

[0055] Sensor cable assembly **130** further comprises biosensor **126** which is a biosensor implemented in accordance with one or more of U.S. Pat. Nos. 5,391,199, 5,443,489, 6,788,967 and 6,690,963 to Ben-Haim, whose disclosures are incorporated herein by reference. Magnetic field based information from biosensor **126** is an electrical current induced by the magnetic field in which the patient is placed and is used in a manner similar to that used in the Carto™ EP mapping systems manufactured and sold by Biosense Webster, Inc. The electrical current from biosensor **126** is conducted through three twisted pair conductors of the sensor cable assembly **130** to biosensor cable which connects to an EP mapping and localization system where the information is used. Biosensor **126** is housed in biosensor housing **138**. Isolation layer **139** is thin piece of plastic material preferably polypropylene, ABS or polycarbonate which isolates the 4KV defibrillation pulse from ACL wire to the biosensor **126**.

[0056] As can be seen from FIGS. 1 and 2, it is advantageous to have the biosensor **126**, ACL sensor **114** and the sensor cable **124** in the reusable sensor cable assembly **130** in order to reduce the cost of the disposable patch assembly **110**. The sensor cable assembly **130** is connected to the patch assembly using an easy to operate snap-fit connection. This force will hold the re-usable to the disposable part. The sensor cable assembly may be positioned in one of several orientations around the central axis of the patch assembly but rotation is prohibited by the combination of the engagement element **114** and the matching indentations in the foam disk **112**.

[0057] FIG. 3 depicts a perspective view of the sensor housing **122** showing the upper sensor housing **122a**, the lower sensor housing **122b** and the ridge **123**. Sensor assembly **122** preferably includes the strain relief element **125** but may also be substantially circular without such element. Strain relief element **125** may be integral with sensor housing **122** or may comprise a separate polymeric sleeve that covers a portion of sensor cable **124**.

[0058] FIG. 4 depicts a perspective view of a further embodiment of a patch and sensor cable connector in accordance with the present invention. Sensor housing **222** has a plurality of indentations **223** which are adapted to engage under flexible engagement members **215** which form a portion of engagement element **214**. As in the previous embodiment described above, sensor housing **222** forms a part of a sensor cable assembly **230** and engagement element **214** form a part of the patch assembly **110**. Engagement element **214** is made from a polymer that is sufficiently flexible to enable flexible engagement members **215** to be pushed toward the periphery while the sensor cable assembly **230** is inserted into the engagement element **214**. The snap of re-useable to disposable part is held using a cantilever beam tab. The disposable part will have the lever which deflects during the snapping operation. The normal forces exerted from the cantilever beam hold the snap together.

[0059] FIGS. 5 and 6 depict a planar top view and cross sectional view of another embodiment of a patch and sensor assembly in accordance with the present invention. Patch and sensor assembly **300** comprises two portions: a patch cable assembly **310** and a sensor cable assembly **330**. Patch cable assembly **310** comprises a foam disk **312** having indentation **313** (with portions **313a** and **313b**) to accommodate the sensor housing **322** and engagement element **314**. Two separate cables are used to connect the biosensor and ACL sensor to the mapping and localization system. ACL cable **334** is used to connect the ACL sensor layer **316** to the system for transmittal of current information to the localization system. Alternatively, the ACL cable **334** can be substantially shorter than the length necessary to reach to the mapping and localization system and can be adapted to have a fitting that is designed to connect to a mated fitting on a cable that is collinear with the sensor cable. In the configuration, the fitting on the ACL cable is attached to the fitting on the additional cable that forms part of the sensor cable. In this manner, a substantial length of the ACL cable becomes part of the reusable sensor cable assembly. ACL cable **334** is stranded **28** gauge wire that is sandwiched between the foam disk **312** and the ACL sensor layer **316**. ACL

sensor layer **316** is a silver chloride coated carbon film of approximately 1mm with a silver chloride coating of approximately 0.5 mm. Below the ACL sensor layer **316** is a hydrogel layer **317** substantially the same as the one described above with respect to the other embodiment.

[0060] Figure 5 has the snap feature in the form of three legs. This feature also works similar to principle of cantilever beam of Fig. 4. The legs deflect on the reusable part conforming to the opening on the disposable side. When snapped the beam expands providing the normal force to hold the two parts together.

[0061] Sensor cable assembly **330** comprises the engagement element **314**, sensor housing **322** with biosensor **326** mounted inside. Sensor cable **324** is used to connect the biosensor **326** that provides magnetic based localization information to the system. Sensor cable **324** is a 48 gauge braided copper wire coated with a protective polymer with an exposed end welded or bonded, preferably using a conductive epoxy to the biosensor **326**. Strain relief element **325** covers a portion of the sensor cable **324** in order to reduce mechanical stress on the connection of the sensor cable to the biosensor and sensor housing. Biosensor **326** is substantially similar to biosensor **126** for the embodiment described above. Engagement element **314** is a mechanical snap designed to engage patch cable assembly **310**. Engagement element **314** has moveable elements **314a** and **314b** that are depressed in order to release and/or engage the engagement element onto the patch assembly.

[0062] An alternative embodiment for a patch and sensor cable assembly in accordance with the present invention is depicted in FIGS. 7-11. FIGS. 7-9 depict the disposable patch cable assembly **410** comprising hydrogel layer **417** which is exposed for adhesion to the patient after removal of release liner **411**. Hydrogel layer **417** is preferably a hydrogel such as Amgel AG603 and is approximately 0.025 inch in thickness. Release liner **411** is approximately 4.5 inches square and is comprised of 0.005 inch thick polyethylene terephthalate (PET) with a silicone

coating on the side facing the hydrogel layer **417**. Above hydrogel layer **417** is ACL sensor layer **416** which is a carbon silver chloride disk. More specifically, ACL sensor layer **416** has a base material of conductive carbon and medical grade polyvinyl chloride (PVC) of approximately 0.004 inch in thickness with a patient facing (bottom) coating of silver-chloride and a top coating of silver both approximately 0.001 inch in thickness.

[0063] In electrical contact with ACL sensor layer **416** is the distal end of the cable assembly **434** which is placed under sensor engagement element **414**. Cable assembly **434** is comprised of a 19 strands of tin plated copper wire which are stripped at the distal end **434a** and fanned out to provide contact with the top side of the ACL sensor layer **416**. Cable assembly **434** should be covered with a jacket and meet requirements of all ANSI standards related to cables for medical devices. The proximal end of the cable assembly **434b** should have a socket assembly which is adapted to connect to the mapping and localization system or an interface cable for such a system for which it is adapted. The overall length of cable assembly **434** is approximately 36 inches. Sensor engagement element **414** is made of Lexan® material or other polycarbonate material and is adapted to receive the distal end of the sensor cable assembly which is adapted to fit under lip **414a** and be secured by prongs **414b**. Foam disk **412a** is a circular disk of approximately 0.005 inch thick white polyethylene foam with a medical grade acrylic pressure sensitive adhesive on its patient facing side and adheres to sensor engagement element **414**, the distal end of the cable assembly **434** and a portion of the ACL sensor layer **416**. Foam disk **412b** is a circular foam disk with a plurality of indentations for structural integrity and one for placement of the sensor cable **424**. Foam disk **412b** has an adhesive on its patient facing side that causes it to adhere to the top side of foam disk **412a**. Foam disk **412b** is comprised of white volara type-A closed cell polyethylene foam or an equivalent.

[0064] FIGS. 10-11 depict the reusable sensor cable assembly **430** for use with the patch cable assembly of FIGS. 7-9. Sensor cable assembly **430** comprises the

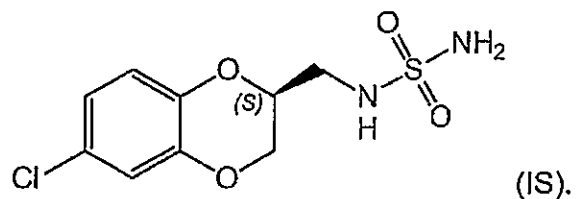
engagement elements **414c** and **414d**, sensor housing **422** with biosensor **426** mounted inside. Sensor cable **424** is used to connect the biosensor **426** that provides magnetic based localization information to the mapping and localization system (such as the Carto® system described herein) through a connector **428**. Sensor cable **424** is a 48 gauge braided copper wire coated with a protective polymer with an exposed end welded or bonded, preferably using a conductive epoxy **427** to the biosensor **426**. Strain relief element **425** covers a portion of the sensor cable **424** in order to reduce mechanical stress on the connection of the sensor cable to the biosensor and sensor housing. Biosensor **426** is substantially similar to biosensor **126** for the embodiment described above. Engagement element **414c** is an indentation in the top of the sensor housing substantially around the circumference of the housing and which is designed to engage the lip **414a** of sensor engagement element of the patch cable assembly **410**. Engagement element **414b** is an indentation in the proximal end of the bottom of the sensor housing **422** that are adapted to engage prongs **414b** of patch cable assembly **410** in a snap-fit manner.

[0065] The preceding description has been presented with reference to presently preferred embodiments of the invention. Workers skilled in the art and technology to which this invention pertains will appreciate that alterations and changes in the described structure may be practiced without meaningfully departing from the principal, spirit and scope of this invention.

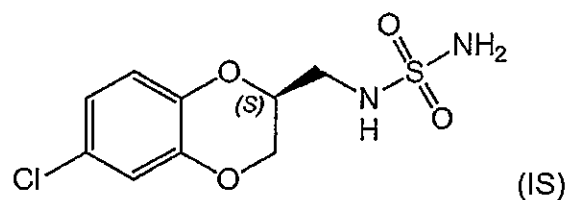
[0066] Accordingly, the foregoing description should not be read as pertaining only to the precise structures described and illustrated in the accompanying drawings, but rather should be read consistent with and as support to the following claims which are to have their fullest and fair scope.

We claim:

1. Crystalline form (IS-VI) of a compound of formula (IS)



2. A crystalline form of a compound of formula (IS)



comprising the following powder X-ray diffraction peaks:

Pos.[° 2θ.]	d-spacing[Å]
13.07	6.78
18.53	4.79
19.64	4.52
19.91	4.46
21.15	4.20
22.09	4.02

3. A crystalline form as in Claim 2, comprising the following powder X-ray diffraction peaks:

Pos.[° 2θ.]	d-spacing[Å]
6.54	13.51
13.07	6.78
16.50	5.37
18.53	4.79
19.64	4.52
19.91	4.46
20.17	4.40
21.15	4.20
22.09	4.02
22.52	3.95
23.51	3.79

26.28	3.39
27.56	3.24
28.20	3.17
33.60	2.67

4. A pharmaceutical composition comprising a pharmaceutically acceptable carrier and a crystalline form as in Claim 1.
5. A pharmaceutical composition made by mixing a crystalline form as in Claim 1 and a pharmaceutically acceptable carrier.
6. A process for making a pharmaceutical composition comprising mixing a crystalline form as in Claim 1 and a pharmaceutically acceptable carrier.
7. The use of a crystalline form as in Claim 1 for the preparation of a medicament for treating: (a) anxiety and related disorders; (b) bipolar depression (c) mania; (d) depression; (e) epilepsy and related disorders; (f) epileptogenesis; (g) glucose related disorders; (h) lipid related disorders; (i) migraine; (j) obesity; (k) pain; (l) substance abuse and (m) for neuroprotection, in a subject in need thereof.
8. A crystalline form as in Claim 1, wherein the crystalline form exhibits a peak temperature of about 101.5°C, as measured by differential scanning calorimetry.
9. A crystalline form as in Claim 1, wherein the crystalline form exhibits a heat of melting of about 96.2J/g, as measured by differential scanning calorimetry.
10. A crystalline form as in Claim 1, wherein the crystalline form is a non-hydrate.
11. A crystalline form as in Claim 1, wherein the crystalline form is non-hygroscopic.

12. A crystalline form as in Claim 1, wherein the crystalline form is non-hygroscopic and a non-hydrate.