

CONNECTOR DEVICE FOR A NEGATIVE PRESSURE WOUND THERAPY SYSTEM

TECHNICAL FIELD

- 5 The present disclosure relates to a connector device. More specifically, the present disclosure relates to a connector device for a negative pressure wound therapy system. Moreover, the present disclosure relates to a method of connecting the connector device to a wound side assembly.

10 BACKGROUND

Some types of wound are advantageously treated by so called negative pressure wound therapy. In the field of negative pressure wound therapy, a negative pressure is applied to the wound for a relatively long time and it has been realized that the healing process may be expedited by using such wound therapy.

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To this end, a negative pressure wound therapy system may be used which generally comprises a wound cover member and an underlying wound filler that is adapted to be placed over a wound. The system further generally comprises a negative pressure source, such as a vacuum pump, which is in fluid

- 20 communication with the wound site via a suction interface attached to the wound cover member and a fluid communication assembly comprising fluid conduit(s).

The negative pressure source furthermore generally comprises a canister for collection of wound exudate removed from the wound site via the fluid communication assembly.

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For convenient assembly of the negative pressure source with a fluid communication assembly, the negative pressure source may as well be provided with fluid conduit(s) comprising coupling means in the end portion, e.g. an end portion distal to the portion connected to the negative pressure source, allowing

- 30 coupling connection with an end portion of the fluid conduit(s) of the fluid

communication assembly, e.g. an end portion distal to the portion of the fluid conduit(s) connected to the suction interface, via corresponding, such as mating, coupling means.

- 5 Negative pressure wound therapy systems may generally be divided into two categories, single conduit devices and multiple conduit devices. A single conduit device comprises a single suction conduit providing the suction interface and consequently the wound site with a negative pressure. This single conduit also removes and transports wound exudate from the wound site to a negative
10 pressure source. The negative pressure is normally a pump and is also provided with a canister to collect exudate. The multiple conduit devices additionally comprise one conduit supplying gas, such as air, to the suction interface in order to provide flushing and removal of wound exudate from the suction conduit, this gas flow may be air circulated from the pump.

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- In negative pressure wound therapy systems, there is in principle always a static pressure difference introduced by gravity between the pressure inside the canister and the pressure at the wound site. This is due to the height difference between the negative pressure wound therapy device and the wound site and a liquid
20 column of exudate often present in the suction conduits. A problem relating to a change in the static pressure, decrease or increase, is due to the liquid column phenomena and may affect the ability to provide the correct level of negative pressure at the wound site when compared to the pressure at the negative pressure source canister. This issue may have undesired consequences on the
25 pressure at the wound site. One possible consequence is pooling of exudate, which in turn can cause leakage due to detachment of the wound cover and even maceration of surrounding skin.

- There is also a need for quick disconnection of the conduits with the dressing and
30 suction interface still in place, for instance when the patient should take a shower, or undergo certain examinations, such as an MRI or X ray. Furthermore, there is

still a need to avoid imprints that could be caused by non-soft components in the sensitive skin close to wound site.

SUMMARY

- 5 One object of the present disclosure is to provide a connector device for a negative pressure wound treatment system allowing the provision of a correct level of negative pressure at the wound site with a flexible, safe and convenient system.
- 10 This and other objects of the present disclosure may be achieved by a connector device according to the appended claims.

As such, the present disclosure relates to a connector device for a negative pressure wound therapy system. The connector device comprises a connector housing, a fluid outlet connected to the connector housing, an air feeding port, an air filter and coupling means. The fluid outlet is adapted to be connected to a negative pressure source. The connector device is adapted to be engaged with a wound side connector of a wound side assembly by means of the coupling means. The wound side assembly comprises a fluid removing conduit and an air supplying conduit, wherein a portion of each one of the fluid removing conduit and the air supplying conduit is connected to the wound side connector. The connector device is such that when the connector device is engaged with the wound side connector, the fluid removing conduit is fluidly connected to the fluid outlet and the air supplying conduit is fluidly connected to the air feeding port such that air ambient of the connector device can be fed to the air supplying conduit via the air feeding port and the air filter.

By *filter* herein is meant a material, such as a porous material, through which air may pass but which captures elements, such as particles, bacteria and spores from the ambient air. The filter may be a three-dimensional porous material component, such as, a cylindrical, rectangular or square shaped porous material

component. For example, the porous material may be a sintered plastic, wherein the air flow through a sintered plastic material may be controlled by adapting the pore size (porosity) thereof.

- 5 The connector housing is provided with an air feeding port to there through allow ambient air to enter the air supplying conduit of the wound side assembly when coupled to the connector device and thereby provide a flushing functionality to the fluid removing conduit.
- 10 The fact that the connector device allows air to be fed via the air filter and the air feeding port ensures that ambient air enters the connector housing in a controlled and continuous manner and allows e.g. particles and potentially harmful bacteria to be captured.
- 15 The wound side assembly may be connectable to a suction interface being attached or being attachable to a wound cover material. The fluid removing conduit is adapted to remove fluid from a wound, through an opening provided in the wound cover material and through the suction interface attached to the wound cover material. The air supplying conduit is adapted to supply air through at least a
20 portion of the suction interface and into the fluid removing conduit to provide flushing of the fluid removing conduit.

The connector device is thus intended to be attached at a distance from a wound site, with the wound side assembly as an intermediate module. This has found to
25 be advantageous in that assemble or disassemble of the modules, i.e. the wound side assembly and the connector device, are effected at a distance from the wound site, which is more convenient for both the patient and the person performing assemble and/or disassemble of the connector device. Additionally, the risk of imprints from the connector on the patient's skin is reduced. To perform the
30 assemble or disassemble of the modules at a distance from the suction interface is also safer in terms of decreased risk of infection and a reduced risk to in other ways harm to the wound.

Optionally, the connector device comprises an air feeding conduit comprising the air feeding port and an air inlet opening. The air feeding conduit is an integrated part of the connector housing.

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Optionally, the air filter is completely integrated within air feeding conduit and the connector housing.

Optionally, the air filter is provided within an air filter housing provided with at least one air inlet opening allowing air to flow through the air filter. Optionally, the air filter housing is provided with at least two or at least three air inlet openings to ensure sufficient air flow.

The air filter housing may either be provided as an integrated part of the connector housing or as a separate compartment.

The fact that the air feeding conduit is an integrated part of the connector housing or that the air filter is provided within an air filter housing is specifically an advantage for a connector device according to the present disclosure due to the modularity of the system and that the connector device is an intermediate module intended to be positioned at a distance between the patient and the negative pressure source and thus exposed to the surroundings. For example, in embodiments of the present disclosure, the connector device is positioned at a distance of at least 5 cm, such as 10 cm, from the wound side connector. For example, the connector device may be positioned at a distance of between 5 to 20 cm from the wound side connector. In embodiments of the present disclosure, the connector device is positioned at a relatively equal distance between the patient and the negative pressure source, which may typically be about 60 to 80 cm from the wound side connector. The risk of a separate part or a non-protected air filter getting caught somewhere or being obstructed has been found particularly important for this type of connector device.

The air filter situated in a connector at a distance from the wound site cause less risk of obstruction, such as by wound cover films or adhesive tapes or similar unintentionally applied on top of it for fixation or underneath it for padding to avoid imprints.

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Optionally, the connector housing has a connector housing device side and a connector housing coupling side, where the connector device is adapted to be connected to the wound side assembly at the connector housing coupling side. The air inlet opening is provided on the connector housing device side.

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Optionally, the fluid outlet is also provided on the connector housing device side.

Optionally, the connector housing device side is positioned on the opposite side of the connector housing coupling side.

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The connector device may be provided as a separate part interconnecting the wound side assembly and the negative pressure source via a conduit extending from the negative pressure source. The connector device may also be provided at the end of a fluid conduit(s) extending from, or adapted to connect to, the negative
20 pressure source.

When the connector device is supplied as a separate part, i.e. without any conduits connected thereto, it may be provided device side coupling means at the connector housing device side for connection of the connector device with a
25 negative source side assembly comprising a fluid removing conduit being connected to a negative pressure source side connector.

The fact that the air inlet opening is provided on the connector housing device side implies that the air inlet opening is provided on a side of the connector housing,
30 and thus not on a part of the connector housing facing upwards or downwards when placed on a surface, such as a bed, during use, which reduces the risk for obstruction of the air inlet opening. An advantage coherent with air inlet opening

being provided at the same side as the fluid outlet is that the proximity to a protruding part further minimizes the risk for obstructing the air inlet opening.

Optionally, the connector housing device side may be positioned on the opposite
5 side of the connector housing coupling side.

Optionally, the air inlet opening is arranged at a radial distance from the fluid outlet.

10 The fact that the connector housing device side, and thus the air inlet opening, is provided on the opposite side of the connector housing coupling side additionally to the advantages described above, ensures a straight fluid and air passage, minimizing the risk for obstruction of the air inlet opening. That the air inlet opening is arranged at a radial distance from the fluid outlet also minimizes the risk of
15 obstruction of the air inlet opening and possible protruding parts at the connector device.

Optionally, the air filter is at least partly located within said connector housing so that maximum 2 cm of the air filter protrudes outside the connector housing, or
20 maximum 1 cm of the air filter protrudes outside the connector housing, or maximum 0.5 cm of the air filter protrudes outside the connector housing.

Optionally, a fluid conduit is connected to the fluid outlet. Optionally, a portion of the fluid conduit, being a portion opposite to the side connected to the connector
25 device, is connected to a device side connector comprising coupling means adapted to be connected to a negative pressure source side connector.

Optionally, the air filter provides an air leakage of between 0.5 to 70 ml/min at a pressure of 120 mmHg, or between 1 to 40 ml/min at a pressure of 120 mmHg.

Optionally, the air filter provides an air leakage of between 10ml/min to 70 ml/min at a pressure of 120 mmHg, or between 15ml/min to 55 ml/min at a pressure of 120 mmHg.

- 5 At high air leakage rates, the pump has to work harder, which in turn can have negative effects on noise and battery consumption. It is also more difficult to maintain a controlled therapy pressure at the wound site. At lower air leakage rates, efficient exudate removal is difficult to obtain. It is therefore important to find a good balance between those different parameters.

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- In embodiments of the present disclosure, the air filter may advantageously be adapted to provide an air leakage of about 1 to 5 ml/min, for example about 1.5 to 2.5 ml/min, such as about 2 ml/min, thereby reducing noise and battery. An air leakage rate in the range of about 1 to 5 ml/min may in particular be advantageous
- 15 in case a relatively small pump is being used, e.g. a pump with a suction capacity of up to around 1.0 liter/min (e.g. suction capacity between 0.1 to 1.0 liter/min, such as 0.5 liter/min) and with relatively limited battery capacity.

- In embodiments of the present disclosure, in particular when a pump with a
- 20 suction capacity of more than 1.0 liter/min being used, e.g. a suction capacity of from 1.5 to 5 liter/min, the air filter may be adapted to provide an air leakage of 10 to 30 ml/min, for example 15 to 25 ml/min, such about 20 ml/min.

- The continuous and controlled inflow of air allows the creation of an air flow well
- 25 defined at all values of relevant negative pressure minimizing the problems of liquid column phenomena. The connector device according to the present disclosure thus provides an improved and secure negative pressure wound therapy which is simple to handle and requires less supervision.

- 30 Optionally, the connector device coupling means are adapted to form a snap-on, threaded, luer-lock or bayonet engagement with the wound side connector.

Optionally, the connector device coupling means are adapted to form a release snap-on, threaded or bayonet engagement with the wound side connector.

A second aspect of the present disclosure relates to a branched connector device.

The branched connector device comprises a branched conduit which in turn

5 comprises a first and at least a second branch portion. The branched connector device further comprises a connector device according the first aspect of the present disclosure, wherein the first branch portion is connected to the fluid outlet of the connector device.

10 Optionally, a portion of the second branch portion, being a portion opposite to the side of the conduit connected to the connector device, is connected to a device side connector comprising coupling means adapted to be connected to a negative pressure source side connector.

15 Optionally, the branched connector device comprises a second connector device comprising a second connector housing and coupling means and a second fluid outlet connected to the second connector housing and wherein the second branch portion is connected to the second fluid outlet.

20 The fact that the branched connector device comprises a second connector device comprising coupling means allows for easy connection to more than one fluid communication assembly, while providing air supply and flushing functionality to the fluid removing conduit(s).

25 The second connector device may, for example, by means of second coupling means be connected to a second wound side assembly comprising a fluid removing conduit adapted to connect to a suction interface and to remove fluid therethrough.

30 Such a branched connector device allows for simple treatment of larger wounds or multiple wounds.

Optionally, the second connector device comprises a second air feeding port.

Such a branched connector device allows connection of one single negative pressure source to at least two wound sites via two wound fluid communication
5 assemblies, each comprising a fluid removing conduit and an air supplying conduit, and each being able to connect to a suction interface, ensuring the provision of a correct level of negative pressure at each of the wound sites.

The capacity of the branched connector device to maintain the correct level of
10 negative pressure at each of the wound sites while only needing one single negative pressure source and without constantly needing to adjust the negative pressure from each of the negative pressure sources to ensure correct levels at the wound size leads to an improved and secure wound treatment which is simple to handle and requires less supervision.

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Optionally, a second conduit is connected to the second air feeding port.

Optionally, the second conduit and the branched conduit are provided with coupling means at the end portions for coupling connection with, for example, a
20 further connector device provided with a fluid outlet and an air feeding port comprising an air filter, such as a connector device according to the first aspect of the present disclosure. This provides a fluid passage to the negative pressure source while ensuring an ambient air supply to the second air feeding port even though connected to a second conduit.

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Optionally, the second connector device is a connector device according the first aspect of the present disclosure.

Optionally, the branched connector device is a Y-connector device.

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Optionally, the branched conduit comprises a third branch portion which is connected to a third fluid outlet of a third connector device.

A third aspect of the disclosure relates to a method comprising providing a connector device according to the first aspect of the present disclosure, connecting the connector device to a wound side assembly comprising a fluid removing conduit and an air supplying conduit, by further connecting said fluid
5 removing conduit to said first fluid outlet and said air supplying conduit to said air feeding port via said connector housing.

Optionally, the method further comprises applying negative pressure to a suction interface via the fluid outlet and the fluid removing conduit.

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BRIEF DESCRIPTION OF THE DRAWINGS

The various aspects of the present disclosure, including its particular features and advantages will be readily understood from the following detailed description and the accompanying drawings, in which:

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Fig. 1 illustrates an embodiment of a negative pressure wound therapy system;
Fig. 2a illustrates a perspective view of an embodiment of a connector device;
Fig. 2b illustrates a cross sectional view of the connector device according to Fig. 2a;

20 Fig. 3 illustrates a perspective view of an embodiment of a Y connector device and exemplified connecting parts, and

Fig. 4 illustrates a perspective view of an embodiment of a branched connector device.

25 DETAILED DESCRIPTION

Fig. 1 illustrates a negative pressure wound therapy system 18. The purpose of a negative pressure wound therapy system 18 is to obtain a negative pressure in the area of a wound 9.

30 The negative pressure wound therapy system illustrated in Fig. 1 comprises a negative pressure source 23, which in Fig. 1 is in the form of a vacuum pump. The

negative pressure wound therapy system 18 according to Fig. 1 includes a wound cover member 24, attached over and covering the wound 9 and a wound filler 27, such as a foam or a gauze, placed on or in the wound to be treated by the negative pressure wound therapy system.

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The wound cover member 24 is generally adapted to be attached to the skin surrounding the wound. Purely by way of example, the wound cover member 24 may comprise a wound cover film. The wound cover member 24 may preferably be attached to the skin by an adhesive. Examples of adhesives that may be used
10 include, but are not limited to, acrylic adhesives and/or silicone gel adhesives.

Moreover, the negative pressure wound therapy system illustrated in Fig. 1 includes a suction interface 20 and a wound side assembly 19 comprising a fluid removing conduit 21 adapted to remove fluid, such as air and wound exudates,
15 through the suction interface 20 and to a canister comprised in the negative pressure source 23 and an air supplying conduit 22 adapted to supply air through at least a portion of said suction interface 20 and directly in to the fluid removing conduit 21.

20 Fig. 1 further illustrates that the negative pressure wound therapy system 18 comprises a connector device 1 comprising a connector housing 2 and a fluid outlet 3 connected to the connector housing 2. The fluid outlet 3 is in Fig. 1 connected to a fluid conduit 7 connected to the negative pressure source 23 e.g. comprising a canister for collection of the wound exudate. The direction of the fluid
25 in the negative pressure wound therapy system 18 is illustrated in Fig. 1 with the dotted arrows. The connector housing 2 further comprises an air feeding port 4 and an air filter 5 to create a controlled air leak to the suction interface 20. The direction of the air flow in the negative pressure wound therapy system 18 is illustrated in Fig. 1 with unbroken arrows. The air filter 5 may be a porous material
30 filtering and capturing particles while allowing air to flow/leak through the porous structure. The air filter 5 may for example be a cylindrical, square or rectangular shaped porous material. The air leakage provided by the air filter 5 may be

between 10ml/min to 70 ml/min at a pressure of 120 mmHg, or between 15ml/min to 55 ml/min at a pressure of 120 mmHg.

In embodiments of the present disclosure, the air leakage provided by the air filter
5 5 may be between 0.5 ml/min to 70 ml/min at a pressure of 120 mmHg, or
between 1 ml/min to 40 ml/min at a pressure of 120 mmHg. For example, the air
leakage provided by the air filter 5 may be between about 1 to 5 ml/min. For
example, the air leakage provided by the air filter 5 may be between about 15 to
25 ml/min.

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In fig. 1 the air filter 5 is provided in an air filter housing 16, provided with at least
one air inlet opening 17, and herein illustrated with three openings, being an
integrated extending part of the connector housing 2. However, the air filter
housing 16 may also be provided as a separate part, for example connected either
15 directly to the connector housing 2.

The connector housing 2 comprises coupling means 6 for fluidly connecting the
fluid removing conduit 21 to the fluid outlet 3 and the air supplying conduit 22 to
the air feeding port 4.

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In negative pressure wound therapy systems there is in principle always a static
pressure difference introduced by gravity between the pressure inside the canister
and the pressure at the wound site. This is due to the height difference between
the negative pressure source 23 and the wound 9. The amount of exudate inside
25 the fluid removing conduit 21 and the fluid conduit 7 may increase, decrease or
not influence the pressure at the wound site compared with the pressure inside the
canister depending on the orientation of the tubing. A purpose of introducing the
air volume is to ensure that transport of exudates takes place, e.g. by preventing
clogging in or moving exudate from the fluid removing conduit 21 and the fluid
30 conduit 7, between the wound area and a canister provided in connection with the
vacuum pump despite static pressure differences introduced by gravity and
consequently secure a correct pressure level at the wound site.

Fig. 2a and 2b illustrate an embodiment of the connector device 1 according to the present disclosure, wherein fig. 2b is a cross sectional view of the connector device according to fig. 2a. The connector device 1 comprises a fluid outlet 3, connected to a fluid conduit 7 connectable to the negative pressure source 23.

5 The fluid outlet may be in the form of an extending body portion provided with coupling means, such as gripping means for receiving and retaining fluid conduit 7, for fluid connection to the negative pressure source 23. The fluid conduit 7 may be, at a portion opposite to the side connected to the connector device, connected to a device side connector comprising coupling means adapted to be connected to

10 a negative pressure source side connector. The wound side assembly 19 is provided with wound side assembly coupling means 15 for coupling connection with the connector device coupling means 6. Non-limiting example of a coupling connection is a snap-on, threaded, luer-lock and bayonet connections.

15 As clearly illustrated in Fig. 2b showing a cross sectional view of the connector device 1, the connector device 1 may comprise an air feeding conduit 33 comprising the air feeding port 4 and an air inlet opening 17. Moreover, as is indicated in Fig. 2b, the air feeding conduit 33 is an integrated part of the connector housing 2 and may accommodate the air filter 5 or may be connected to

20 an air filter housing 16. The air feeding conduit 33 may be adapted to be connected to the air supplying conduit 22 and the fluid outlet 3 may be securely connected to the fluid removing conduit 21.

Fig. 3 illustrates a branched connector device 10, and more specifically a Y

25 connector device 100, according to the present disclosure. The Y connector device 100 illustrated in Fig. 3 comprises a first connector device 1 comprising a connector housing 2 and a fluid outlet 3 connected to the connector housing 2. The Y connector device 100 furthermore comprises a branched conduit 14 comprising a first and a second branch portion 11, 12, the fluid outlet 3 being

30 directly connected to the first branch portion 11.

The direction of the fluid in the Y connector device 100 and the fluid communication assemblies is illustrated in Fig. 3 with the dotted arrows. The connector housing 2 further comprises an air feeding port 4 and an air filter 5 to create a controlled air leak via the air supplying conduit 22. The direction of the air in the Y connector device 100 and the fluid communication assemblies is illustrated in Fig. 3 with the unbroken arrows. The air filter 5 may be a porous material filtering and capturing particles while allowing air to flow/leak through the porous structure. The air filter 5 may be a three-dimensional porous material. The air leakage provided by the air filter 5 may be between 0.5 ml/min to 70ml/min at a pressure of 120 mmHg. For example, the air leakage provided by the air filter 5 may be between 10ml/min to 70 ml/min at a pressure of 120 mmHg, or between 15ml/min to 55 ml/min at a pressure of 120 mmHg, or between 1 ml/min to 40 ml/min at a pressure of 120 mmHg, or between about 1 ml/min to 5 ml/min, or between about 15 to 25 ml/min.

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Preferably, the air leakage provided by the air filter 5 is adapted such that a continuous flow of air is ensured via the air supplying conduit 22, whilst at the same time reducing unnecessary work load of the negative pressure source 23, thereby minimizing noise and battery usage from the negative pressure source 23. For example, in case the negative pressure source 23 has a suction capacity of up to about 1 L/min, the air leakage provided by the air filter 5 may preferably be adapted to be between about 1 to 5 ml/min at a pressure of 120 mmHg. For example, in case the negative pressure source 23 has a suction capacity of up to about 5 L/min, the air leakage provided by the air filter 5 may preferably be adapted to be between about 15 to 55 ml/min at a pressure of 120 mmHg, such as between about 15 ml/min to 25 ml/min at a pressure of 120 mmHg.

In Fig. 3 the air filter 5 is provided in an air filter housing 16, provided with three openings 17, being an integrated extending part of the connector housing 2. However, the air filter housing 16 may also be provided as a separate part, for example connected either directly to the connector housing 2.

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The connector housing 2 comprises coupling means 6 for fluidly connecting the fluid removing conduit 21 to the fluid outlet 3 and the air supplying conduit 22 to the air feeding port 4. In Fig. 3 the connector device 1 is adapted to be connected to the wound side assembly 21 at the connector housing coupling side 2b and the
5 air feeding port is provided on the connector housing device side 2a, which is positioned on the opposite side of the connector housing coupling side 2b.

In negative pressure wound therapy systems there is in principle always a static pressure difference introduced by gravity between the pressure inside the canister
10 and the pressure at the wound. This is due to the height difference between the negative pressure wound therapy system 18' and the different wounds 9 and the fact that exudate often is present in the conduits. The liquid column of exudate inside the fluid removing conduit 21 and the fluid conduit 7 may increase, decrease or not influence the pressure at the wound site compared with the
15 pressure inside the canister depending on the orientation of the tubing. A purpose of introducing the air volume is to ensure that transport of exudate takes place between the wound area and a canister provided in connection with the vacuum pump, despite static pressure differences introduced by gravity, and consequently secures a correct pressure at the wound site. This is an even more crucial issue
20 for negative wound therapy systems connectable to more than one fluid communication assembly and thus able to perform treatment at more than one wound site using only one negative pressure source.

The wound side assembly 19 is provided with wound side assembly coupling
25 means 15 for coupling connection with the connector device coupling means 6. A non-limiting example of a coupling connection is a snap-on connection.

The Y connector device 100 according to Fig. 3 furthermore comprises a second connector device 1', with a second connector housing 2' and a second fluid outlet
30 3', wherein the second branch portion 12 is connected to the second fluid outlet 3'. The second connector device 1' furthermore comprises a second air feeding port 4' connected to the second connector housing 2'. In Fig. 3, a second conduit 8 is

connected to the second air feeding port 4'. However, it is also conceivable that the configuration of the air feeding port of the second connector device 1' is identical to the air feeding port configuration of the first connector device 1, shown in fig. 1-2.

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The second connector housing 2' furthermore comprises second coupling means 6' for fluidly connecting a second fluid removing conduit 21' to the second fluid outlet 3' and the second air supplying conduit 22' to the second air feeding port 4'. The second connector device 1' is adapted to be engaged with a second wound
10 side connector 25' of a second wound side assembly 19' at the second connector housing coupling side 2b' or alternatively to a branched connector device 10, such as an Y connector device 100, according to the present disclosure.

The end portion of the branched conduit 14 is provided with a device side
15 connector comprising coupling means 26 for coupling connection to a connector device 1'''. The connector device 1''' may be a connector device identical to the connector device 1, a branched connector device 10, such as a Y connector device 100, all comprising a fluid outlet for fluid communication with the first and second branch portions 11, 12 via the end portion of the branched conduit 14, and
20 an air feeding port to supply air via the second conduit 8 to the air feeding port 3' of the second connector device 2'. It is of course also conceivable that the device side connector comprising coupling means 26 is coupled to a negative pressure source side connector connected to an fluid removing conduit leading to a negative pressure source 23 comprising a canister for receiving wound exudate.

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Fig. 4 illustrates a further branched connector device 10. The branched connector device 10 illustrated in Fig. 4 comprises a first connector device 1 comprising a connector housing 2 comprising coupling means 6 and a fluid outlet 3 connected to the connector housing 2. The branched connector device 10 furthermore
30 comprises a branched conduit 14' comprising a first, a second and a third branch portion 11, 12, 13, wherein the fluid outlet 3 is directly connected to the first branch portion 11.

The branched connector device 10 furthermore comprises a second connector device 1', with a second connector housing 2' and a second fluid outlet 3', wherein the second branch portion 12 is connected to the second fluid outlet 3'. The second connector device 1' furthermore comprises a second air feeding port 4' connected to the second connector housing 2'. A third connector device 1'', with a third connector housing 2'' and a third fluid outlet 3'', is connected to the third branch portion 13 via the third fluid outlet 3''. The third connector device 1'' furthermore comprises a third air feeding port 4'' connected to the third connector housing 2''.

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Each of the first, second and third connector devices 1, 1', 1'' furthermore comprises air filters 5, 5', 5'' provided in air filter housings 16, 16', 16''.

As illustrated in Fig. 3 and Fig. 4, a unique advantage with the branched connector devices according to the present disclosure is that air is allowed to enter into each of the fluid communications assemblies connected via each of the connector devices ensuring flushing of each fluid communication assembly even when only one negative pressure source is used.

CLAIMS

1. A connector device (1) for a negative pressure wound therapy system, said connector device (1) comprising:

- 5 - a connector housing (2),
- a fluid outlet (3) connected to said connector housing (2),
- an air feeding port (4),
- an air filter (5), and
- coupling means (6),

10 wherein:

- said fluid outlet (3) is adapted to be connected to a negative pressure source (23),

- said connector device (1) being adapted to be engaged with a wound side connector (25) of a wound side assembly (19) by means of said coupling means

15 (6),

- said wound side assembly (19) comprising a fluid removing conduit (21) and an air supplying conduit (22),

- a portion of each one of said fluid removing conduit (21) and said air supplying conduit (22) being connected to said wound side connector (25), and

20 - said connector device (1) being such that when said connector device (1) is engaged with said wound side connector (25), said fluid removing conduit (21) is fluidly connected to said fluid outlet (3) and said air supplying conduit (22) is fluidly connected to said air feeding port (4) such that air ambient of said connector device (1) can be fed to said air supplying conduit (22) via said air filter

25 (5) and said air feeding port (4),

characterized in that:

- said connector device (1) further comprises an air feeding conduit (33) comprising said air feeding port (4) and an air inlet opening (17), said air feeding conduit (33) being an integrated part of said connector housing (2),

30 - said connector housing (2) has a connector housing device side (2a) and a connector housing coupling side (2b), said connector housing device side (2a)

being positioned on the opposite side of said connector housing coupling side (2b),

- said connector device (1) adapted to be connected to said wound side connector (25) at said connector housing coupling side (2b),

5 - said air filter (5) is arranged inside an air filter housing (16) comprising the air inlet opening (17) arranged to allow air to flow through said air filter (5), wherein said air inlet opening (17) is provided on said connector housing device side (2a),

- said air filter housing (16) is arranged as an integrated part of the connector housing (2), and

10 - said air filter (5) provides an air leakage of between 10ml/min to 70 ml/min at a pressure of 120 mmHg.

2. The connector device (1) according to any one of the preceding claims, wherein said air inlet opening (17) is arranged at a radial distance from said fluid
15 outlet (3).

3. The connector device (1) according to any one of the preceding claims, wherein a fluid conduit (7) is connected to said fluid outlet (3).

20 4. The connector device (1) according to any one of the preceding claims, wherein said air filter (5) provides an air leakage of between 15ml/min to 55 ml/min at a pressure of 120 mmHg.

5. The connector device (1) according to any one of the preceding claims,
25 wherein said connector device (1) by means of said coupling means (6) is adapted to form a snap-on, threaded, luer-lock, or bayonet engagement, preferably a release snap-on, threaded or bayonet engagement, with said wound side connector (25).

30 6. A branched connector device (10) comprising a branched conduit (14) which in turn comprises a first and a second branch portion (11, 12), said branched connector device (10) further comprising a connector device (1)

according to any one of claims 1 – 5, wherein said first branch portion (11) is connected to said fluid outlet (3) of said connector device (1).

7. The branched connector device (10) according to claim 6, wherein said
5 branched connector device (10) comprises a second connector device (1') comprising a second connector housing (2') and second coupling means (6') and a second fluid outlet (3') connected to said second connector housing (2'), said second branch portion (12) being connected to said second fluid outlet (3').

10 8. The branched connector device (10) according to claim 7, wherein said second connector device (1') comprises a second air feeding port (4').

9. The branched connector device (10) according to claim 8, wherein a second conduit (8) is connected to said second air feeding port (4').

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10. The branched connector device (10) according to claim 8 or 9, wherein said second connector device (1') is a connector device according to any one of claim 1 to 5.

20 11. The branched connector device (10) according to any one of claims 6 to 10, wherein said branched connector device 10 is a Y-connector device (100).

12. The branched connector device (10) according to any one of claims 6 to 11, wherein said branched connector device (10) comprises a third connector
25 device (1'') with a third fluid outlet (3'') and a branched conduit (14) comprising a third branch portion (13), said third branch portion (13) being connected to said third fluid outlet (3'').