TARGETED LIPOSOMES

BACKGROUND OF THE INVENTION

Field of the Invention

[0001] The present invention is in the field of drug delivery, and specifically, cationic liposome-based drug delivery. In embodiments, this invention provides methods of making ligand-targeted (e.g., antibody- or antibody fragment-targeted) liposomes useful for the delivery of liposomes to tumors, including brain tumors. In embodiments, the liposomes deliver temozolomide across the blood-brain barrier for treatment of primary or metastatic brain tumors. Additional cancers that can be treated with the liposomes include neuroendocrine tumors, melanoma, prostate, head and neck, ovarian, lung, liver, breast, urogenital, gastric, colorectal, cervical, liposarcoma, rhabdomyosarcoma, choriocarcinoma, pancreatic, retinoblastoma, multiple myeloma and other types of cancer. In another embodiment the liposomes deliver melphalan for the treatment of multiple myeloma, other tumors of the blood or other solid tumors. In still other embodiments the liposomes can deliver other drugs such as atropine, pemetrexed or irinotecan across the blood-brain barrier.

Background of the Invention

[0002] Primary brain tumors, and particularly gliomas, are one of the most difficult cancers to treat. In addition to primary tumors, metastatic brain cancer from a variety of primary sources [predominately lung (60%), breast (20%) and melanoma (10%)], is diagnosed in over 150,000 patients a year (Newton H and Malkin M (2010) Neurologic Complications of Systemic Cancer and Antineoplastic Therapy. Informa Healthcare). Thus, there is a critical need for improved therapies for brain cancers, which is confirmed by the fact that the NCI has made brain cancers one of its top 5 funding priorities. The lack of improvement in the prognosis of patients with brain cancer over the last few years, despite recent advances in drug discovery and development of targeted therapies, is due in large part to the inability of the therapeutics to cross the

blood-brain barrier (BBB) (Blakeley, J. (2008): Drug delivery to brain tumors. Current Neurology & Neuroscience Reports, 8:235-241).

[0003] The current standard of therapy for glioblastoma multiforme (GBM) is surgical resection, followed by radiotherapy and chemotherapy with Temozolomide (TMZ). TMZ, a second-generation alkylating (methylating) agent causes cytotoxic DNA lesions, and is also approved for treatment of anaplastic astrocytoma (AA) and is in clinical trials for treatment of brain metastases from other non-CNS solid tumors. The mechanism of action and pharmacological properties have been recently reviewed (Tentori L and Graziani G (2009) Recent Approaches to Improve the Antitumor Efficacy of Temozolomide. Current Medicinal Chemistry 16: pp 245-257; and Mrugala MM, Adair J and Kiem H P (2010) Temozolomide: Expanding Its Role in Brain Cancer. Drugs of Today 46: pp 833-846). TMZ is relatively well tolerated (Jiang G, Wei Z P, Pei D S, Xin Y, Liu Y Q and Zheng J N (2011) A Novel Approach to Overcome Temozolomide Resistance in Glioma and Melanoma: Inactivation of MGMT by Gene Therapy. Biochemical and Biophysical Research Communications 406: pp 311-314), however myelosuppression, neutropenia and thrombocytopenia are among its side effects and therapeutic dosages are limited by these. Extended TMZ dosing regimens were also found to provoke lymphocytopenia and opportunistic infections (Tentori L and Graziani G (2009) Recent Approaches to Improve the Antitumor Efficacy of Temozolomide. Current Medicinal Chemistry 16: pp 245-257). The extensive tissue distribution that results from the non-tumor specific uptake of the orally administered TMZ is a major cause of these side effects. Thus, tumor-targeting delivery of TMZ could help reduce these adverse events.

[0004] TMZ has shown survival benefit in a subset of GBM patients, however this median increase is only 2.5 months compared to radiation alone (Chamberlain MC (2010) Temozolomide: Therapeutic Limitations in the Treatment of Adult High-Grade Gliomas. Expert Review of Neurotherapeutics 10: pp 1537-1544). Recent studies have also indicated that 60-75% of GBM patients and 50% of AA patients do not benefit from TMZ (Chamberlain MC (2010) Temozolomide: Therapeutic Limitations in the Treatment of Adult High-Grade Gliomas. Expert Review of Neurotherapeutics 10: pp 1537-1544). The failure of chemotherapy can be attributed to a number of factors including, short half-life in circulation, efflux of drugs from the tumor by p-glycoprotein, resistance of the tumors to the drug and failure to cross the blood-brain

barrier. The primary mechanism of resistance to TMZ is overexpression of O^6-methylguanine-DNA-methyl transferase (MGMT), which repairs the TMZ-induced DNA lesion by removing the O^6-guanine adducts (Mrugala MM, Adair J and Kiem H P (2010) Temozolomide: Expanding Its Role in Brain Cancer. Drugs of Today 46: pp 833-846). Thus, a means to down modulate MGMT activity, for example via the tumor specific delivery of the p53 tumor suppressor gene, would enhance the therapeutic effect of TMZ.

[0005] There is, therefore, an urgent need to develop new therapies for treatment of brain and other cancers. The present invention fulfills these needs by providing a cationic-liposome-based drug delivery system for delivery of temozolomide.

BRIEF SUMMARY OF THE INVENTION

[0006] In embodiments, methods of preparing a targeted temozolomide cationic liposome complex are provided. Such methods suitably comprise preparing a lipid solution comprising one or more cationic lipids in ethanol, preparing a solution of temozolomide, mixing the lipid solution with the solution of temozolomide, injecting the mixture of lipid and temozolomide into an aqueous solution, thereby forming a temozolomide cationic liposome, and mixing the temozolomide cationic liposome with a ligand to form the targeted temozolomide cationic liposome, wherein the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome.

[0007] Suitably, the ligand is an antibody, an antibody fragment or a protein, including a single chain Fv antibody fragment, such as an anti-transferrin receptor single chain Fv (TfRscFv).

[0008] Suitably the solution of temozolomide is prepared in dimethyl sulfoxide (DMSO). Suitably the solution of temozolomide is prepared at a concentration of about 1 mM to about 200 mM, or about 50 mM to about 200 mM.

[0009] In embodiments the lipid solution comprises 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE).

[0010] Suitably the molar ratio of lipid:temozolomide is about 0.1:1 to about 5:1, more suitably about 0.5:1 to about 2:1 or about 1:1. Suitably the concentration of the liposome is about 1 mM to about 2 mM, or about 2 mM to about 10 mM

[0011] In embodiments, the weight ratio of ligand:lipid is about 0.01:1 to about 0.5:1, more suitably about 0.3:1 to about 0.4:1. In embodiments the weight ratio of TfRscFv:lipid is about 0.33:1.

[0012] Suitably, a method of preparing a targeted temozolomide cationic liposome complex is provided. In embodiments, the methods comprise preparing a lipid solution comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE)in ethanol, preparing a solution of temozolomide, mixing the lipid solution with the solution of temozolomide, injecting the mixture of lipid and temozolomide into an aqueous solution, thereby forming a temozolomide cationic liposome, mixing the temozolomide cationic liposome with an anti-transferrin receptor single chain Fv (TfRscFv) to form the targeted temozolomide cationic liposome complex, wherein the TfRscFv is directly complexed with, but not chemically conjugated to, the cationic liposome.

[0013] In another embodiment, a method of preparing a targeted melphalan cationic liposome complex is provided. In embodiments, the methods comprise preparing a lipid solution comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE) in ethanol, preparing a solution of melphalan, mixing the lipid solution with the solution of melphalan, injecting the mixture of lipid and melphalan into an aqueous solution, thereby forming a melphalan cationic liposome, mixing the melphalan cationic liposome with a ligand, including for example, an anti-transferrin receptor single chain Fv (TfRscFv), to form the targeted melphalan cationic liposome complex, wherein the ligand (e.g., TfRscFv) is directly complexed with, but not chemically conjugated to, the cationic liposome.

[0014] In further embodiments, methods of treating cancer in a patient, comprising administering to the patient a targeted temozolomide cationic liposome complex are provided. Suitably the targeted temozolomide cationic liposome complex comprises a cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), temozolomide and a ligand complexed with, but not chemically conjugated to, the cationic liposome.

[0015] In further embodiments, methods of treating cancer in a patient, comprising administering to the patient a targeted melphalan cationic liposome complex are provided. Suitably, the targeted melphalan cationic liposome complex comprises a cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP)

and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), melphalan and a ligand complexed with, but not chemically conjugated to, the cationic liposome

[0016] In embodiments, the administration is intravenous (IV), intratumoral (IT), intralesional (IL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), intraocular (IO), intraperitoneal (IP), sublingual (SL), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump

[0017] Suitably the cancer being treated is a brain cancer, for example a glioma or an astrocytoma.

[0018] In other embodiments, the cancer being treated is a metastatic brain tumor, neuroendocrine tumors, melanoma, prostate, head and neck, ovarian, lung, liver, breast, urogenital, gastric, colorectal, cervical, liposarcoma, rhabdomyosarcoma, choriocarcinoma, pancreatic, retinoblastoma, multiple myeloma and other types of cancer.

[0019] In another embodiment the liposomes deliver melphalan for the treatment of multiple myeloma.

[0020] In still other embodiments the liposomes can deliver other drugs such as atropine, pemetrexed or irinotecan and/or derivatives thereof.

[0021] In embodiments, the methods further comprise administering an additional therapy to the patient in combination with the targeted temozolomide, melphalan, atropine, premetrexed or irinotecan cationic liposome complex. Suitably the additional therapy comprises administration of a chemotherapeutic agent, a small molecule, radiation therapy or a nucleic acid-based therapy. In embodiments, the nucleic acid-based therapy comprises administration of a cationic liposome complex comprising a plasmid DNA expressing wild-type p53. In embodiments the additional therapy comprises administration of any molecule that down-regulates, modifies or otherwise negates the effect of MGMT in the cancer cell. In additional embodiments the additional therapy comprises administration of any molecule that interferes with the production of acetylcholine, or binding of acetylcholine to its receptor.

[0022] In embodiments, methods of treating brain cancer in a patient, comprising administering to the patient a targeted temozolomide cationic liposome complex are provided. Suitably the targeted temozolomide cationic liposome complex comprises a

cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), temozolomide and an anti-transferrin receptor single chain Fv (TfRscFv) complexed with, but not chemically conjugated to, the cationic liposome.

[0023] Methods of treating cancer in a patient, are also provided, suitably comprising administering to the patient a targeted temozolomide cationic liposome complex prepared by the methods described herein.

[0024] In still other embodiments, methods of treating multiple myeloma in a patient, comprising administering to the patient a targeted cationic liposome complex, are provided. Suitably the targeted melphalan cationic liposome complex comprises a cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), melphalan and an anti-transferrin receptor single chain Fv (TfRscFv) directly complexed with, but not chemically conjugated to, the cationic liposome.

[0025] In still other embodiments, methods of treating any cancer in a patient, comprising administering to the patient a targeted cationic liposome complex are provided. Suitably the targeted melphalan cationic liposome complex comprises a cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), melphalan and an anti-transferrin receptor single chain Fv (TfRscFv) directly complexed with, but not chemically conjugated to, the cationic liposome.

[0026] Methods of treating cancer in a patient, are also provided, suitably comprising administering to the patient a targeted melphalan cationic liposome complex prepared by the methods described herein.

[0027] Methods are also provided of treating a brain cancer in a patient, comprising administering to the patient a cationic liposome complex comprising a cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE) a plasmid DNA expressing wild-type p53 and an anti-transferrin receptor single chain Fv (TfRscFv) directly complexed with, but not chemically conjugated to, the cationic liposome; and temozolomide.

[0028] Further embodiments, features, and advantages of the embodiments, as well as the structure and operation of the various embodiments, are described in detail below with reference to accompanying drawings.

BRIEF DESCRIPTION OF THE DRAWINGS/FIGURES

[0029] FIG. 1 shows U251 cell survival versus concentration of TMZ for free TMZ and three cationic liposomes comprising TMZ, as described herein.

[0030] FIG. 2 shows U87 cell survival versus concentration of TMZ for free TMZ and cationic liposomes comprising TMZ, as described herein.

[0031] FIG. 3A shows T98G cell survival versus concentration of TMZ for free TMZ and a targeted cationic liposome comprising TMZ, as described herein.

[0032] FIG. 3B shows KMS-11 cell survival versus concentration of TMZ for free TMZ and a targeted cationic liposome comprising TMZ, as described herein.

[0033] FIG. 4A shows fluorescence intensity of the brain tumors using the Maestro™ *in vivo* fluorescence imaging system.

[0034] FIG. 4B shows magnetic resonance imaging (MRI) images of U87MG-luc2 glioblastoma tumor xenografts in response to treatment with free TMZ and scL-TMZ.

[0035] FIG. 5 shows the size of brain tumors measured by MRI after treatment with free TMZ or scL-TMZ.

[0036] FIG. 6 shows bioluminescence imaging of mice treated with free TMZ and scL-TMZ.

[0037] FIG. 7 shows additional bioluminescence imaging of mice treated with free TMZ and scL-TMZ.

[0038] FIG. 8 shows the quantification of bioluminescence signal intensities of mice treated with free TMZ and scL-TMZ.

[0039] FIG. 9 shows the quantification of bioluminescence signal intensities of mice treated with free TMZ and scL-TMZ.

[0040] FIG. 10 shows body weight measurements of mice during and after treatment with free TMZ and scL-TMZ.

[0041] FIG. 11 shows a Kaplan-Meier plot demonstrating long term survival for animals treated with free TMZ and scL-TMZ.

[0042] FIG. 12 shows a Kaplan-Meier plot demonstrating long term survival for animals treated with free TMZ and scL-TMZ at different doses.

[0043] FIG. 13 shows weights of brain tumors demonstrating the effect of free TMZ and scL-TMZ.

[0044] FIG. 14 shows results of flow cytometric analysis for the level of apoptosis as determined by cleaved caspase-3 antibody staining of single cells isolated from brain tumors.

[0045] FIG. 15 shows tumor size for free TMZ and scL-TMZ treated mice.

[0046] FIG. 16 shows body weight of mice treated with free TMZ and scL-TMZ.

[0047] FIG. 17 shows TUNEL staining of CD133+ CSCs and CD133- non-CSCs isolated from subcutaneous T98G xenograft tumors.

[0048] FIG. 18 shows levels of apoptosis assessed by cleaved caspase-3 antibody staining of SSEA-1+ CSCs from subcutaneous T98G brain tumors.

[0049] FIG. 19 shows T98G cell survival versus concentration of TMZ for free TMZ, scL-TMZ, as described herein and the combination scL-TMZ along with targeted cationic liposomes expressing the p53 gene.

[0050] FIG. 20 shows tumor-targeted delivery of systemically administered scL-6FAM-ODN to U251 xenograft brain tumors.

[0051] FIG. 21 shows flow cytometric analysis of scL-delivered 6FAM-ODN uptake in CD133+ and CD133- non-CSC cells isolated from U251 xenograft tumors after systemic administration.

[0052] FIG. 22 shows tumor specific targeting of CSCs in IC GBM by scL-Delivered ODN after systemic administration.

[0053] FIG. 23 shows XTT assay after the addition of the TMZ to the cells and IC_{50} values.

[0054] FIG. 24 shows bioluminescence imaging of U87 IC tumors using Xenogen showing the synergistic effect of the combination of SGT-53 + TMZ.

[0055] FIG. 25 shows the synergistic effect of SGT-53 plus TMZ on IC U87 GBM.

[0056] FIG. 26 shows the synergistic Effect of the combination of systemically administered scL-p53 plus TMZ.

[0057] FIG. 27 shows Kaplan-Meier plots demonstrating SGT-53 sensitization to TMZ treatment significantly enhances survival in an IC U87 model of GBM.

[0058] FIG. 28 shows Kaplan-Meier plots demonstrating SGT-53 sensitization to TMZ treatment significantly enhances survival in an IC TMZ Resistant Model of GBM (T98G Cells).

[0059] FIG. 29 shows percent of tumor cells in apoptosis post-treatment as indicated.

[0060] FIG. 30 shows down modulation of MGMT expression in T98G TMZ-resistant brain tumor cells and SQ xenograft tumors by systemic complex p53 gene therapy.

[0061] FIG. 31 shows down modulation of MGMT expression in T98G TMZ-resistant intracranial brain tumors by systemic complex p53 gene therapy.

[0062] FIG. 32 shows a proposed dosing schedule for scL-p53.

[0063] FIG. 33 shows KMS-11 cell survival versus concentration of MEL for free MEL and a targeted cationic liposome comprising MEL, as described herein.

[0064] FIG. 34 shows comparison of unencapsulated MEL, with Lip/MEL without the targeting moiety and with the full scL/MEL complex, as well as with liposome only.

[0065] FIG. 35 shows comparison of unencapsulated MEL, with fresh and lyophilized scL/MEL complex.

[0066] FIG. 36 shows the effect of targeted p53 therapy on KMS-11 cells.

[0067] FIG. 37 shows the effect of free (unencapsulated) MEL alone, scL/MEL alone, or the combination of free (unencapsulated) or scL encapsulated MEL plus scL-p53 on KMS-11 cells.

DETAILED DESCRIPTION OF THE INVENTION

[0068] It should be appreciated that the particular implementations shown and described herein are examples and are not intended to otherwise limit the scope of the application in any way.

[0069] The published patents, patent applications, websites, company names, and scientific literature referred to herein are hereby incorporated by reference in their entireties to the same extent as if each was specifically and individually indicated to be incorporated by reference. Any conflict between any reference cited herein and the specific teachings of this specification shall be resolved in favor of the latter. Likewise, any conflict between an art-understood definition of a word or phrase and a definition of the word or phrase as specifically taught in this specification shall be resolved in favor of the latter.

[0070] As used in this specification, the singular forms "a," "an" and "the" specifically also encompass the plural forms of the terms to which they refer, unless the content clearly dictates otherwise. The term "about" is used herein to mean approximately, in the region of, roughly, or around. When the term "about" is used in conjunction with a numerical range, it modifies that range by extending the boundaries above and below the numerical values set forth. In general, the term "about" is used herein to modify a numerical value above and below the stated value by a variance of 20%.

[0071] Technical and scientific terms used herein have the meaning commonly understood by one of skill in the art to which the present application pertains, unless otherwise defined. Reference is made herein to various methodologies and materials known to those of ordinary skill in the art.

[0072] In embodiments, methods of preparing targeted temozolomide cationic liposome complexes are provided. Suitably, the methods comprise preparing a lipid solution comprising one or more cationic lipids in ethanol. A solution of temozolomide is prepared. The lipid solution is mixed with the solution of temozolomide. The mixture of cationic lipid and temozolomide is injected into an aqueous solution, thereby forming a temozolomide cationic liposome. The temozolomide cationic liposome is then mixed with a ligand to form the targeted temozolomide cationic liposome complex. Suitably, the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome.

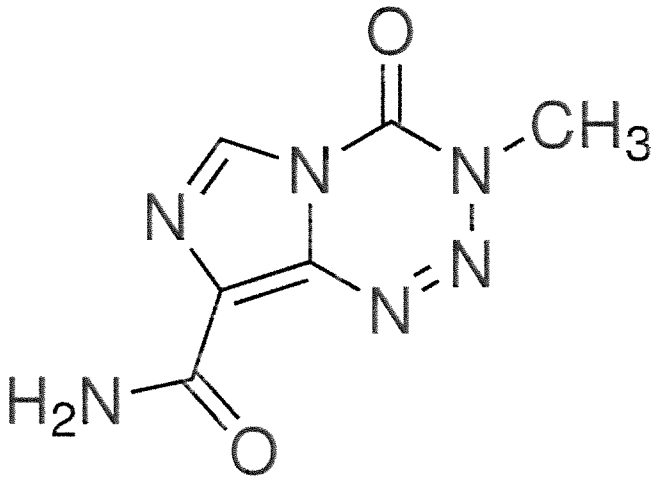
[0073] In embodiments, methods of preparing targeted melphalan cationic liposome complexes are provided. Suitably, the methods comprise preparing a lipid solution comprising one or more cationic lipids in ethanol. A solution of melphalan is prepared, suitably in absolute ethanol containing enough hydrochloric acid to facilitate dissolving the melphalan. The lipid solution is mixed with the solution of melphalan. The mixture of cationic lipid and melphalan is injected into an aqueous solution, thereby forming a melphalan cationic liposome. The melphalan cationic liposome is then mixed with a ligand to form the targeted melphalan cationic liposome complex. Suitably, the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome.

[0074] In embodiments, methods of preparing targeted atropine, irinotecan or premetrexed cationic liposome complexes are provided. Suitably, the methods comprise preparing a lipid solution comprising one or more cationic lipids in ethanol. A solution of atropine, irinotecan or premetrexed is prepared in an appropriate solvent

such as absolute ethanol, DMSO, water or a buffer solution such as a Phosphate buffer or a HEPES buffer or a TRIS buffer. The lipid solution is mixed with the solution of atropine, irinotecan or premetrexed. The mixture of cationic lipid and atropine, irinotecan or premetrexed is injected into an aqueous solution, thereby forming a cationic atropine, irinotecan or premetrexed liposome. The atropine, irinotecan or premetrexed cationic liposome is then mixed with a ligand to form the targeted atropine, irinotecan or premetrexed cationic liposome complex. Suitably, the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome.

[0075] The terms "complex," "nanocomplex," "liposome complex" and "cationic liposome complex" are used interchangeably throughout to refer to the cationic liposomes of the present invention.

[0076] As described herein, temozolomide is a second-generation alkylating (methylating) agent causes cytotoxic DNA lesions, and is also approved for treatment of anaplastic astrocytoma (AA). The structure of temozolomide shown below, has an empirical formula: $C_6H_6N_6O_2$.



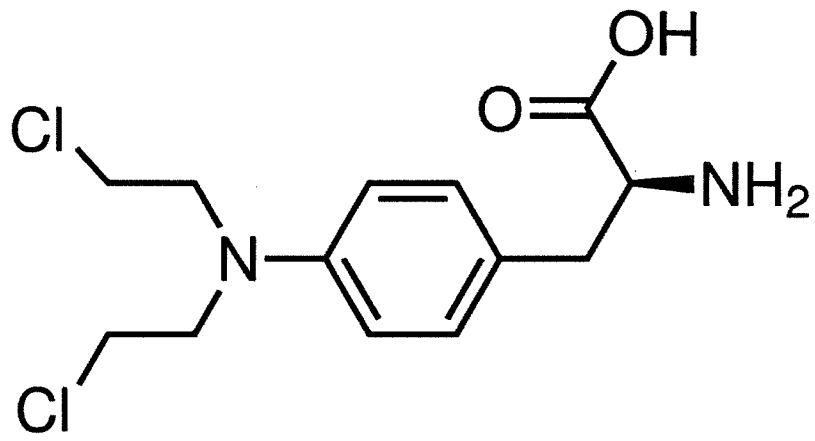
Temozolomide, MW=194.15

In embodiments, a salt of temozolomide, e.g., an HCl salt, can also be used in the methods described herein.

[0077] Suitably, the solution of temozolomide (TMZ) is prepared in dimethyl sulfoxide (DMSO) or other appropriate solvent. The solution of TMZ can be prepared at any desired concentration. In embodiments, the concentration of TMZ in the solution is about 0.1 mM to about 500 mM, more suitably about 1 mM to about 200 mM, about 50 mM to about 200 mM, about 50 mM to about 100 mM, or about 50 mM, about 60 mM,

about 70 mM, about 80 mM, about 90 mM, about 100 mM, about 110 mM, about 120 mM, about 130 mM, about 140 mM, about 150 mM, about 160 mM, about 170 mM, about 180 mM, or about 200 mM.

[0078] Melphalan is an antineoplastic agent belonging to the class of nitrogen mustard alkylating agents. An alkylating agent adds an alkyl group (C_nH_{2n+1}) to DNA. It attaches the alkyl group to the guanine base of DNA, at the number 7 nitrogen atom of the imidazole ring. The structure of melphalan shown below, has an empirical formula: $C_{13}H_{18}C_{l2}N_2O_2$.



Melphalan, MW=305.20

[0079] Suitably, the solution of melphalan is prepared in absolute ethanol containing enough hydrochloric acid to facilitate dissolving the melphalan or other appropriate solvent. The solution of melphalan can be prepared at any desired concentration. In embodiments, the concentration of melphalan in the solution is about 0.1 mM to about 500 mM, more suitably about 1 mM to about 200 mM, about 50 mM to about 200 mM, about 50 mM to about 100 mM, or about 50 mM, about 60 mM, about 70 mM, about 80 mM, about 90 mM, about 100 mM, about 110 mM, about 120 mM, about 130 mM, about 140 mM, about 150 mM, about 160 mM, about 170 mM, about 180 mM, or about 200 mM.

[0080] Suitably, the solution of atropine, irinotecan or premetrexed is prepared in an appropriate solvent such as absolute ethanol, DMSO, water or a buffer solution such as a Phosphate buffer or a HEPES buffer or a TRIS buffer. The solution of atropine, irinotecan or premetrexed can be prepared at any desired concentration. In embodiments, the concentration of atropine, irinotecan or premetrexed in the solution is about 0.1 mM to about 500 mM, more suitably about 1 mM to about 200 mM, about 50

mM to about 200 mM, about 50 mM to about 100 mM, or about 50 mM, about 60 mM, about 70 mM, about 80 mM, about 90 mM, about 100 mM, about 110 mM, about 120 mM, about 130 mM, about 140 mM, about 150 mM, about 160 mM, about 170 mM, about 180 mM, or about 200 mM.

[0081] A wide variety of lipids are useful in the methods described herein. Published PCT application WO 99/25320 describes the preparation of several cationic liposomes. Examples of suitable lipids include phosphatidylcholine (PC), phosphatidylserine (PS), as well as mixtures of dioleoyltrimethylammonium propane (DOTAP) and dioleoylphosphatidylethanolamine (DOPE) and/or cholesterol (chol); a mixture of dimethyldioctadecylammonium bromide (DDAB) and DOPE and/or chol. The ratio of the lipids can be varied to optimize the efficiency of loading of the TMZ, melphalan, atropine, pemetrexed or irinotecan and uptake in the specific target cell type. The liposome can comprise a mixture of one or more cationic lipids and one or more neutral or helper lipids. A desirable ratio of cationic lipid(s) to neutral or helper lipid(s) is about 1:(0.5-3), preferably 1:(1-2) (molar ratio). Exemplary lipids for use in preparing the cationic liposomes described herein are well known in the art and include, for example, 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE).

[0082] Examples of ratios of various lipids useful in the practice of methods described herein include, but are not limited, to:

[0083]	LipA	DOTAP/DOPE	1:1 molar ratio
[0084]	LipB	DDAB/DOPE	1:1 molar ratio
[0085]	LipC	DDAB/DOPE	1:2 molar ratio
[0086]	LipD	DOTAP/Chol	1:1 molar ratio
[0087]	LipE	DDAB/Chol	1:1 molar ratio
[0088]	LipG	DOTAP/DOPE/Chol	2:1:1 molar ratio
[0089]	LipH	DDAB/DOPE/Chol	2:1:1 molar ratio

[0090] (DOTAP = 1,2-dioleoyl-3-trimethylammonium propane, DDAB = dimethyldioctadecylammonium bromide; DOPE = dioleoylphosphatidylethanolamine; chol = cholesterol).

[0091] As described herein, the lipids are suitably prepared in ethanol (e.g., absolute ethanol) prior to preparing the complexes described herein.

[0092] Following solubilization in ethanol of the lipid components of the complexes, the appropriate amount of TMZ, melphalan atropine, irinotecan or premetrexed, dissolved in DMSO or other suitable solvent, is added to the lipid mixture. Suitably, the lipid mixture is maintained at a temperature of about 50-60 °C, prior to and during the addition of the TMZ, melphalan, atropine, irinotecan or premetrexed.

[0093] To prepare the liposomes, the solution of lipids and TMZ, melphalan, atropine, irinotecan or premetrexed is injected into an aqueous solution to form the liposomes. As used herein "injected" means to force or drive the solution of lipids and TMZ, melphalan, atropine, irinotecan or premetrexed into an aqueous solution. Suitably, the aqueous solution is water, though additional buffers and salts can be present in the aqueous solution. In embodiments, the aqueous solution is endotoxin free LAL reagent water (suitably having an endotoxin content of <0.005 EU/ml) (BioWhittaker). Suitably the injection is carried out utilizing a syringe or similar device to produce the liposomes. In embodiments, the aqueous solution is stirred rapidly during addition of the lipid/TMZ, melphalan, atropine, irinotecan or premetrexed solution so as to facilitate liposome formation.

[0094] It has been unexpectedly found that no extrusion or sonication is required to form the liposomes having the desired size and Zeta Potential characteristics, according to the methods described herein. In embodiments, sonication and/or extrusion of the liposomes is specifically excluded from the disclosed methods. In further embodiments, the methods of preparing targeted cationic liposomes described throughout suitably consist of or consist essentially of the recited elements. In such embodiments, addition of steps such as extrusion, are considered a material alterations to such methods and thus are specifically excluded from such methods that consist essentially of the recited elements.

[0095] Preparation of liposomes by mixing the lipids (in Chloroform) together, evaporating to dryness and reconstituting with water containing the drug in solution (a common procedure for liposome encapsulation of drugs), did not produce a homogeneous population. Measurement by light scattering gave poor results, with the quality report indicating that the cumulant fit error was high, thus the data quality was too poor for cumulant analysis, and the sample too polydisperse for cumulant analysis. The Z-Average (d-nm) for this preparation was 743.9nm (number average).

[0096] The temozolomide, melphalan, atropine, irinotecan or premetrexed cationic liposomes formed according to the injection methods described herein are then mixed with a ligand to form the targeted temozolomide, melphalan, atropine, irinotecan or premetrexed cationic liposomes. As described throughout, the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome. In other embodiments, the ligand can be chemically conjugated to the cationic liposome.

[0097] As used herein the term "ligand" refers to any suitable targeting moiety that can be either chemically conjugated to, or directly associated/complexed with, but not chemically conjugated to, the cationic liposomes. In embodiments where the ligand is directly associated/complexed with the cationic liposomes, no linker, spacer or other bridging molecule is used complex the ligands to the liposomes. Exemplary ligands for use in the practice of the present invention include, but are not limited to, proteins (e.g., transferrin or folate), peptides (e.g., L-37pA), antibodies, antibody fragments (including Fab' fragments and single chain Fv fragments (scFv)) and sugars (e.g., galactose), as well as other targeting molecules.

[0098] In exemplary embodiments, a whole antibody or an antibody fragment can be used as the ligand to make the complexes of this invention. In a suitable embodiment, an antibody fragment is used, including Fab fragments and single chain Fv fragments (scFv) of an antibody. One suitable antibody is an anti-Transferrin receptor (anti-TfR) monoclonal antibody, and a suitable antibody fragment is an scFv based on an anti-TfR monoclonal antibody (TfRscFv). An scFv contains the complete antibody binding site for the epitope of the TfR recognized by this MAb as a single polypeptide chain of approximate molecular weight 26,000. An scFv is formed by connecting the component VH and VL variable domains from the heavy and light chains, respectively, with an appropriately designed peptide, which bridges the C-terminus of the first variable region and N-terminus of the second, ordered as either VH-peptide-VL or VL-peptide-VH. Additional ligands, such as those described throughout, can also be used in the practice of the present invention.

[0099] In one embodiment, a cysteine moiety is added to the C-terminus of the scFv. Although not wishing to be bound by theory, it is believed that the cysteine, which provides a free sulfhydryl group, may enhance the formation of the complex between the antibody and the liposome in both the chemically conjugated and non-chemically conjugated embodiments. With or without the cysteine, the protein can be expressed in

E. coli inclusion bodies and then refolded to produce the antibody fragment in active form.

[00100] Suitable ligands, for example, proteins/peptides, antibody or antibody fragments, are those which will bind to the surface of the target cell, and preferably to a receptor that is differentially expressed on the target cell. The ligands are mixed with the cationic liposome at room temperature and at a ligand (e.g., protein, antibody or antibody fragment):lipid ratio (weight:weight) in the range of about 1:10 (0.01:1) to about 1:50, suitably about 1:20 to about 1:40 (w:w). Suitably, the weight ratio of ligand:lipid is about 0.01:1 to about 0.5:1, about 0.3:1 to about 0.4:1, or about 0.33:1, including any ratio within these ranges. The ligand (e.g., the protein/peptide, antibody or antibody fragment) and the liposome are allowed to incubate at room temperature for a short period of time, typically for about 10-15 minutes.

[00101] The size of the liposome complex is typically within the range of about 5-1000 nm as measured by dynamic light scattering using a Malvern ZETASIZER® 3000 or a Malvern ZETASIZER® NANO-ZS. *See* U.S. Published Patent Application No. 2003/0044407 and U.S. Patent Application No. 11/520,796, the disclosures of which are incorporated by reference herein in their entireties. The size of the liposomes is demonstrated by a single peak, representing a homogenous size population. More suitably, the size of the liposome complex prior to the addition of the ligand is in the range of about 5 nm to about 500 nm, about 5 nm to about 300 nm, about 5 nm to about 200 nm, about 5 nm to about 100 nm, about 10 nm to about 70 nm, or about 20 nm to about 60 nm. The size of the liposome complex following addition of the ligand is suitably in the range of about 5 nm to about 800 nm, about 10 nm to about 500 nm, about 20 nm to about 400 nm, about 20 nm to about 200 nm, or about 30 nm to about 200 nm.

[00102] Suitably the liposomes described herein have a positive Zeta Potential. Suitably the Zeta Potential of the liposomes prior to the addition of the ligand are about 1 mV to about 200 mV, about 1 mV to about 100 mV, about 10 mV to about 100 mV, about 20 mV to about 60 mV, or about 30 mV to about 50 mV. Suitable the Zeta Potential of the liposomes following the addition of the ligand are about 1 mV to about 200 mV, about 1 mV to about 100 mV, about 10 mV to about 80 mV, about 10 mV to about 60 mV, or about 25 mV to about 50 mV.

[00103] In embodiments, liposomes used to form the complex as described herein are sterically stabilized liposomes. Sterically stabilized liposomes are liposomes into which a hydrophilic polymer, such as PEG, poly(2-ethylacrylic acid), or poly(n-isopropylacrylamide (PNIPAM) has been integrated. Such modified liposomes can be particularly useful, as they typically are not cleared from the bloodstream by the reticuloendothelial system as quickly as are comparable liposomes that have not been so modified. To make a sterically stabilized liposome complex of the present invention, a cationic liposome comprising temozolomide, melphalan, atropine, irinotecan or premetrexed is prepared as above. To this liposome is added a solution of a PEG polymer in a physiologically acceptable buffer at a ratio of about 0.1:100 (nmol of PEG:nmol of liposome), suitably, about 0.5:50, for example, about 1:40 (nmol of PEG:nmol of liposome). The resultant solution is incubated at room temperature for a time sufficient to allow the polymer to integrate into the liposome complex. The ligand (e.g., protein/peptide, antibody or antibody fragment) then is mixed with the stabilized liposome complex at room temperature and at a ligand (e.g., protein):lipid ratio in the range of about 1:5 to about 1:40 (w:w).

[00104] As described herein, the ligand (e.g., protein/peptide, antibody or antibody fragment) is suitably directly associated (complexed) with the liposome via an interaction (e.g., electrostatic, van der Walls, or other non-chemically conjugated interaction) between the ligand and the liposome. In general, a linker or spacer molecule (e.g., a polymer or other molecule) is not used to attach the ligands and the liposome when non-chemically conjugated.

[00105] As described herein, in additional embodiments, the ligand (e.g., protein/peptide, antibody or antibody fragment) is chemically conjugated to the cationic liposomes, for example, via a chemical interaction between the cationic liposome which contains a maleimidyl group or other sulfhydryl-reacting group, and a sulfur atom on the ligand (e.g., protein/peptide, antibody or antibody fragment). Such methods of direct chemical conjugation are disclosed in U.S. Patent Application No. 09/914,046, filed October 1, 2001, the disclosure of which is incorporated by reference herein in its entirety.

[00106] Suitable ratios of lipid:temozolomide for use in the methods and liposomes are described throughout. In exemplary embodiments, the molar ratio of

lipid:temozolomide is about 0.1:1 to about 1:100, about 0.05:1 to about 1:50, about 1:1 to about 1:20, about 2:1 to about 10:0.1, about 0.5:1 to about 2:1, or about 1:1.

[00107] Suitable ratios of lipid:melphalan for use in the methods and liposomes are described throughout. In exemplary embodiments, the molar ratio of lipid: melphalan is about 0.1:1 to about 1:100, about 0.05:1 to about 1:50, about 1:1 to about 1:20, about 2:1 to about 10:0.1, about 0.5:1 to about 2:1, or about 1:1.

[00108] Suitable ratios of lipid:atropine, irinotecan or premetrexed for use in the methods and liposomes are described throughout. In exemplary embodiments, the molar ratio of lipid: atropine, irinotecan or premetrexed is about 0.1:1 to about 1:100, about 0.05:1 to about 1:50, about 1:1 to about 1:20, about 2:1 to about 10:0.1, about 0.5:1 to about 2:1, or about 1:1.

[00109] Encapsulation efficiency for the TMZ liposomes is suitably in the range of about 20% to about 100%, about 20% to about 80%, about 20 % to about 60%, or about 20% to about 55%, encapsulated TMZ. This is a surprising an unexpected result of the ethanol injection method for encapsulating TMZ in the liposomes.

[00110] Encapsulation efficiency for the melphalan liposomes is suitably in the range of about 20% to about 100%, about 20% to about 80%, about 20 % to about 60%, or about 20% to about 40%, encapsulated melphalan. This is a surprising an unexpected result of the ethanol injection method for encapsulating melphalan in the liposomes.

[00111] Encapsulation efficiency for the atropine, irinotecan or premetrexed liposomes is suitably in the range of about 20% to about 100%, about 20% to about 80%, about 20 % to about 60%, or about 20% to about 40%, encapsulated atropine, irinotecan or premetrexed. This is a surprising an unexpected result of the ethanol injection method for encapsulating atropine, irinotecan or premetrexed in the liposomes.

[00112] In additional embodiments, the liposomes can also comprise endosomal disrupting peptides, such as the $K[K(H)KKK]_5$-K(H)KKC (HoKC) (HK) (SEQ ID NO: 1) peptide manufactured by Sigma-Genosys (The Woodlands, TX), associated with the liposomes. The endosomal disrupting peptide HoKC may help the release of TMZ, melphalan, atropine, pemetrexed or irinotecan in the cytoplasm of the cells. In such embodiments, the liposomes suitably also comprise MPB-DOPE at 5 molar percent of total lipid. Since the HoKC peptide ($K[K(H)KKK]_5$-K(H)KKC) carries a terminal cysteine, MPB-DOPE is included to allow conjugation of the peptide to the liposome. The Lip-HoKC liposomes were prepared using the coupling reaction between the

cationic liposomes carrying the maleimide group (Lip-MPB) and the peptide. An aliquot of 0.1 mmol of the peptide with a free thiol group on cysteine was added to 2 mmol of Lip-MPB in 10 mM HEPES, pH 7.4, solution and rotated at room temperature (20-30 r.p.m.) for 2 h.

[00113] The liposomal complexes prepared in accordance with the present invention can be formulated as a pharmacologically acceptable formulation for *in vivo* administration. The complexes can be combined with a pharmacologically compatible vehicle or carrier. The compositions can be formulated, for example, for intravenous administration to a mammal, for example a human patient to be benefited by administration of the TMZ, melphalan, atropine, irinotecan or premetrexed in the complex. The complexes are sized appropriately so that they are distributed throughout the body following i.v. administration. Alternatively, the complexes can be delivered via other routes of administration, such as intratumoral (IT), intralesional (IL), sublingual (SL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), intraocular (IO), intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump. Preparation of formulations for delivery via such methods, and delivery using such methods, are well known in the art.

[00114] The complexes can be optimized for target cell type through the choice and ratio of lipids, the ratio of ligand (e.g., protein/peptide, antibody or antibody fragment) to liposome, the ratio of ligand and liposome to TMZ, melphalan, atropine, irinotecan or premetrexed and the choice of ligand.

[00115] The complexes made in accordance with the methods of this invention can be provided in the form of kits for use in the delivery of TMZ, melphalan, atropine, irinotecan or premetrexed. Suitable kits can comprise, in separate, suitable containers, the targeted TMZ, melphalan, atropine, irinotecan or premetrexed cationic liposome complexes (suitably dried, lyophilized powders) and a suitable buffer. The components can be mixed under sterile conditions in the appropriate order and administered to a patient within a reasonable period of time, generally from about 30 minutes to about 24 hours, after preparation. Liposomes are suitably prepared in sterile water-for-injection, along with appropriate buffers, osmolarity control agents, etc. The complete complex is suitably formulated as a dried powder (lyophilized) (*see, e.g.*, U.S. Published Patent

Application No. 2005/0002998, the disclosure of which is incorporated by reference herein in its entirety).

[00116] The cationic liposome complexes of the present invention suitably comprise an anti-transferrin receptor single chain antibody molecule (TfRscFv) on their surface. It has been determined that this targeting molecule enhances delivery across the blood-brain barrier and targeted delivery to brain cancer cells. The targeted liposomes can also be used to treat other cancers in the body and to deliver other drugs.

[00117] Also provided are cationic liposome complexes prepared according to the methods described throughout. For example, ligand-targeted (e.g., protein/peptide, antibody- or antibody fragment-targeted) cationic liposome complexes comprising a cationic liposome, a ligand (e.g., protein/peptide, antibody or antibody fragment), and TMZ, melphalan, atropine, pemetrexed or irinotecan, wherein the ligand is directly complexed/associated with, but not chemically conjugated to the cationic liposome, are provided.

[00118] The TMZ, melphalan, atropine, irinotecan or premetrexed can be encapsulated within the cationic liposome (i.e., in the hydrophilic, aqueous interior of the liposomes), contained within a hydrocarbon chain region of the cationic liposome, associated with an inner or outer monolayer of the cationic liposome (e.g., the head-group region), or any combination thereof. Suitably, the cationic liposomes of the present invention are unilamellar liposomes (i.e. a single bilayer), though multilamellar liposomes which comprise several concentric bilayers can also be used. Single bilayer cationic liposomes of the present invention comprise an interior aqueous volume in which TMZ, melphalan, atropine, irinotecan or premetrexed can be encapsulated. They also comprise a single bilayer which has a hydrocarbon chain region (i.e., the lipid chain region of the lipids) in which TMZ, melphalan, atropine, irinotecan or premetrexed can be contained. In addition, TMZ, melphalan, atropine, irinotecan or premetrexed can be complexed or associated with either, or both, the inner monolayer and/or the outer monolayer of the liposome membrane (i.e., the head-group region of the lipids). In further embodiments, TMZ, melphalan, atropine, irinotecan or premetrexed can be encapsulated/associated/complexed in any or all of these regions of the cationic liposome complexes of the present invention.

[00119] In further embodiments, pharmaceutical compositions comprising the ligand-targeted cationic liposome complexes described throughout are provided. In

suitable embodiments, the pharmaceutical compositions further comprise one or more excipients selected from the group consisting of one or more antibacterials (e.g., amphotericin B, chloretracycline, gentamicin, neomycin), one or more preservatives (e.g., benzethonium chloride, EDTA, formaldehyde, 2-phenoxyethanol), one or more buffers (e.g., phosphate buffers, sodium borate, sodium chloride), one or more surfactants (polysorbate 20, 80), one or more protein stabilizers (e.g., albumin, lactose, potassium glutamate), sugars e.g. sucrose or dextrose, and adjuvants (e.g., aluminum hydroxide, aluminum phosphate). Additional excipients are well known in the art and can be readily used in the practice of the present invention.

[00120] Also provided are pharmaceutical compositions comprising a first ligand-targeted cationic liposome complex comprising a cationic liposome, a ligand (e.g., protein/peptide, antibody or antibody fragment), and TMZ, melphalan, atropine, irinotecan or premetrexed wherein the ligand is directly complexed/associated with, but not chemically conjugated to the cationic liposome. In further embodiments, the ligand can be chemically conjugated to the cationic liposome. The pharmaceutical compositions also suitably comprise a second ligand-targeted cationic liposome complex comprising a cationic liposome, a ligand (e.g., protein/peptide, antibody or antibody fragment), and one or more nucleic acid molecules (including plasmid DNA, siRNA or antisense nucleic acids), wherein the ligand is directly complexed/associated with, but not chemically conjugated to the cationic liposome. (*See* US Patent No. 7,780,822 and US Published Patent Application No. 2007/0065449, the disclosures of which are incorporated by reference herein in their entireties). In further embodiments, the compositions can also comprise a ligand-targeted cationic liposome complex comprising a ligand (e.g., protein/peptide, antibody or antibody fragment), and one or more small molecules (*see* U.S. Published Patent Application No. 2007/0231378, the disclosure of which is incorporated by reference herein in its entirety) or one or more imaging agents (*see* U.S. Published Patent Application No. 2007/0134154, the disclosure of which is incorporated by reference herein in its entirety), wherein the ligand is directly complexed/associated with, but not chemically conjugated to the cationic liposome. In further embodiments, the ligand can be chemically conjugated to the cationic liposome in such compositions.

[00121] Also provided are pharmaceutical compositions comprising a first ligand-targeted cationic liposome complex comprising a cationic liposome, a ligand

(e.g., protein/peptide, antibody or antibody fragment), and TMZ, melphalan, atropine, irinotecan or premetrexed wherein the ligand is directly complexed/associated with, but not chemically conjugated to the cationic liposome. In further embodiments, the ligand can be chemically conjugated to the cationic liposome. The pharmaceutical compositions also suitably comprise a second ligand-targeted cationic liposome complex comprising a cationic liposome, a ligand (e.g., protein/peptide, antibody or antibody fragment), and one or more nucleic acid molecules (including plasmid DNA, siRNA or antisense nucleic acids), one or more small molecules, or one or more imaging agents (including superparamagnetic iron oxide, or gadolinium) wherein the nucleic acid molecules, small molecules, or imaging agents down-regulates, modifies or otherwise negates the effect of MGMT in the cancer cell.

[00122] In further embodiments, methods of treating cancer in a patient are provided. Suitably, such methods comprise administering to a patient a targeted cationic liposome complex as described herein. Suitably the complexes are prepared according to the methods described throughout.

[00123] In embodiments, the methods of treatment comprise administering to a patient a targeted temozolomide or melphalan cationic liposome complex, wherein the cationic liposome complex comprises a cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), temozolomide or melphalan, and a ligand complexed with, but not chemically conjugated to, the cationic liposome.

[00124] As described throughout, the ligand is suitably an antibody, an antibody fragment or a protein, including a single chain Fv antibody fragment. In exemplary embodiments, the single chain Fv antibody fragment is an anti-transferrin receptor single chain Fv (TfRscFv).

[00125] Also provided of methods of treating organophosphate poisoning (i.e., nerve gas poisoning) in a patient, comprising administering to the patient a targeted atropine cationic liposome complex, wherein the targeted atropine cationic liposome complex comprises cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), atropine and a ligand directly complexed with, but not chemically conjugated to, the cationic liposome. Exemplary ligands are described herein.

[00126] Suitably the temozolomide is administered to the patients utilizing the methods described herein at a dose of about 1 mg/m^2 to about 1000 mg/m^2, more suitably at a dose of about 10 mg/m^2 to about 500 mg/m^2, or about 50 mg/m^2 to about 400 mg/m^2, about 80 mg/m^2 to about 300 mg/m^2, about 50 mg/m^2 to about 250 mg/m^2, about 50 mg/m^2 to about 250 mg/m^2, or about 50 mg/m^2, about 60 mg/m^2, about 70 mg/m^2, about 80 mg/m^2, about 90 mg/m^2, about 100 mg/m^2, about 110 mg/m^2, about 120 mg/m^2, about 130 mg/m^2, about 140 mg/m^2, about 150 mg/m^2, about 160 mg/m^2, about 170 mg/m^2, about 180 mg/m^2, about 190 mg/m^2, about 200 mg/m^2, about 210 mg/m^2, about 220 mg/m^2, about 230 mg/m^2, about 240 mg/m^2, about 250 mg/m^2, about 260 mg/m^2, about 270 mg/m^2, about 280 mg/m^2, about 290 mg/m^2, or about 300 mg/m^2.

[00127] Suitably the melphalan is administered to the patients utilizing the methods described herein at a dose of about 1 mg/m^2 to about 500 mg/m^2, more suitably at a dose of about 1 mg/m^2 to about 100 mg/m^2, or about 1 mg/m^2 to about 50 mg/m^2, about 1 mg/m^2 to about 30 mg/m^2, about 5 mg/m^2 to about 20 mg/m^2, or about 6 mg/m^2 to about 16 mg/m^2, or about 1 mg/m^2, about 2 mg/m^2, about 3 mg/m^2, about 4 mg/m^2, about 5 mg/m^2, about 6 mg/m^2, about 7 mg/m^2, about 8 mg/m^2, about 9 mg/m^2, about 10 mg/m^2, about 11 mg/m^2, about 12 mg/m^2, about 13 mg/m^2, about 14 mg/m^2, about 15 mg/m^2, about 16 mg/m^2, about 17 mg/m^2, about 18 mg/m^2, about 19 mg/m^2, about 20 mg/m^2, about 21 mg/m^2, about 22 mg/m^2, about 23 mg/m^2, about 24 mg/m^2, or about 25 mg/m^2.

[00128] Suitably the atropine, irinotecan or premetrexed is administered to the patients utilizing the methods described herein at a dose of about 1 mg/m^2 to about 1000 mg/m^2, more suitably at a dose of about 10 mg/m^2 to about 500 mg/m^2, or about 50 mg/m^2 to about 400 mg/m^2, about 80 mg/m^2 to about 300 mg/m^2, about 100 mg/m^2 to about 250 mg/m^2, or about 50 mg/m^2, about 60 mg/m^2, about 70 mg/m^2, about 80 mg/m^2, about 90 mg/m^2, about 100 mg/m^2, about 110 mg/m^2, about 120 mg/m^2, about 130 mg/m^2, about 140 mg/m^2, about 150 mg/m^2, about 160 mg/m^2, about 170 mg/m^2, about 180 mg/m^2, about 190 mg/m^2, about 200 mg/m^2, about 210 mg/m^2, about 220 mg/m^2, about 230 mg/m^2, about 240 mg/m^2, about 250 mg/m^2, about 260 mg/m^2, about 270 mg/m^2, about 280 mg/m^2, about 290 mg/m^2, or about 300 mg/m^2.

[00129] In embodiments, the atropine is administered to the patients (suitably intramuscularly) utilizing the methods described herein at a dose of about 0.01 mg to about 100 mg, more suitably at a dose of about 0.1 mg to about 50 mg, or about 1 mg to

about 40 mg, about 1 mg to about 30 mg, about 1 mg to about 20 mg, about 1 mg to about 10 mg, about 2 mg to about 6 mg, or about 1 mg, about 2 mg, about 3 mg, about 4 mg, about 5 mg, about 6 mg, about 7 mg, about 8 mg, about 9 mg, about 10 mg, about 11 mg, about 12 mg, about 13 mg, about 14 mg, about 15 mg, about 16 mg, about 17 mg, about 18 mg, about 19 mg or about 20 mg.

[00130] As described herein, in embodiments, the molar ratio of lipid in the cationic liposome:temozolomide, melphalan, atropine, irinotecan or premetrexed for use in the methods described herein is about 0.1:1 to about 5:1. More suitably, the molar ratio of lipid in the cationic liposome:temozolomide, melphalan, atropine, irinotecan or premetrexed is about 0.1:1 to about 1:100, about 0.05:1 to about 1:50, about 1:1 to about 1:20, about 2:1 to about 10:0.1, about 0.5:1 to about 2:1, or about 1:1.

[00131] The weight ratio of ligand:lipid in the cationic liposome for use in the methods described herein is suitably about 0.01:1 to about 0.5:1. Suitably, the weight ratio of ligand:lipid in the cationic liposome is about 0.01:1 to about 0.5:1, about 0.3:1 to about 0.4:1, or about 0.33:1, including any ratio within these ranges.

[00132] Suitable methods of administration include, but are not limited to, intravenous (IV), intratumoral (IT), intralesional (IL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), sublingual (SL), intradermal (ID), intraocular (IO), intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump. They can be administered as a bolus or as an infusion. In additional embodiments, the ligand can be chemically conjugated to the cationic liposome using the various methods described herein or otherwise known in the art.

[00133] Exemplary cancers that can be treated using the methods described herein include, but are not limited to, cancers of the head and neck, breast, prostate, pancreatic, brain, including glioblastoma and astrocytoma, neuroendocrine, cervical, lung, liver, liposarcoma, rhabdomyosarcoma, choriocarcinoma, melanoma, retinoblastoma, ovarian, urogenital, gastric, colorectal cancers, multiple myeloma and cancers of the blood.

[00134] As described herein, it has been surprisingly found that the targeted cationic liposomes prepared by the disclosed methods are able to cross the blood-brain barrier. Generally, this barrier is a significant hindrance to treatments designed to treat cancers

and other diseases or conditions of the brain or other treatments designed to deliver drugs to the brain. Thus, in embodiments, the methods described in herein are useful in the successful treatment of brain cancers, including gliomas, and in general to deliver drugs across the blood-brain barrier

[00135] In another embodiment the methods described herein can also be used as a treatment for organophosphate poisoning.

[00136] As described herein, it has been surprisingly found that the targeted cationic liposomes prepared by the disclosed methods are able to efficiently deliver enough TMZ to target tumor cells that are resistant to standard unencapsulated TMZ to overcome their inherent resistance, which may be due to activated MGMT, resulting in these tumor cells now responding to TMZ.

[00137] As described herein, it has been surprisingly found that the targeted cationic liposomes prepared by the disclosed methods are able to induced cell death (apoptosis) in tumor cells that are resistant to the killing effects of TMZ administered without the targeted cationic liposomes.

[00138] As described herein, it has been surprisingly found that the targeted cationic liposomes prepared by the disclosed methods are able to induced apoptosis in cancer stem cells (CSC) as well as differentiated cancer cells (non-CSC) in tumors irrespective of their response to TMZ administered without the targeted cationic liposomes.

[00139] As described herein, it has been surprisingly found that the level of apoptosis induced by the targeted cationic liposomes prepared by the disclosed methods is proportionally greater in cancer stem cells (CSC) than in differentiated cancer cells (non-CSC) in tumors.

[00140] As described herein, it has been surprisingly found that treatment of tumors with the targeted cationic liposomes prepared by the disclosed methods not only induce tumor growth inhibition, but also result in tumor regression and that this response can be maintained even after the treatment has ended.

[00141] As described herein, it has been surprisingly found that treatment of tumor cells with the targeted cationic liposomes prepared by the disclosed methods not only induce tumor growth inhibition, but also result in tumor regression and that this response can be maintained even after the treatment has ended.

[00142] In suitable embodiments, the methods further comprise administering an additional therapy to the patient in combination with the targeted temozolomide

cationic liposome complex. Exemplary therapies that can be utilized include, administration of chemotherapeutic agent, small molecule, radiation therapy or a nucleic acid-based therapy. Exemplary chemotherapeutic agents include docetaxel, mitoxantrone, doxorubicin and gemcitabine. Exemplary small molecules include, but are not limited to, imatinib mesylate (GLEEVEC™), Erlotinib hydrochloride (TARCEVA™), Sunitinib Malate (SU11248, SUTENT™) and Gefitinib (IRESSA™). Exemplary nucleic acid-acid based therapies (including tumor suppressor genes, antisense oligonucleotides or siRNA) include those disclosed in U.S. Published Patent Application No. 2007/0065499 and U.S. Patent No. 7,780,882, the disclosures of each of which are incorporated by reference herein in their entireties. In suitable embodiments, the nucleic acid-based therapy comprises administration of a cationic liposome complex comprising plasmid DNA encoding the wtp53 gene and targeted via TfRscFv (scL-p53), as described in U.S. Patent No. 7,780,882.

[00143] Also provided are methods treating a brain cancer of a patient, comprising administering to the patient a cationic liposome complex as described in U.S. Patent No. 7,780,882. Suitably, the complex comprises a cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), a plasmid DNA expressing wild-type p53 and an anti-transferrin receptor single chain Fv (TfRscFv) directly complexed with, but not chemically conjugated to, the cationic liposome. The methods further comprise administering temozolomide, suitably at the same time or after administration of the cationic liposome complex.

[00144] It will be readily apparent to one of ordinary skill in the relevant arts that other suitable modifications and adaptations to the methods and applications described herein may be made without departing from the scope of the invention or any embodiment thereof. Having now described the present invention in detail, the same will be more clearly understood by reference to the following examples, which are included herewith for purposes of illustration only and are not intended to be limiting of the invention.

Example 1

Preparation of Cationic Liposomes Comprising Temozolomide

Materials:

[00145] DOTAP (1,2-dioleoyl-3-trimethylammonium propane, chloride salt)
Obtained from Avanti Polar Lipids, Inc. Cat. #890890E, MW 698.55
Concentration: 25 mg/mL ethanol solution
Dilute lipid to 20mg/ml with absolute ethanol before use

[00146] DOPE (1,2-dioleoyl-sn-glycero-3-phosphoethanolamine)
Obtained from Avanti Polar Lipids, Inc. Cat. # 850725E, MW 744.04
Concentration: 25 mg/mL ethanol solution.
Dilute lipid to 20mg/ml with absolute ethanol before use

[00147] Temozolomide (TMZ, M.W. 194.15), powder
Obtained from Sigma, Cat. # T2577 – 100 mg
Dissolve TMZ in pure DMSO to desired concentration. For example, 19.415 mg/ml = 100mM of TMZ; 28 mg/ml = 144.218mM of TMZ

[00148] Ultra-pure, endotoxin free LAL Reagent Water (e.g. BioWhittaker, Cat.# W50-500, endotoxin <0.005 EU/ml)

[00149] Injector: Hamilton Gastight Syringe, 1ml (Hamilton #81230) with a 22 gauge needle, part #81365)

Procedure:

[00150] 1) Fresh TMZ solution is prepared by dissolving TMZ in DMSO to the desired concentration by vortexing at high speed for 5-10 mins (must be clear). The solution is held at room temperature until used to mix with lipids.

[00151] 2) Place lipid solutions at 37° C for 10-15 min. The lipid solutions are then placed in a 65° C water bath with occasional shaking for 5 min.

[00152] 3) To prepare the Lip-TMZ: Place a brown glass bottle with stir bar on a hot plate set to 50°C to 60°C. While stirring at high speed without splashing, add the lipids

and TMZ to the bottle in the following order. It should be noted that other component ratios and concentrations as described herein can be prepared using the same protocol as shown below.

[00153] For 0.5:1 (Lip:TMZ) molar ratio (2 mM TMZ in formulation)

DOTAP 87.5 µl (of 20 mg/ml) = 2.5 µmol or 1.75 mg

DOPE 93.75 µl (of 20 mg/ml) = 2.5 µmol or 1.875 mg

Add TMZ-HCl soln., 100 µl (of 19.41 mg/ml) = 10 µmol,

[00154] Continue stir for 3 min. after all 3 are added

[00155] For 1:1 (Lip:TMZ) molar ratio (2 mM TMZ in formulation)

DOTAP 175 µl (of 20 mg/ml) = 5 µmol or 3.5 mg

DOPE 187.5 µl (of 20 mg/ml) = 5 µmol or 3.75 mg

Add TMZ-HCl soln., 100 µl (of 19.41 mg/ml) = 10 µmol,

[00156] Continuously stir for 3 min. after all 3 added

[00157] For 1:1 (Lip:TMZ) molar ratio (8 mM TMZ in formulation)

DOTAP 560 µl (of 25 mg/ml) = 20 µmol or 14 mg

DOPE 600 µl (of 25 mg/ml) = 20 µmol or 15 mg

Add TMZ soln., 277.36 µl (of 28 mg/ml) = 40 µmol,

[00158] Continuously stir for 3 min. after all 3 added

[00159] For 2:1 (Lip:TMZ) molar ratio (2 mM TMZ in formulation)

DOTAP 350 µl (of 20 mg/ml) = 10 µmol or 7 mg

DOPE 375 µl (of 20 mg/ml) = 10 µmol or 7.5 mg

Add TMZ-HCl soln., 100 µl (of 19.41 mg/ml) = 10 µmol,

[00160] Continuously stir for 3 min. after all 3 added

[00161] 4) Warm 4 mL LAL water to 65° C in water bath in brown glass bottle with stir bar. Immediately prior to addition of the Lipid-TMZ solution, move the bottle to a hot plate (50° - 60° C). Stir water at high speed with no splashing for a few seconds to remove bubbles from the stir bar.

[00162] 5) Keep the water on the hot plate. Continue stirring the water at high speed (without splashing) during lipid addition. After mixing lipids and TMZ as above, immediately and as rapidly as possible, using the Hamilton syringe for injection, inject the mixture into the hot water on the hot plate (50° - 60° C) directly into the center of the vortex. Continue stirring on high speed (without splashing) for 1 min after the addition of the lipid mixture while loosely covered.

[00163] 6) Move the glass bottle to a room temperature stir plate and continue to stir slowly until the loosely covered solution cools down to 20-25° C (room temperature).

[00164] 7) Adjust the volume to 5 ml with room temperature LAL water.

[00165] 8) Filter the solution using a 0.22 μm pore Milex GV filter if desired.

[00166] 9) Measure particle size and zeta potential if desired.

[00167] Results of these preparation methods demonstrate approximately at least 30-40% loading, suitably at least 50-55% loading, of TMZ and liposomes having a particle size of about 20-60 nm and a Zeta Potential of about 30 to 50 mV.

Example 2

Preparation of scL-TMZ Without Chemical Conjugation (By Simple Mixing)

[00168] Using the TMZ-comprising cationic liposomes prepared according to the procedure described in Example 1, the ligand targeted TMZ cationic liposome complex as described herein is prepared by simple mixing of the components and without chemical conjugation. The preparation of the complexes was in accordance with the following general procedure:

[00169] To the liposome-water (or buffer) the appropriate amount of targeting moiety is added to give the desired ratio and mixed by gentle inversion 5-10 seconds. The targeting moiety can be a ligand including but not limited to transferrin or folate, or other proteins. It can also be an antibody or an antibody fragment that targets a cell surface receptor including, but not limited to the transferrin or HER-2 receptor (e.g., TfRscFv). This mixture is kept at room temperature for 10-15 minutes (again inverted gently for 5-10 seconds after approximately 5 minutes). To yield the desired final volume the targeting moiety-Lip-TMZ admixture is mixed with any volume (including none) of water (suitably deionized water) or a buffer of any pH including, but not limited to, Tris buffers, HEPES buffers or Phosphate Buffered Saline, required to give a desired volume and inverted gently for 5-10 seconds to mix. This mixture is kept at room temperature for 10-15 minutes (again inverted gently for 5-10 seconds after approximately 5 minutes).

[00170] Typically, for use in an *in vitro* assay, it is desirable that the amount of TMZ in the final complex is in the range of about 1 μM to 300 μM per well; for *in vivo* use, it is desirable to provide about 1mg/kg to about 50mg/kg of TMZ per injection. For use *in vivo* dextrose or sucrose is added last to a final concentration of about 1-50% (V:V) dextrose or sucrose, suitably 5% dextrose or 10% sucrose, and mixed by gentle inversion for 5-10 seconds. This mixture is kept at room temperature for 10-15 minutes (again inverted gently for 5-10 seconds after approximately 5 minutes).

[00171] A specific example at a suitable ratio of 1:30 (antibody fragment:liposome, w:w) and 1:1 Liposome:TMZ (molar ratio) is as follows: For a final volume of approximately 700 uL, at a TMZ concentration of 25mg/kg/injection, mix 319 μL of Lip:TMZ (8 mM stock) with 305 μL of antibody fragment (at an anti-transferrin receptor single chain antibody fragment [TfRscFv] concentration of 0.2 mg/mL). Add 6 μL of water or buffer and, as the last step, 70 μL of 50% Dextrose or no water or buffer and 140uL of 50% sucrose.

[00172] A second specific example at a preferred ratio of 1:30 (antibody fragment:liposome, w:w) and 1:1 Liposome:TMZ (molar ratio) is as follows: For a final volume of approximately 1.8 mL, at a TMZ concentration of 25mg/kg/injection, mix 1276 μL of Lip:TMZ (2 mM stock) with 305 μL of antibody fragment (at an anti-transferrin receptor single chain antibody fragment [TfRscFv] concentration of 0.2 mg/mL). 39 μL of water or buffer is added and 180 μL of 50% Dextrose is added as the last step.

[00173] Another specific example at a preferred ratio of 1:30 (antibody fragment:liposome, w:w) and 1:1 Liposome:TMZ (molar ratio) is as follows: For a final volume of approximately 400 μL, at a TMZ concentration of 5mg/kg/injection, mix 280 μL of Lip:TMZ (2 mM stock) with 64 μL of antibody fragment (at an anti-transferrin receptor single chain antibody fragment [TfRscFv] concentration of 0.2 mg/mL). 16.5 μL of water or buffer is added and 40 μL of 50% Dextrose is added as the last step.

[00174] The size (number average) of the final complex prepared by the methods is between about 10 to 800 nm, suitably about 20 to 400 nm, most suitably about 25 to 200 nm with a zeta potential of between about 1 and 100 mV, more suitably 10 to 60 mV and most suitably 25 to 50mV as determined by dynamic light scattering using a

Malvern Zetasizer ZS. This size is small enough to efficiently pass through the tumor capillary bed, or cross the blood brain barrier, and reach the tumor cells.

Example 3

In Vitro Efficacy of Targeted Cationic Liposomes Comprising Temozolomide

[00175] Human glioblastoma multiforme (GBM) cell lines U87MG and T98G were obtained from ATCC (Manassas, VA). U87 is derived from a grade IV glioblastoma, and carries wtp53 (Van Meir EG, Kikuchi T, Tada M, Li H, Diserens A C, Wojcik B E, Huang H J S, Friedmann T, Detribolet N and Cavenee W K (1994) Analysis of the P53 Gene and Its Expression in Human Glioblastoma Cells. Cancer Research 54: pp 649-652). A version of U87MG that stably expresses the luciferase gene has been obtained from Caliper Life Sciences for use in *in vivo* studies where tumor growth and response will be monitored by the IVIS® Imaging System, Xenogen. The human GBM cell line U251 was obtained from the Division of Cancer Treatment and Diagnosis Tumor Repository, National Cancer Institute-Frederick (Frederick, MD). Cells were maintained at 37°C in a 5% CO_2 atmosphere in modified IMEM (Gibco, Grand Island, NY; U87 and U87MG-luc2 cells), MEM (Mediatech Manassas, VA; T98G cells), or RPMI 1640 medium (Gibco; U251 cells) supplemented with 10% heat-inactivated fetal bovine serum (Omega Scientific, Tarzana, CA), 2 mmol/L L-glutamine (Mediatech, Manassas, VA), and 50 μg/mL each of penicillin, streptomycin, and neomycin (PSN). Cells were grown to 70-80% confluence before the next passage or further experiments through trypsinization using TrypLE Express (Gibco). Sodium 3'-[1-(phenylamino-carbonyl)-3, 4-tetrazolium]-bis (4-methoxy-6-nitro)benzene sulfonate (XTT) was purchased from Polysciences (Warrington, PA).

[00176] The human multiple myeloma cell line KMS-11 was maintained at 37°C in a 5% CO_2 atmosphere in RPMI 1640 medium supplemented with 10% heat-inactivated fetal bovine serum 2 mmol/L L-glutamine and 50 μg/mL each of penicillin, streptomycin, and neomycin (PSN). Cells were grown to 70-80% confluence before the next passage or further experiments. These cells grow in suspension and not as monolayers.

[00177] U87MG is categorized as being sensitive to TMZ (Patil R, Portilla-Arias J, Ding H, Inoue S, Konda B, Hu J W, Wawrowsky K A, Shin P K, Black K L, Holler E and Ljubimova J Y (2010) Temozolomide Delivery to Tumor Cells by a Multifunctional Nano Vehicle Based on Poly(Beta-L-Malic Acid). Pharmaceutical Research 27: pp 2317-2329). This is a well established orthotopic mouse model of GBM (Liu Y, Lang F, Xie X, Prabhu S, Xu J, Sampath D, Aldape K, Fuller G and Puduvalli V K (2011) Efficacy of Adenovirally Expressed Soluble TRAIL in Human Glioma Organotypic Slice Culture and Glioma Xenografts. Cell Death & Disease 2). U87MG cells reproducibly develop tumors within 10 days when 5 x 10^5 cells are intracranially injected in athymic nude mice. The mice succumb to tumor burden within 30-40 days. T98G is also isolated from a human glioblastoma. However, this cell line is known to be resistant to TMZ (Patil R, Portilla-Arias J, Ding H, Inoue S, Konda B, Hu J W, Wawrowsky K A, Shin P K, Black K L, Holler E and Ljubimova J Y (2010) Temozolomide Delivery to Tumor Cells by a Multifunctional Nano Vehicle Based on Poly(Beta-L-Malic Acid). Pharmaceutical Research 27: pp 2317-2329) and carries a mutant form of the p53 gene (Van Meir EG, Kikuchi T, Tada M, Li H, Diserens A C, Wojcik B E, Huang H J S, Friedmann T, Detribolet N and Cavenee W K (1994) Analysis of the P53 Gene and Its Expression in Human Glioblastoma Cells. Cancer Research 54: pp 649-652). T98G xenograft tumors are induced via subcutaneous inoculation of 5-10 x 10^6 cells in Matrigel™ (Torres S, Lorente M, Rodriguez-Fornes F, Hernandez-Tiedra S, Salazar M, Garcia-Taboada E, Barcia J, Guzman M and Velasco G (2011) A Combined Preclinical Therapy of Cannabinoids and Temozolomide Against Glioma. Molecular Cancer Therapeutics 10: pp 90-103). Both cell lines have elevated TfR expression (Sang H, Kelley P Y, Hatton J D and Shew J Y (1989) Proto-Oncogene Abnormalities and Their Relationship to Tumorigenicity in Some Human Glioblastomas. Journal of Neurosurgery 71: pp 83-90).

[00178] Studies were carried out to compare the efficacy of standard free (unencapsulated) TMZ; and unliganded TMZ-containing liposomes (Lip-TMZ) The Lip-TMZ was prepared as described above in Example 1 using a liposome concentration of 2mM. The zeta potentials of the Lip-TMZ molecules ranged from 35.6-40.1mV. The TMZ concentration used was varied from 1 to about 250uM. The ratios of Liposome to TMZ was 0.5:1, 1:1 or 2:1 (molar ratio).

[00179] Human brain tumor derived U251 cells were plated in triplicate at 2×10^3 per well in a 96-well plate. Following overnight incubation, the medium was replaced with serum-free medium, overlaid with 100 μL of indicated concentrations of either Lip-TMZ, or free TMZ, incubated for 5 h, and then supplemented with fetal bovine serum. After incubation for an additional 91 h, cell viability was determined by the XTT assay as described previously (Rait A, Pirollo KF, Rait V, et al. Inhibitory effects of the combination of HER-2 antisense oligonucleotide and chemotherapeutic agents used for the treatment of human breast cancer. Cancer Gene Ther 2001;8:728–39.). Formazan absorbance, which correlates to cell viability, was measured at 450 nm using a microplate reader (Bio-Rad, Hercules, CA). The IC_{50} value, the drug concentration resulting in 50% cell kill, was interpolated from the graph of the log of drug concentration versus the fraction of surviving cells.

[00180] FIG. 1 demonstrates that in human brain tumor (GBM) cell line U251, compared with the effects of free TMZ, *in vitro* treatment with the liposome encapsulated TMZ as described herein resulted in a significant reduction in IC_{50} values in human GBM cells. Whereas, at the concentrations of TMZ used to treat the cells the unencapsulated TMZ had virtually no cell killing effect, when encapsulated in the liposome 50% of the cells were killed at TMZ concentrations of only 46.3 μM , 28.8 μM and 16 μM at Lip/TMZ molar ratios of 0.5:1, 1:1 and 2:1, respectively. The higher the ratio of Lip to TMZ, the greater the increase in cell killing effect, yielding a lower IC_{50} value. It is well known by those familiar with the art that free, unencapsulated TMZ is the form of the drug most commonly used to treat tumors in patients.

[00181] Similar results are shown in FIG. 2 with human GBM tumor cell line U87 comparing free TMZ and the Lip-TMZ at molar ratios of Liposome to TMZ of 1:1 and 2:1. Once again the unencapsulated TMZ has virtually no cell killing effect on these brain tumor cells. In contrast when encapsulated in the Liposome at molar ratios of 1:1 or 2:1 (Lip:TMZ) using the method of this invention, TMZ concentrations of only 11.4 and 21.5 μM, respectively resulted in significant tumor cell death.

Example 4

Increased Effect of scL-TMZ On Tumor Cells Compared to Free (unencapsulated) TMZ

[00182] The scL-TMZ complex was prepared as described above in Examples 1-2 using an anti-transferrin receptor single-chain antibody fragment (TfRscFv) as the targeting moiety, a Lip:TMZ molar ratio of 1:1(size = 46.2nm; zeta potential = 42.5mV) (liposome concentration = 2mM) and an TfRscFv to Liposome ratio if 1:30 (w:w). The size of the scL-TMZ complex was about 27.5nm. The *in vitro* cell killing ability of the scL-TMZ was compared to free, unencapsulated TMZ in TMZ resistant human brain tumor cell line T98G using the XTT assay.

[00183] FIG. 3A shows that tumor targeting scL-TMZ complex, has significantly improved anti-cancer efficacy compared to free TMZ. The free TMZ has an IC_{50} value > 1000 μM. In contrast, when prepared according to the methods described herein and delivered to the tumor cell by means of the tumor-targeting complex, at least 20 fold less TMZ effectively kills the cancer cells. This is especially significant as this GBM cell line is well known in the art to be resistant to the killing effects of TMZ. This reversal of resistance is due to the efficient delivery and uptake of the TMZ payload into the tumor cell by means of the binding of the targeting ligand (protein, antibody or antibody fragment) to its receptor on the cell and the triggering of uptake via either passive means or through active transport mechanisms like receptor mediated endocytosis. This process "floods" the cells with drug overcoming the mechanisms the tumor cell has in place to repair the DNA damage caused by TMZ (such as upregulation of MGMT), and/or the mechanisms to pump the TMZ out of the cells. Thus the cell dies.

[00184] There are a number of ramifications as a result of the tumor-targeting delivery of TMZ via the targeted cationic liposomes described herein.

[00185] 1) Increased efficacy means less drug needs to be delivered to the patient to see improved anti-tumor effect.

[00186] 2) Tumor-specific delivery (tumor specificity) will decrease the deleterious side-effects currently associated with TMZ as the drug will not be taken up by non-target cells.

[00187] 3) The efficient delivery of TMZ to the tumor cells overcomes the resistance to TMZ inherent in a significant population of brain tumors (GBM and astrocytomas) and other cancer types including, but not limited to, prostate cancer,

multiple myeloma, lung cancer, liver cancer, ovarian cancer, pancreatic cancer, head and neck cancer, kidney cancer, stomach cancer, and melanoma. This reversal of resistance broadens the scope of use for TMZ as an anti-cancer treatment.

[00188] FIG. 3B demonstrates that the method of this invention is not limited to sensitization of brain tumor cells to TMZ. The killing effects of scL-TMZ were compared to that of free (unencapsulated TMZ) in multiple myeloma cell line KMS-11. The scL-TMZ complex was prepared with different increasing doses of TMZ (0 to 100uM TMZ) as described above using an anti-transferrin receptor single-chain antibody fragment (TfRscFv) as the targeting moiety, a Lip:TMZ molar ratio of 1:1 (liposome concentration = 8mM) and an TfRscFv to Liposome ratio if 1:30 (w:w). The size of the scL-TMZ complex was about 143 nm. The *in vitro* cell killing ability of the scL-TMZ was compared to free, unencapsulated TMZ in multiple myeloma cell line KMS-11. Transfection was performed and the viability of the KMS-11 cells 48 hours post-transfection was assessed. TMZ has not previously been used to treat multiple myeloma, thus, it was very surprising that delivery of TMZ to these cells by encapsulation in the scL complex resulted in significant cell death , even at a very low concentration (25uM) of TMZ.

[00189] The identical methodology and procedures described above were used to prepare Lip-TMZ and scL-TMZ and the resultant scL-TMZ nanocomplex was also used to transfect prostate (DU145), lung (A549), ovarian (Hey-A8), pancreatic (PANC-1) and hepatocellular carcinoma (HEP-G2) cells. In all cases there was a significant increase in tumor cell response to the TMZ when it was encapsulated in the scL nanocomplex when compared to free (unencapsulated) TMZ, the current standard method of delivery.

Example 5

TfRscFV Liposomes Crossing the Blood Brain Barrier

[00190] Studies were performed to determine if the TfRscFv targeted liposome (scL) complex (scL) can cross the blood-brain barrier (BBB) and target tumors after i.v injection. Brain tumors were induced in nude mice by intracranial inoculation of $5x10^5$ U87 cells. Three weeks later, the mice were I.V. injected with uncomplexed free Cy5-ODN, scL-Cy5-ODN, or unliganded Lip-Cy5-ODN (without the targeting moiety;

unL-Cy5-ODN) (25μg/ mouse) (2 mice/group). Twenty-four hours post- injection, mice were euthanized and tumor-bearing brains imaged using the Maestro™ *in vivo* fluorescence imaging system. Fluorescence intensity of the brain tumors were compared using the Maestro™ software. I.V. injection of scL-Cy5-ODN resulted in a strong fluorescence signal specifically in the brain tumor (FIG. 4A). In contrast, only low levels of fluorescence were observed in the tumors after injection of either free Cy5-ODN or unL-Cy5-ODN. This result demonstrates the ability of scL to cross the BBB and efficiently deliver a payload to brain tumors.

Example 6

Efficacy of scL-TMZ in Animal Models of Brain Cancer Compared to Free, Unencapsulated TMZ

[00191] Intra cranial GBM tumors were induced in 5-6 week old female athymic nude mice by stereotaxic inoculation of U87MG-luc2 cells that stably carry the luciferase gene. Seven to ten days post-inoculation, tumors were evaluated by bioluminescence using Xenogen IVIS *in vivo* imaging system (Caliper Life Sciences) and mice were evenly divided into treatment groups. Treatment was initiated on the day of randomization (day 0). Animals were injected intravenously (i.v.) via the tail vein with 5 mg/kg (per injection per mouse) of TMZ alone or TfRscFv-targeted TMZ cationic liposome complex (scL-TMZ). The scL-TMZ complex was prepared as described above in Examples 1-2 using an anti-transferrin receptor single-chain antibody fragment (TfRscFv) as the targeting moiety, a Lip:TMZ molar ratio of 1:1 (liposome concentration = 2mM) and an TfRscFv to Liposome ratio of 1:30 (w:w). Mice were injected twice per week with each reagent for 5 weeks. Control animals (Vehicle) received Liposome only (no TMZ, no TfRscFv). The sizes of the scL-TMZ complexes iv injected into the mice during this study were found to average about 100.5 + 14.7 nm (number average) (Mean + S.E.).

[00192] *Assessment of in vivo efficacy*: The *in vivo* response to treatment was evaluated based upon the changes in tumor growth, body weight change, and overall survival. Tumor growth was monitored by bioluminescence imaging (BLI) using Xenogen IVIS *in vivo* imaging system before, during, and after the treatments at the indicated date.

U87MG-luc2 cells were genetically engineered to express luciferase gene which results in the emission of bioluminescence signal when treated with the substrate luciferin. The bioluminescence intensity of the brain tumors, a measure of tumor size/growth, was measured and compared between treatment groups. Half-way through treatment (after mice received 3 weeks of treatment with each reagent), all animals were scanned with magnetic resonance imaging (MRI) to evaluate the brain tumor. The animal imaging was done with a 7T with a Bruker Biopsin (Billerica, MA), using a respiratory gated (BioPac Physiological Data Monitor) T1-Weighted, 2 dimensional Turbo Multi-slice Multi-echo imaging sequences. Tumor volume was calculated form MRI scan and compared between treatment groups. Body weight change was monitored weekly. Overall survival was recorded and plotted by Kaplan-Meier method.

[00193] FIG. 4B shows the comparison of *in vivo* anti-tumor efficacy of the scL-TMZ and free, unencapsulated TMZ on intracranial U87MG-luc2 glioblastoma tumor xenografts. The brain tumors were imaged using MRI before treatment began and again after the mice had received 3 weeks of treatment (6 injections). The outlined areas indicate the glioblastoma tumors. Over this 3 week period the tumors in the control mice grew significantly larger as expected. As this cell line is known to be responsive to TMZ, some tumor growth inhibition was expected and was evident in the mice that received free TMZ. However, in the animals that received the scL-TMZ, not only was tumor growth inhibition evident, but tumor regression had also occurred, even over this short period of treatment, indicating the increased effectiveness of the scL-TMZ as a therapeutic agent. This was an unexpected result.

[00194] A comparison of the tumor sizes in the animals of all three groups is shown graphically in FIG. 5 and show the consistent dramatic response and small tumor size of the mice treated with the scL-TMZ.

[00195] FIG. 6 shows the BLI imaging via Xenogen of a representative animal from each group followed from pre-treatment through the treatment period and post-treatment. The intensity of the Bioluminescence signal, which correlates to tumor size, is shown in a color map: Red color = a stronger signal, Violet color = a weaker signal. Free TMZ, the current method of administration for brain tumors, was able to control the growth of the tumor for ~2.5 weeks. However, once treatment ended after 5 weeks, significant tumor growth occurred. In fact, recurrence was even evident at day 31 of treatment. In contrast, in the animal that was treated with scL-TMZ, not only was

the tumor growth inhibition maintained throughout treatment and post treatment, but an unexpected result of tumor regression (see Day 51) was observed that lasted at least 2 weeks after the end of treatment. FIG. 7 shows an additional comparison of the results. A graphic representation of the BLI signal intensities from the mice in FIG. 6 is shown in FIG. 8 (bar at bottom of graph indicates the duration of treatment). A similar plot of the signal intensities over time for all of the mice in each group is given in FIG. 9. Here again the unexpected result of lack of tumor recurrence after the end of treatment in the scL-TMZ treated group is evident. This is unexpected since tumor recurrence is a common problem in cancers of all types including brain cancers.

[00196] The lack of toxicity of the scL-TMZ treatment is shown by body weight measurements during treatment and post-treatment (FIG. 10). The steep decrease in weight of the animals in the Vehicle (Day 21) and Free TMZ (Day 51) groups is caused by the advanced disease state. Compared to these other groups, the animals treated with scL-TMZ evidenced no decrease in weight over the course of the experiment and even gained weight at the end. This demonstrates the lack of toxicity of this approach.

[00197] The long term survival of the animals in this experiment is shown in a Kaplan–Meier plot (FIG. 11). All of the mice in the Vehicle group had died by day 30. Although the free TMZ extended the lifespan of these mice compared to the control group, there was a significant increase in long term survival after treatment with scL-TMZ compared the Free TMZ group.

[00198] In a second experiment, different doses/number of injections per week of scL-TMZ, prepared as described herein, were compared. Groups of mice bearing U87MG-luc2 glioblastoma intracranial xenograft tumors were iv tail vein injected for 5 weeks with scL-TMZ at: 2.5 mg/kg one injection per week; 5 mg/kg one injection per week; or 5 mg/kg two injections per week and survival determined. The Kaplan–Meier plot in FIG. 12 shows a dose dependent response and that even a single injection at a dose of 5mg/kg can extend the life span of mice bearing intracranial brain tumors. Furthermore injections at a lower dose of TMZ can also be effective if the number of injections/week is increased.

[00199] Results Summary: Compared to the treatment with free TMZ, intravenous treatment with scL-encapsulated TMZ resulted in a robust inhibition against tumor growth monitored by either MRI or BLI, and prolonged the survival in an intracranial U87MG-luc2 GBM tumor xenograft model. However, no significantly increased

toxicity assessed by body weight change was observed in scL-TMZ treated animals compared to those of free TMZ treated animals. Also, an unexpected result was the maintenance of the tumor response, including tumor regression, for at least 2 weeks after treatment had ended.

Example 7

In Vivo Induction of Apoptosis by scL-TMZ in Cancer Stem Cells and Differentiated Cancer Cells

[00200] Intracranial U87MG-luc2 tumor was induced in 5-6 week old female athymic nude mice as described above. Three weeks after inoculation, tumor bearing mice were randomly divided into groups and treatment was started. Animals were injected i.v. via the tail vein with 5 mg/kg (per injection per mouse) of TMZ alone or TMZ encapsulated in tumor targeting liposome complex. The scL-TMZ complex was prepared as described above using an anti-transferrin receptor single-chain antibody fragment (TfRscFv) as the targeting moiety, a Lip:TMZ molar ratio of 1:1 (liposome concentration = 2mM) and an TfRscFv to Liposome ratio if 1:30 (w:w). Control animals (Vehicle) received Liposome only (no TMZ, no TfRscFv). Prepared as described above, the sizes of the scL-TMZ liposomes iv injected into the mice during this study were found to average 85.5 + 4.96 nm (number average) (Mean + S.E.).

[00201] The mice were treated two times per week. After receiving 3 injections, all animals were euthanized and brains were harvested. Brain tumors were carefully dissected from normal brain tissue and weighed. The *in vivo* anti-tumor efficacy was evaluated by assessing the level of apoptosis. After weighing the tumors, single-cell suspensions were obtained from the tumors by collagenase digestion in Hank's balanced solution containing 1 mg/mL collagenase (Roche) and 2 mmol/L DNase I (Sigma) 1 h at 37°C. The fractionated cells were passed through a 70-μm cell strainer (Fisher Scientific, Pittsburgh, PA) and washed with PBS. To determine the level of apoptosis, single cells were stained with antibodies for cleaved caspase-3 (Cell Signaling Technology, Danvers, MA), and human CD133 (Miltenyi Biotec). The labeled cells were analyzed by flow-activated cell sorting (FACS) on BD FACS Aria flow cytometer (BD Biosciences, San Jose, CA).

[00202] Assessment of *in vivo* efficacy: The anti-tumor efficacy was assessed by evaluating the induction of apoptosis in the intracranial U87MG-luc2 brain tumors. The weights of the brain tumors after 3 iv injections of Vehicle (liposome only, no TMZ, no TfRscFv), Free unencapsulated TMZ or scL-TMZ are shown in FIG. 13. Unexpectedly, even after only three injections a difference in the tumor size between the free TMZ and scL-TMZ is evident.

[00203] Cancer stem cells (CSC) are often responsible for tumor recurrence and resistance to chemotherapy. Because of the unexpected finding described above wherein the tumor growth inhibition and even regression were observed after the end of treatment with scL-TMZ (but NOT with free TMZ), the level of apoptosis was assessed in cancer stem cells, as well as in differentiated cancer cells (non-CSC) in these tumors. FIG. 14 shows the results of flow cytometric analysis for the level of apoptosis as determined by cleaved caspase-3 antibody staining of single cells isolated from the brain tumors. CD133, a marker of GBM cancer stem cells (CSCs) was used to distinguish CSCs from differentiated cancer cells. The CSC population (CD133+) clearly show a significant increase in the % of cells undergoing apoptosis compared to free TMZ. Thus the scL-TMZ can target and efficiently transfect CSCs resulting in significant tumor cell death.

[00204] Results Summary: In an intracranial U87MG-luc2 GBM tumor xenograft model, intravenous treatment with scL-TMZ resulted in a significant inhibition of tumor growth demonstrated by tumor weight compared to those treated with free TMZ. In addition, intravenous treatment with scL-TMZ resulted in a significantly increased induction of apoptosis not only in CD133- differentiated cancer cells but also in CD133+ CSCs.

Example 8

In Vivo Efficacy of scL-TMZ in TMZ Resistant Brain Cancer Cell Line T98G Subcutaneous Xenograft Tumors

[00205] T98G GBM tumor cells are known to be resistant to treatment with TMZ. For the TMZ-resistant GBM tumor model, subcutaneous T98G xenografts were used. T98G xenograft tumors were induced in female athymic nude mice by the subcutaneous injection of T98G cells or tumor particles suspended in Matrigel collagen basement

membrane (BD Biosciences, San Jose, CA) on the lower back above the tail, two sites per mouse. When the subcutaneous T98G tumors reached ~100 to 300 mm^3, the mice were randomly divided into groups and i.v. injected with 25 or 66 mg/kg (per injection per mouse) of free TMZ or 25 mg/kg (per injection per mouse) TMZ encapsulated in tumor targeting complex (1:1 molar ratio). The scL-TMZ complex was prepared as described above in using an anti-transferrin receptor single-chain antibody fragment (TfRscFv) as the targeting moiety, a Lip:TMZ molar ratio of 1:1 (liposome concentration = 8mM) and an TfRscFv to Liposome ratio if 1:30 (w:w). Control animals (Vehicle) received Liposome only (no TMZ, no TfRscFv). Prepared by the methods described above, the sizes of the scL-TMZ complexes iv injected into the mice during this study were found to average 130.8 + 13.5 nm (number average) (Mean + S.E.). The mice were treated once per day for 5 consecutive days. They were euthanized 48 hours after the last injection and the tumors harvested. Treatment was started on day 0.

[00206] Assessment of *in vivo* efficacy: The *in vivo* response of T98G subcutaneous tumors to treatment with either free TMZ or scL-TMZ complex was evaluated based upon the changes in tumor growth, body weight change, and induction of apoptosis. The size of each tumor was measured and tumor volume (L × W × H) in mm^3 was plotted versus time. Body weight change was also monitored during injection. The *in vivo* efficacy was further evaluated by assessing the level of apoptosis by TUNEL assay or cleaved caspase-3 staining with flow cytometry. Forty eight hours after the last injection the mice were euthanized and tumors harvested. Single-cell isolation was performed as described above. To determine the level of apoptosis, single cells were stained either for TUNEL assay or with antibodies for cleaved caspase-3, human CD133 and SSEA-1. SSEA-1 is known to be a marker for CSCs in GBM tumors. The labeled cells were analyzed by FACS.

[00207] The tumor size (volume in mm^3) of the tumors over this short period of time is shown in FIG. 15. Here again there is a significant difference in growth of these TMZ resistant tumors between those animals that received the free TMZ and the scL-TMZ complex, both administered at 25mg/kg, in which there is significant tumor growth inhibition. As T98G tumors are known to be resistant to TMZ it is novel and unexpected that TMZ could control tumor growth. As discussed above for use *in vitro*, this reversal of resistance is due to the efficient delivery and uptake of the TMZ payload

into the tumor cell by means of the binding of the targeting ligand (protein, antibody or antibody fragment) to its receptor on the cell and the triggering of uptake via either passive means or through active transport mechanisms like receptor mediated endocytosis. This process "floods" the cells with drug overcoming the mechanisms the tumor cell has in place to repair the DNA damage caused by TMZ (such as upregulation of MGMT), and/or the mechanisms to pump the TMZ out of the cells. Thus the tumor cell and consequently the tumor dies. Based upon this *in vivo* data, the same mechanism works *in vivo* and thus demonstrates the potential use of the scL-TMZ complex as an anticancer agent for brain and other tumors, including those currently resistant to TMZ. The lack of toxicity of the iv administered scL-TMZ is indicated by the minimal change in body weight over the short term of this experiment (FIG. 16).

[00208] The level of apoptosis in the tumors from animals that had been iv injected with 66 mg/kg (per injection per mouse) of free TMZ or 25 mg/kg (per injection per mouse) TMZ encapsulated in tumor targeting complex was assessed 8 hours post-injection by TUNEL staining of CD133+ CSCs and CD133- non-CSCs isolated from subcutaneous T98G xenograft tumors. As shown in FIG. 17, even though the animals were treated with more than double the dose of free TMZ compared to the amount of TMZ encapsulated in scL, the level of apoptosis induced by scL-TMZ was more than 5 fold higher in the non-CSCs and 8 fold higher in the CSCs.

[00209] Similar results were obtained when the level of apoptosis was assessed by cleaved caspase-3 antibody staining of SSEA-1+ CSCs from the same subcutaneous T98G brain tumors (FIG. 18). SSEA-1, another marker of CSCs was used to distinguish CSCs from differentiated cancer cells. Here also the scL-TMZ induced a 5 fold (SSEA-1-) and 9.5 fold (SSEA-1+) higher level of apoptosis than free TMZ even though more than twice the amount of free TMZ was administered.

[00210] Results Summary: Compared to the treatment with free TMZ, intravenous treatment with scL-TMZ (at the same or even lower dose of TMZ) resulted in a significantly enhanced growth inhibition against TMZ-resistant T98G tumor xenografts. However, no significantly increased toxicity based upon body weight change was observed in scL-TMZ treated animals compared to those of free TMZ treated animals. In addition, intravenous treatment with scL-TMZ resulted in a significantly increased level of apoptosis not only in CD133- and SSEA-1- differentiated cancer cells, but also in CD133+ or SSEA-1+ CSCs.

[00211] These results demonstrate that delivery of TMZ by scL can induce massive apoptosis and overcome the inherent resistance of tumors cells (including, but not limited to brain, multiple myeloma, lung cancer, prostate cancer, liver cancer, ovarian cancer, pancreatic cancer, head and neck cancer, kidney cancer, melanoma, stomach cancer) to this drug.

Example 9

Combination Therapy for TMZ-Resistant Tumors

[00212] Although the first-line chemotherapeutic agent Temozolomide (TMZ) has shown benefit in patients with brain tumors, it also has significant therapeutic dose limiting toxicities (Villano JL, Seery T E and Bressler L R (2009) Temozolomide in Malignant Gliomas: Current Use and Future Targets. Cancer Chemotherapy and Pharmacology 64: pp 647-655), including myelosuppression. Thus, ways to tumor-target TMZ so that it is specifically and efficiently delivered to, and taken up by, tumor cells in the brain thereby reducing non-specific toxicities, would be of significant benefit to those patients who are currently candidates for use of this drug.

[00213] However, even if efficiently delivered to the tumor cells, one significant drawback to the widespread use of TMZ for glioblastomas and other brain cancers is that a significant percent of tumors are resistant to TMZ. This is primarily due to overexpression of O^6-methylguanine-DNA-methyl transferase (MGMT), which repairs the TMZ-induced DNA lesions by removing the O^6-guanine adducts (Mrugala MM, Adair J and Kiem H P (2010) Temozolomide: Expanding Its Role in Brain Cancer. Drugs of Today 46: pp 833-846), thus negating the therapeutic action of TMZ. Therefore, it is imperative to develop ways to overcome this resistance.

Tumor-targeting scL-p53 Nanocomplex for Gene Therapy

[00214] As described in U.S. Patent No. 7,780,822, the disclosure of which is incorporated by reference herein in its entirety, a delivery system carrying a plasmid DNA encoding the wtp53 gene and targeted via TfRscFv (scL-p53) has been successfully developed. scL-p53 has also been developed for use in combination with

chemotherapy/radiation to increase the tumor response to these standard therapeutic modalities.

[00215] Although TMZ is a first-line chemotherapeutic for the treatment of brain tumors, only a subset of GBM patients respond to this drug. Based on the work of Stupp et al., (Stupp R, Hegi M E, Mason W P, van den Bent M J, Taphoorn M J B, Janzer R C, Ludwin S K, Allgeier A, Fisher B, Belanger K, Hau P, Brandes A A, Gijtenbeek J, Marosi C, Vecht C J, Mokhtari K, Wesseling P, Villa S, Eisenhauer E, Gorlia T, Weller M, Lacombe D, Cairncross J G and Mirimanoff R O (2009) Effects of Radiotherapy With Concomitant and Adjuvant Temozolomide Versus Radiotherapy Alone on Survival in Glioblastoma in a Randomised Phase III Study: 5-Year Analysis of the EORTC-NCIC Trial. Lancet Oncology 10: pp 459-466) as well as that of Hegi et al.,(Hegi ME, Diserens A, Gorlia T, Hamou M, de Tribolet N, Weller M, Kros J M, Hainfellner J A, Mason W, Mariani L, Bromberg J E C, Hau P, Mirimanoff R O, Cairncross J G, Janzer R C and Stupp R (2005) MGMT Gene Silencing and Benefit From Temozolomide in Glioblastoma. New England Journal of Medicine 352: pp 997-1003) two distinct groups of patients were indentified regarding response to TMZ treatment: those with a downregulated MGMT promoter with better prognosis and those with an active MGMT promoter with worse prognosis.

[00216] Thus, development of a means to down-regulate MGMT would increase the number of patients that respond to TMZ. There have been a number of reports indicating that increasing wtp53 expression could down-regulate expression of DNA repair genes such as MGMT (Bocangel D, Sengupta S, Mitra S, Bhakat K.K (2009) P53-Mediated Down-Regulation of the Human DNA Repair Gene O6-Methylguanine-DNA Methyltransferase (MGMT) Via Interaction With Sp1 Transcription Factor. Anticancer Research; Harris LC, Remack J S, Houghton P J and Brent T P (1996) Wild-Type P53 Suppresses Transcription of the Human O6-Methylguanine-DNA Methyltransferase Gene. Cancer Research 56: pp 2029-2032; Srivenugopal KS, Shou J, Mullapudi S R S, Lang F F, Rao J S and Ali-Osman F (2001) Enforced Expression of Wild-Type P53 Curtails the Transcription of the O6-Methylguanine-DNA Methyltransferase Gene in Human Tumor Cells and Enhances Their Sensitivity to Alkylating Agents. Clinical Cancer Research 7: pp 1398-1409). The use of the scL-p53 nanocomplex, shown to efficiently target primary and metastatic tumors and to cross the BBB, should be an effective means to overcome

the MGMT induced resistance to TMZ observed in a significant percentage of GBM and other tumors, thus broadening the application of this drug for use in, and improving the prognosis of, patients with primary and metastatic brain tumors. Moreover, since TMZ is also being evaluated for use in other non-brain refractory or advanced malignancies including pancreatic, neuroendocrine and areodigestive tract cancers (Tentori L and Graziani G (2009) Recent Approaches to Improve the Antitumor Efficacy of Temozolomide. Current Medicinal Chemistry 16: pp 245-257.), treatment with scL-p53 will enhance the potential of TMZ to be an effective therapeutic agent for a variety of cancers.

scL-TMZ and scL-p53 Combination Therapy

[00217] Described herein is the use of the combination of scL-TMZ and scL-p53. The development of scL-TMZ for use as a monotherapy will be of benefit to patients that currently are candidates for TMZ treatment. However, the combinatorial approach will have an even greater therapeutic potential. The decreased tumor resistance due to scL-p53, along with the improved properties that result from tumor-targeted delivery of scL-TMZ, would result in converting currently TMZ unresponsive brain tumors (and possibly other cancers) to responsive. Therefore, this approach has the potential to be developed into a new, less toxic, more effective therapeutic regimen for the treatment of GBM and other cancers.

Experimental Approach

[00218] The experiments are designed to demonstrate development of a new, more effective treatment regimen for GBM with use of scL-TMZ, both alone and when used in combination with scL-p53.

Human Brain Tumor Cell lines and In Vivo Models

[00219] Human brain cancer cell lines U87MG and T98G were described above. A version of U87MG that stably expresses the luciferase gene has been obtained from Caliper Life Sciences for use in *in vivo* studies where tumor growth and response will be monitored by the IVIS® Imaging System Xenogen.

Imaging Protocol

[00220] The MR imaging for brain tumors will be performed on a 7T Bruker Biopsin (Billerica, MA) horizontal spectrometer/imager with a 20 cm bore equipped with 100 gauss/cm microimaging gradients and run by Paravision 4.0 software. The imaging protocol is a T1-weighted Turbo rapid acquisition with rapid enhancement three-dimensional imaging sequence as previously described (Haggerty T, Credle J, Rodriguez O, Wills J, Oaks A W, Masliah E and Sidhu A (2011) Hyperphosphorylated Tau in an Alpha-Synuclein-Overexpressing Transgenic Model of Parkinson's Disease. European Journal of Neuroscience 33: pp 1598-1610).

Demonstration of *In Vivo* Efficacy of scL-TMZ Alone and in Combination with scL-p53

[00221] In these studies, the U87-Luc orthotopic intracranial (TMZ sensitive) and T98G (TMZ resistant) subcutaneous tumor models will be used to examine the effect of scL-TMZ alone and in combination with scL-p53 on tumor growth and/or regression. It should be noted that although U87MG has wt p53, an increased *in vivo* response is observed when U87 intracranial tumors are treated with the combination of scL-p53 and free TMZ. Groups of mice (6 mice/group/tumor model) will receive i.v (tail vein) injections of Free TMZ alone, scL-TMZ alone, scL-p53 alone, scL-p53 plus free TMZ or scL-TMZ. Untreated mice will serve as controls. The p53 dose will be 30ug/mouse/ injection, and TMZ will be used at 5mg/kg. Both treatments will be administered twice weekly for 5 weeks. Tumor growth inhibition/regression will be assessed by size for T98G and with the Xenogen for the intracranial tumors where tumor volume will be determined by MRI. Xenogen/MRI imaging will be done pre-treatment, once/week during treatment and immediately after treatment has ended. Half-way through treatment, tumors and various normal organs and tissues will be taken from 3 mice in each group and coded. Half of each tissue will be used for the analysis described in Aim II and the remainder examined by histology for markers of apoptosis (Tunnel, Caspase -3) and for proliferation marker Ki67. One day after treatment has ended, 3 mice will be humanely euthanized and necropsied by a commercial CRO (BioReliance, Rockville MD) to look for differences in myelotoxic effects and lymphopenia associated with TMZ.

In Vitro Results

[00222] To test the hypothesis that treatment with scLp53 could down modulated MGMT activity and sensitize TMZ resistant brain tumors to this drug, a preliminary XTT cell survival assay was performed. TMZ resistant T98G cells were plated at 2×10^3 per well in a 96-well plate and transfected with scL-p53 in combination with either Free TMZ or scL-TMZ. The cells were also transfected with just free TMZ or just scL-TMZ. The XTT assay was performed 90 h later and the IC_{50} values (the concentration yielding 50% growth inhibition) determined. Transfection with scL-p53 in combination with either free or scL complexed TMZ resulted in an increased level of response compared to single agent TMZ in this known TMZ resistant cell line (Patil R, Portilla-Arias J, Ding H, Inoue S, Konda B, Hu J W, Wawrowsky K A, Shin P K, Black K L, Holler E and Ljubimova J Y (2010) Temozolomide Delivery to Tumor Cells by a Multifunctional Nano Vehicle Based on Poly(Beta-L-Malic Acid). Pharmaceutical Research 27: pp 2317-2329) (FIG. 19). Moreover, compared to free TMZ alone, transfection with the scL-TMZ nanocomplex resulted in a significant level of chemosensitization to the drug.

Example 10

In Vivo Targeting of Cancer Stem Cells by Systemically Administered scL-Complex in a Mouse Brain Tumor Model

[00223] Human brain tumor xenografts were induced in nude mice by subcutaneous inoculation of U251 cells. Three weeks later, the mice were I.V. injected with 6FAM-ODN (100 μg/ mouse) administered as either uncomplexed free 6FAM-ODN, scL-6FAM-ODN (scL-ODN), or the unliganded Lip-6FAM-ODN (the liposome without the targeting moiety) (LIP-ODN). 24 hours post-injection, the tumors were imaged using the Maestro™ *in vivo* fluorescence imaging system to determine the level of fluorescence in the tumors. After Maestro™ imaging, single cells were isolated from the tumors by enzyme digestion, and the amount of 6FAM-ODN uptake in CD133+ (Cancer Stem Cell (CSC)) and CD133- (non-CSC) cells analyzed and quantitated by FACS. Systemic administration of both free 6FAM-ODN and unliganded Lip-ODN resulted in very little, if any, fluorescence in the tumors. In contrast, a strong

fluorescence signal was evident in the tumor from the mouse that received the scL-ODN nanocomplex (FIG. 20).

[00224] More importantly, this significant difference was also reflected in the transfection efficiency of CSCs (FIG. 21). Whereas less than 10% of the CSC and Non-CSC cells were transfected with the free or unliganded 6FAM-ODN, >60% of both CSC and non-CSC cell populations demonstrated the presence of the payload after I.V. injection. Gray histograms represent untreated controls. These findings confirm that with systemic administration, the scL delivery system described herein can target and efficiently deliver payloads to CSCs *in vivo*.

Example 11

Tumor Specific Targeting of CSCs in IC GBM by scL-Delivered ODN After Systemic Administration

[00225] FIG. 22 shows the comparison of *in vivo* delivery efficiency of payload delivered by tumor-targeting complex, non-targeting complex, and payload itself without the delivery system in an animal model of intracranial U87MG-luc2 glioblastoma multiforme (GBM) brain tumors. Fluorescently labeled (Cy5) oligonucleotide (Cy5-ODN) was encapsulated in tumor-targeted complexes (scL-Cy5-ODN) (prepared as described in U.S. Patent No. 7,780,882) or complexes without tumor-targeting ligand (Lip-Cy5-ODN). Twenty five micrograms of Cy5-ODN (free or encapsulated with or without the targeting moiety) were injected intravenously to each animal bearing a U87MG-luc2 intracranial tumor. At 60 hr after injection, the animals were euthanized and tumors were harvested to assess the efficiency of delivery to cancer stem cells (CSCs) in these intracranial tumors by flow cytometry using markers for cancer stem cells, CD133 and SSEA, both of which are known by those familiar with the art to be markers of CSC in general (CD133+) and CSC in brain tumors (SSEA-1+). Single cells were isolated from brain tumors and subjected to FACS analysis after staining with CSC marker antibodies (CD133+ or SSEA-1+). The shift in the curve in each histogram in FIG. 22 represents Cy5-ODN uptake in cancer stem cells. Only the curves representing the CSCs isolated from the mice receiving the scL-Cy5-ODN demonstrated a significant shift, indicating that neither the free

Cy5-ODN, nor the Lip- Cy5-ODN (without the targeting moiety) efficiently transfected CSCs in the brain tumor.

Example 12

In Vitro Sensitization of Brain Tumor cells to Temozolomide (TMZ) by scL-p53

[00226] To assess the ability of scL delivered wtp53 to sensitize brain tumor cells to first-line chemotherapeutic agent TMZ, human brain tumor derived U87 and U251 cells were treated with TMZ alone, or the combination of TMZ plus scL-p53 (prepared as described in U.S. Patent No. 7,780,882). As a control, cells were also treated with the combination of TMZ and the scL delivery system carrying the same vector used to construct the pSCMVp53 plasmid, but without the p53 insert (scL-vec). The cells were plated in a 96-well plate and treated 24 hours later with scL-p53 or scL-vec. 6 hours post-transfection, the TMZ was added in increasing concentrations. The XTT assay was performed 144 h after the addition of the TMZ to the wells and the IC_{50} values (the concentration yielding 50% growth inhibition) determined. As these two cell lines are known to be sensitive to TMZ, it was not unexpected that there was some response to TMZ alone. However, as shown in FIG. 23, there is a significant increase in sensitization to TMZ when the cells are transfected with wtp53 delivered by the scL delivery system when compared to TMZ alone for both cell lines. Minimal to no sensitization (U87 and U251, respectively) was observed with the complex carrying the empty vector, demonstrating that the effect is due to the p53 and not the delivery system.

[00227] However, as only a subset of brain tumor patients respond to TMZ it was more critical to assess the ability of scL-p53 to sensitize TMZ resistant tumors to this chemotherapeutic agent. Thus, to assess the ability of scL delivered wtp53 to sensitize TMZ resistant brain tumor cells to this first-line chemotherapeutic agent, human brain tumor derived LN-18 and T98G cells were treated with TMZ alone, or the combination of TMZ plus scL-p53 (FIG. 23). As a control, cells were also treated with the combination of TMZ and the scL delivery system carrying the same vector used to construct the pSCMVp53 plasmid, but without the p53 insert (scL-vec). The cells were

plated in a 96-well plate and treated 24 hours later with scL-p53 or scL-vec. 24 hours post-transfection, the TMZ was added in increasing concentrations. The XTT assay was performed 72h after the addition of the TMZ to the wells and the IC_{50} values (the concentration yielding 50% growth inhibition) determined. As shown in FIG. 23 with LN-18 cells, after transfection with scL-p53 these TMZ resistant cells are now responding to even very low doses of TMZ. More than 50 % of the cells are killed at a dose of TMZ as low as ~50uM compared to TMZ alone, in which no significant cell death is observed until a dose of ~1000uM. With the T98G cells (FIG. 23), although not as responsive as to TMZ as LN-18 after treatment with scL-p53, these highly resistant cells are also sensitized to the killing effects of this drug. The cells treated with scL-p53 prior to exposure to TMZ have an IC_{50} of 600uM while those receiving TMZ only do not reach IC_{50} until the TMZ dose is ~ 2000uM. As above, there is minimal or no effect on the response of the cells to TMZ after transfection with the control scL-vec indicating that the response in these resistant cell lines is due to the presence of wtp53.

Example 13

In Vivo Sensitization of Brain Tumor Cells to Temozolomide (TMZ) by Systemically Administered scL-p53

Tumor Regression in an Intracranial (IC) Mouse Model of Brain Cancer Induced by Systemic Treatment with the combination of scL-p53 plus TMZ

[00228] An experiment was performed to examine tumor growth inhibition induced by the sensitization of IC brain tumors to TMZ by systemic administration of scL-p53 prepared as described in U.S. Patent No. 7,780,882. U87MG-Luc xenograft brain tumors were induced in nude mice by intracranially inoculating U87MG-luc cells. This cell line, obtained from Caliper Life Sciences, has been modified to stably express the Luciferase gene. 10 days post-inoculation, tumor-bearing animals were i.v. tail vein injected with TMZ alone (5.0 mg/kg/injection), scL-p53 alone (30 ug DNA/mouse/injection) or TMZ in combination with scL-p53. As a control, one group received PBS (vehicle). All i.v. injections were administered 2X/week to a total of 10 injections. To assess tumor response, bioluminescence imaging (BLI) was performed using IVIS® Imaging System's Xenogen. FIG. 24 is a comparison of *in vivo* anti-tumor efficacy of the various groups. Bioluminescence signals which correlate to tumor size

are shown in a color map. Red color (at the top of the scale bar): the stronger signal, Violet color (at the bottom of the scale bar): the weaker signal. The bioluminescence intensity of the brain tumors, a measure of tumor size/growth, was compared between groups using Xenogen Living Image® software and is plotted over time in FIG 25. The horizontal bar indicates the duration of treatment (Last treatment = Day 24).

[00229] While TMZ alone and scL-p53 alone had some minimal effect on IC tumor growth during treatment, the tumors in both groups rapidly increased in size after the end of treatment. In contrast, the tumors in the group of mice that received the combination of scL-p53 and TMZ displayed not only tumor growth inhibition, but tumor regression during treatment. More significantly, this regression continued for more than 20 days after treatment had ended.

[00230] To confirm the bioluminescence findings, the mice were also imaged by MRI, without contrast agent, before and after the mice received 3 weeks of treatment. The tumor regression observed in the combination treatment group by bioluminescence was also observed here. In FIG. 26 the outlines indicate the glioblastoma tumors. It is evident that instead of increasing in size post treatment as is evident in the single agent treatment groups, any residual tumor is barely detectable in the these animals that received both scL-p53 and TMZ. Therefore, this experiment demonstrates that the presence of scL-delivered wtp53 can sensitize GBM tumors to TMZ leading to significant tumor response (regression) not just tumor growth inhibition.

Significantly Increased Survival of Mice Bearing Intracranial GBM Tumors After treatment with the Combination of scL-p53 and TMZ

[00231] As the above experiments demonstrated significant tumor responses, including regression post-treatment, the effect of this combination treatment on survival was next assessed. U87MG-Luc xenograft brain tumors were induced in nude mice as described above. 10 days post-inoculation, tumor-bearing animals were i.v. tail vein injected with TMZ alone (25.0 mg/kg/injection), scL-p53 alone (30 ug DNA/mouse/injection) (prepared as described in U.S. Patent No. 7,780,882) or TMZ in combination with scL-p53. As a control, one group received PBS (vehicle). All i.v. injections were administered 2X/week to a total of 10 injections. The animals were monitored 2-3 times/week and euthanized when moribund. The results, analyzed by Kaplan–Meier method, are shown in FIG. 27 and Table 1 below. The gray bar in FIG. 27 indicates the

duration of treatment. Although TMZ alone was able to prolong survival for a period of time in this TMZ responsive cell line, all of the mice succumbed to their tumor by ~day 155 with a Median Survival of 112 days. However, the survival time was extended considerably by the addition of scL-p53 to the treatment regimen. In these animals 60% of the mice were still surviving at day 210. Therefore, the % survival prolongation for mice receiving this combination regimen was >740 times that of the untreated mice, 500 times that of scL-p53 alone and almost twice that of TMZ alone. Thus, this adding scL-p53 to treatment with TMZ results in a significant increase in long term survival.

TABLE 1

Treatment	n	Median Survival (Days)	Survival Prolongation (%) *	Log Rank P-value
Untreated	4	25	-	-
scL-p53	5	35	40	0.0117
TMZ	5	112	348	0.0088
TMZ + scL-p53	5	>210	>740	0.0058

*Determined as a ratio of the median survival of untreated GBM xenografts

Significantly Increased Survival of Mice Bearing TMZ Resistant Intracranial GBM Tumors After treatment with the Combination of scL-p53 and TMZ

[00232] The *in vitro* studies described above indicated that transfection of TMZ resistant brain tumor cells could be sensitized to TMZ by transfection of scL-p53. Thus an experiment was performed to assess survival of mice bearing intracranial tumors derived from TMZ resistant human GBM cell line T98G. Athymic nude mice were intracranially inoculated with T98G human glioblastoma cell line. Ten days after the inoculation, animals were imaged by MRI and evenly divided into 3 groups. Treatment was started immediately after imaging. The animals were iv treated with 100 mg/m^2 of TMZ once a day for 14 consecutive days, iv administered scL-p53 (30 ug DNA/injection) (prepared as described in U.S. Patent No. 7,780,882) twice weekly for 2 weeks, or the combination of both treatments. Survival was monitored. The results, analyzed by Kaplan–Meier method, are shown in FIG. 28. The number of mice surviving/group at day 14 is indicated for each group. Over this 2 week time of treatment a significant number of animals succumbed to their disease in the two groups

that received TMZ or scL-p53 as a single agent. In contrast, 4 of 5 mice that had received the combination therapy were still surviving. Thus, this small efficacy experiment confirms the *in vitro* data and indicates that treatment with scL-p53 can sensitize previously resistant GBM tumors to TMZ.

Example 14

Enhanced Apoptosis in Intracranial Brain Tumors by the Combination of scL-p53 and TMZ

[00233] Tumor suppressor p53 is known to play a role in the apoptotic pathway. To begin to evaluate the mechanism responsible for the increase in tumor cell response and increase in animal survival observed with the combination of scL-p53 and TMZ, the level of apoptosis induced in intracranial U87MG-luc2 brain tumors after various treatments was determined using Annexin V-FITC and Flow Cytometry. U87MG-luc2 brain tumors were induced as described above. 10 days post inoculation of the cells, the mice were treated with either TMZ alone (5 mg/kg per injection per mouse, 2 injections per week), scL-p53 alone (30 ug DNA per injection per mouse, 2 injections per week) (prepared as described in U.S. Patent No. 7,780,882) or the combination of scL-p53 and free TMZ. Each animal received a total of 3 injections after which the animals were euthanized, single cell population isolated from the tumors and subjected to the Annexin V assay.

[00234] As shown in FIG. 29, there is a significant increase in the percent of the tumors cells in apoptosis after treatment with the combination of scL-p53 and TMZ compared to either treatment alone. Thus, these results indicate that uptake of systemically administered scL-p53 by the IC tumors results in an enhanced apoptotic response to chemotherapeutic agent TMZ.

Example 15

Treatment of TMZ Resistant GBM Tumors with scL-p53 Downmodulates MGMT Expression *In Vitro* and *In Vivo*

[00235] The primary mechanism of resistance to TMZ is over expression of O^6-methylguanine-DNA-methyl transferase (MGMT), which repairs the TMZ-induced DNA lesion by removing the O^6-guanine adducts. Thus, a means to down modulate MGMT activity would enhance the therapeutic effect of TMZ. A number of reports have indicated that increasing wtp53 expression could down-regulate expression of DNA repair genes such as MGMT and increase the sensitivity of tumor cells to alkylating agents such as TMZ. The *in vitro* and *in vivo* data described in the Examples above indicated that treatment with scL-p53 could reverse resistance to TMZ in brain tumor cells. One possible mechanism for this sensitization is p53 dependent down modulation of MGMT. Uptake of scL-delivered wtp53 was examined to determine if it had an effect on the level of MGMT expression in TMZ-resistant T98G human glioblastoma cells *in vitro* and in *in vivo* subcutaneous xenograft tumors. T98G cells were transfected with scL-p53 (prepared as described in U.S. Patent No. 7,780,882). 16 and 24 hours post-transfection, the cells were harvested, protein isolated and 40ug micrograms total protein was electrophoretically fractionated using a Nu-PAGE Precast 4-12 % gradient gel, transferred to nitrocellulose membrane, and probed for expression of MGMT and GAPDH by Western blot analysis. The signal was detected by ECL reagent (FIG. 30).

[00236] For the *in vivo* experiment shown in FIG. 30, scL-p53 (30 ug DNA/injection/mouse) was i.v. injected three times over a 24 hr period. At 16 and 24 hours after the last scL-p53 treatment, the mice were euthanized, tumors harvested, and protein extracted. Four mice were harvested at each time point. One group as a control did not receive SGT-53. 40ug micrograms total protein was electrophoretically fractionated using a Nu-PAGE Precast 4-12 % gradient gel, transferred to nitrocellulose membrane, and probed for expression of MGMT and GAPDH by Western blot analysis. The signal was detected by ECL reagent.

[00237] *In vitro*, there was complete down modulation of MGMT expression by 16 hours, which lasted as long as 24 hours post-transfection. Similarly, in the *in vivo* study, a significant decrease in the expression of MGMT was evident at 16 hours, with virtual elimination of the protein in two of the animals. By 24 hours after the last injection, virtually complete down modulation of MGMT was evident in all of the mice treated with SGT-53. Consistent expression of GAPDH protein demonstrated equal

protein loading. The lack of MGMT to repair the DNA damage induced by TMZ in these tumors, along with the exogenous SGT delivered wtp53's positive effect on the apoptotic pathway, likely plays a role in overcoming the resistance of T98G to the killing effects of TMZ.

[00238] More significantly, similar results were observed in an intracranial tumor model with T98G (FIG. 31). In this experiment, scL-p53 (at 30 ug DNA/ mouse) was i.v. injected only once. At various time points between 16 and 72 hours after the scL-p53 injection, mice were euthanized, tumors harvested, and protein extracted. One group as a control (UT) did not receive SGT-53. 40ug micrograms total protein was electrophoretically fractionated using a Nu-PAGE Precast 4-12 % gradient gel, transferred to nitrocellulose membrane, and probed for expression of p53, MGMT and GAPDH by Western blot analysis. The signal was detected by ECL reagent.

[00239] At 16 and 24 hours after the single scL-p53 i.v. injection, an increase in the level of p53 protein is evident as compared to the UT animal indicating the presence of the exogenous p53. By 43 and 72 hours this signal had decreased back to a level similar to that of the UT control. More, importantly, as observed with the subcutaneous tumors, in these Intracranial tumors a significant decrease in expression of MGMT was observed at both 43 and 72 hours after treatment with scL-p53. This timing for the observed decrease in MGMT signal is consistent with the mechanism of action of p53 in sensitizing cells to TMZ by interfering with DNA repair mechanisms.

Example 16

Combination Treatment of scL-p53 and TMZ in Patients with Glioblastoma or Gliosarcoma

[00240] Standard administration of temozolomide requires a daily dose of Temozolomide for 21 days. To optimize effectiveness of the potential chemosensitization of scL-p53, in a preferred embodiment, scL-p53 treatment will begin 1 day before temozolomide treatment. Pre-clinical studies have shown that the wtp53 tumor suppressor gene delivered by the scL-p53 complex functions to sensitize tumors to the chemotherapeutic agent, making them more responsive to the drug. Thus, it is critical that p53 is being expressed when temozolomide is administered in order to

have the benefit of the scL-p53. Using the proposed schedule shown in FIG. , scL-p53is being expressed at the start of temozolomide treatment.

[00241] In an alternate embodiment, two scL-p53 treatments will be administered before the start of temozolomide treatment. Here, scL-p53 will be administered on the same scheduled indicated in the table in FIG. 33, beginning on Day 1. However, the first TMZ treatment will not be until Day 6. Temozolomide will be administered orally at 100-250mg/m^2 every day (including weekends) for 21 days (from day 6 to day 26).

Example 17

Preparation of Targeted Cationic Liposomes Comprising Melphalan (MEL)

Materials:

[00242] DOTAP (1,2-dioleoyl-3-trimethylammonium propane, chloride salt)

-Obtained from Avanti Polar Lipids, Inc. Cat. #890890E, MW 698.55

-Concentration: 25 mg/mL ethanol solution

Dilute lipid to 20mg/ml with absolute ethanol before use

[00243] DOPE (1,2-dioleoyl-sn-glycero-3-phosphoethanolamine)

-Obtained from Avanti Polar Lipids, Inc. Cat. # 850725E, MW 744.04

-Concentration: 25 mg/mL ethanol solution.

Dilute lipid to 20mg/ml with absolute ethanol before use

[00244] Melphalan Hydrochloride (Mel), powder (M Wt = 341.7)

-Obtained from Sigma, M2011-100mg,

- Dissolve in absolute ethanol to a concentration of 50 mg/ml, with 10-15 ul of 6N HCl to aid in dissolution

[00245] Ultra-pure, endotoxin free LAL Reagent Water (e.g. BioWhittaker, Cat.# W50-500, endotoxin <0.005 EU/ml)

[00246] Injector: Hamilton Gastight Syringe, 1ml (Hamilton #81230) with a 22 gauge needle, part #81365)

Procedure:

[00247] 1. Fresh Mel solution is prepared each time by dissolving Mel in absolute ethanol to a concentration of 50 mg/ml (146.3mM) with the addition of 6N HCl

(~10-15uL) by vortexing at high speed until dissolved (must be clear). Hold at room temperature until used to mix with lipids (Step 3 below).

[00248] 2. Place lipid solutions at 37° C for 10-15 min, following which place the lipid solutions in a 65° C water bath with occasional shaking for 5 min.

[00249] 3. To prepare the Lip-Mel: Place a brown glass bottle with stir bar on a hot plate set to 50°C to 60°C. While stirring at high speed without splashing, add the lipids and Mel to the bottle in the following order (important):

[00250] For 1:1 (Lip:Mel) molar ratio

DOTAP	175 µl (of 20 mg/ml) = 5 µmol or 3.5 mg
DOPE	187.5 µl (of 20 mg/ml) = 5 µmol or 3.75 mg
Add Mel soln.,	68.3 µl (of 50 mg/ml) = 10 µmol,

Continuously stir for 3 min. after all 3 have been added

[00251] 4. In the meantime, warm 4,569 uL LAL water to 65° C in water bath in brown glass bottle with stir bar. Immediately prior to addition of the Lipid-Mel solution, move the bottle to a hot plate (50 °- 60° C). Stir water at high speed with no splashing for a few sec to remove bubbles from the stir bar.

[00252] 5. Keep the water on the hot plate. Continue stirring the water at high speed (without splashing) during lipid addition. After mixing lipids and Mel as above (Step 2), immediately and as rapidly as possible, using the Hamilton syringe for injection, inject the mixture into the hot water on the hot plate (50° - 60° C) directly into the center of the vortex.. Continue stirring on high speed (without splashing) for 1 min after the addition of the lipid mixture while loosely covered.

[00253] 6. Move the glass bottle to a RT stir plate, and, continue to stir slowly until the loosely covered solution cools down to 20-25°C (room temperature)

[00254] 7. Adjust the volume to 5 ml with room temperature LAL water.

[00255] 8. Filter the solution using a 0.22 µm pore Milex GV filter.

[00256] 9. Measure particle size and zeta potential if desired.

[00257] Results of these preparation methods demonstrate liposomes having a particle size of about 20-60 nm and a Zeta Potential of about 10 to 50 mV.

Example 18

Preparation of Targeted Cationic Liposome Containing Melphalan (scL/MEL) Without Chemical Conjugation (By Simple Mixing)

[00258] Using the MEL-comprising cationic liposomes prepared according to the procedure described above, the ligand targeted MEL cationic liposome complex as described herein is prepared by simple mixing of the components and without chemical conjugation. The preparation of the complexes was in accordance with the following general procedure:

[00259] To the liposome-water (or buffer) the appropriate amount of targeting moiety is added to give the desired ratio and mixed by gentle inversion 5-10 seconds. The targeting moiety can be a ligand including but not limited to transferrin or folate, or other proteins. It can also be an antibody or an antibody fragment that targets a cell surface receptor including, but not limited to the transferrin or HER-2 receptor (e.g., TfRscFv). This mixture is kept at room temperature for 10-15 minutes (again inverted gently for 5-10 seconds after approximately 5 minutes). To yield the desired final volume the targeting moiety-Lip-MEL admixture is mixed with any volume (including none) of water (suitably deionized water) or a buffer of any pH including, but not limited to, Tris buffers, HEPES buffers or Phosphate Buffered Saline, required to give a desired volume and inverted gently for 5-10 seconds to mix. This mixture is kept at room temperature for 10-15 minutes (again inverted gently for 5-10 seconds after approximately 5 minutes).

[00260] Typically, for use in an in vitro assay, it is desirable that the amount of MEL in the final complex is in the range of about 1 μM to 30 μM per well; for *in vivo* use, it is desirable to provide about 1mg/kg to about 50mg/kg of MEL per injection. For use *in vivo* dextrose or sucrose is added last to a final concentration of about 1-50% (V:V) dextrose or sucrose, suitably 5% dextrose or 10% sucrose, and mixed by gentle inversion for 5-10 seconds. This mixture is kept at room temperature for 10-15 minutes (again inverted gently for 5-10 seconds after approximately 5 minutes).

[00261] A specific example for *in vitro* transfection at a suitable ratio of 1:30 (antibody fragment:liposome, w:w) and 1:1 Liposome:MEL (molar ratio) is as follows: For a final volume of approximately 600 uL, mix 250 μL of Lip:TMZ (2 mM stock) with 56.7

μL of antibody fragment (at an anti-transferrin receptor single chain antibody fragment [TfRscFv] concentration of 0.21 mg/mL). Add 293.3μL of water or buffer.

[00262] The size (number average) of the final complex prepared by the method is between about 10 to 800 nm, suitably about 15 to 400 nm, most suitably about 20 to 200 nm with a zeta potential of between about 1 and 100 mV, more suitably 5 to 60 mV and most suitably 10 to 50mV as determined by dynamic light scattering using a Malvern Zetasizer ZS. This size is small enough to efficiently pass through the tumor capillary bed, or cross the blood brain barrier, and reach the tumor cells.

[00263] The complex prepared as described above containing dextrose or sucrose (1-50%, volume to volume) can also be lyophilized to dryness and stored at room temperature, 2-8oC, or -20 to -80oC. The samples are reconstituted with water prior to use. The size (number average) of the final lyophilized complex after reconstitution is between about 10 to 800 nm, suitably about 15 to 400 nm, more suitably about 20 to 200 nm and most suitably 50 to 150 nm with a zeta potential of between about 1 and 100 mV, more suitably 5 to 60 mV and most suitably 10 to 50mV as determined by dynamic light scattering using a Malvern Zetasizer ZS. These complexes retain at least 80% of the original biological activity.

Example 19

Increased Effect of Lip/MEL On Tumor Cells Compared to Free (unencapsulated) MEL

[00264] The scL/MEL nanocomplex was prepared as described above using an anti-transferrin receptor single-chain antibody fragment (TfRscFv) as the targeting moiety, a Lip:MEL molar ratio of 1:1 and 0.75:1 (sizes = 30 and 25nm, respectively) (liposome concentration = 2mM) and an TfRscFv to Liposome ratio if 1:30 (w:w). The size of the scL/MEL nanocomplex was 45 and 57nm, respectively. The *in vitro* cell killing ability of the scL/MEL was compared to free, unencapsulated MEL in KMS-11 cells.

[00265] For these *in vitro* cell survival studies, the human multiple myeloma cell line KMS-11 was used. These are non-adherent cells and grow in suspension. 4×10^5 cells in 2.6 ml of serum free media were incubated in a sterile 50 ml centrifuge tube with 400ul of the scL/MEL (at either ratio) or unencapsulated MEL for one hour. Following

this incubation, the medium was supplemented with fetal bovine serum to a final concentration of 10% (0.3ml/tube). After incubation for an additional 47 h, cell viability was determined by Trypan Blue counting of the cells. To accomplish this, one part trypan blue solution is mixed with 1 part cell suspension (1:1 dilution) in a 2 mL eppendorf tube (e.g. 200 µL trypan blue is mixed with 200 µL cell suspension). Using a hemacytometer and a microscope the number of viable cells (unstained) and dead cells (stained) are counted. The average number of cells per 0.1 mm^3 is calculated and the number of cells per mL determined. The percent of viable cells is calculated as follows:

Viable Cells % = (Number of viable cells / Number of Cells) * 100

[00266] The results are plotted and the IC_{50} and IC_{30} values, the drug concentration resulting in 50% and 30% cell kill, respectively, was interpolated from the graph of the drug concentration versus the percent of viable cells.

[00267] FIG. 33 shows that tumor targeting scL/MEL nano complex, in which the MEL is encapsulated in the liposome, has significantly improved anti-cancer efficacy compared to unencapsulated MEL. The unencapsulated MEL has an IC_{50} value of 17.6 uM. In contrast, when encapsulated in the liposome via the method of this invention at a 1:1 molar ratio of Liposome to MEL, and delivered to the tumor cell by means of the tumor-targeting nanocomplex of this invention at approximately 2 fold less MEL will effectively kill the cancer cells (IC_{50} of 9.6uM). Although not as dramatic, there was also a 30 % decrease in the IC_{50} values between the unencapsulated MEL and scL/MEL when the Lip/MEL was prepared at a Liposome:Mel ratio of 0.75:1 (molar ratio). Transfection with the Liposome alone did not result in any significant cell kill (IC_{50} > 33 µM) indicating that the sensitization observed with the scL/MEL is not a result of non-specific cell kill by the liposome. Thus a variety of different molar ratios of liposome to Melphalan when used in the methods of this invention will result in a compound which when complexed to the targeting moiety by simple mixing and without chemical conjugation using the methods of this invention will result in a complex that has unexpected enhanced efficacy against multiple myeloma cells.

[00268] Similar results are shown in FIG. 34 comparing unencapsulated MEL, with Lip/MEL as described herein without the targeting moiety and with the full scL/MEL nanocomplex, as well as with liposome only. The Lip/MEL and scL/MEL were prepared as described in Examples 1 and 2 at molar ratios of Liposome to MEL of

1:1)(liposome concentration = 2mM). An anti-transferrin receptor single-chain antibody fragment (TfRscFv) was used as the targeting moiety, with a TfRscFv to Liposome ratio of 1:30 (w:w). Once again the liposome only has virtually no cell killing effect on these multiple myeloma cells. In contrast, even without the targeting moiety, when encapsulated in the Liposome at molar ratios of 1:1 (Lip:MEL) using the methods described herein, there was a significant decrease in the IC_{50} value compared to free (unencapsulated) MEL. This level of sensitization was even greater (almost 2 fold) when the full scL/Mel complex was used. This level of sensitization of multiple myeloma cells after encapsulation in liposomes via the method of this invention is unexpected.

Example 20

Maintenance of Biological Activity of scL/MEL After Lyophilization and Reconstitution

[00269] The scL/MEL complex containing sucrose (final concentration = 10%) was prepared as described above using an anti-transferrin receptor single-chain antibody fragment (TfRscFv) as the targeting moiety, a Lip:MEL molar ratio of 1:1 (size = 21nm) (liposome concentration = 2mM) and an TfRscFv to Liposome ratio if 1:30 (w:w). This complex was subsequently lyophilized and the samples stored in a desiccator at 2-8°C. After one week of storage the lyophilized scL/Mel complex was reconstituted with endotoxin free water and used to transfect KMS-11 cells as described above. The size of the reconstituted scL/MEL was 56nm (number average), within the preferred size range of the complex prepared by the method of this invention when freshly prepared. Thus, lyophilization did not significantly alter the size of the complex. The cell killing ability of the lyophilized/reconstituted scL/MEL was compared with freshly prepared scL/MEL and free (unencapsulated) MEL. The results are shown in FIG. 35. Both the IC_{50} and IC_{20} values for the freshly prepared and lyophilized scL/MEL nanocomplex are virtually identical. Thus, this lyophilized complex is also able to maintain at least 80% of its biological activity.

Example 21

Combination Therapy with scL/MEL and Tumor Suppressor Gene p53

[00270] Restoration or activation of the tumor suppressor p53 pathway has been shown to induce apoptosis (programmed cell death), in multiple myeloma cells (Ludwig H, Beksac M, Blade J, Boccadoro M, Cavenagh J, Cavo M, et al. Current MM treatment strategies with novel agents: a European perspective. Oncologist 2010; 15(1):6-25; Hurt EM, Thomas SB, Peng B, Farrar WL. Reversal of p53 epigenetic silencing in multiple myeloma permits apoptosis by a p53 activator. Cancer Biology & Therapy 2006;5:1154-60). Furthermore, studies investigating the molecular causes of multiple myeloma disease have shown that myeloma cells often have healthy (i.e., unmutated) p53 genes but very little p53 protein. Restoration of p53 levels slows the growth of multiple myeloma cells and causes their death. Thus p53 gene therapy is a logical treatment strategy for multiple myeloma.

Tumor-targeting scL-p53 Nanocomplex for Gene Therapy

[00271] As described in U.S. Patent No. 7,780,822, the disclosure of which is incorporated by reference herein in its entirety, a delivery system carrying a plasmid DNA encoding the wtp53 gene and targeted via TfRscFv (scL-p53) has been successfully developed. Systemic administration of scL-p53 results in high levels of wtp53 expression in numerous different tumor types. scL-p53 has also been developed for use in combination with chemotherapy/radiation to increase the tumor response to these standard therapeutic modalities by inducing apoptosis.

[00272] The use of the scL-p53 nanocomplex, shown to efficiently target and efficiently deliver wtp53 to both primary and metastatic tumors, should be an effective means to increase the levels of p53 protein in multiple myeloma cells.

scL/MEL and scL-p53 Combination Therapy

[00273] Described herein is the use of the combination of scL/MEL and scL-p53. The development of scL/MEL for use as a monotherapy will be of benefit to patients in that we have shown the unexpectedly high increase in multiple myeloma cell death after treatment with scL/MEL as compared the unencapsulated MEL, the form that is currently used for treatment. However, as increasing expression of p53 in multiple

myeloma cells also has therapeutic potential, the combinatorial approach will have an even greater therapeutic potential.

Experimental Approach

[00274] The experiments are designed to demonstrate development of a new, more effective treatment regimen for multiple myeloma with use of scL/MEL, when used in combination with scL-p53.

In Vitro Results

[00275] To test the hypothesis that treatment with scL-p53 could result in multiple myeloma cell death a preliminary cell viability assay was performed as described above. Human multiple myeloma cell line KMS-11, described above, was transfected with scL-p53 alone. scL-p53 was prepared by simple mixing of the components in a defined order as described in U.S. Patent No. 7,780,822. The complex was prepared with increasing doses of a plasmid encoding the normal human wtp53 gene. Plasmid DNA doses ranged from 0 to 1.3ug DNA. The KMS-11 cells were transfected using the identical procedure described above. The percent of viable cells was determined 24 h post-transfection and the IC_{50} and IC_{20} values determined. Transfection with scL-p53 resulted in a dose-dependent level of cell death indicating that increasing the expression of wtp53 in multiple myeloma cells by itself can result in significant level of cell death (FIG. 36). This is unexpected since the reports in the art regarding modulation of p53 expression in multiple myeloma have all employed either additional activating agents or indirectly, not directly, affected p53 by blocking expression of other proteins.

[00276] The combination of scL/MEL and scL-p53, both of which were shown to increase the level of cell death on their own were transfected simultaneously to assess the response of KMS-11 cells to this combination therapy. KMS-11 cells were transfected using the procedure described above. scL/MEL was prepared as described above using an anti-transferrin receptor single-chain antibody fragment (TfRscFv) as the targeting moiety, a Lip:MEL molar ratio of 1:1 (liposome concentration = 2mM) and an TfRscFv to Liposome ratio if 1:30 (w:w). Cells ($4x10^5$ per tube) were transfected with different scL/MEL complexes containing increasing doses of MEL. The scL-p53 was prepared as previously described (U.S. Patent No. 7,780,822). The DNA dose used for all transfections was $0.2ug/4x10^5$ cells. This dose was based upon

the data from FIG. 36 wherein the IC_{20} was found to be a dose of approximately 0.2ug. The IC_{20} was used to allow detection of an additive or synergistic effect of the two treatments. The KMS-11 cells were transfect with Free (unencapsulated) MEL alone, scL/MEL alone, or the combination of Free (unencapsulated) or scL encapsulated MEL plus scL-p53 (FIG. 37).

[00277] When compared to free MEL alone, transfection with the scL/Mel complex resulted in a significant level of chemosensitization to the drug. Moreover, when used in combination with either free or scL complexed MEL the addition of scL-p53 was able to significantly improve the response of the KMS-11cells to this chemotherapeutic agent, with the combination of scL/MEL and scL-p53 being the most effective. Compared to the IC_{50} of unencapsulated MEL, the standard form used as a therapeutic (IC_{50} = 10.9) the IC_{50} of the scL/MEL plus scL-p53 was 4.57, a greater that 2 fold increase in cell death.

[00278] Although these studies have been performed *in vitro*, it is fully expected that similar results (increased multiple myeloma cell death) will also occur when scL/Mel and scL-p53 are administered systemically in combination to human patients. The dose of scL-p53 is expected to be between 2.4 and 3.6 mg/infusion with twice weekly infusions for 5 weeks. The scL/MEL will be administered as a single intravenous infusion of a dose of between 6 and 16mg/m^2 at two week intervals for four doses.

[00279] The unexpected level of enhancement of the combination observed here indicates the potential of this combination approach as a new therapeutic modality for the treatment of multiple myeloma in human patients.

[00280]

Example 22

Preparation of Cationic Liposomes Comprising Atropine

Materials:

[00281] DOTAP (1,2-dioleoyl-3-trimethylammonium propane, chloride salt)

-Obtained from Avanti Polar Lipids, Inc. Cat. #890890E, MW 698.55

-Concentration: 25 mg/mL ethanol solution

Dilute lipid to 20mg/ml with absolute ethanol before use

[00282] DOPE (1,2-dioleoyl-sn-glycero-3-phosphoethanolamine)

-Obtained from Avanti Polar Lipids, Inc. Cat. # 850725E, MW 744.04

-Concentration: 25 mg/mL ethanol solution.

Dilute lipid to 20mg/ml with absolute ethanol before use

[00283] Atropine, powder (M Wt = 289.37)

-Obtained from Sigma

- Dissolve in absolute ethanol to a concentration of 100mM.

[00284] Ultra-pure, endotoxin free LAL Reagent Water (e.g. BioWhittaker, Cat.# W50-500, endotoxin <0.005 EU/ml)

[00285] Injector: Hamilton Gastight Syringe, 1ml (Hamilton #81230) with a 22 gauge needle, part #81365)

Procedure:

[00286] 1. Fresh Atropine solution is prepared each time by dissolving Atropine in absolute ethanol to a concentration of 100mM by vortexing at high speed until dissolved (must be clear). Hold at room temperature until used to mix with lipids (Step 3 below).

[00287] 2. Place lipid solutions at 37° C for 10-15 min, following which place the lipid solutions in a 65° C water bath with occasional shaking for 5 min.

[00288] 3. To prepare the Lip-Atropine: Place a brown glass bottle with stir bar on a hot plate set to 50°C to 60°C. While stirring at high speed without splashing, add the lipids and Atropine to the bottle in the following order (important):

[00289] For 1:1 (Lip:Atropine) molar ratio

DOTAP	175 µl (of 20 mg/ml) = 5 µmol or 3.5 mg
DOPE	187.5 µl (of 20 mg/ml) = 5 µmol or 3.75 mg
Add Atropine soln.,	100 µl (of 100mM) = 10 µmol,

Continuously stir for 3 min. after all 3 have been added

[00290] 4. In the meantime, warm 4,569 uL LAL water to 65° C in water bath in brown glass bottle with stir bar. Immediately prior to addition of the Lipid-Atropine solution, move the bottle to a hot plate (50 °- 60° C). Stir water at high speed with no splashing for a few sec to remove bubbles from the stir bar.

[00291] 5. Keep the water on the hot plate. Continue stirring the water at high speed (without splashing) during lipid addition. After mixing lipids and Atropine as above (Step 2), immediately and as rapidly as possible, using the Hamilton syringe for injection, inject the mixture into the hot water on the hot plate (50° - 60° C) directly into

the center of the vortex. Continue stirring on high speed (without splashing) for 1 min after the addition of the lipid mixture while loosely covered.

[00292] 6. Move the glass bottle to a RT stir plate, and, continue to stir slowly until the loosely covered solution cools down to 20-25°C (room temperature)

[00293] 7. Adjust the volume to 5 ml with room temperature LAL water.

[00294] 8. Filter the solution using a 0.22 μm pore Milex GV filter.

[00295] 9. Measure particle size and zeta potential if desired.

Results of these preparation methods demonstrate liposomes having a particle size of about 20-100nm and a Zeta Potential of about 10 to 50 mV.

Example 23

Preparation of Targeted Cationic Liposomes Containing Atropine Without Chemical Conjugation (By Simple Mixing)

[00296] Using the Atropine-comprising cationic liposomes prepared according to the procedure described above, the ligand targeted Atropine cationic liposome complex as described herein is prepared by simple mixing of the components and without chemical conjugation. The preparation of the complexes was in accordance with the following general procedure.

[00297] To the liposome-water (or buffer) the appropriate amount of targeting moiety is added to give the desired ratio and mixed by gentle inversion 5-10 seconds. The targeting moiety can be a ligand including but not limited to transferrin or folate, or other proteins. It can also be an antibody or an antibody fragment that targets a cell surface receptor including, but not limited to the transferrin or HER-2 receptor (e.g., TfRscFv). This mixture is kept at room temperature for 10-15 minutes (again inverted gently for 5-10 seconds after approximately 5 minutes). To yield the desired final volume the targeting moiety-Lip-Atropine admixture is mixed with any volume (including none) of water (suitably deionized water) or a buffer of any pH including, but not limited to, Tris buffers, HEPES buffers or Phosphate Buffered Saline, required to give a desired volume and inverted gently for 5-10 seconds to mix. This mixture is kept at room temperature for 10-15 minutes (again inverted gently for 5-10 seconds after approximately 5 minutes).

[00298] For use *in vivo* dextrose or sucrose is added last to a final concentration of about 1-50% (V:V) dextrose or sucrose, suitably 5% dextrose or 10% sucrose, and mixed by gentle inversion for 5-10 seconds. This mixture is kept at room temperature for 10-15 minutes (again inverted gently for 5-10 seconds after approximately 5 minutes).

[00299] The size (number average) of the final complex prepared by the method is between about 10 to 800 nm, suitably about 15 to 400 nm, most suitably about 20 to 200 nm with a zeta potential of between about 1 and 100 mV, more suitably 5 to 60 mV and most suitably 10 to 50mV as determined by dynamic light scattering using a Malvern Zetasizer ZS. This size is small enough to efficiently pass through the tumor capillary bed, or cross the blood brain barrier.

[00300] It will be readily apparent to one of ordinary skill in the relevant arts that other suitable modifications and adaptations to the methods and applications described herein can be made without departing from the scope of any of the embodiments.

[00301] It is to be understood that while certain embodiments have been illustrated and described herein, the claims are not to be limited to the specific forms or arrangement of parts described and shown. In the specification, there have been disclosed illustrative embodiments and, although specific terms are employed, they are used in a generic and descriptive sense only and not for purposes of limitation. Modifications and variations of the embodiments are possible in light of the above teachings. It is therefore to be understood that the embodiments may be practiced otherwise than as specifically described.

[00302] All publications, patents and patent applications mentioned in this specification are herein incorporated by reference to the same extent as if each individual publication, patent or patent application was specifically and individually indicated to be incorporated by reference.

WHAT IS CLAIMED IS:

1. A method of preparing a targeted temozolomide cationic liposome complex, comprising:
   (a) preparing a lipid solution comprising one or more cationic lipids in ethanol;
   (b) preparing a solution of temozolomide;
   (c) mixing the lipid solution with the solution of temozolomide;
   (d) injecting the mixture of lipid and temozolomide into an aqueous solution, thereby forming a temozolomide cationic liposome;
   (e) mixing the temozolomide cationic liposome with a ligand to form the targeted temozolomide cationic liposome, wherein the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome.

2. The method of claim 1, wherein the ligand is an antibody, an antibody fragment or a protein.

3. The method of claim 2, wherein the ligand is a single chain Fv antibody fragment.

4. The method of claim 3, wherein the single chain Fv antibody fragment is an anti-transferrin receptor single chain Fv (TfRscFv).

5. The method of claim 1, wherein the solution of temozolomide is prepared in dimethyl sulfoxide (DMSO).

6. The method of claim 1, wherein the lipid solution comprises 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE).

7. The method of claim 1, wherein the solution of temozolomide is prepared at a concentration of about 1 mM to about 200 mM.

8. The method of claim 7, wherein the solution of temozolomide is prepared at a concentration of about 50 mM to about 200 mM.

9. The method of claim 1, wherein the molar ratio of lipid:temozolomide is about 0.1:1 to about 5:1.

10. The method of claim 9, wherein the molar ratio of lipid:temozolomide is about 0.5:1 to about 2:1.

11. The method of claim 10, wherein the molar ratio of lipid:temozolomide is about 1:1.

12. The method of claim 1, wherein the weight ratio of ligand:lipid is about 0.01:1 to about 0.5:1.

13. The method of claim 12, wherein the weight ratio of ligand:lipid is about 0.3:1 to about 0.4:1.

14. The method of claim 4, wherein the weight ratio of TfRscFv:lipid is about 0.33:1.

15. A method of preparing a targeted temozolomide cationic liposome complex, comprising:

(a) preparing a lipid solution comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE) in ethanol;

(b) preparing a solution of temozolomide;

(c) mixing the lipid solution with the solution of temozolomide;

(d) injecting the mixture of lipid and temozolomide into an aqueous solution, thereby forming a temozolomide cationic liposome;

(e) mixing the temozolomide cationic liposome with an anti-transferrin receptor single chain Fv (TfRscFv) to form the targeted temozolomide cationic liposome complex, wherein the TfRscFv is directly complexed with, but not chemically conjugated to, the cationic liposome.

16. The method of claim 15, wherein the solution of temozolomide is prepared in dimethyl sulfoxide (DMSO).

17. The method of claim 15, wherein the solution of temozolomide is prepared at a concentration of about 1 mM to about 200 mM.

18. The method of claim 17, wherein the solution of temozolomide is prepared at a concentration of about 50 mM to about 200 mM.

19. The method of claim 15, wherein the molar ratio of lipid:temozolomide is about 0.1:1 to about 5:1.

20. The method of claim 19, wherein the molar ratio of lipid:temozolomide is about 0.5:1 to about 2:1.

21. The method of claim 20, wherein the molar ratio of lipid:temozolomide is about 1:1.

22. The method of claim 15, wherein the weight ratio of TfRscFv:lipid is about 0.01:1 to about 0.5:1.

23. The method of claim 22, wherein the weight ratio of TfRscFv:lipid is about 0.3:1 to about 0.4:1.

24. The method of claim 23, wherein the weight ratio of TfRscFv:lipid is about 0.33:1.

25. Use of a targeted temozolomide cationic liposome complex prepared by:

i. preparing a lipid solution comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE) in ethanol;

ii. preparing a solution of temozolomide;

iii. mixing the lipid solution with the solution of temozolomide;

iv. injecting the mixture of lipid and temozolomide into an aqueous solution, thereby forming a temozolomide cationic liposome; and

v. mixing the temozolomide cationic liposome with a ligand to form the targeted temozolomide cationic liposome, wherein the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome,

for the manufacture of a medicament for treating cancer in a patient.

26. The use of claim 25, wherein the ligand is an antibody, an antibody fragment or a protein.

27. The use of claim 26, wherein the ligand is a single chain Fv antibody fragment.

28. The use of claim 27, wherein the single chain Fv antibody fragment is an anti-transferrin receptor single chain Fv (TfRscFv).

29. The use of claim 25, wherein the temozolomide is formulated for administration to the patient at a dose of about 10 mg/m^2 to about 500 mg/m^2.

30. The use of claim 29, wherein the temozolomide is formulated for administration to the patient at a dose of about 50 mg/m^2 to about 250 mg/m^2.

31. The use of claim 25, wherein the molar ratio of lipid in the cationic liposome:temozolomide is about 0.1:1 to about 5:1.

32. The use of claim 31, wherein the molar ratio of lipid in the cationic liposome:temozolomide is about 0.5:1 to about 2:1.

33. The use of claim 32, wherein the molar ratio of lipid in the cationic liposome:temozolomide is about 1:1.

34. The use of claim 25, wherein the weight ratio of ligand:lipid in the cationic liposome is about 0.01:1 to about 0.5:1.

35. The use of claim 34, wherein the weight ratio of ligand:lipid in the cationic liposome is about 0.3:1 to about 0.4:1.

36. The use of claim 28, wherein the weight ratio of TfRscFv:lipid in the cationic liposome is about 0.33:1.

37. The use of claim 25, wherein the medicament is formulated for intravenous (IV), intratumoral (IT), intralesional (IL), sublingual (SL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), intraocular (IO), intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump.

38. The use of claim 25, wherein the cancer is head and neck cancer, breast cancer, prostate cancer, pancreatic cancer, brain cancer, neuroendocrine cancer, cervical cancer, lung cancer, liver cancer, liposarcoma, rhabdomyosarcoma, choriocarcinoma, melanoma, retinoblastoma, ovarian cancer, urogenital cancer, gastric cancer, colorectal cancer, multiple myeloma or a cancer of the blood.

39. The use of claim 38, wherein the brain cancer is a glioma, astrocytoma or a glioblastoma.

40. The use of claim 25, wherein the targeted temozolomide cationic liposome complex medicament is to be administered in combination with an additional therapy.

41. The use of claim 40, wherein the additional therapy comprises administration of a chemotherapeutic agent, a small molecule, radiation therapy or a nucleic acid-based therapy.

42. The use of claim 41, wherein the nucleic acid-based therapy comprises administration of a cationic liposome complex comprising a plasmid DNA expressing wild-type p53.

43. Use of a targeted temozolomide cationic liposome complex prepared by:

i. preparing a lipid solution comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE) in ethanol;

ii. preparing a solution of temozolomide;

iii. mixing the lipid solution with the solution of temozolomide;

iv. injecting the mixture of lipid and temozolomide into an aqueous solution, thereby forming a temozolomide cationic liposome; and

v. mixing the temozolomide cationic liposome with an anti-transferrin receptor single chain Fv (TfRscFv) to form the targeted temozolomide cationic liposome, wherein the anti-transferrin receptor single chain Fv (TfRscFv) is directly complexed with, but not chemically conjugated to, the cationic liposome,

for the manufacture of a medicament for treating brain cancer in a patient.

44. The use of claim 43, wherein the temozolomide is formulated for administration to the patient at a dose of about 10 mg/m^2 to about 500 mg/m^2.

45. The use of claim 44, wherein the temozolomide is formulated for administration to the patient at a dose of about 100 mg/m^2 to about 250 mg/m^2.

46. The use of claim 43, wherein the molar ratio of lipid in the cationic liposome:temozolomide is about 0.1:1 to about 5:1.

47. The use of claim 46, wherein the molar ratio of lipid in the cationic liposome:temozolomide is about 0.5:1 to about 2:1.

48. The use of claim 47, wherein the molar ratio of lipid in the cationic liposome:temozolomide is about 1:1.

49. The use of claim 43, wherein the weight ratio of TfRscFv:lipid in the cationic liposome is about 0.01:1 to about 0.5:1.

50. The use of claim 49, wherein the weight ratio of TfRscFv:lipid in the cationic liposome is about 0.3:1 to about 0.4:1.

51. The use of claim 50, wherein the weight ratio of TfRscFv:lipid in the cationic liposome is about 0.33:1.

52. The use of claim 43, wherein the medicament is formulated for intravenous (IV), intratumoral (IT), intralesional (IL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), sublingual (SL), intraocular (IO), intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump.

53. The use of claim 43, wherein the brain cancer is a glioma, astrocytoma or a glioblastoma.

54. Use of a targeted temozolomide cationic liposome complex prepared by the method of claim 1 for the manufacture of a medicament for treating cancer in a patient.

55. The use of claim 54, wherein the ligand is an antibody, an antibody fragment or a protein.

56. The use of claim 55, wherein the ligand is a single chain Fv antibody fragment.

57. The use of claim 56, wherein the single chain Fv antibody fragment is an anti-transferrin receptor single chain Fv (TfRscFv).

58. The use of claim 54, wherein temozolomide is formulated for administration to the patient at a dose of about 10 mg/m^2 to about 500 mg/m^2.

59. The use of claim 58, wherein temozolomide is formulated for administration to the patient at a dose of about 50 mg/m^2 to about 250 mg/m^2.

60. The use of claim 54, wherein the molar ratio of lipid:temozolomide is about 0.1:1 to about 5:1.

61. The use of claim 57, wherein the molar ratio of lipid:temozolomide is about 0.5:1 to about 2:1.

62. The use of claim 60, wherein the molar ratio of lipid:temozolomide is about 1:1.

63. The use of claim 54, wherein the weight ratio of ligand:lipid is about 0.01:1 to about 0.5:1.

64. The use of claim 63, wherein the weight ratio of ligand:lipid is about 0.3:1 to about 0.4:1.

65. The use of claim 54, wherein the medicament is formulated for intravenous (IV), intratumoral (IT), intralesional (IL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), sublingual (SL), intraocular (IO), intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump

66. The use of claim 54, wherein the cancer is head and neck cancer, breast cancer, prostate cancer, pancreatic cancer, brain cancer, neuroendocrine cancer, cervical cancer, lung cancer, liver cancer, liposarcoma, rhabdomyosarcoma, choriocarcinoma, melanoma, retinoblastoma, ovarian cancer, urogenital cancer, gastric cancer, colorectal cancer, multiple myeloma or a cancer of the blood.

67. The use of claim 66, wherein the brain cancer is a glioma, astrocytoma or a glioblastoma.

68. The use of claim 54, wherein the targeted temozolomide cationic liposome complex medicament is to be administered in combination with an additional therapy to the patient.

69. The use of claim 68, wherein the additional therapy comprises administration of a chemotherapeutic agent, a small molecule, radiation therapy or a nucleic acid-based therapy.

70. The use of claim 69, wherein the nucleic acid-based therapy comprises administration of a cationic liposome complex comprising a plasmid DNA expressing wild-type p53.

71. A method of preparing a targeted melphalan cationic liposome complex, comprising:

(a) preparing a lipid solution comprising one or more cationic lipids in ethanol;

(b) preparing a solution of melphalan;

(c) mixing the lipid solution with the solution of melphalan;

(d) injecting the mixture of lipid and melphalan into an aqueous solution, thereby forming a melphalan cationic liposome;

(e) mixing the melphalan cationic liposome with a ligand to form the targeted melphalan cationic liposome, wherein the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome.

72. The method of claim 71, wherein the ligand is an antibody, an antibody fragment or a protein.

73. The method of claim 72, wherein the ligand is a single chain Fv antibody fragment.

74. The method of claim 73, wherein the single chain Fv antibody fragment is an anti-transferrin receptor single chain Fv (TfRscFv).

75. The method of claim 71, wherein the solution of melphalan is prepared in absolute ethanol plus hydrochloric acid.

76. The method of claim 71, wherein the lipid solution comprises 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE).

77. The method of claim 71, wherein the solution of melphalan is prepared at a concentration of about 1 mM to about 200 mM.

78. The method of claim 77, wherein the solution of melphalan is prepared at a concentration of about 50 mM to about 200 mM.

79. The method of claim 71, wherein the molar ratio of lipid:melphalan is about 0.1:1 to about 5:1.

80. The method of claim 79, wherein the molar ratio of lipid:melphalan is about 0.5:1 to about 2:1.

81. The method of claim 80, wherein the molar ratio of lipid:melphalan is about 1:1.

82. The method of claim 71, wherein the weight ratio of ligand:lipid is about 0.01:1 to about 0.5:1.

83. The method of claim 82, wherein the weight ratio of ligand:lipid is about 0.3:1 to about 0.4:1.

84. The method of claim 74, wherein the weight ratio of TfRscFv:lipid is about 0.33:1.

85. A method of preparing a targeted melphalan cationic liposome complex, comprising:

(a) preparing a lipid solution comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE)in ethanol;

(b) preparing a solution of melphalan;

(c) mixing the lipid solution with the solution of melphalan;

(d) injecting the mixture of lipid and melphalan into an aqueous solution, thereby forming a melphalan cationic liposome;

(e) mixing the melphalan cationic liposome with an anti-transferrin receptor single chain Fv (TfRscFv) to form the targeted melphalan cationic liposome complex, wherein the TfRscFv is directly complexed with, but not chemically conjugated to, the cationic liposome.

86. The method of claim 85, wherein the solution of melphalan is prepared in absolute ethanol plus hydrochloric acid.

87. The method of claim 85, wherein the solution of melphalan is prepared at a concentration of about 1 mM to about 200 mM.

88. The method of claim 87, wherein the solution of melphalan is prepared at a concentration of about 50 mM to about 200 mM

89. The method of claim 88, wherein the solution of melphalan is prepared at a concentration of about 145 mM to about 150 mM.

90. The method of claim 85, wherein the molar ratio of lipid:melphalan is about 0.1:1 to about 5:1.

91. The method of claim 90, wherein the molar ratio of lipid:melphalan is about 0.5:1 to about 2:1.

92. The method of claim 91, wherein the molar ratio of lipid:melphalan is about 1:1.

93. The method of claim 85, wherein the weight ratio of TfRscFv:lipid is about 0.01:1 to about 0.5:1.

94. The method of claim 93, wherein the weight ratio of TfRscFv:lipid is about 0.3:1 to about 0.4:1.

95. The method of claim 93, wherein the weight ratio of TfRscFv:lipid is about 0.33:1.

96. Use of a targeted melphalan cationic liposome complex prepared by:

i. preparing a lipid solution comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE) in ethanol;

ii. preparing a solution of melphalan;

iii. mixing the lipid solution with the solution of melphalan;

iv. injecting the mixture of lipid and melphalan into an aqueous solution, thereby forming a melphalan cationic liposome; and

v. mixing the melphalan cationic liposome with a ligand to form the targeted melphalan cationic liposome, wherein the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome,

for the manufacture of a medicament for treating cancer in a patient.

97. The use of claim 96, wherein the ligand is an antibody, an antibody fragment or a protein.

98. The use of claim 97, wherein the ligand is a single chain Fv antibody fragment.

99. The use of claim 98, wherein the single chain Fv antibody fragment is an anti-transferrin receptor single chain Fv (TfRscFv).

100. The use of claim 96, wherein the melphalan is formulated for administration to the patient at a dose of about 1 mg/m2 to about 100 mg/m2.

101. The use of claim 100, wherein the melphalan is formulated for administration to the patient at a dose of about 5 mg/m2 to about 20 mg/m2.

102. The use of claim 96, wherein the molar ratio of lipid in the cationic liposome:melphalan is about 0.1:1 to about 5:1.

103. The use of claim 102, wherein the molar ratio of lipid in the cationic liposome:melphalan is about 0.5:1 to about 2:1.

104. The use of claim 103, wherein the molar ratio of lipid in the cationic liposome:melphalan is about 1:1.

105. The use of claim 96, wherein the weight ratio of ligand:lipid in the cationic liposome is about 0.01:1 to about 0.5:1.

106. The use of claim 105, wherein the weight ratio of ligand:lipid in the cationic liposome is about 0.3:1 to about 0.4:1.

107. The use of claim 99, wherein the weight ratio of TfRscFv:lipid in the cationic liposome is about 0.33:1.

108. The use of claim 96, wherein the medicament is formulated for intravenous (IV), intratumoral (IT), intralesional (IL), sublingual (SL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), intraocular (IO), intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump.

109. The use of claim 96, wherein the cancer is head and neck cancer, breast cancer, prostate cancer, pancreatic cancer, brain cancer, neuroendocrine cancer, cervical cancer, lung cancer, liver cancer, liposarcoma, rhabdomyosarcoma, choriocarcinoma, melanoma, retinoblastoma, ovarian cancer, urogenital cancer, gastric cancer, colorectal cancer, multiple myeloma or a cancer of the blood.

110. The use of claim 109, wherein the cancer is multiple myeloma.

111. The use of claim 96, wherein the targeted melphalan cationic liposome complex medicament is to be administered in combination with an additional therapy.

112. The use of claim 111, wherein the additional therapy comprises administration of a chemotherapeutic agent, a small molecule, radiation therapy or a nucleic acid-based therapy.

113. The use of claim 112, wherein the nucleic acid-based therapy comprises administration of a cationic liposome complex comprising a plasmid DNA expressing wild-type p53.

114. Use of a targeted melphalan cationic liposome complex prepared by:

i. preparing a lipid solution comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE) in ethanol;

ii. preparing a solution of melphalan;

iii. mixing the lipid solution with the solution of melphalan;

iv. injecting the mixture of lipid and melphalan into an aqueous solution, thereby forming a melphalan cationic liposome; and

v. mixing the melphalan cationic liposome with an anti-transferrin receptor single chain Fv (TfRscFv) to form the targeted melphalan cationic liposome, wherein the anti-transferrin receptor single chain Fv (TfRscFv) is directly complexed with, but not chemically conjugated to, the cationic liposome,

for the manufacture of a medicament for treating cancer in a patient.

115. The use of claim 114, wherein the melphalan is formulated for administration to the patient at a dose of about 1 mg/m^2 to about 100 mg/m^2.

116. The use of claim 115, wherein the melphalan is formulated for administration to the patient at a dose of about 5 mg/m^2 to about 20 mg/m^2.

117. The use of claim 114, wherein the molar ratio of lipid in the cationic liposome:melphalan is about 0.1:1 to about 5:1.

118. The use of claim 117, wherein the molar ratio of lipid in the cationic liposome:melphalan is about 0.5:1 to about 2:1.

119. The use of claim 118, wherein the molar ratio of lipid in the cationic liposome:melphalan is about 1:1.

120. The use of claim 114, wherein the weight ratio of TfRscFv:lipid in the cationic liposome is about 0.01:1 to about 0.5:1.

121. The use of claim 120, wherein the weight ratio of TfRscFv:lipid in the cationic liposome is about 0.3:1 to about 0.4:1.

122. The use of claim 121, wherein the weight ratio of TfRscFv:lipid in the cationic liposome is about 0.33:1.

123. The use of claim 114, wherein the medicament is formulated for intravenous (IV), intratumoral (IT), intralesional (IL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), sublingual (SL), intraocular (IO), intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump.

124. The use of claim 114, wherein the cancer is multiple myeloma.

125. Use of a targeted melphalan cationic liposome complex prepared by the method of claim 71 for the manufacture of a medicament for treating cancer in a patient.

126. The use of claim 125, wherein the ligand is an antibody, an antibody fragment or a protein.

127. The use of claim 126, wherein the ligand is a single chain Fv antibody fragment.

128. The use of claim 127, wherein the single chain Fv antibody fragment is an anti-transferrin receptor single chain Fv (TfRscFv).

129. The use of claim 125, wherein melphalan is formulated for administration to the patient at a dose of about 1 mg/m^2 to about 100 mg/m^2.

130. The use of claim 129, wherein melphalan is formulated for administration to the patient at a dose of about 5 mg/m^2 to about 20 mg/m^2.

131. The use of claim 125, wherein the molar ratio of lipid:melphalan is about 0.1:1 to about 5:1.

132. The use of claim 128, wherein the molar ratio of lipid:melphalan is about 0.5:1 to about 2:1.

133. The use of claim 131, wherein the molar ratio of lipid:melphalan is about 1:1.

134. The use of claim 125, wherein the weight ratio of ligand:lipid is about 0.01:1 to about 0.5:1.

135. The use of claim 134, wherein the weight ratio of ligand:lipid is about 0.3:1 to about 0.4:1.

136. The use of claim 125, wherein the medicament is formulated for intravenous (IV), intratumoral (IT), intralesional (IL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), sublingual (SL), intraocular (IO), intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump

137. The use of claim 125, wherein the cancer is head and neck cancer, breast cancer, prostate cancer, pancreatic cancer, brain cancer, neuroendocrine cancer, cervical cancer, lung cancer, liver cancer, liposarcoma, rhabdomyosarcoma, choriocarcinoma, melanoma, retinoblastoma, ovarian cancer, urogenital cancer, gastric cancer, colorectal cancer, multiple myeloma or a cancer of the blood.

138. The use of claim 137, wherein the cancer is multiple myeloma.

139. The use of claim 125, wherein the targeted melphalan cationic liposome complex medicament is to be administered in combination with an additional therapy.

140. The use of claim 139, wherein the additional therapy comprises administration of a chemotherapeutic agent, a small molecule, radiation therapy or a nucleic acid-based therapy.

141. The use of claim 140, wherein the nucleic acid-based therapy comprises administration of a cationic liposome complex comprising a plasmid DNA expressing wild-type p53.

142. Use of:

(a) a cationic liposome complex comprising:

(1) a cationic liposome comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE);

(2) a plasmid DNA expressing wild-type p53; and

(3) an anti-transferrin receptor single chain Fv (TfRscFv) directly complexed with, but not chemically conjugated to, the cationic liposome; and

(b) temozolomide,

for the manufacture of a medicament for treating a brain cancer in a patient.

143. The use of claim 142, wherein the temozolomide is formulated for administration at the same time or after the cationic liposome complex.

144. The use of claim 142, wherein the temozolomide is formulated for administration to the patient at a dose of about 10 mg/m^2 to about 500 mg/m^2.

145. The use of claim 144, wherein the temozolomide is formulated for administration to the patient at a dose of about 100 mg/m^2 to about 250 mg/m^2.

146. The use of claim 142, wherein the medicament is formulated for intravenous (IV), intratumoral (IT), intralesional (IL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), sublingual (SL), intraocular (IO),

intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump.

147. The use of claim 142, wherein the brain cancer is a glioma, astrocytoma or glioblastoma.

148. Use of a targeted atropine cationic liposome complex prepared by:

i. preparing a lipid solution comprising 1,2-dioleoyl-3-trimethylammonium propane (DOTAP) and 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE) in ethanol;

ii. preparing a solution of atropine;

iii. mixing the lipid solution with the solution of atropine;

iv. injecting the mixture of lipid and atropine into an aqueous solution, thereby forming an atropine cationic liposome; and

v. mixing the atropine cationic liposome with a ligand to form the targeted atropine cationic liposome, wherein the ligand is directly complexed with, but not chemically conjugated to, the cationic liposome,

for the manufacture of a medicament for treating organophosphate poisoning in a patient.

149. The use of claim 148, wherein the ligand is an antibody, an antibody fragment or a protein.

150. The use of claim 149, wherein the ligand is a single chain Fv antibody fragment.

151. The use of claim 150, wherein the single chain Fv antibody fragment is an anti-transferrin receptor single chain Fv (TfRscFv).

152. The use of claim 148, wherein the atropine is formulated for administration to the patient at a dose of about 1 mg to about 10 mg.

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153. The use of claim 152, wherein the atropine is formulated for administration to the patient at a dose of about 2 mg to about 6 mg.

154. The use of claim 148, wherein the molar ratio of lipid in the cationic liposome: atropine is about 0.1:1 to about 5:1.

155. The use of claim 154, wherein the molar ratio of lipid in the cationic liposome: atropine is about 0.5:1 to about 2:1.

156. The use of claim 155, wherein the molar ratio of lipid in the cationic liposome: atropine is about 1:1.

157. The use of claim 148, wherein the weight ratio of ligand:lipid in the cationic liposome is about 0.01:1 to about 0.5:1.

158. The use of claim 157, wherein the weight ratio of ligand:lipid in the cationic liposome is about 0.3:1 to about 0.4:1.

159. The use of claim 151, wherein the weight ratio of TfRscFv:lipid in the cationic liposome is about 0.33:1.

160. The use of claim 148, wherein the medicament is formulated for intravenous (IV), intratumoral (IT), intralesional (IL), sublingual (SL), aerosal, percutaneous, oral, endoscopic, topical, intramuscular (IM), intradermal (ID), intraocular (IO), intraperitoneal (IP), transdermal (TD), intranasal (IN), intracereberal (IC), intraorgan (e.g. intrahepatic), slow release implant, or subcutaneous administration, or via administration using an osmotic or mechanical pump.

161. The use of claim 148, wherein the liposome crosses the blood-brain barrier.