

DESCRIPTION**"Endoluminal prosthesis"**

[0001]. The object of the present invention is an endoluminal prosthesis to be used in passageways or
5 conduits of the human body, such as to restore the passage in blood vessels that have been narrowed or blocked by diseases such as a stenosis.

[0002]. The present endoluminal prosthesis is particularly suitable for use in the vicinity of a
10 bifurcation, mainly of the carotid.

[0003]. The present invention also relates to that type of endoluminal prostheses which are self-expanding, such as made of superelastic or shape memory material, such as Nitinol.

15 [0004]. The present invention also relates to endoluminal prostheses provided with means for a prompt location thereof, such as by means of radioscopy.

[0005]. Endoluminal prosthesis, particularly of the self-expanding type, are known for example from US-A-
20 4665771, US-A-4665905, US-A-4925445, EP-A-0928606, or WO 2005/104991.

[0006]. Though being acceptable in many respects, particularly for their great flexibility and resilience, which enable them to be easily positioned in narrow and
25 tortuous passages in their collapsed state, these

endoluminal prostheses, in some cases, are not sufficiently suitable, when expanded, to support the vessel walls, in order to maintain a proper free lumen for the blood to pass therethrough.

5 [0007]. Furthermore, in some cases the complex geometry of such known stents may be harmful, since it can hang up to or pinch the vessel wall, thus favouring the re-forming of obstructions, such as plaques and stenosis.

10 [0008]. Particularly, in the carotid, the endoluminal prosthesis must ensure a considerable radial strength in the middle portion thereof, or generally in the portion positioned at the stenosis. Furthermore, the endoluminal prosthesis must be made with the least amount
15 of material as possible, mainly in the end portions, or generally in those portions that are positioned outside the stenosis. In fact, it has been estimated that the ratio of the metal and the artery must remain within well defined limits, about 15%. Too high values lead to
20 restenosis and high mechanical rigidity.

 [0009]. The problem at the heart of the present invention is to provide an endoluminal prosthesis, having such structural and functional characteristics to overcome the drawbacks mentioned with reference to the
25 prior art and meet said requirements thereby obtaining

the best results for both.

[0010]. This problem is solved by means of an endoluminal prosthesis in accordance with claim 1.

[0011]. Further embodiments are described in the
5 secondary claims.

[0012]. Further characteristics and the advantages of the prosthesis according to the invention will become apparent from the description given below of preferred embodiments thereof, being merely illustrative and non-
10 limiting, with reference to the annexed figures, in which:

[0013]. Fig. 1 illustrates a plane development of a possible embodiment of an endoluminal prosthesis according to the present invention, illustrated in the
15 collapsed or non-expanded condition;

[0014]. Fig. 2 and 3 illustrate a plane development of a variant embodiment of the prosthesis from Fig. 1, illustrated in a collapsed or non-expanded condition;

20 [0015]. Fig. 4 illustrates, in a perspective view, the prosthesis from Fig. 1 in the expanded condition;

[0016]. Fig. 4a illustrates an enlargement of a detail from Fig. 4;

[0017]. Fig. 5 illustrates, in a perspective view,
25 a possible variant embodiment of the prosthesis from Fig.

4;

[0018]. Fig. 6a-6c illustrates an enlarged detail of the prosthesis from Fig. 5, at a distal, middle and proximal portion, respectively;

5 [0019]. Fig. 7a illustrates diagrams of the radial compression force (N) of the distal, middle and proximal portion of two prostheses according to Fig. 5 as compared with a prior art prosthesis;

[0020]. Fig. 8 illustrates a carotid portion to
10 which the prosthesis according to the present invention is advantageously applied.

[0021]. With reference to the above mentioned figures, with 500 has been generally indicated an endoluminal prosthesis, such as a prosthesis of the self-
15 expanding type for ducts or vessels of living bodies, particularly for application in the carotid, at the bifurcation.

[0022]. In accordance with a general embodiment of the present invention, the endoluminal prosthesis
20 comprises a tubular body 502 suitable to turn from a collapsed condition to an expanded or partially expanded condition (Fig. 4 or 5).

[0023]. By "collapsed condition" is meant a state of the prosthesis as being contracted such as to have a
25 smaller bulk than in an operating use condition, e.g. a

condition where the tubular body 502 has smaller size or outer diameter than in an operating use condition. For example, the prosthesis is arranged in a collapsed condition when it is either accommodated or arranged on a transport and delivery device suitable to travel along a duct or vessel to the area to be treated. For example, in the case of a self-expanding prosthesis, this is accommodated in a sheath such as to be maintained in the collapsed condition.

[0024]. By "expanded or partially expanded condition" is meant a condition where the prosthesis is free from restrictions or an operating use condition with the prosthesis being widened upon pressure contact against the inner surfaces of duct or vessel walls (Fig. 4 and 5).

[0025]. The tubular body 502 develops along a longitudinal axis 504.

[0026]. By "longitudinal axis" is meant for example either a symmetry axis of a cylindrical body or the stretch axial direction of a tubular body.

[0027]. The tubular body 502 comprises a plurality of serpentes 506a-506d, 508a-508e, 510a-510d, or closed meander paths, developing along a substantially circumferential direction.

[0028]. By "serpentine" is meant an element that

develops zig-zag/to-and-fro around a main direction of stretching.

[0029]. Each of said serpentine comprises arm portions, or arms 511.

5 [0030]. each of said serpentine comprises bend portions, or bends 512, joining two subsequent arms 511 to form said meander path.

[0031]. With further advantage, the bends 512 facing an adjacent serpentine are circumferentially
10 offset relative to the respective and opposite bends 512 of the adjoining serpentine, both when the prosthesis is collapsed and when the prosthesis is expanded or partially expanded.

[0032]. In other words, considering a tract of a
15 first serpentine corresponding to a pitch, the adjacent serpentine is offset X up to about half pitch (Fig. 4). With a half-pitch offset, two adjacent serpentine are substantially mirror-like relative to a middle circumferential line between the two serpentine.

20 [0033]. In accordance with a possible embodiment, the arms are connected by bends such as to form a sequence of peaks and valleys along the circumferential direction of the corresponding serpentine. With a half-pitch offset, to a bend of a first serpentine defining a
25 peak 512a there corresponds a bend of the adjacent

serpentine defining a valley 512b, "peak" and "valley" meaning the substantially sinusoidal development of the serpentine (Fig. 4a). Two respective peaks and valleys of two adjacent serpentine define a pair of bends located
5 at the shortest longitudinal distance between the two serpentine.

[0034]. Advantageously, at least one bridge 514a-514c, of main longitudinal extension, connects two adjacent serpentine. Particularly, the bridge connects
10 two adjacent serpentine at two respective bends being at the shortest longitudinal distance between the two serpentine.

[0035]. Preferably, the at least one bridge 514a-514c connecting adjacent serpentine extends
15 substantially rectilinear.

[0036]. Advantageously, the serpentine are grouped in at least two portions 506 and 510, 508 arranged along the longitudinal axis 504, in which a first portion 506 or 510 comprises at least two adjacent
20 serpentine being interconnected by at least one bridge 514a. In the first portion 506 or 510 at least one pair of bends being at the shortest longitudinal distance between the two adjacent serpentine is not connected by a bridge.

25 [0037]. A second portion 508 comprises at least

two adjacent serpentines interconnected by bridges 514b in equal number to the pairs of bends of the two serpentines being at the shortest longitudinal distance between the two serpentines. In other words, all the
5 bends of a first serpentine facing the adjacent serpentine are connected to all the bends of the adjacent serpentine that face the first serpentine by means of a respective bridge 514b.

[0038]. Preferably, the first portion is a distal
10 and/or proximal end portion of the endoluminal prosthesis and the second portion is a middle portion of the endoluminal prosthesis.

[0039]. The example from Fig. 1 comprises three portions, two first portions 506 and 510 and a second
15 portion 510, respectively.

[0040]. The end portion designated with 506 comprises the serpentines indicated with 506a-506d and corresponds to the first portion described above. In fact, two adjacent serpentines along the longitudinal
20 axis 504 (for example, the serpentine 506a and the serpentine 506b) are interconnected by at least one bridge 514a. Several pairs of bends being at the shortest longitudinal distance between the two adjacent serpentines 506a and 506b are not connected by a bridge.
25 In the example from Fig. 1, three bridges 514a are

provided, which join two adjacent serpentines (506a and 506b, or 506b and 506c, or 506c and 506d) of the first portion 506. Furthermore, between two subsequent bridges 514a in the circumferential direction there are provided
5 five pairs of bends situated at the shortest longitudinal distance between the two adjacent serpentines and not connected by a bridge. Considering the arms and bends between two subsequent bridges 514a in the circumferential direction a cell or perimeter is obtained
10 that comprises at least one pair of bends (five, in the case of Fig. 1) which are situated at the shortest longitudinal distance between the two adjacent serpentines and not connected by a bridge (in Fig. 4, said cell or perimeter defines the dotted area A1).

15 **[0041]**. Again, considering Fig. 1, the portion designated with 506 is an end portion (that can be either proximal or distal, since the prosthesis in the expanded configuration has a substantially cylindrical conformation).

20 **[0042]**. In addition, in Fig. 1 the prosthesis comprises a further first portion, such as described above, that is defined by the end portion designated with 510 comprising the serpentines designated with 510a-510d. What has been described above with reference to the
25 portion 506 from Fig. 1 can be applied thereto. The

respective bridges between the two adjacent serpentine (such as the serpentine 510c and the serpentine 510d) have been designated with 514a. Also in this case, the portion designated with 510 is an end portion (that can be either proximal or distal, since the prosthesis in the expanded configuration has a substantially cylindrical conformation). With reference to Fig. 4, with A2 has been designated the area enclosed by the cell or perimeter defined between two subsequent bridges 514a in the circumferential direction and comprising at least one pair of bends (five, in the case of Fig. 1 or 4) which are situated at the shortest longitudinal distance between the two adjacent serpentine and not connected by a bridge.

15 **[0043]**. In accordance with what has been described in general terms, the prosthesis from Fig. 1 further comprises a portion designated with 508 comprising, in turn, the serpentine designated with 508a-508e. This portion 508 corresponds to the second portion described above. In fact, two adjacent serpentine along the longitudinal axis 504 (for example, the serpentine 508a and the serpentine 508b) are interconnected by a number of bridges 514b equal to the number of pairs of bends of the two serpentine situated at the shortest longitudinal distance between the two serpentine. In other words, all

the bends of a first serpentine 508a facing the adjacent serpentine are connected to all the bends of the adjacent serpentine 508b that face the first serpentine 508a.

[0044]. In the case of Fig. 1, the portion 508 is
5 a middle portion of the endoluminal prosthesis that is interposed between the end portion 506 and the end portion 510.

[0045]. Considering the arms and the bends between two subsequent bridges 514b in the circumferential
10 direction a cell or perimeter is obtained, which comprises four arms (belonging two-by-two to one of the two adjacent serpentine), a pair of bends situated at the longest longitudinal distance between the two adjacent serpentine and two bridges 514b (in Fig. 4,
15 said cell or perimeter defines the dotted area A3).

[0046]. Fig. 2 is substantially similar to above-described Fig. 1 except that both the end portion 506 defining a first portion, and the end portion 510 also defining a first portion, and the middle portion 508
20 defining a second portion comprise four serpentine 506a-506d, 510a-510d, 508a-508d, respectively.

[0047]. Fig. 3 is also substantially similar to above-described Fig. 1 except that both the end portion 506 defining a first portion, and the end portion 510
25 also defining a first portion, comprise three serpentine

506a-506c, 510a-510c, respectively, whereas the middle portion 508 defining a second portion comprises four serpentine 508a-508d.

[0048]. Fig. 4 illustrates the prosthesis from Fig. 1 in the expanded configuration, whereas Fig. 5 illustrates a prosthesis that, in the expanded configuration, has the shape of a truncated cone, though having the same arrangement of portions and serpentine as the prosthesis from Fig. 1.

10 [0049]. In accordance with a possible embodiment, the first and second serpentine portions are connected by bridges 514c that join pairs of bends of the two serpentine situated at the shortest longitudinal distance between the two serpentine, each being a part of one of the two portions. Advantageously, the bridges 15 514c that join the first and second portions are in a number comprised between the number of the bridges 514a connecting two adjacent serpentine of the first portion and the number of bridges 514b connecting two adjacent 20 serpentine to the second portion. In accordance with a possible embodiment, the bridges 514c joining the first and second portions are about twice the bridges 514a connecting two adjacent serpentine of the first portion.

[0050]. With reference to Fig. 1, with 514c have 25 been designated the bridges joining the end portion 506

to the middle portion 508 (particularly, the serpentine 506d and the serpentine 508a) and the middle portion 508 to the other end portion 510 (particularly, the serpentine 508e and the serpentine 510a). Advantageously, the bridges 514c are in a number comprised between the number of the bridges 514a connecting two adjacent serpentines of the first portion (end portion 506 or 510) and the number of bridges 514b connecting two adjacent serpentines of the second portion (or middle portion 508). Preferably, as illustrated in Fig. 1, the bridges 514c joining the first and second portions are about twice (six) the bridges 514a connecting two adjacent serpentines of the first portion.

[0051]. Fig. 2 and 3 are similar in connection with this aspect.

[0052]. In accordance with a possible embodiment, the first portion 506 or 510 comprises at least two, preferably at least three serpentines and the bridges 514a connecting two adjacent serpentines are circumferentially offset relative to the immediately subsequent bridges along the longitudinal axis. An example of this arrangement is illustrated in Fig. 1-3, for example with reference to the bridges connecting the serpentines 506a and 506b that are circumferentially offset relative to the immediately subsequent bridges

connecting the serpentines 506b and 506c. A similar arrangement is provided for the portion 510.

[0053]. Preferably, the first portion is a proximal portion of the endoluminal prosthesis and
5 comprises at least one marker or radiopaque element 518. Furthermore, the first portion is also a distal portion of the endoluminal prosthesis and comprises at least one marker or radiopaque element 518.

[0054]. Preferably, the endoluminal prosthesis
10 comprises a proximal portion 506 provided as the first portion, a middle portion 508 provided as the second portion and a distal portion 510 provided as the first portion. Advantageously, both in the collapsed and in the expanded condition each proximal, middle and distal
15 portion develops by about one third of the length of the endoluminal prosthesis.

[0055]. According to a possible example, the prosthesis comprises a proximal portion 506 provided as the first portion, a middle portion 508 provided as the
20 second portion and a distal portion 510 provided as the first portion. In addition, the distal portion 510 and the proximal portion 506 comprise four serpentines, respectively, and the middle portion comprises five serpentines (Fig. 1).

25 [0056]. According to a different example, the

prosthesis comprises a proximal portion 506 provided as the first portion, a middle portion 508 provided as the second portion and a distal portion 510 provided as the first portion. Furthermore, the distal portion, the middle portion and the proximal portion comprise four serpentine, respectively (Fig. 2).

[0057]. According to a further different exemplary embodiment, the prosthesis comprises a proximal portion 506 provided as the first portion, a middle portion 508 provided as the second portion and a distal portion 510 provided as the first portion. In addition, the distal portion and the proximal portion comprise three serpentine, respectively, and the middle portion comprises four serpentine (Fig. 3).

[0058]. Particularly, it is advantageous to provide that in a prosthesis comprising a proximal portion 506 provided as the first portion, a middle portion 508, arranged as the second portion and a distal portion 510 arranged as the first portion, the distal portion and the proximal portion comprise a number of serpentine less than or equal to the central portion.

[0059]. In accordance with a possible embodiment, the bridges 514a-514c are rectilinear and slightly inclined relative to the longitudinal axis. Preferably, all the bridges are inclined in the same direction

relative to the longitudinal axis. Even more preferably, all the bridges are parallel to each other.

[0060]. In accordance with a possible embodiment, the prosthesis defines a cylindrical tubular body in the
5 expanded condition (Fig. 4). In accordance with a different embodiment, the endoluminal prosthesis defines a truncated-cone-shaped tubular body in the expanded condition (Fig. 5).

[0061]. In accordance with a possible embodiment,
10 the width of the bridges as measured substantially in the circumferential direction is about twice the width of the arms, also measured substantially in the circumferential direction. This aspect can be advantageously observed with reference to all the bridges in the prosthesis, i.e.
15 with reference to the bridges of the first portion, second portion or the bridges connecting two different portions.

[0062]. In several exemplary embodiments, the radial compression strength has been measured (N).
20 Several values are reported in Fig. 7a.

[0063]. Generally, the second portion 508 is capable of withstanding a compression force ranging between 0,10 and 0,20 N. In addition, the first portion 506 or 510 is capable of withstanding a compression force
25 ranging between 0,04 and 0,06 N.

[0064]. For example, Fig. 7a relates to a tubular truncated-cone-shaped body with a diameter of 6-9 mm and 30 mm in length. The first value A corresponds to the prior art (without differentiation in the radial force along the longitudinal direction). The other values B, C, D correspond to the distal, middle, and proximal portion of the prosthesis, respectively. In the instant case, A=0,10N, B=0,04N, C=0,14N and D=0,06N.

[0065]. Fig. 6a-6c illustrate a further characteristic of a prosthesis according to the present invention defined as "scaffolding" with reference to the proximal 506, middle 508 and distal 510 portion of the prosthesis, respectively. This characteristic is connected to the geometry of the stent and the support capacity of the latter. This characteristic can be indicated by measuring the diameter of the maximum circumference inscribed within a cell. The value is about 2 mm for the second portion and about 1 mm for the first portion. The lower this value, the closer the serpentine, the support being thereby increased.

[0066]. The configuration as described allows obtaining an optimum ratio of the metal extension and the artery, expressed as a percentage. Preferably, this value expressed as a percentage is the same in the end portions and different in the middle with reference to the example

illustrated above. The values of the proximal and distal portions are relatively low. The middle portion value is slightly greater, but, however, sufficiently low to avoid a wide contact area between the prosthesis material and
5 the vessel tissue.

[0067]. Furthermore, with reference to the flexibility, meaning the capacity of bending and assume a circular shape without breaking, it has been seen that the second portion (middle portion) is advantageously
10 rather rigid, whereas the first portion/s (end portions or distal and proximal portions) are rather flexible. This allows the stent to be more easily guided to the position where it has to be implanted.

[0068]. The present invention also relates to the
15 use of an endoluminal prosthesis as described above that can be implanted at a bifurcation, particularly in the carotid. The prosthesis in the expanded condition can have the shape of a truncated cone and a distal portion of the prosthesis having a smaller circumference than the
20 opposite proximal portion is positioned at the bifurcation.

[0069]. In accordance with an embodiment, said prosthesis 500 is made as one piece. For example, said body 502 is obtained by cutting a tubular element,
25 preferably by means of laser cutting.

[0070]. Advantageously, said body is made of a superelastic material. In accordance with a different embodiment, said body is made of a strain hardened pseudoelastic material. In other words, a material being
5 in the austenitic state at room temperature ($A_f < 15^\circ\text{C}$) when annealed can be used, to which a sufficient strain hardening is then applied, such as greater than 30%, which allows to get 3%-4% elastic recovery after deformation or more. Preferably, 50% strain hardening is
10 applied.

[0071]. In accordance with an embodiment, said body 502 is made of a shape memory material.

[0072]. Advantageously, said body is made of Nitinol, or a Ni and Ti based alloy, such as with Nickel
15 nominal weight percentage of 55,8%.

[0073]. For example, a material with Austenite-to-Martensite phase transition can be used that, when being in the annealed or stress-relieved state, during a heating of the same, the highest temperature at the end
20 of the transformation into austenite, or A_f , is lower than 15°C .

[0074]. In accordance with an embodiment, in order to form the marker 518, the first serpentine 506a and/or the last serpentine 510d comprises at least one frame 521
25 defining a slot or housing 522. The frame 521 is arranged

at a bend between two arms. Particularly, the frame 521 and the slot 522 can be arranged in place of at least two arms and one bend relative to the immediately adjacent serpentine along the longitudinal axis.

5 [0075]. According to a possible embodiment, the second serpentine and the third serpentine comprise the same number of arms and the same number of bends.

10 [0076]. Preferably the frame 521 and the slot 522 are arranged at the bend between two arms in place of four arms and three bends relative to the second or third serpentine. Advantageously the frame 521 totally occupies the width cleared by the replaced arms and bends, as measured along the circumferential direction, when the endoluminal prosthesis is in the collapsed
15 condition.

 [0077]. In accordance with a possible embodiment, the slot or housing 522 passes all through the thickness of the tubular body 502.

20 [0078]. Advantageously the frame 521 is arranged in the concave part of the bend between the two arms that are directly connected to the frame 521.

 [0079]. According to a possible embodiment, the prosthesis is formed as one piece from a tubular body 502 by means of cutting, such as laser cutting of a
25 cylindrical wall thereof.

[0080]. Advantageously, the frame 521 is formed as one piece in the tubular body 502 obtained by means of laser cutting of a cylindrical wall.

[0081]. In accordance with a possible embodiment, the slot 522 has an elongated shape in the direction of the longitudinal axis of the prosthesis, preferably elliptical or rectangular with short rounded sides. Advantageously, the frame 521 has an elongated shape in the direction of the longitudinal axis of the prosthesis. Preferably the short side of frame 521 corresponding to the bend between both arms that are directly connected to the frame is substantially rectilinear in the circumferential direction, when considered in a plane development of the prosthesis.

[0082]. Advantageously, the two arms that are directly connected to the frame 521 join to the frame at end points.

[0083]. Advantageously the frame 521 comprises two elongated sides 523 having substantially the same width as the arms 511 of the prosthesis, as measured along the circumferential direction 508, and a shorter length than the arms 511 of the prosthesis, as measured along the longitudinal direction 504.

[0084]. Advantageously, a radiopaque material is provided within the slot 522, preferably welded or melted

within the slot. The radiopaque material may be any material having a greater visibility to X-rays than the material used for the prosthesis.

[0085]. In the case where the prosthesis is made
5 of a superelastic or shape memory material, such as Nitinol (or an alloy with Ni and Ti as the main part), the radiopaque material can be selected from Tantalum, Gold, Platinum, Tungsten or other materials suitable for the purpose and clearly biocompatible.

10 [0086]. According to a possible embodiment, the first serpentine 506a housing the frame 521 is an end serpentine of the prosthesis. Advantageously, both end serpentines of the prosthesis, i.e. the first and the last serpentines, comprise at least one frame 521,
15 respectively.

[0087]. From what has been stated above, it may be appreciated how providing an endoluminal prosthesis according to the present invention allows to meet such contrasting requirements as having a high strength to
20 radial compression force in the middle of the prosthesis, while avoiding having to excessively increase the amount of material in that area.

[0088]. Furthermore, a good level of flexibility is obtained on the sides, while a more undeformed shaped
25 is maintained in the middle.

[0089]. These aspects are particularly advantageous with respect to the carotid, which may be subjected to impacts or compressions due to its location. In fact, the prosthesis according to the present
5 invention ensures that the carotid channel will be opened also in the event of impact or compression, since the prosthesis withstands compression at least in the middle thereof, follows the deformation of the carotid, and however ensures a passage lumen.

10 [0090]. Due to the prosthesis provided, endoluminal operations can be carried out in tortuous vessels or ducts, and at the same time, an optimum and constant support of the treated vessel wall can also be ensured when the prosthesis is in the expanded state.

15 [0091]. Particularly advantageous is the provision and shape of the markers, which make the prosthesis visible and easily positionable, without interfering with the delicate geometries involved, which are suitably designed for ensuring the above-mentioned results.

20 [0092]. It should be understood that variations and/or additions may be provided to what has been described and illustrated above.

[0093]. The number of serpentines, arms or bends may vary from what has been described or illustrated. The
25 serpentine shape may also vary.

[0094]. Generally all the embodiments which have been described as being feasible above can be made as such in the absence of those characteristics described as belonging to other possible embodiments.

5 [0095]. In accordance with a possible embodiment, the prosthesis can be coated with a coating material, such as PTFE, biodegradable material, polyester fibers, polyurethane, or the like.

[0096]. To the preferred embodiments of the
10 endoluminal prosthesis described above, those skilled in the art, aiming at satisfying contingent and specific needs, may carry out a number of modifications, variants and replacements of elements with others functionally equivalent, without departing from the scope of the
15 claims below.

CLAIMS

1. An endoluminal prosthesis (500) comprising:

a tubular body (502) suitable to turn from a collapsed state to an expanded or partially expanded state,

said tubular body (502) developing along a longitudinal axis (504),

said tubular body (502) comprises a plurality of serpentines (506a-506d, 508a-508e, 510a-510d), or closed meander paths, developing along a substantially circumferential direction,

each of said serpentines comprising arm portions, or arms (511), and bend portions, or bends (512) which join two subsequent arms (511) to form said serpentine or meander path, wherein

the bends (512) facing an adjacent serpentine are circumferentially offset relative to the respective and opposite bends (512) of the contiguous serpentine, both when the prosthesis is collapsed and when the prosthesis is expanded or partially expanded, wherein

at least one bridge (514a-514c), having a main longitudinal extension, which connects two adjacent serpentines at two respective bends (512a, 512b) situated at the shortest longitudinal distance between the two serpentines, wherein

said serpentines are grouped in at least two portions (506, 508, 510) arranged along said longitudinal axis (504), wherein

a first portion (506, 510) comprises at least two adjacent serpentines interconnected by at least one bridge (514a), at least one pair of bends, not being connected by a bridge, that is situated at the shortest longitudinal distance between the two serpentines, and wherein

a second portion (508) comprises at least two adjacent serpentines interconnected by a number of bridges (514b) equal to the pairs of bends of the two serpentines being at the shortest longitudinal distance between the two serpentines.

2. The endoluminal prosthesis according to claim 1, wherein said first portion (506, 510) is a distal and/or proximal end portion of said endoluminal prosthesis and said second portion (508) is a middle portion of said endoluminal prosthesis.

3. The endoluminal prosthesis in accordance with claim 1 or 2, wherein said first (506, 510) and second (508) serpentine portions are connected by bridges (514c) that join pairs of bends of the two serpentines situated at the shortest longitudinal distance between the two serpentines, each being a part of one of the two

portions.

4. The endoluminal prosthesis according to claim 3, wherein the bridges (514c) that join the first (506, 510) and second (508) portions are in a number comprised
5 between the number of the bridges (514a) connecting two adjacent serpentines of the first portion (506, 510) and the number of bridges (514b) connecting two adjacent serpentines to the second portion (508).

5. The endoluminal prosthesis according to any
10 preceding claim, wherein the first portion (506, 510) comprises at least three serpentines (506a-506c) and wherein the bridges (514a) connecting two adjacent serpentines are circumferentially offset relative to the immediately subsequent bridges (514a) according to the
15 longitudinal axis (504).

6. The endoluminal prosthesis according to any preceding claim, wherein said first portion (506, 510) is a proximal portion of the endoluminal prosthesis and comprises at least one marker (518) or radiopaque
20 element.

7. The endoluminal prosthesis according to any preceding claim, wherein said first portion (506, 510) is a distal portion of the endoluminal prosthesis and comprises at least one marker (518) or radiopaque
25 element.

8. The endoluminal prosthesis according to any preceding claim, comprising a proximal portion (506) provided as said first portion, a middle portion (508) provided as said second portion and a distal portion
5 (510) provided as said first portion, wherein both in the collapsed and in the expanded condition each of said proximal, middle and distal portion develops by about one third of the length of the endoluminal prosthesis.

9. The endoluminal prosthesis according to any
10 preceding claim, comprising a proximal portion (506) provided as said first portion, a middle portion (508), provided as said second portion and a distal portion (510) provided as said first portion, wherein said distal portion and said proximal portion comprise four
15 serpentines, respectively, and wherein said middle portion comprises five serpentines.

10. The endoluminal prosthesis according to any preceding claim, comprising a proximal portion (506) provided as said first portion, a middle portion (508),
20 provided as said second portion and a distal portion (510) provided as said first portion, wherein said distal portion and said proximal portion comprise four serpentines, respectively, and wherein said middle portion comprises five serpentines.

25 11. The endoluminal prosthesis according to any

claim 1 to 8, comprising a proximal portion (506) provided as said first portion, a middle portion (508), provided as said second portion and a distal portion (510) provided as said first portion, wherein said distal
5 portion and said proximal portion comprise three serpentine, respectively, and wherein said middle portion comprises four serpentine.

12. The endoluminal prosthesis according to any claim 1 to 8, comprising a proximal portion (506)
10 provided as said first portion, a middle portion (508), provided as said second portion and a distal portion (510) provided as said first portion, wherein said distal portion and said proximal portion comprise a number of serpentine less than or equal to the number of
15 serpentine of said middle portion.

13. The endoluminal prosthesis according to any preceding claim, defining a cylindrical tubular body in the expanded condition.

14. The endoluminal prosthesis according to any
20 claim 1 to 12, defining a truncated-cone-shaped tubular body in the expanded condition.

15. The endoluminal prosthesis according to any preceding claim, comprising a coating material.

16. The endoluminal prosthesis according to claim
25 15, wherein said coating material is PTFE.

17. The endoluminal prosthesis according to claim 15, wherein said coating material is a biodegradable material.

18. The endoluminal prosthesis according to claim 5 15, wherein said coating material comprises polyester fibers.

19. The endoluminal prosthesis according to one of the preceding claims, wherein the width of the bridges (514a, 514b, 512c) as measured substantially in the 10 circumferential direction is about twice the width of the arms (511), also measured substantially in the circumferential direction.

20. Use of an endoluminal prosthesis (500) according to any preceding claim, which can be implanted 15 at a bifurcation, particularly in the carotid.

21. Use of an endoluminal prosthesis according to claim 20, wherein said prosthesis in the expanded condition is truncated-cone shaped and wherein a distal portion (510) of said prosthesis having a smaller 20 circumference than the opposite proximal portion is positioned at the bifurcation.