

DESCRIPTION

METHOD AND APPARATUS FOR MEASURING ANESTHETIC DEPTH

TECHNICAL FIELD

[0001] The present invention relates to a method for measuring an anesthetic depth, and more particularly, to a method and an apparatus for measuring an anesthetic depth, capable of providing an accurate measurement value of an anesthetic depth despite a change in an anesthetic condition, providing anesthetic depth information timely according to a change in an anesthetic condition by significantly improving a tracking speed, and having compatibility with a conventional anesthetic depth analyzing apparatus, thereby having high utilization.

BACKGROUND ART

[0002] Generally, in the field of medical practice including an operation and a treatment, when pain is applied to a subject, neurotransmission is blocked through anesthesia so that the pain is removed or reduced. During an operation for a severe disease or symptom, general anesthesia is performed, and a patient under general anesthesia should be continuously observed. An anesthetic state of a patient should be checked by sensing an anesthetic depth, and there is a problem. While an operation should be performed under sufficient anesthesia, there is a problem in that a patient suffers from mental pain due to awakening during the operation.

[0003] Accordingly, during an operation, an anesthetic depth should be continuously measured, and a method for observing a clinical aspect and a method for analyzing a bioelectric signal have been mainly used as a method for measuring an anesthetic depth. The method for analyzing a bioelectric signal includes a method for measuring and analyzing

brainwaves so as to evaluate an effect of an anesthetic agent on the central nervous system, and there are also various kinds of monitoring apparatuses to which a method of using brainwaves is applied. The reason there are various kinds of anesthetic depth monitoring apparatuses using brainwaves is that the respective apparatuses have different algorithms for analyzing and evaluating brainwaves.

[0004] Currently, a bispectral index (hereinafter, referred to as “BIS”) analyzing apparatus is most popularly used as an anesthetic depth monitoring apparatus. The BIS analyzing apparatus, is one of the apparatuses in which a brainwave-based anesthetic depth measuring technique is developed and adopted for the first time therein, displays an anesthetic depth as “BIS” to be digitized within a range of 0-100, and verifies the clinical reliability of BIS by comparing BIS with a conventional anesthetic depth measuring standard or with an index calculated in another anesthetic depth instrument.

[0005] With a conventional anesthetic depth monitoring apparatus including such as BIS analyzing apparatus, a user, who is an anesthetic depth clinical subject or an anesthetic depth monitor, is unable to improve or change brainwave analyzing algorithms of instruments, so that an algorithm suitable for patient’s characteristics of a patient may not be applied and accordingly an anesthetic depth of the patient cannot be accurately monitored. Furthermore, since the details of analyzing algorithms installed in instruments are not disclosed, the apparatus is not suitable for a clinical anesthetic depth study and there are many difficulties in proving an algorithm error.

[0006] Moreover, an anesthetic depth monitoring apparatus such as the BIS analyzing apparatus has a problem in that an anesthetic state of a patient is unable to be rapidly sensed because a speed for tracking a rapid change in an anesthetic state is slow.

[0007] Patent Document 1 relates to a system and a method for measuring a brain activity

and an anesthetic depth through a brainwave signal analysis, wherein values may be very accurately calculated compared to a conventional spectrum analysis, wavelet analysis, or entropy analysis, although the structure of a basic algorithm is very simple.

[0008] (Patent Document 1) Korean Patent Application Laid-open Publication No. 2012-0131027 (publicized on December 4, 2012)

DISCLOSURE OF THE INVENTION

TECHNICAL PROBLEM

[0009] To resolve the above-described problem, an object of the present invention is to provide a method and an apparatus for measuring an anesthetic depth, capable of providing an accurate measurement value of an anesthetic depth despite a change in an anesthetic condition, providing anesthetic depth information timely despite a rapid change in an anesthetic state, and having compatibility with a conventional anesthetic depth analyzing apparatus.

TECHNICAL SOLUTION

[0010] To resolve the above-described problem, a method for measuring an anesthetic depth according to the present invention includes: dividing, by an epoch dividing part, an EEG signal into multiple epoch signals in time units, extracting, by a counting part, a CAI calculation value (CAI) by counting the number of points in epoch of a value higher than a determined critical value, extracting, by a Shannon entropy calculating part, a Shannon entropy calculation value (ShEn) by performing a Shannon entropy calculation from the EEG signal, and extracting, by a spectra entropy calculation part, a spectra entropy calculation value (SpEn) by performing a spectra entropy calculation; extracting, by a modified Shannon entropy calculating part, a modified Shannon entropy calculation value (MshEn) by multiplying the Shannon entropy calculation value (ShEn) and spectra entropy

calculation value (SpEn); and extracting, by a CAI extracting part, an anesthetic depth index (MsCAI) by performing a logical operation on the modified Shannon entropy calculation value (MshEn) and CAI calculation value (CAI).

[0011] According to a preferable embodiment of the present invention, the extracting of the anesthetic depth index (MsCAI) includes extracting the anesthetic depth index (MsCAI) by multiplying the modified Shannon entropy calculation value (MshEn) by a first constant (L) and multiplying the CAI calculation value (CAI) by a second constant (U) to be summed up according to the equation $MsCAI = L * MshEn + U * CAI$ ($L = 0.243, 0.65 \leq U \leq 0.74$).

[0012] According to a preferable embodiment of the present invention, the extracting of the Shannon entropy calculation value (ShEn) and spectra entropy calculation value (SpEn) includes: performing low frequency band pass filtering on the EEG signal; performing high frequency band pass filtering on the signal obtained after the low frequency band pass filtering; generating a first epoch signal by dividing the signal obtained after the low frequency band pass filtering by predetermined time units; generating a second epoch signal by dividing the signal obtained after the high frequency band pass filtering by predetermined time units; removing noise from the first epoch signal; and performing normalization by dividing the second epoch signal by a root mean square value of the epoch signal having noise removed therefrom.

[0013] According to a preferable embodiment of the present invention, the method includes: calculating a power spectrum density of a frequency component outputted by performing high speed Fourier transformation on the epoch signal with noise removed; and extracting the spectra entropy calculation value by performing a spectra entropy calculation from the power spectrum density.

[0014] According to a preferable embodiment of the present invention, the method includes

extracting the Shannon entropy calculation value by performing a Shannon entropy calculation from the normalized signal.

[0015] According to a preferable embodiment of the present invention, the method includes performing high speed Fourier transformation on the normalized signal and extracting the spectra entropy calculation value the power spectrum density.

[0016] According to a preferable embodiment of the present invention, the method includes calculating the critical value by performing discrete Fourier transformation on the normalized signal to be multiplied at least twice, summed up to a predetermined frequency band, and multiplied by a constant.

[0017] According to a preferable embodiment of the present invention, the method includes extracting the CAI calculation value by counting the number of points which are larger than the critical value, dividing the counted number by the total number of points of the epoch signal, and multiplying the divided value by a predetermined value.

[0018] According to another embodiment of the present invention, an apparatus for measuring an anesthetic depth according to the present invention includes: a CAI extracting part for configured to divide an EEG signal in a time section to generate an epoch signal, setting a predetermined critical value from the epoch signal, and extracting a cortical activity index (CAI) calculation value (CAI) by counting the number of points in an epoch signal exceeding the critical value; a modified Shannon entropy extracting part configured to output a modified Shannon entropy calculation value (MshEn) by multiplying a Shannon entropy calculation value (ShEn) calculated from the EEG signal and a spectra entropy calculation value (SpEn) calculated from the EEG signal; and an MsCAI extracting part configured to extract an anesthetic depth index (MsCAI) by performing a logical operation on the modified Shannon entropy calculation value (MshEn) and CAI calculation value (CAI).

[0019] According to a preferable embodiment of the present invention, the MsCAI extracting part extracts the anesthetic depth index (MsCAI) by multiplying the modified Shannon entropy calculation value (MshEn) by a first constant (L) and multiplying the CAI calculation value (CAI) by a second constant (U) to be summed up according to the equation $MsCAI = L * MshEn + U * CAI$ ($L = 0.243, 0.65 \leq U \leq 0.74$).

[0020] According to a preferable embodiment of the present invention, the CAI extracting part further includes a critical value extracting part configured to fluidly change a constant multiplied by the critical value according to an anesthetic degree or a frequency band, so as to apply the anesthetic degree or frequency band to the critical value.

[0021] According to a preferable embodiment of the present invention, the critical value extracting part extracts the critical value by multiplying a value after discrete Fourier transformation performed on a normalized signal at least twice to be summed up to a predetermined frequency band and multiplied by a constant.

[0022] According to a preferable embodiment of the present invention, the CAI extracting part further includes a counter for configured to count the number of points which are larger than the critical value in the epoch signal and divide the counted number by the total number of points in the epoch signal.

[0023] According to a preferable embodiment of the present invention, the apparatus further includes: a first epoch dividing part configured to generate a first epoch signal by dividing a signal, which is obtained by performing low frequency band pass filtering on the EEG signal, by predetermined time units; and a second epoch dividing part configured to generate a second epoch signal by performing high frequency band pass filtering on the signal obtained after the low frequency band pass filtering and by dividing the resultant signal by predetermined time units.

[0024] According to a preferable embodiment of the present invention, the apparatus further includes: a noise removing part configured to remove noise through a wavelet technique from an output of the first epoch dividing part; a normalizing part configured to calculate a root mean square value of an output epoch signal of the noise removing part and divide an output epoch signal of the second epoch dividing part by the root mean square value; and a Shannon entropy calculating part configured to calculate Shannon entropy from an output of the normalizing part so as to output the Shannon entropy calculation value.

[0025] According to a preferable embodiment of the present invention, the apparatus further includes: a power spectrum calculating part configured to perform high speed Fourier transformation on an output of the noise removing part and output a power spectrum density; and a spectra entropy calculating part configured to output a spectra entropy calculation value by calculating spectra entropy from an output of the power spectrum calculating part.

ADVANTAGEOUS EFFECTS

[0026] In the present invention, a fisher score is 74.6365, and an anesthetic degree may thus be more accurately measured compared to a conventional BIS anesthetic depth analyzing apparatus (fisher score 47.11).

[0027] A conventional problem in that when an anesthetic degree is rapidly changed, a reaction speed is low because of a low tracking speed of a conventional BIS technique, is solved, and therefore a change in a state of from an awakening state to an anesthetic state (hypnosis) can be accurately and timely detected by more rapidly reacting than a conventional anesthetic depth analyzing apparatus with a reaction speed, which is averagely 15 seconds faster.

[0028] In the present invention, through a Shannon entropy technique and a modified Shannon entropy technique improved from a spectra entropy technique, not only irregularity

in a time domain and a frequency domain is applied but also the brainwave's own characteristics are applied through a combination with a CAI technique, thereby accurately and rapidly providing a measured value of an anesthetic state according to various anesthetic conditions.

[0029] The present invention has a high correlation of 0.9877 with a conventional BIS apparatus, high compatibility with a conventional BIS apparatus thereby, and high compatibility with a structure concomitantly used for the BIS apparatus, and ensures high utilization.

[0030] According to the present invention, a real-time process may be easily performed due to a simple algorithm, thereby more accurately capturing a change in a state during anesthesia.

[0031] The present invention may be applied to a medical instrument for evaluating an anesthetic depth and may also be applied to a brainwave signal processing-related instrument having a different signal treating technique.

BRIEF DESCRIPTION OF THE DRAWINGS

[0032] FIG. 1 is a graph showing a change in brainwaves according to an anesthetic degree.

[0033] FIG. 2 illustrates an apparatus for measuring an anesthetic depth according to the present invention.

[0034] FIG. 3 shows an algorithm of a method for measuring an anesthetic depth according to the present invention.

[0035] FIG. 4 is a conceptual diagram of an error removing part illustrated in FIG. 2.

[0036] FIG. 5 illustrates a screen display part illustrated in FIG. 2.

MODE FOR CARRYING OUT THE INVENTION

[0037] Hereinafter, specific embodiments for carrying out the present invention will be described with reference to the accompanying drawings. In the drawings, the dimensions of main parts are exaggerated and ancillary parts are omitted for clarity of illustration. Thus, the present invention should not be construed as limited to the drawings.

[0038] According to studies, it has been known that changes in characteristics of brainwaves during an operation have a great correlation with an anesthetic degree. Referring to FIG. 1, FIG. 1(a) shows measured brainwaves during an awake state, and brainwaves during an awake state have a small amplitude and a high frequency component. As a subject is entering into anesthesia (hypnosis), the amplitude becomes larger and the frequency component becomes lower as shown in FIGS. 1(b) and 1(c). When the subject is very deeply anesthetized, flat signals are outputted as shown in FIG. 1(d), and signals (burst suppression) having a high amplitude and a high frequency component are intermittently observed. Bio-signals such as changes in a heart rate, an electrocardiogram, and an electromyogram have a low direct correlation with an anesthetic degree. It is because various other reasons may affect a heart rate. On the other hand, unlike the correlation of a heart rate, it has been known through several researches that the characteristics of a brainwave signal have a direct correlation with an anesthetic degree of a patient when components of the brainwave signals are changed.

[0039] Hereinafter, referring to an apparatus for measuring an anesthetic depth illustrated in FIG. 2 and an algorithm for measuring an anesthetic depth illustrated in FIG. 3, description will be given of a method and an apparatus for measuring an anesthetic depth of the present invention.

[0040] The apparatus for measuring an anesthetic depth, according to the present invention, illustrated in FIG. 2 includes: a low frequency band pass filter 1; a high frequency band pass

filter 7; a first epoch dividing part 2; a second epoch dividing part 8; a noise removing part; a normalizing part 9; a power spectrum calculating part 4; a Shannon entropy calculating part 10; a spectra entropy calculating part 5; a modified Shannon entropy (MsCAI) calculating part 11; a critical value extracting part 6; a counter 12; a cortical activity index (CAI) extracting part 13; a modified Shannon entropy with cortical activity index (MsCAI) extracting part 14; an error removing part 16; a screen display part 17; and a data storing part 19.

[0041] The low frequency band pass filter 1 removes electric noise of approximately 60 Hz or more from an electroencephalography (hereinafter, referred to as “EEG”) signal through a patch adhered on the forehead of a subject. Although information that can be obtained from an EEG signal exists in various frequency bands, the low frequency band pass filter 1 performs an analysis by using a frequency between approximately 0-60 Hz and considers the signal having approximately 60 Hz or more as noise.

[0042] The high frequency band pass filter 7 performs high frequency band pass filtering on the signal passing through the low frequency band pass filter 1. Since a change in electrical power in a brainwave of a high frequency band has more direct correlation with an anesthetic depth, the output signal of the low frequency band pass filter 1 is filtered as a low frequency band signal.

[0043] The first epoch dividing part 2 divides the serially entering output signal of the low frequency band pass filter 1 into epoch signals (hereinafter referred to as a first epoch signal to be distinguished from an epoch signal of the second epoch diving part) each having a predetermined time unit (for examples, 16 seconds). The divided signal may overlap an adjacent signal. For example, the adjacent signal overlaps for a 15 second section, a divided signal is generated at every second to be outputted to the noise removing part 3.

[0044] The second epoch dividing part 8 has the same structure as the first epoch dividing part 2 but is different from the first epoch dividing part because an input signal is the output signal of the high frequency band pass filter 7. The second epoch dividing part 8 divides the output signal of the high frequency band pass filter 7 into epoch signals (hereinafter referred to as a second epoch signal to be distinguished from the epoch signal of the first epoch dividing part) to be outputted to the normalizing part 9.

[0045] The noise removing part 3 removes noise (artifact) caused by the eyes and noise caused by the movement of a subject from the first epoch dividing part 2. The noise removing part 3, for example, performs a wavelet-based denoising technique.

[0046] The normalizing part 9 calculates a root mean square (hereinafter, referred to as “RMS”) of an output epoch signal of the noise removing part 3 and divides an output epoch signal of the second epoch dividing part 8 by the RMS to be normalized.

[0047] The power spectrum calculating part 4 performs fast Fourier transformation (FFT) on the signal from which the noise has been removed, and power spectrum density (PSD) of an outputted frequency component is obtained. That is, a histogram of power (a squared value) of signal points is obtained.

[0048] The Shannon entropy calculating part 10, as shown in Equation 1, calculates Shannon Entropy of an output signal of the normalizing part 9 and outputs a Shannon entropy calculation value (ShEn). $p(a_i)$ is the number and frequency of factors corresponding to each block after the signal is divided by k ($k > 1$) according to size. For example, assuming that the sizes of absolute values for each epoch signal are 1, 2, 2, 3, are divided into three portions, [0.5, 1.5], [1.5, 2.5], and [2.5, 3.5] and each block is respectively a_1 , a_2 , or a_3 , $p(a_2) = 2/4$. The calculation may be performed by applying irregularity of the histogram of the EEG signal, that is, irregularity of a time domain, by means of a Shannon entropy

technique. Shannon entropy technique may be applied to a well-known art.

$$ShEn = \frac{-\sum_{i=1}^n p(a_i) \log p(a_i)}{\log k} \dots\dots\dots (Eq. 1)$$

[0049] The spectra entropy calculating part 5, as shown in Equation 2, performs a spectra entropy calculation on an output signal of the power spectrum calculating part 4 to extract a spectra entropy calculation value (SpEn). The spectra entropy calculation is similar to Shannon entropy but performs a Shannon entropy (ShEn) calculation by using a value obtained for the power spectrum density (PSD). Through the spectra entropy calculation, power spectrum of the EEG signal, that is, irregularity of a frequency domain, may be applied to an anesthetic depth index. A spectra entropy calculating technique may be applied to a well-known art.

$$SpEn = \frac{-\sum_{i=1}^n PSD(f_i) \log PSD(f_i)}{\log k} \dots\dots\dots (Eq. 2)$$

[0050] The modified Shannon entropy (hereinafter, referred to as “MshEn”) extracting part 11 scales, in a predetermined range, and multiplies a Shannon entropy (ShEn) calculation value and a spectra entropy (SpEn) calculation value for each epoch signal. A scaling standard may be mapped onto a value, for example approximately 1-100, inversely proportional to an anesthetic degree of an output signal.

[0051] The critical value (threshold) extracting part 6, as shown in Equation 3, outputs a critical value (threshold) by squaring a value obtained after discrete Fourier transformation (DFT), summing up the value to a predetermined frequency band, and then multiplying a constant (K). A critical value for calculating the density of an impulse signal is calculated. Since the amplitude of the signal tends to increase when a subject is deeply anesthetized, the critical value is not fixed as one value but fluidly changed according to characteristics of the

signal. Accordingly, a size of a low frequency band is set as the critical value. In Equation 3 below, K is an experimentally figured out coefficient, DFT is discrete Fourier transformation, $\overline{x_{\text{norm}}}$ is an output epoch signal of the normalizing part, and M is a 4 Hz band in a discrete time domain. The critical value extracting part 6 may compensate a bias error that is generated as the amplitude of the signal increases, by increasing the critical value when the low frequency band is large and the subject is deeply anesthetized.

$$\text{Threshold} = K \sum_{k=1}^M |DFT(\overline{x_{\text{norm}}})|^2 \quad \dots\dots\dots (\text{Eq. 3})$$

[0052] The counter 12 counts, in epoch, the number of points larger than the critical value extracted from the critical value extracting part 6 and dividing the counted number by the total number of points of epoch.

[0053] The cortical activity index (hereinafter, referred to as “CAI”) extracting part 13 outputs a CAI calculation value (CAI) by scaling an output of the counter 12. The CAI extracting part 13 considers a signal emitted from a human brain cell as the sum of an impulse signal (or a peak signal), and the EEG signal as the sum of the impulse in a measuring point. Since brain activity is high in an awakening state, there are many impulse signals in the EEG signal. A CAI calculation value (CAI) is measured based on the fact that impulse is low during anesthesia.

[0054] The MsCAI extracting part 14 calculates an anesthetic depth index (MsCAI) by multiplying the modified Shannon entropy calculation value (MshEn) and CAI calculation value (CAI) by a predetermined coefficient obtained through an experiment. The anesthetic depth index (MsCAI) in the MsCAI extracting part 14 is calculated through, for example, Equation 4 and Equation 5.

$$MsCAI = ((A * ShEn) * (B * SpEn)) + U * CAI \dots\dots\dots (Eq. 4)$$

$$MsCAI = L * MshEn + U * CAI \quad (L = A * B) \dots\dots\dots (Eq. 5)$$

[0055] Constant A, constant B, and constant U are experimentally figured out coefficients, which allow a fisher score to be optimized through repeated experiments and simulations. When the constant A, constant B, and constant U are changed in a 0.01 unit between 0 and 1, a change in a fisher score of an Ms CAI technique may be exemplified as Table 1. When A= 0.54, B= 0.45, and U= 0.71, the fisher score is 74.6365, which is the best. Moreover, when A= 0.54, B= 0.45, $0.65 \leq U \leq 0.74$, that is, when $L (A*B) = 0.243$ and $0.65 \leq U \leq 0.74$, the anesthetic depth index (MsCAI) of the present invention is increased by at least approximately 40% compared to a BIS algorithm. Referring to Table 1 and Table 2, it can be seen that the apparatus for measuring an anesthetic depth according to the present invention has a remarkably improved function compared to a conventional BIS technique.

[Table 1]

Test No.	A	B	C	Fisher Score
1	0.54	0.45	0.54	56.9255
2	0.54	0.45	0.55	58.589
3	0.54	0.45	0.56	60.337
4	0.54	0.45	0.57	59.2556
5	0.54	0.45	0.58	61.3602
6	0.54	0.45	0.59	62.3691
7	0.54	0.45	0.6	60.9082
8	0.54	0.45	0.61	62.3814
9	0.54	0.45	0.62	61.3606
10	0.54	0.45	0.63	63.1417

11	0.54	0.45	0.64	64.7456
12	0.54	0.45	0.65	69.5645
13	0.54	0.45	0.66	67.4387
14	0.54	0.45	0.67	69.2384
15	0.54	0.45	0.68	69.813
16	0.54	0.45	0.69	71.0052
17	0.54	0.45	0.7	70.8148
18	0.54	0.45	0.71	74.6356
19	0.54	0.45	0.72	68.5861
20	0.54	0.45	0.73	66.1987
21	0.54	0.45	0.74	67.3864
22	0.54	0.45	0.75	64.6739

[Table 2]

Name of algorithm	Fisher score
MsCAI	74.6365
BIS	47.11
MshEn	58.6232
CAI	42.4912

[0056] The error removing part 16 removes abnormal signals from an output of the MsCAI extracting part 14. It is highly likely that values resulted from noise are not correct values. A difference in a size from an adjacent point is represented as a histogram, as shown in FIG. 4, and then points corresponding to top 0.5% are determined to be inappropriate values. For the inappropriate values, the predetermined number (for example, approximately 15-30) of past values is averaged, and calculation is performed by adding higher weighting to recent values.

[0057] The screen display part 17, as illustrated in FIG. 5, displays an output of the error removing part 16 on a screen. When scaled signals are transmitted to monitoring software every second, the screen display part 17 displays an anesthetic depth on a screen by means of the monitoring software. At the same time, raw EEG signal and anesthetic depth index tendencies, signal quality, and other bio-signals (heart rate and electromyogram) are displayed together, thereby enabling an examiner to make an accurate determination.

[0058] The data storing part 19 stores measured anesthetic depth data, and the data may be extracted after an operation to be utilized as research materials in the future.

[0059] The apparatus for measuring an anesthetic depth according to the present invention may measure an anesthetic depth by applying irregularity of a time axis and irregularity of a frequency band by multiplying the Shannon entropy calculation value and spectra calculation value, so that the fisher score is higher and a reaction speed according to an anesthetic degree is higher than those obtained through the Shannon entropy calculation technique or spectra entropy calculation technique. Moreover, an optimal anesthetic depth analysis coefficient is extracted through an experiment by respectively weighting the modified Shannon entropy technique and the CAI technique having characteristics of brainwaves applied thereto, wherein the Shannon entropy calculation technique and spectra entropy calculation technique are multiplied, and irregularity in the time domain and frequency domain may be applied to the modified Shannon entropy technique. As a result, referring to Table 2, the fisher score of the MsCAI technique according to the present invention is greatly improved to 74.6365 (CAI is 42.4912 and MshEn is 58.6232), and reaction speed and tracking speed according to an anesthetic degree are also averagely 15 seconds faster than convention apparatuses. Furthermore, a correlation with a BIS apparatus in a stable state is high (0.9877), thereby showing an excellent result in terms of

compatibility with an BIS analysis apparatus.

[0060] Although embodiments have been described with reference to a number of illustrative embodiments thereof, it should be understood that numerous other modifications and embodiments can be devised by those skilled in the art that will fall within the spirit and scope of the following claims.

WHAT IS CLAIMED IS:

1. A method for measuring an anesthetic depth, the method comprising:

dividing, by an epoch dividing part, an EEG signal into multiple epoch signals on a time axis, extracting, by a counting part, a CAI calculation value (CAI) by counting the number of epoch signal points of a value higher than a determined critical value, extracting, by a Shannon entropy calculating part, a Shannon entropy calculation value (ShEn) by performing a Shannon entropy calculation from the EEG signal, and extracting, by a spectra entropy calculation part, a spectra entropy calculation value (SpEn) by performing a spectra entropy calculation;

extracting, by a modified Shannon entropy calculating part, a modified Shannon entropy calculation value (MshEn) by multiplying the Shannon entropy calculation value (ShEn) and spectra entropy calculation value (SpEn); and

extracting, by a CAI extracting part, an anesthetic depth index (MsCAI) by performing a logical operation on the modified Shannon entropy calculation value (MshEn) and CAI calculation value (CAI).

2. The method of claim 1, wherein the extracting of the anesthetic depth index (MsCAI) comprises extracting the anesthetic depth index (MsCAI) by multiplying the modified Shannon entropy calculation value (MshEn) by a first constant (L) and multiplying the CAI calculation value (CAI) by a second constant (U) to be summed up according to the equation $MsCAI = L * MshEn + U * CAI$ ($L = 0.243, 0.65 \leq U \leq 0.74$).

3. The method of claim 1, wherein the extracting of the spectra entropy calculation

value (SpEn) comprises:

- performing low frequency band pass filtering on the EEG signal;
- performing high frequency band pass filtering on the signal obtained after the low frequency band pass filtering;
- generating a first epoch signal by dividing the signal obtained after the low frequency band pass filtering by predetermined time units;
- generating a second epoch signal by dividing the signal obtained after the high frequency band pass filtering by predetermined time units;
- removing noise from the first epoch signal; and
- performing normalization by dividing the second epoch signal by a root mean square value of the epoch signal having noise removed therefrom.

4. The method of claim 3, wherein the extracting of the spectra entropy calculation value (SpEn) further comprises:

- calculating a power spectrum density of a frequency component outputted by performing high speed Fourier transformation on the epoch signal with noise removed; and
- extracting the spectra entropy calculation value by performing a spectra entropy calculation from the power spectrum density.

5. The method of claim 4, further comprising extracting the Shannon entropy calculation value by performing a Shannon entropy calculation from the normalized signal.

6. The method of claim 5, further comprising performing high speed Fourier transformation on the normalized signal and extracting the spectra entropy calculation value

the power spectrum density.

7. The method of claim 5, further comprising calculating the critical value by performing discrete Fourier transformation on the normalized signal to be multiplied at least twice, summed up to a predetermined frequency band, and multiplied by a constant.

8. The method of claim 7, further comprising extracting the CAI calculation value (CAI) by counting the number of points which are larger than the critical value, dividing the counted number by the total number of points of the epoch signal, and multiplying the divided value by a predetermined value.

9. An apparatus for measuring an anesthetic depth, the apparatus comprising:

a CAI extracting part configured to divide an EEG signal in a time section to generate an epoch signal, setting a predetermined critical value from the epoch signal, and extracting a cortical activity index (CAI) calculation value (CAI) by counting the number of points in an epoch signal exceeding the critical value;

a modified Shannon entropy extracting part configured to output a modified Shannon entropy calculation value (MshEn) by multiplying a Shannon entropy calculation value (ShEn) calculated from the EEG signal and a spectra entropy calculation value (SpEn) calculated from the EEG signal; and

an MsCAI extracting part configured to extract an anesthetic depth index (MsCAI) by combining the modified Shannon entropy calculation value (MshEn) and CAI calculation value (CAI).

10. The apparatus of claim 9, wherein the MsCAI extracting part extracts the anesthetic depth index (MsCAI) by multiplying the modified Shannon entropy calculation value (MshEn) by a first constant (L) and multiplying the CAI calculation value (CAI) by a second constant (U) to be summed up according to the equation $MsCAI = L * MshEn + U * CAI$ ($L = 0.243, 0.65 \leq U \leq 0.74$).
11. The apparatus of claim 10, wherein the CAI extracting part further comprises a critical value extracting part configured to fluidly change a constant multiplied by the critical value according to an anesthetic degree or a frequency band, so as to apply the anesthetic degree or frequency band to the critical value.
12. The apparatus of claim 11, wherein the critical value extracting part extracts the critical value by multiplying a value after discrete Fourier transformation performed on a normalized signal acquired by dividing the epoch signal by a root mean square of the epoch signal which the noise has been removed at least twice to be summed up to a predetermined frequency band and multiplied by a constant.
13. The apparatus of claim 9, wherein the CAI extracting part further comprises a counter configured to count the number of points which are larger than the critical value in the epoch signal and divide the counted number by the total number of points in the epoch signal.
14. The apparatus of claim 9, further comprising:
a first epoch dividing part configured to generate a first epoch signal by dividing a signal, which is obtained by performing low frequency band pass filtering on the EEG signal,

by predetermined time units; and

a second epoch dividing part configured to generate a second epoch signal by performing high frequency band pass filtering on the signal obtained after the low frequency band pass filtering and by dividing the resultant signal by predetermined time units.

15. The apparatus of claim 14, further comprising:

a noise removing part configured to remove noise through a wavelet technique from an output of the first epoch dividing part;

a normalizing part configured to calculate a root mean square value of an output epoch signal of the noise removing part and divide an output epoch signal of the second epoch dividing part by the root mean square value; and

a Shannon entropy calculating part configured to calculate Shannon entropy from an output of the normalizing part so as to output the Shannon entropy calculation value.

16. The apparatus of claim 15, further comprising:

a power spectrum calculating part configured to perform high speed Fourier transformation on an output of the noise removing part and output a power spectrum density; and

a spectra entropy calculating part configured to output a spectra entropy calculation value by calculating spectra entropy from an output of the power spectrum calculating part.

17. A computer-readable recording medium, in which a computer program for performing the method for measuring an anesthetic depth of any one claim of claim 1 to claim 8 is stored.