

5 A method of generation of pharmaceutical substances into an
aerosol.

Technical Field

10 The invention relates to the methods of obtaining medical
aerosols and can be applied in medicine for treatment of
respiratory conditions as well as systemic diseases.

Background Art

15 The aerosol drug delivery methods are increasingly widely
used in the modern treatment methods of various diseases for
drug delivery to the patient's lungs. This method of drug
delivery is used to treat respiratory diseases such as asthma,
bronchitis, cystic fibrosis, bacterial or fungal infection,
chronic obstructive pulmonary disease, and primary pulmonary
hypertension. A prior art discloses such drug delivery methods
20 [1-3], moreover inhaled drug administration has a high potential
for treatment of systemic diseases [4-7]. The major advantage of
inhaled drug delivery is the fast therapeutic effect, simple
administration, absence of necessity for healthcare stuff,
absence of pain. Furthermore, the lungs have high solute
25 permeability, a large surface area for absorption, limited
proteolytic activity and pulmonary delivery is non-invasive. In
addition, aerosol delivery has no restrictions associated with
the use of water-insoluble drugs, unlike injection therapy.

30 Successful inhalation therapy depends on the precise
delivery of the drug to the target area of the airway. The
desirable area for delivering systemic drugs through the
respiratory system is the alveolar area of the lungs, due to the
wide surface area, ample blood supply and high permeability of
the walls of the alveoli, which enables direct entry of drugs
35 into the pulmonary and then into the systemic circulation.
Aerosol administration methods will not only accelerate the
therapeutic effect of the drug compared to oral administration,

5 but will also reduce the administered dose, which can help reduce undesirable side effects of the drugs.

The efficiency of delivery of the aerosol particles to the alveolar lung area is defined by the size of the particles. As it is known based on published materials, the maximum deposition efficiency is shown by the particles of 10-20 nm diameter [5, 8 - 14]. The volume of the particles of such size that settle in alveolar area is 50%. Particles within the size range of 200 - 500 nm have reduced efficiency in depositing in alveolar area that reaches less than 10%, however the particles of 1- 3 micron demonstrate increased efficiency of alveolar deposition and reach - 20%. There are three types of inhalers used in modern practice of aerosol therapy: nebulizers, metered-dose aerosol inhalers and powder inhalers. All these inhalers allow generation of aerosol of particle size not lower than 1-3 micron. It is an obvious point that in order to ensure an efficient aerosol therapy the alternative methods will be a substantial addition that will allow high stable concentration of the particles in a wider size range including nanosize scale. One of the alternative methods is the thermal condensation method, based on the evaporation of the initial pharmaceutical substance of the drug followed by nucleation of supersaturated vapor and further the condensation growth of the formed aerosol particles. The thermal condensation method allows obtaining an aerosol with the particle size range from 3 nm to 10 micron with concentration up to 10^8 cm^{-3} . Such a high concentration allows delivery of a sufficient dose to the patient within a minimum time interval to achieve the desired therapeutic effect.

One of the problems related to the development of the aerosol drug administration method is the possibility of precise dose calculation. Therefore, it is necessary to develop such methods of aerosol drug administration that enable increase of the efficiency of converting the starting substance into an

5 aerosol and allow precise determination of the amount of the drug delivered to the patient.

To date, there are a large number of devices that allow drug evaporation and subsequent condensation to form an aerosol. There is a method of generating aerosol by drug evaporation and
10 subsequent condensation in a tube furnace, followed by cooling the resulting vapor by diluting it with air or inert gases [15]. The disadvantage of this equipment is the difficulty of determining the mass of the evaporated and condensed drug.

There is a device for generating medical aerosol that
15 applies a pressed foamed graphite impregnated with a liquid composition containing pharmaceutical substances [16] as a vapor generating element. The disadvantage of this device is the complexity of manufacturing of the vapor generating element, the variation of drug concentration in aerosol during evaporation
20 and inability to use pharmaceutical substances in solid form.

Closest to the claimed invention is the method of aerosol generation via a fast heating of thin film of drug without excipients, coated onto a solid surface of a metal cylinder [17]. This method allows to evaporate and then condense the drug
25 to form aerosol of a particle size from several nanometers to several microns within about 50-300 ms. The disadvantage of this method is the possibility of drug application only as thin solid form films.

Disclosure of invention

30 The object of the present invention is the development of an efficient method of generation of drugs in aerosol form using evaporation of the initial drug substance applied on a solid surface of a carrier allowing evaporation with subsequent condensation of drugs not only in solid state but also
35 transferred from solid to liquid as a result of heating.

Technical result of the invention: aerosol administration methods not only accelerate the therapeutic effect of the drug compared to oral administration forms, but also reduce the

5 administered dose, which can help reduce undesirable side effects of the drugs.

The presented method of drug generation in a form of an aerosol comprises supplying heated air to the initial drug substance, sublimation of the initial drug substance followed by
10 nucleation of the obtained supersaturated vapor and delivery to the patient's lungs in a form of an aerosol. According to the invention, the initial substance of the drug is placed on an inert carrier (for example cellulose) in the form of a two- or three-layer tablet, which is produced using a mold, wherein a
15 measured amount of the drug and cellulose is placed in the matrix alternately and then is pressed at a pressure in the range from 0.5 to 20 atm, in order that the drug is located either on one side or on both sides of the cellulose.

Advantageous effect of the presented method is reached as
20 result of the fact that the initial drug substance - a multilayer tablet allows sublimating various range of drugs in both solid state and those that experience melting during heating. A liquid phase is held on the porous surface of the pressed cellulose due to the adhesion force. Furthermore,
25 application of the tablet allows:

- Precisely dose the amount of drug transferred into an aerosol;
- Increase the efficiency of the conversion of drugs of the original substance into aerosol.

30 **Brief description of drawings**

Fig. 1 - an example of a three-layer tablet with a drug and compressed cellulose: 1 - a drug layer, 2 - compressed cellulose, that due to it's adhesive properties allows retaining the drug which was initially not only in the solid state, but
35 also in the liquid state, or transitioned from solid to liquid state as a result of heating.

Fig.2 - a dependency diagram of the concentration of aerosol obtained by evaporation and condensation of the drug -

5 isoniazid, on the heating temperature of the air flow in the generator;

Fig.3 - a dependency diagram of the average size of the aerosol of isoniazid on the heating temperature of the air flow in the generator.

10 **Mode for Carrying Out the Invention**

The method of generation of an aerosol of a pharmaceutical substance can be implemented as follows. Air is supplied at the inlet of an inhalation device for generating aerosol and heated to the required temperature indicated on the graphs (see Figs. 2
15 and 3).

Air heating temperature is within the range of 80 - 220 °C for a wide range of drugs. Further, the heated air is supplied to the drug substance in the form of a multilayer tablet with the drug 1 and a layer of pressed cellulose 2. A saturated vapor
20 is formed in the result of evaporation of the drug substance from the surface of the tablet. After that the vapor is transferred with an air flow to the nucleation sector where it is cooling. As a result, the vapor becomes supersaturated, which leads to homogeneous nucleation, i.e. to aerosolization - the
25 phase transition stage. The resulting aerosol of the drug is transferred with an air flow for therapeutic effect in the respiratory organs of the patient.

The tablet with a drug 1 and a cellulose layer 2 is an important element of the aerosol generation. The tablet is made
30 as a "sandwich", the upper and lower layers of which are composed of a drug 1, and the inner layer is a pressed cellulose 2. The tablet is manufactured with a mold as follows: A layer of a drug, a layer of cellulose, a layer of a drug etc. are sequentially placed in the matrix alternately. Followed by
35 pressing at a pressure in the range from 0.5 to 20 atm. The result is a stable three-layer tablet with a measured amount of a drug in it. A measured amount of a drug in the tablet allows

5 precise dosing of the amount of the pharmaceutical substance in
the generated aerosol and consequently the inhalation dose.

An example of implementation of the drug aerosolization.

The experiments were conducted aimed at confirmation of the
implementation of the method with the drug - isoniazid. The
10 tablet has been manufactured in which the lower drug layer was
composed of 50 mg of powder isoniazid, middle layer - 100 mg of
cellulose, the upper layer - 50 mg of powder isoniazid. The
method of aerosol generation of the drug - isoniazid was
performed on an experimental equipment. The results of the
15 experimental works are presented in fig. 2, 3 - it demonstrates
the dependency of the concentration and aerosol particle size of
isoniazid obtained with the above-described method on the air
heating temperature. Control of concentration and particle size
or the drug aerosols was performed with an aerosol spectrometer
20 [18].

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Claim

A method of generation of an aerosol of a drug comprising supplying of heated air to an initial drug substance, evaporating the initial drug substance with a subsequent nucleation of the obtained supersaturated vapor and delivering
10 the drug to patient's lungs in a form of the aerosol, characterized in that the initial drug substance is made in a form of a multi-layer tablet manufactured with a press mould wherein an inert carrier and a measured amount of the drug are alternately loaded in the matrix of the press mould and
15 subsequently pressed at a pressure in a range from 0,5 to 20 atm.