GLYCOPOLYSIALYLATION OF NON-BLOOD COAGULATION PROTEINS

FIELD OF THE INVENTION

[0001] The present invention relates to materials and methods for conjugating water soluble polymers, in particular polysialic acid, to carbohydrate-containing compounds, in particular glycoproteins other than a blood coagulation proteins, and to the conjugates obtained.

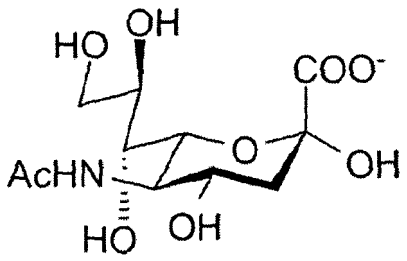
BACKGROUND OF THE INVENTION

[0002] Conjugation of polypeptide drugs such as by PEGylation or polysialylation protects them from degradation in the blood circulation and thus improves their pharmacodynamic and pharmacokinetic profiles (Harris and Chess, Nat Rev Drug Discov. 2003;2:214-21; S. Jain, D. Hreczuk-Hirst, P. Laing and G. Gregoriadis, Drug Delivery Systems and Sciences, 4 (No 1): 3-9, 2004.). The PEGylation process attaches repeating units of ethylene glycol (polyethylene glycol (PEG)) to a polypeptide drug. PEG molecules have a large hydrodynamic volume (5–10 times the size of globular proteins), are highly water soluble and hydrated, non-toxic, non-immunogenic and rapidly cleared from the body. PEGylation of molecules can lead to increased resistance of drugs to enzymatic degradation, increased half-life *in vivo*, reduced dosing frequency, decreased immunogenicity, increased physical and thermal stability, increased solubility, increased liquid stability, and reduced aggregation. The first PEGylated drugs were approved by the FDA in the early 1990s. Since then, the FDA has approved several PEGylated drugs for oral, injectable, and topical administration.

[0003] Sialic acids (also called N-acetyl neuraminic acids) and polysialic acids are found widely distributed in animal tissues and to a lesser extent in other species ranging from plants and fungi to yeasts and bacteria, mostly in glycoproteins and gangliosides.

[0004] The abbreviation "PSA" used herein refers to the term "polysialic acid". Similarly, the term "mPSA" used herein refers to the term "modified polysialic acid".

[0005] PSAs consist of polymers (generally homopolymers) of N-acetylneuraminic acid. The secondary amino group normally bears an acetyl group, but it may instead bear a glycolyl group. Possible substituents on the hydroxyl groups include acetyl, lactyl, ethyl, sulfate, and phosphate groups.



N-Acetylneuraminic acid
Neu5Ac

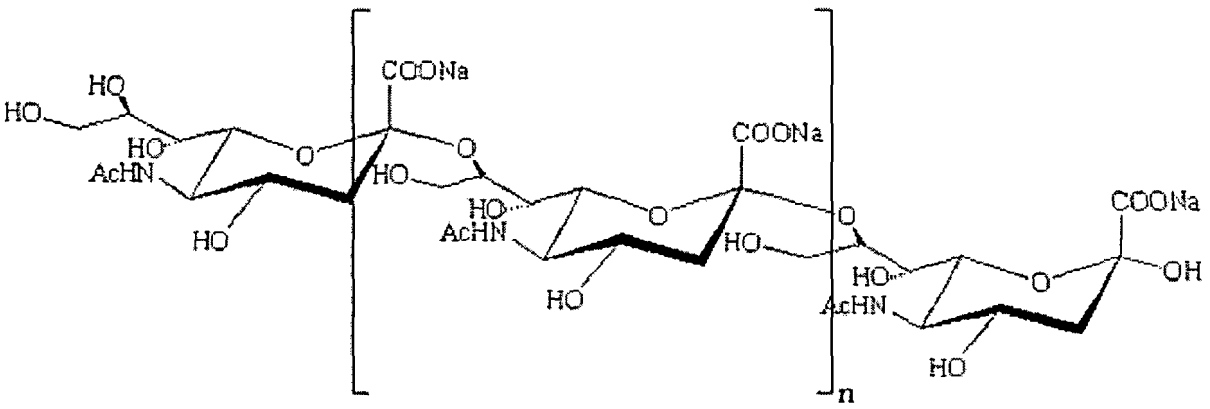
Structure of sialic acid (N-acetylneuraminic acid)

[0006] PSAs and mPSAs generally comprise linear polymers consisting essentially of N-acetylneuraminic acid moieties linked by 2,8- or 2,9- glycosidic linkages or combinations of these (e.g. alternating 2,8- and 2,9- linkages). In particularly preferred PSAs and mPSAs, the glycosidic linkages are α-2,8. Such PSAs and mPSAs are conveniently derived from colominic acids, and are referred to herein as "CAs" and "mCAs". Typical PSAs and mPSAs comprise at least 2, preferably at least 5, more preferably at least 10 and most preferably at least 20 N-acetylneuraminic acid moieties. Thus, they may comprise from 5 to 500 N-acetylneuraminic acid moieties, preferably from 10 to 300 N-acetylneuraminic acid moieties. PSAs and CAs can be polymers comprising different sugar moieties. They can be copolymers. PSAs and CAs preferably are essentially free of sugar moieties other than N-acetylneuraminic acid. PSAs and CAs preferably comprise at least 90%, more preferably at least 95% and most preferably at least 98% N-acetylneuraminic acid moieties.

[0007] Where PSAs and CAs comprise moieties other than N-acetylneuraminic acid (as, for example in mPSAs and mCAs) these are preferably located at one or both of the ends of the polymer chain. Such "other" moieties may, for example, be moieties derived from terminal N-acetylneuraminic acid moieties by oxidation or reduction.

[0008] For example, WO-A-0187922 describes such mPSAs and mCAs in which the non-reducing terminal N-acetylneuraminic acid unit is converted to an aldehyde group by reaction with sodium periodate. Additionally, WO 2005/016974 describes such mPSAs and mCAs in which the reducing terminal N-acetylneuraminic acid unit is subjected to reduction to reductively open the ring at the reducing terminal N-acetylneuraminic acid unit, whereby a vicinal diol group is formed, followed by oxidation to convert the vicinal diol group to an aldehyde group.

[0009] Sialic acid rich glycoproteins bind selectin in humans and other organisms. They play an important role in human influenza infections. For example, sialic acid can hide mannose antigens on the surface of host cells or bacteria from mannose-binding lectin. This prevents activation of complement. Sialic acids also hide the penultimate galactose residue thus preventing rapid clearance of the glycoprotein by the galactose receptor on the hepatic parenchymal cells.



Structure of colominic acid (homopolymer of N-acetylneuraminic acid)

[0010] CAs are produced, *inter alia,* by particular strains of *Escherichia coli* possessing the K1 antigen. CAs have many physiological functions. They are important as a raw material for drugs and cosmetics.

[0011] Comparative studies *in vivo* with polysialylated and unmodified asparaginase revealed that polysialylation increased the half-life of the enzyme (Fernandes and Gregoriadis, Biochimica Biophysica Acta 1341: 26-34, 1997).

[0012] The preparation of conjugates by forming a covalent linkage between the water soluble polymer and the therapeutic protein can be carried out by a variety of chemical methods. One approach for coupling PSA to therapeutic proteins is the conjugation of the polymers via the carbohydrate moieties of the protein. Vicinal hydroxyl (OH) groups of carbohydrates in proteins can be easily oxidized with sodium periodate ($NaIO_4$) to form active aldehyde groups (Rothfus and Smith, J Biol Chem 1963; 238:1402-10; van Lenten and Ashwell, J Biol Chem 1971;246:1889-94). Subsequently the polymer can be coupled to the aldehyde groups of the carbohydrate by use of reagents containing, for example, an active hydrazide group (Wilchek M and Bayer EA, Methods Enzymol 1987;138:429-42). A more recent technology is the use of reagents containing aminooxy groups which react with aldehydes to form oxime linkages (WO 96/40662, WO2008/025856).

[0013] Additional examples describing conjugation of a PSA to a therapeutic protein are described in US Publication No. 2009/0076237 which teaches the oxidation of rFVIII and subsequent coupling to PSA and other water soluble polymers (e.g. PEG, HES, dextran) using hydrazide chemistry; WO 2008/025856 which teaches oxidation of different coagulation factors, e.g. rFIX, FVIII and FVIIa and subsequent coupling to a polymer, e.g. PEG.

[0014] Recently, an improved method was described comprising mild periodate oxidation of sialic acids to generate aldehydes followed by reaction with an aminooxy group containing reagent in the presence of catalytic amounts of aniline (Dirksen A and Dawson PE, Bioconjugate Chem. 2008;19,2543-8; and Zeng Y et al., Nature Methods 2009;6:207-9). The aniline catalysis dramatically accelerates the oxime ligation, allowing the use of very low concentrations of reagents.

[0015] Notwithstanding the methods available of conjugating water soluble polymers to therapeutic proteins, there remains a need to develop materials and methods for conjugating water soluble polymers to carbohydrate-containing compounds other than blood coagulation proteins that improve the compound's pharmacodynamic and/or pharmacokinetic properties while minimizing the costs associated with the various reagents.

SUMMARY OF THE INVENTION

[0016] The present invention provides materials and methods for conjugating a water soluble polymer to a carbohydrate-containing compound other than a blood coagulation protein that improve the compound's pharmacodynamic and/or pharmacokinetic properties while minimizing the costs associated with the various reagents.

[0017] In one embodiment of the invention there is provided a method of conjugating a water soluble polymer to an oxidized carbohydrate moiety of a carbohydrate-containing compound other than a blood coagulation protein, comprising contacting the oxidized carbohydrate moiety with water soluble polymer under conditions that allow conjugation, wherein said water soluble polymer contains an aminooxy group and an oxime linkage is formed between the oxidized carbohydrate moiety and the aminooxy group on the water soluble polymer, or wherein said water soluble polymer contains a hydrazide group and a hydrazone linkage is formed between the oxidized carbohydrate moiety and the hydrazide group on the water soluble polymer. The compound may be (1) a glycoprotein other than a

blood coagulation protein, (2) a ganglioside, or (3) a drug delivery system comprising a carbohydrate group.

[0018] The carbohydrate moiety may be oxidized using a sugar-specific oxidizing enzyme (e.g. galactose or glucose oxidase) or by incubation with a buffer comprising an oxidizing agent selected from sodium periodate ($NaIO_4$), lead tetraacetate ($Pb(OAc)_4$) and potassium perruthenate ($KRuO_4$).

[0019] The carbohydrate moiety may be oxidized at a sialic acid, mannose, galactose or glucose residue.

[0020] The water-soluble polymer used in the invention can be, but is not limited to, polyethylene glycol (PEG), branched PEG, PEG derivative, PSA, mPSA, CA, mCA, hydroxyethyl cellulose (HEC), dextrin, polyoxazoline, carbohydrate, polysaccharides, pullulane, chitosan, hyaluronic acid, chondroitin sulfate, dermatan sulfate, starch, dextran, carboxymethyl-dextran, polyalkylene oxide (PAO), polyalkylene glycol (PAG), polypropylene glycol (PPG) polyoxazoline, poly acryloylmorpholine, polyvinyl alcohol (PVA), polycarboxylate, polyvinylpyrrolidone, polyphosphazene, polyoxazoline, polyethylene-co-maleic acid anhydride, polystyrene-co-maleic acid anhydride, poly(1-hydroxymethylethylene hydroxymethylformal) (PHF), 2-methacryloyloxy-2'-ethyltrimethylammoniumphosphate (MPC).

[0021] In particular embodiments of the invention illustrated in examples below, the water soluble polymer is PEG or branched PEG.

[0022] In further particular embodiments of the invention illustrated in examples below, the water soluble polymer is polysialic acid (PSA) or a modified PSA (mPSA). The PSA or mPSA may have a molecular weight range of 350 Da to 120,000 Da, 500 Da to 100,000 Da,1000 Da to 80,000 Da, 1500 Da to 60,000 Da, 2,000 Da to 45,000 Da or 3,000 Da to 35,000 Da.

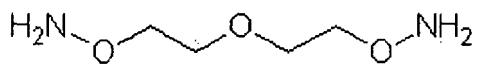
[0023] The PSA or mPSA may be colominic acid or modified colominic acid.

[0024] In another embodiment of the invention, the PSA or mPSA is comprised of about 2-500 or 10 – 300 sialic acid units. In yet another embodiment, the aforementioned method is provided wherein the oxidizing agent is sodium periodate ($NaIO_4$).

[0025] The method of the invention may comprise oxidizing the water soluble polymer to form an aldehyde group on a terminal sialic acid unit of the water soluble polymer, and reacting the oxidized water soluble polymer with an aminooxy linker.

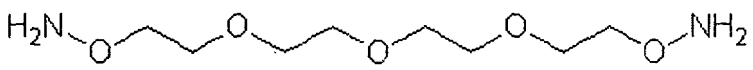
[0026] In yet another embodiment of the invention, the aforementioned method is provided wherein the water soluble polymer is prepared by reacting an activated aminooxy linker with oxidized water soluble polymer wherein the linker is a homobifunctional or heterobifunctional linker. The homobifunctional linker can have the general formula $NH_2[OCH_2CH_2]_nONH_2$, wherein n = 1-50, preferably 1-11, more preferably 1-6. The linker may specifically be selected from:

a 3-oxa-pentane-1,5-dioxyamine linker of the formula:



and

a 3,6,9-trioxa-undecane-1,11-dioxyamine linker of the formula:



PSA or mPSA may be oxidized by incubation with an oxidizing agent to form a terminal aldehyde group at the non-reducing end of the PSA.

[0027] The method may comprise oxidizing the water soluble polymer to form an aldehyde group on a terminal unit of the water soluble polymer, e.g. a terminal sialic acid unit of the PSA or mPSA, and reacting the oxidized water soluble polymer with an aminooxy linker. In still another embodiment, an aforementioned method is provided wherein the aminooxy linker is 3-oxa-pentane-1,5-dioxyamine. In a related embodiment, the oxidizing agent is $NaIO_4$.

[0028] In another embodiment of the invention, the aforementioned method is provided wherein the contacting of the oxidized carbohydrate moiety with the activated water soluble polymer occurs in a buffer comprising a nucleophilic catalyst selected from the group consisting of aniline and aniline derivatives.

[0029] A hydrazide group may be formed on the water soluble polymer by reacting oxidized water soluble polymer with a hydrazide linker. The hydrazide linker can suitably be adipic acid dihydrazide or hydrazine.

[0030] In yet another embodiment of the invention, an aforementioned method is provided further comprising the step of reducing an oxime or hydrazone linkage in the conjugated protein, for example by incubating the conjugated protein in a buffer comprising a reducing compound selected from the group consisting of sodium cyanoborohydride ($NaCNBH_3$) and ascorbic acid (vitamin C). In a related embodiment the reducing compound is sodium cyanoborohydride ($NaCNBH_3$).

[0031] In another embodiment of the invention, a conjugated glycoprotein produced by any aforementioned method is provided. In still another embodiment of the invention, a conjugated glycoprotein other than a blood coagulation protein, a ganglioside or a drug delivery system comprises (a) the said glycoprotein, ganglioside or drug delivery system; and (b) at least one aminooxy water soluble polymer bound to the glycoprotein of (a), wherein said aminooxy water soluble polymer is attached to the glycoprotein, ganglioside or drug delivery system via one or more carbohydrate moieties. In a still further embodiment of the invention, a conjugated glycoprotein other than a blood coagulation protein, a ganglioside or a drug delivery system comprises (a) the said glycoprotein, ganglioside or drug delivery system; and (b) at least one hydrazide water soluble polymer bound to the glycoprotein of (a), wherein said hydrazide water soluble polymer is attached to the glycoprotein ganglioside or drug delivery system via one or more carbohydrate moieties.

FIGURES

[0032] Figure 1 shows the synthesis of the water soluble di-aminoxy linkers 3-oxa-pentane-1,5-dioxyamine and 3,6,9-trioxa-undecane-1,11-dioxyamine.

[0033] Figure 2 shows the preparation of aminooxy-PSA.

DETAILED DESCRIPTION OF THE INVENTION

[0034] The pharmacological and immunological properties of carbohydrate-containing compounds, such as glycoproteins other than blood coagulations proteins can be improved by chemical modification and conjugation with water soluble polymer, in particular PEG or PSA or mPSA. The properties of the resulting conjugates generally strongly depend on the structure and the size of the polymer. Thus, polymers with a defined and narrow size distribution are usually preferred. PSA and mPSA, used in specific examples, can be purified in such a manner that results in a final PSA preparation with a narrow size distribution.

GLYCOPROTEINS

[0035] As described herein, glycoproteins other than blood coagulation proteins including, but not limited to cytokines such as interleukins, alpha-, beta-, and gamma-interferons, colony stimulating factors including granulocyte colony stimulating factors, fibroblast growth factors, platelet derived growth factors, phospholipase-activating protein (PUP), insulin, plant proteins such as lectins and ricins, tumor necrosis factors and related alleles, soluble forms of tumor necrosis factor receptors, interleukin receptors and soluble forms of interleukin receptors, growth factors, tissue growth factors, transforming growth factors such as TGFαs or TGFβs and epidermal growth factors, hormones, somatomedins, pigmentary hormones, hypothalamic releasing factors, antidiuretic hormones, prolactin, chorionic gonadotropin, follicle-stimulating hormone, thyroid-stimulating hormone, tissue plasminogen activator, and immunoglobulins such as IgG, IgE, IgM, IgA, and IgD, monoclonal antibodies, erythropoietin (EPO), blood factors other than blood coagulation proteins, galactosidases, α-galactosidases, β-galactosidases, DNAses, fetuin, fragments thereof, and any fusion proteins comprising any of the above mentioned proteins or fragments thereof together with therapeutic glycoproteins in general are contemplated by the invention. In an embodiment the glycoprotein is EPO. In a further embodiment the glycoprotein is a galactosidase. In a still further embodiment the glycoprotein is a DNAse. In a yet further embodiment the glycoprotein is fetuin. Lastly, in a still yet further embodiment the glycoprotein is a granulocyte colony stimulating factor.

[0036] As used herein "biologically active derivative" or "biologically active variant" includes any derivative or variant of a molecule having substantially the same functional and/or biological properties of said molecule, such as binding properties, and/or the same structural basis, such as a peptidic backbone or a basic polymeric unit.

[0037] An "analog," "variant" or "derivative" is a compound substantially similar in structure and having the same biological activity, albeit in certain instances to a differing degree, to a naturally-occurring molecule. For example, a polypeptide variant refers to a polypeptide sharing substantially similar structure and having the same biological activity as a reference polypeptide. Variants or analogs differ in the composition of their amino acid sequences compared to the naturally-occurring polypeptide from which the analog is derived, based on one or more mutations involving (i) deletion of one or more amino acid residues at one or more termini of the polypeptide and/or one or more internal regions of the naturally-

occurring polypeptide sequence (e.g., fragments), (ii) insertion or addition of one or more amino acids at one or more termini (typically an "addition" or "fusion") of the polypeptide and/or one or more internal regions (typically an "insertion") of the naturally-occurring polypeptide sequence or (iii) substitution of one or more amino acids for other amino acids in the naturally-occurring polypeptide sequence. By way of example, a "derivative" refers to a polypeptide sharing the same or substantially similar structure as a reference polypeptide that has been modified, e.g., chemically.

[0038] Variant or analog polypeptides include insertion variants, wherein one or more amino acid residues are added to a protein amino acid sequence of the invention. Insertions may be located at either or both termini of the protein, and/or may be positioned within internal regions of the protein amino acid sequence. Insertion variants, with additional residues at either or both termini, include for example, fusion proteins and proteins including amino acid tags or other amino acid labels. In one aspect, the protein molecule optionally contains an N-terminal Met, especially when the molecule is expressed recombinantly in a bacterial cell such as E. coli.

[0039] In deletion variants, one or more amino acid residues in a protein or polypeptide as described herein are removed. Deletions can be effected at one or both termini of the protein or polypeptide, and/or with removal of one or more residues within the protein amino acid sequence. Deletion variants, therefore, include fragments of a protein or polypeptide sequence.

[0040] In substitution variants, one or more amino acid residues of a protein or polypeptide are removed and replaced with alternative residues. In one aspect, the substitutions are conservative in nature and conservative substitutions of this type are well known in the art. Alternatively, the invention embraces substitutions that are also non-conservative. Exemplary conservative substitutions are described in Lehninger, [Biochemistry, 2nd Edition; Worth Publishers, Inc., New York (1975), pp.71-77] and are set out immediately below.

CONSERVATIVE SUBSTITUTIONS

SIDE CHAIN CHARACTERISTIC	**AMINO ACID**
Non-polar (hydrophobic):	

A. Aliphatic	A L I V P
B. Aromatic	F W
C. Sulfur-containing	M
D. Borderline	G
Uncharged-polar:	
A. Hydroxyl	S T Y
B. Amides	N Q
C. Sulfhydryl	C
D. Borderline	G
Positively charged (basic)	K R H
Negatively charged (acidic)	D E

[0041] Alternatively, exemplary conservative substitutions are set out immediately below.

CONSERVATIVE SUBSTITUTIONS II

ORIGINAL RESIDUE	**EXEMPLARY SUBSTITUTION**
Ala (A)	Val, Leu, Ile
Arg (R)	Lys, Gln, Asn
Asn (N)	Gln, His, Lys, Arg
Asp (D)	Glu
Cys (C)	Ser
Gln (Q)	Asn
Glu (E)	Asp
His (H)	Asn, Gln, Lys, Arg
Ile (I)	Leu, Val, Met, Ala, Phe,
Leu (L)	Ile, Val, Met, Ala, Phe
Lys (K)	Arg, Gln, Asn

Met (M)	Leu, Phe, Ile
Phe (F)	Leu, Val, Ile, Ala
Pro (P)	Gly
Ser (S)	Thr
Thr (T)	Ser
Trp (W)	Tyr
Tyr (Y)	Trp, Phe, Thr, Ser
Val (V)	Ile, Leu, Met, Phe, Ala

GANGLIOSIDES

[0042] In embodiments, of the invention, gangliosides are conjugated to water soluble polymers, e.g. PEG or PSA or mPSA. Gangliosides are known to provide cells with distinguishing surface markers that can serve in cellular recognition and cell-to-cell communication. They are useful as therapeutic agents.

[0043] Conjugates of the invention may comprise a ganglioside and a water soluble polymer, in which the ganglioside comprises a glycosphingolipid (ceramide and oligosaccharide) with one or more sialic acids linked on the sugar chain. Gangliosides can be classified according to how many sialic acid units are present on the molecule. Examples of gangliosides are GM1, GM2 and GM3 (monosialo-gangliosides), GD1a, GD1b, GD2 and GD3 (disialo-gangliosides), GT1b (trisialo-ganglioside) and GQ1 (tetrasialo-ganglioside).

[0044] For use in the present invention, preferred gangliosides comprise a ceramide linked to glucose, which is linked to a first galactose, which is linked to N-acetylgalactosamine, which is linked to a second galactose. This second galactose can be linked to one sialic acid. The first galactose can be linked to one, two, three or four sialic acids. Sialic acids may be linked either as monomers (one on each of the galactose molecules), or as oligosialic acids (2-4 sialic acids) to the first galactose.

[0045] Where administered therapeutic gangliosides need to circulate in the blood for long periods. So that their action on target tissues is more effective, gangliosides can be polysialylated, for example, by the method of the invention.

DRUG DELIVERY SYSTEMS

[0046] In further embodiments, of the invention, drug delivery systems are conjugated to a water soluble polymer, e.g. PEG or PSA or mPSA. In general, a drug delivery system (DDS) is any molecular or particulate entity which can control the fate and effect of drugs associated with the entity. DDSs can be separated into two general types. The first type comprises macromolecules (MDDSs), for instance antibodies, neoglycoproteins as well as synthetic polymers, such as poly(hydroxypropylmethacrylamide), polylysine and polymerised alkyl cyanoacrylates. The association of drugs with various types of macromolecular carriers, including monoclonal antibodies to target the drug to the desired sites is described for instance by Gregoriadis in Nature 265, 407-411 (1977). The second type is particulate DDSs (PDDSs), which comprises for instance nanospheres or microspheres, which comprise biodegradable materials such as albumin or semibiodegradable materials such as dextran and alkylcyanoacrylate polymers, or vesicles formed of nonionic surfactants or liposomes – for details of which see for example Gregoriadis in NIPS, 4, 146-151 (1989).

[0047] Drugs can either be covalently linked to, or passively entrapped into, the DDS. For instance, PDDS comprising surfactant vesicles or liposomes may entrap hydrophilic or hydrophobic pharmaceutically active compounds by being formed of an appropriate combination of layers of surfactant or lipid molecules. Pharmaceutically active compounds are usually covalently linked to MDDSs, by a bond which may or may not be lysed in the body, for instance before or after the active compound performs its function.

[0048] Many of the MDDSs have an intrinsic (e.g. antibodies) or acquired (e.g. neoglycoproteins) ability to be recognised by target cells or tissues through receptors on the latter's surface. Typically, such DDSs are taken up specifically by the target upon injection. Specific uptake is, however, limited with the bulk of the DDSs being taken up by other, irrelevant (to therapy) tissues. The reason for this is that antibodies and other DDS proteins (regardless of their specificity for the target) must be, like other proteins, catabolised at the end of their biological life.

[0049] Synthetic polymers used in the macromolecular type MDDSs are for instance poly(hydroxypropylmethacrylamide) polylysine and polymerised alkyl cyanoacrylates. These may be catabolised in the reticuloendothelial system (RES) or other tissues by appropriate lysosomal enzymes. It would be desirable to reduce the rate of catabolism of such biodegradable macromolecular type DDS by some means, for instance by reducing uptake of

the DDS by the RES or other tissues, or by reducing degradation by lysosomal enzymes once taken up by the RES.

[0050] Particulate DDSs (PDDSs) are, as a rule, removed from the circulation by the RES. Because of their propensity for the RES, PDDSs are often used for the delivery of drugs to these tissues. It is often desirable however, that PDDSs are directed to tissues other than those of the RES. To achieve this goal, one must block or delay RES interception of PDDSs.

[0051] DDSs for use in the invention may not initially contain glycons. An option is to add or otherwise incorporate a glycon into the DDS structure. Examples of such cases are liposomes incorporating a mannosylated or a galactosylated lipid. These glycoliposomes will target actives to tissues which express a mannose or galactose receptor respectively.

[0052] Where DDSs need to circulate in the blood for long periods so that e.g. uptake by target tissues is more effective (as with hepatic parenchymal cells), they are advantageously polysialylated by the methods of the invention.

ADMINISTRATION

[0053] In one embodiment a conjugated compound of the present invention may be administered by injection, such as intravenous, intramuscular, or intraperitoneal injection. The compositions may be useful as therapeutic, diagnostic and/or similar agents

[0054] To administer compositions comprising a conjugated compound of the present invention to human or test animals, in one aspect, the compositions comprise one or more pharmaceutically acceptable carriers. The terms "pharmaceutically" or "pharmacologically acceptable" refer to molecular entities and compositions that are stable, inhibit protein degradation such as aggregation and cleavage products, and in addition do not produce allergic, or other adverse reactions when administered using routes well-known in the art, as described below. "Pharmaceutically acceptable carriers" include any and all clinically useful solvents, dispersion media, coatings, antibacterial and antifungal agents, isotonic and absorption delaying agents and the like, including those agents disclosed above.

[0055] As used herein, "effective amount" includes a dose suitable for treating a mammal having a clinically defined disorder.

[0056] The compositions may be administered orally, topically, transdermally, parenterally, by inhalation spray, vaginally, rectally, or by intracranial injection. The term parenteral as used herein includes subcutaneous injections, intravenous, intramuscular,

intracisternal injection, or infusion techniques. Administration by intravenous, intradermal, intramuscular, intramammary, intraperitoneal, intrathecal, retrobulbar, intrapulmonary injection and or surgical implantation at a particular site is contemplated as well. Generally, compositions are essentially free of pyrogens, as well as other impurities that could be harmful to the recipient.

[0057] Single or multiple administrations of the compositions can be carried out with the dose levels and pattern being selected by the treating physician. For the prevention or treatment of disease, the appropriate dosage will depend on the type of disease to be treated, as described above, the severity and course of the disease, whether drug is administered for preventive or therapeutic purposes, previous therapy, the patient's clinical history and response to the drug, and the discretion of the attending physician.

[0058] The present invention also relates to a pharmaceutical composition comprising an effective amount of a conjugated compound or protein as defined herein. The pharmaceutical composition may further comprise a pharmaceutically acceptable carrier, diluent, salt, buffer, or excipient. The pharmaceutical composition can be used for treating clinically-defined disorders. The pharmaceutical composition of the invention may be a solution or a lyophilized product. Solutions of the pharmaceutical composition may be subjected to any suitable lyophilization process.

[0059] As an additional aspect, the invention includes kits which comprise a composition of the invention packaged in a manner which facilitates its use for administration to subjects. In one embodiment, such a kit includes a compound or composition described herein (e.g., a composition comprising a conjugated protein), packaged in a container such as a sealed bottle or vessel, with a label affixed to the container or included in the package that describes use of the compound or composition in practicing the method. In one embodiment, the kit contains a first container having a composition comprising a conjugated protein and a second container having a physiologically acceptable reconstitution solution for the composition in the first container. In one aspect, the compound or composition is packaged in a unit dosage form. The kit may further include a device suitable for administering the composition according to a specific route of administration. Preferably, the kit contains a label that describes use of the therapeutic protein or peptide composition.

[0060] In one embodiment, the derivative retains the full functional activity of native therapeutic compounds, and provides an extended half-life in vivo, as compared to native

therapeutic compounds. In another embodiment, the derivative retains at least 20, 21, 22, 23, 24, 25, 26, 27, 28, 29, 30, 31, 32, 34, 35, 36, 37, 38, 39, 40, 41, 42, 43, 44. 45, 46, 47, 48, 49, 50, 51, 52, 53, 54, 55, 56,57, 58, 59, 60, 61, 62, 63, 64, 65, 66, 67, 68, 69, 70, 71, 72, 73, 74, 75, 76, 77, 78, 79, 80, 81, 82, 83, 84, 85, 86, 87, 88, 89, 90, 91, 92, 93, 94, 95, 96, 97, 98, 99, 100, 110, 120, 130, 140, or 150 percent (%) biological activity relative to native compound.

SIALIC ACID AND PSA

[0061] As used herein, "sialic acid moieties" includes sialic acid monomers or polymers ("polysaccharides") which are soluble in an aqueous solution or suspension and have little or no negative impact, such as side effects, to mammals upon administration of the PSA-protein conjugate in a pharmaceutically effective amount. PSA and mPSA are characterized, in one aspect, as having 1, 2, 3, 4, 5, 10, 20, 30, 40, 50, 60, 70, 80, 90, 100, 200, 300, 400, or 500 sialic acid units. In certain aspects, different sialic acid units are combined in a chain.

[0062] In one embodiment of the invention, the sialic acid portion of the PSA or mPSA compound is highly hydrophilic, and in another embodiment the entire compound is highly hydrophilic. Hydrophilicity is conferred primarily by the pendant carboxyl groups of the sialic acid units, as well as the hydroxyl groups. The saccharide unit may contain other functional groups, such as, amine, hydroxyl or sulphate groups, or combinations thereof. These groups may be present on naturally-occurring saccharide compounds, or introduced into derivative polysaccharide compounds. The PSA and mPSA used in the methods and conjugates of the invention may be further characterized as described above in the Background of the Invention.

[0063] The naturally occurring polymer PSA is available as a polydisperse preparation showing a broad size distribution (e.g. Sigma C-5762) and high polydispersity (PD). Because the polysaccharides are usually produced in bacteria carrying the inherent risk of copurifying endotoxins, the purification of long sialic acid polymer chains may raise the probability of increased endotoxin content. Short PSA molecules with 1-4 sialic acid units can also be synthetically prepared (Kang SH et al., Chem Commun. 2000;227-8; Ress DK and Linhardt RJ, Current Organic Synthesis. 2004;1:31-46), thus minimizing the risk of high endotoxin levels. However PSA preparations with a narrow size distribution and low polydispersity, which are also endotoxin-free, can now be manufactured. Polysaccharide compounds of particular use for the invention are, in one aspect, those produced by bacteria. Some of these

naturally-occurring polysaccharides are known as glycolipids. In one embodiment, the polysaccharide compounds are substantially free of terminal galactose units.

[0064] In various embodiments, the compound is linked to or associated with the PSA or mPSA compound in stoichiometric amounts (e.g., 1:1, 1:2, 1:3, 1:4, 1:5, 1:6, 1:7, 1:7, 1:8, 1:9, or 1:10, etc.). In various embodiments, 1-6, 7-12 or 13-20 PSA and/or mPSA units are linked to the compound. In still other embodiments, 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, 20 or more PSA and/or mPSA units are linked to the compound.

[0065] Optionally, the compound is modified to introduce glycosylation sites (i.e., sites other than the native glycosylation sites). Such modification may be accomplished using standard molecular biological techniques known in the art. Moreover, the compound, prior to conjugation via one or more carbohydrate moieties, may be glycosylated in vivo or in vitro.

AMINOOXY LINKAGE

[0066] In one embodiment of the invention, the reaction of hydroxylamine or hydroxylamine derivatives with aldehydes (e.g., on a carbohydrate moiety following oxidation by sodium periodate) to form an oxime group is applied to the preparation of conjugates of compound. For example, a glycoprotein is first oxidized with a oxidizing agent such as sodium periodate ($NaIO_4$) (Rothfus JA et Smith EL., J Biol Chem 1963, 238, 1402-10; and Van Lenten L and Ashwell G., J Biol Chem 1971, 246, 1889-94). The periodate oxidation of e.g. glycoproteins is based on the classical Malaprade reaction described in 1928, the oxidation of vicinal diols with periodate to form an active aldehyde group (Malaprade L., Analytical application, Bull Soc Chim France, 1928, 43, 683-96). Additional examples for such an oxidizing agent are lead tetraacetate ($Pb(OAc)_4$), manganese acetate ($MnO(Ac)_3$), cobalt acetate ($Co(OAc)_2$), thallium acetate (TlOAc), cerium sulfate ($Ce(SO_4)_2$) (US 4,367,309) or potassium perruthenate ($KRuO_4$) (Marko et al., J Am Chem Soc 1997,119, 12661-2). By "oxidizing agent" a mild oxidizing compound which is capable of oxidizing vicinal diols in carbohydrates, thereby generating active aldehyde groups under physiological reaction conditions is meant.

[0067] The second step is the coupling of the polymer containing an aminooxy group to the oxidized carbohydrate moiety to form an oxime linkage. In one embodiment of the invention, this step can be carried out in the presence of catalytic amounts of the nucleophilic catalyst aniline or aniline derivatives (Dirksen A et Dawson PE, Bioconjugate Chem. 2008; Zeng Y et al., Nature Methods 2009;6:207-9). The aniline catalysis dramatically accelerates

the oxime ligation allowing the use of very low concentrations of the reagents. In another embodiment of the invention the oxime linkage is stabilized by reduction with $NaCNBH_3$ to form an alkoxyamine linkage.

[0068] In one embodiment of the invention, the reaction steps to conjugate PSA or mPSA to a protein are carried out separately and sequentially (i.e., starting materials (e.g., protein, polymer, etc), reagents (e.g., oxidizing agents, aniline, etc) and reaction products (e.g., oxidized carbohydrate on a protein, activated aminooxy polymer, etc) are separated between individual reaction steps).

[0069] Additional information on aminooxy technology can be found in the following references, each of which is incorporated in their entireties: EP 1681303A1 (HASylated erythropoietin); WO 2005/014024 (conjugates of a polymer and a protein linked by an oxime linking group); WO96/40662 (aminooxy-containing linker compounds and their application in conjugates); WO 2008/025856 (Modified proteins); Peri F et al., Tetrahedron 1998, 54, 12269-78; Kubler-Kielb J and Pozsgay V., J Org Chem 2005, 70, 6987-90; Lees A et al., Vaccine 2006, 24(6), 716-29; and Heredia KL et al., Macromolecules 2007, 40(14), 4772-9.

[0070] Advantages of the invention include high recovery of conjugate, high retention of activity of the conjugated glycoprotein compared to unconjugated protein and high conjugation efficiency.

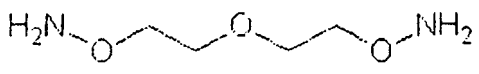
[0071] The invention is now illustrated with reference to the following examples. Examples 1-3, 9 and 11-27 illustrate specific embodiments of the invention. Examples 4-8 and 10 are included as reference examples for their relevance to preparation of corresponding conjugates of the invention.

EXAMPLES

Example 1

Preparation of the homobifunctional linker $NH_2[OCH_2CH_2]_2ONH_2$

[0072] The homobifunctional linker $NH_2[OCH_2CH_2]_2ONH_2$



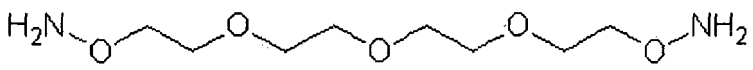
(3-oxa-pentane-1,5-dioxyamine) containing two active aminooxy groups was synthesized according to Boturyn et al. (Tetrahedron 1997;53:5485-92) in a two step organic reaction

employing a modified Gabriel-Synthesis of primary amines. In the first step, one molecule of 2,2-chlorodiethylether was reacted with two molecules of Endo-N-hydroxy-5-norbornene-2,3-dicarboximide in dimethylformamide (DMF). The desired homobifunctional product was prepared from the resulting intermediate by hydrazinolysis in ethanol. Except where otherwise specified, this is referred to as the diaminooxy linker in examples below.

Example 2

Preparation of the homobifunctional linker $NH_2[OCH_2CH_2]_4ONH_2$

[0073] The homobifunctional linker $NH_2[OCH_2CH_2]_4ONH_2$



(3,6,9-trioxa-undecane-1,11-dioxyamine) containing two active aminooxy groups was synthesized according to Boturyn et al. (Tetrahedron 1997;53:5485-92) in a two step organic reaction employing a modified Gabriel-Synthesis of primary amines. In the first step one molecule of Bis-(2-(2-chlorethoxy)-ethyl)-ether was reacted with two molecules of Endo-N-hydroxy-5-norbornene-2,3-dicarboximide in DMF. The desired homobifunctional product was prepared from the resulting intermediate by hydrazinolysis in ethanol.

Example 3

Preparation of aminooxy-PSA

[0074] 500mg of oxidized PSA (MW=18.8kD) obtained from the Serum Institute of India (Pune, India) was dissolved in 8ml 50mM sodium acetate buffer, pH 5.5. Next, 100mg 3-oxa-pentane-1,5-dioxyamine was added. After shaking for 2hrs at room temperature, 44 mg sodium cyanoborohydride was added. After shaking for another 4hrs at 4°C, the reaction mix was loaded into a Slide-A-Lyzer (Pierce, Rockford, IL) dialysis cassette (3.5 kD membrane, regenerated cellulose) and dialyzed against PBS pH 7.2 for 4 days. The product was frozen at -80°C. The preparation of the aminooxy-PSA according to this procedure is illustrated in Figure 2.

Example 4

Coupling of aminooxy-PSA to rFIX and purification of the conjugate

[0075] To 12.6mg rFIX, dissolved in 6.3ml 50mM sodium acetate buffer, pH 6.0, 289µl of an aqueous sodium periodate solution (10mM) was added. The mixture was shaken in the dark for 1h at 4°C and quenched for 15min at room temperature by the addition of 6.5µl 1M glycerol. Low molecular weight contaminates were removed by ultrafiltration/diafiltration (UF/DF) employing Vivaspin (Sartorius, Goettingen, Germany) concentrators (30kD membrane, regenerated cellulose). Next, 43mg aminooxy-PSA was added to the UF/DF retentate and the mixture was shaken for 18hrs at 4°C. The excess PSA reagent was removed by hydrophobic interaction chromatography (HIC). The conductivity of the cooled reaction mixture was raised to 180mS/cm and loaded onto a 5ml HiTrap Butyl FF (GE Healthcare, Fairfield, CT) HIC column (1.6 x 2.5cm), pre-equilibrated with 50mM HEPES, 3M sodium chloride, 6.7mM calcium chloride, 0.01% Tween 80, pH 6.9. The conjugate was eluted within 2.4 column volumes (CV) with 50mM HEPES, 6.7mM calcium chloride, 0.005% Tween 80, pH 7.4 at a flow rate of 5ml/min. The preparation was analytically characterized by measuring total protein (BCA) and FIX chromogenic activity. For the PSA-rFIX conjugate a specific activity of 80.2 IU/mg protein was determined (56.4 % in comparison to native rFIX). The results are summarized in Table 1.

Table 1

Item	BCA [mg/ml]	FIX:Chrom [IU/ml]	Specific Activity [IU FIX:Chrom/mg BCA	Specific Activity [%]
rFIX	8.58	1221	142.3	100
PSA-rFIX	1.15	92.2	80.2	56.4

Example 5

Coupling of aminooxy-PSA to rFIX in the presence of aniline as nucleophilic catalyst

[0076] To 3.0mg rFIX, dissolved in 1.4ml 50mM sodium acetate buffer, pH 6.0, 14.1µl of an aqueous sodium periodate solution (10mM) was added. The mixture was shaken in the dark for 1h at 4°C and quenched for 15min at room temperature by the addition of 1.5µl 1M glycerol. Low molecular weight contaminates were removed by means of size exclusion chromatography (SEC) employing PD-10 desalting columns (GE Healthcare, Fairfield, CT). 1.2mg oxidized rFIX, dissolved in 1.33ml 50mM sodium acetate buffer, pH 6.0 was mixed

with 70µl of aniline (200mM aqueous stock solution) and shaken for 45min at room temperature. Next, 4.0mg aminooxy-PSA was added and the mixture was shaken for 2hrs at room temperature and another 16hrs at 4°C. Samples were drawn after 1h, after 2hrs and at the end of the reaction after 18hrs. Next, excess PSA reagent and free rFIX were removed by means of HIC. The conductivity of the cooled reaction mixture was raised to 180mS/cm and loaded onto a 5ml HiTrap Butyl FF (GE Healthcare, Fairfield, CT) HIC column (1.6 x 2.5cm), pre-equilibrated with 50mM HEPES, 3M sodium chloride, 6.7mM calcium chloride, 0.01% Tween 80, pH 6.9. The conjugate was eluted with a linear gradient to 50mM HEPES, 6.7mM calcium chloride, 0.005% Tween 80, pH 7.4 in 20CV with at a flow rate of 5ml/min.

Example 6

Coupling of aminooxy-PSA to rFIX and reduction with $NaCNBH_3$

[0077] To 10.5mg rFIX, dissolved in 5.25ml 50mM sodium acetate buffer, pH 6.0, 53µl of an aqueous sodium periodate solution (10mM) was added. The mixture was shaken in the dark for 1h at 4°C and quenched for 15min at room temperature by the addition of 5.3µl 1M glycerol. Low molecular weight contaminates were removed by means of UF/DF employing Vivaspin (Sartorius, Goettingen, Germany) concentrators (30 kD membrane, regenerated cellulose). Next, 35.9mg aminooxy-PSA was added to the UF/DF retentate and the mixture was shaken for 2hrs at room temperature. Then 53µl of aqueous sodium cyanoborohydride solution (5M) was added and the reaction was allowed to proceed for another 16 hrs. Then the excess PSA reagent was removed by means of HIC. The conductivity of the cooled reaction mixture was raised to 180mS/cm and loaded onto a 5ml HiTrap Butyl FF HIC (GE Healthcare, Fairfield, CT) column (1.6 x 2.5 cm), pre-equilibrated with 50mM HEPES, 3M sodium chloride, 6.7mM calcium chloride, 0.01% Tween 80, pH 6.9. The conjugate was eluted within 2.4CV with 50mM HEPES, 6.7mM calcium chloride, 0.005% Tween 80, pH 7.4 at a flow rate of 5 ml/min.

Example 7

Coupling of aminooxy-PSA (linker: $NH_2[OCH_2CH_2]_4ONH_2$) to rFIX and purification of the conjugate

[0078] To 5.6mg rFIX, dissolved in 2.8ml 50mM sodium acetate buffer, pH 6.0, 102 µl of an aqueous solution of sodium periodate (10mM) was added. The mixture was shaken in the dark for 1h at 4°C and quenched for 15min at room temperature by the addition of 2.9 µl of

1M glycerol. Low molecular weight contaminates were removed by means of UF/DF employing Vivaspin (Sartorius, Goettingen, Germany) concentrators (30kD membrane, regenerated cellulose). Then 19mg aminooxy-PSA was added to the UF/DF retentate and the mixture was shaken for 18hrs at 4°C. The excess PSA reagent was removed by means of HIC. The conductivity of the cooled reaction mixture was raised to 180mS/cm and loaded onto a 5ml HiTrap Butyl FF (GE Healthcare, Fairfield, CT) HIC column (1.6 x 2.5cm), pre-equilibrated with 50mM HEPES, 3M sodium chloride, 6.7mM calcium chloride, 0.01% Tween 80, pH 6.9. The conjugate was eluted within 2.4CV with 50mM HEPES, 6.7mM calcium chloride, 0.005% Tween 80, pH 7.4 at a flow rate of 5ml/min.

Example 8

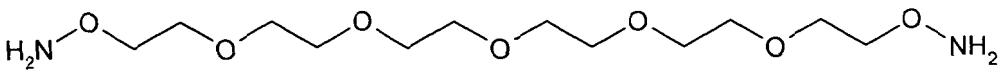
Coupling of aminooxy-PSA to rFVIII

[0079] To 11mg rFVIII, dissolved in 11ml Hepes buffer pH 6 (50mM Hepes, 5mM $CaCl_2$, 150mM NaCl, 0.01% Tween) 57µl 10mM sodium periodate was added. The mixture was shaken in the dark for 30min at 4°C and quenched for 30min at 4°C by the addition of 107µl of an aqueous1M glycerol solution. Then 19.8mg aminooxy-PSA (18.8kD) was added and the mixture was shaken over night at 4°C. The ionic strength was increased by adding a buffer containing 8M ammonium acetate (8M ammonium acetate, 50mM Hepes, 5mM $CaCl_2$, 350mM NaCl, 0.01% Tween 80, pH 6.9) to get a final concentration of 2.5M ammonium acetate. Next, the reaction mixture was loaded on a HiTrap Butyl FF (GE Healthcare, Fairfield, CT) column which was equilibrated with equilibration buffer (2.5M ammonium acetate, 50mM Hepes, 5mM $CaCl_2$, 350mM NaCl, 0.01% Tween 80, pH 6.9). The product was eluted with elution buffer (50mM Hepes, 5mM $CaCl_2$, 0.01% Tween 80, pH 7.4), and the eluate was concentrated by centrifugal filtration using Vivaspin (Sartorius, Goettingen, Germany) devices with 30,000 MWCO.

Example 9

Preparation of the homobifunctional linker $NH_2[OCH_2CH_2]_6ONH_2$

[0080] The homobifunctional linker $NH_2[OCH_2CH_2]_6ONH_2$



(3,6,9,12,15-penatoxa-heptadecane-1,17-dioxyamine) containing two active aminooxy groups was synthesized according to Boturyn et al. (Tetrahedron 1997;53:5485-92) in a two step

organic reaction employing a modified Gabriel-Synthesis of primary amines. In the first step one molecule of hexaethylene glycol dichloride was reacted with two molecules of Endo-N-hydroxy-5-norbornene-2,3-dicarboximide in DMF. The desired homobifunctional product was prepared from the resulting intermediate by hydrazinolysis in ethanol.

Example 10

Polysialylation of rFIX employing a maleimido/aminooxy linker system

A. Preparation of the modification reagent

[0081] An Aminooxy-PSA reagent is prepared by use of a maleimido/aminooxy linker system (Toyokuni et al., Bioconjugate Chem 2003; 14, 1253-9). PSA-SH (20kD) containing a free terminal SH – group is prepared using a two step procedure: a) Preparation of PSA-NH_2 by reductive amination of oxidized PSA with NH_4Cl according to WO05016973A1 and b) introduction of a sulfhydryl group by reaction of the terminal primary amino group with 2-iminothiolane (Traut's reagent / Pierce, Rockford, IL) as described in US7645860. PSA-SH is coupled to the maleimido-group of the linker at pH 7.5 in PBS - buffer using a 10-fold molar excess of the linker and a PSA-SH concentration of 50 mg/ml. The reaction mixture is incubated for 2 hours under gentle shaking at room temperature. Then the excess linker reagent is removed and the aminooxy-PSA is buffer exchanged into oxidation buffer (50mM sodium phosphate, pH 6.0) by diafiltration. The buffer is exchanged 25 times employing a Pellicon XL5kD regenerated cellulose membrane (Millipore, Billerica, MA).

B. Modification of rFIX after prior oxidation with $NaIO_4$

[0082] rFIX is oxidized in 50 mM sodium phosphate buffer, pH 6.0 employing 100 µM sodium periodate in the buffer. The mixture was shaken in the dark for 1h at 4°C and quenched for 15 min at room temperature by the addition of glycerol to a final concentration of 5mM. Low molecular weight contaminates were removed by means of size exclusion chromatography (SEC) employing PD-10 desalting columns (GE Healthcare, Fairfield, CT). Oxidized rFIX is then spiked with aniline to obtain a final concentration of 10mM and mixed with the aminooxy-PSA reagent to achieve a 5 fold molar excess of PSA. The reaction mixture was incubated for 2 hours under gentle shaking in the dark at room temperature.

C. Purification of the conjugates

[0083] The excess of PSA reagent and free rFIX is removed by means of HIC. The conductivity of the reaction mixture is raised to 180 mS/cm and loaded onto a column filled

with 48 ml Butyl - Sepharose FF (GE Healthcare, Fairfield, CT) pre-equilibrated with 50 mM Hepes, 3 M sodium chloride, 6.7 mM calcium chloride, 0.01% Tween 80, pH 6.9. Subsequently the conjugate is eluted with a linear gradient of 60% elution buffer (50mM Hepes, 6.7mM calcium chloride, pH 7.4) in 40 CV. Finally the PSA-rFIX containing fractions are collected and subjected to UF/DF by use of a 30 kD membrane made of regenerated cellulose (Millipore). The preparation is analytically characterized by measuring total protein (BCA) and FIX chromogenic activity. For the PSA-rFIX conjugates prepared with both variants a specific activity of > 50 % in comparison to native rFIX was determined.

Example 11

Preparation of aminooxy-PSA reagent

[0084] An aminooxy - PSA reagent was prepared according to Example 3. The final product was diafiltrated against buffer, pH 7.2 (50 mM Hepes) using a 5 kD membrane (regenerated cellulose, Millipore), frozen at -80°C and lyophilized. After lyophilization the reagent was dissolved in the appropriate volume of water and used for preparation of PSA-protein conjugates via carbohydrate modification.

Example 12

Detailed synthesis of the aminooxy-PSA reagent

[0085] 3-oxa-pentane-1,5 dioxyamine was synthesized according to Botyryn et al (Tetrahedron 1997; 53:5485-92) in a two step organic synthesis as outlined in Example 1.

Step 1:

[0086] To a solution of Endo-N-hydroxy-5-norbonene-2,3- dicarboxiimide (59.0g; 1.00eq) in 700 ml anhydrous N,N-dimethylformamide anhydrous K_2CO_3 (45.51g; 1.00eq) and 2,2-dichlorodiethylether (15.84 ml; 0.41eq) were added. The reaction mixture was stirred for 22 hours at 50°C. The mixture was evaporated to dryness under reduced pressure. The residue was suspended in 2 L dichloromethane and extracted two times with saturated aqueous NaCl-solution (each 1 L). The Dichloromethane layer was dried over Na_2SO_4 and then evaporated to dryness under reduced pressure and dried in high vacuum to give 64.5 g of 3-oxapentane-1,5-dioxy-endo-2',3'-dicarboxydiimidenorbornene as a white-yellow solid (intermediate 1).

Step2:

[0087] To a solution of intermediate 1 (64.25 g; 1.00eq) in 800 ml anhydrous Ethanol, 31.0 ml Hydrazine hydrate (4.26eq) were added. The reaction mixture was then refluxed for 2 hours. The mixture was concentrated to the half of the starting volume by evaporating the solvent under reduced pressure. The occurring precipitate was filtered off. The remaining ethanol layer was evaporated to dryness under reduced pressure. The residue containing the crude product 3-oxa-pentane-1,5-dioxyamine was dried in vacuum to yield 46.3g. The crude product was further purified by column chromatography (Silicagel 60; isocratic elution with Dichloromethane/Methanol mixture, 9+1) to yield 11.7 g of the pure final product 3-oxa-pentane -1,5-dioxyamine.

Example 13

Preparation of aminooxy-PSA polymer

[0088] 1.3 g of oxidized colominic acid (23kDa) was dissolved in 18ml of 50mM sodium acetate pH 5.5±0.02. 20 fold molar excess of 1, 11-diamino-3,6,9-trioxaundecane (also referred to as 3,6,9-trioxa-undecane-1,11-dioxyamine) was dissolved in minimum amount of 50mM sodium acetate (pH 5.5±0.02) and was added to the PSA solution. The final colominic acid concentration was 62.5mg/ml. This reaction mixture was incubated for 2±0.1hr at 22±1.0°C on a gentle mixer (22 oscillations per minute). After this, 0.65ml of 160 mg/ml $NaCNBH_3$ solution was added to the above reaction mixture so as to make the final concentration of 5.00 mg/ml . This was incubated for 3.0±0.20 hours at 4.0±1.0°C on a shaker (22 oscillations per minute) in a endotoxin free air tight container with enough headspace for mixing. For the purification, the sample was diluted with 2mM triethanolamine, pH 8.0±0.02 to make final colominic acid concentration of 20 mg/ml. The reaction mixture was desalted to remove excess of 1,11-diamino-3,6,9-trioxaundecane, $NaCNBH_3$ and byproducts of the reaction. This was followed by desalting on a Sephadex G25 column using 20mM triethanolamine buffer (pH 8.0±0.02). The pH of the desalted sample was adjusted to pH 7.8-8.0 and was ultrafiltered/diafiltered with 20mM TEA pH 8.0 once and 2mM triethanolamine (TEA) pH 8.0 twice. The sample was freeze dried and stored at -80°C.

[0089] Alternatively, purification was done in presence of high salt during desalting and ultrafiltration/diafiltration (UF/DF) steps. Anion exchange chromatography in high salt was also used to make highly pure aminooxy-PSA. By analogy, different molecular weights of aminooxy-PSA were synthesized.

Example 14

Coupling of Diaminooxy (3,6,9-trioxa-undecane-1,11-dioxyamine) – PSA to β-Galactosidase

[0090] For oxidation of β-Galactosidase (β-Gal), different concentrations of $NaIO_4$ (ranging from 0.157 mM to 2 mM) were used. 0.5 mg of β-Gal was oxidized under acidic pH of 5.75 at 4° C for 30 minutes in the dark. Oxidation was stopped by adding $NaHSO_3$ to a final concentration of 5 mM. The conjugation reaction was carried out using the oxidized β-Gal with diaminooxy PSA polymer (22kDa). The final concentration of polymer in the reaction mixture was 1.25 mM whereas the concentration of β-Gal ranged from 0.125 mg/ml to 0.76 mg/ml. All the reactions were done at pH5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17mg/ml. The reaction was carried out at 4°C and samples were collected at time intervals of 1, 2 and 24 hours. Conjugates were characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugate in SDS PAGE and this was also confirmed by western blotting.

[0091] Based on the best reactions conditions, 1.9 mg of β-Gal was oxidized with 1.5 mM of $NaIO_4$ for 30 minutes at 4°C and then oxidation was stopped by adding $NaHSO_3$ to a final concentration of 5 mM. The conjugation reaction was carried out using the oxidized β-Gal with diaminooxy PSA polymer. The final concentrations of polymer and protein in the reaction mixture were 1.25 mM and 0.76 mg/ml respectively. The final pH of the reaction mixture was around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17mg/ml. The reaction was carried out at 4°C for 2 hours. Purified and unpurified conjugates were characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugate in SDS PAGE and this was confirmed by western blotting using anti-PSA antibody. The in vitro activity PSA-βGal conjugates were comparable to native protein using All in one βGal assay kit (Pierce). Less than 50% activity was observed in comparable conjugates made using aldehyde linker chemistry. Further, the overall process was scaled up to 3 fold.

Example 15

Coupling of Diaminooxy-PSA to Fetuin

[0092] Fetuin and was oxidized with 10 mM $NaIO_4$ for 60 minutes at 4°C in the dark and the oxidation was stopped by adding $NaHSO_3$ to a final concentration of 10 mM. The conjugation reaction was carried out using the oxidized Fetuin with diaminooxy PSA polymer (23kDa). The final concentration of polymer in the reaction mixture was 2.5mM at

pH 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50mM or 3.17mg/ml. The final protein concentration in the reaction was 0.714mg/ml and the reaction was carried out at 4°C for 2 hours. These conjugates were characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugates in SDS PAGE and this was also confirmed by western blotting.

[0093] For a scale up reaction, 5 mg Fetuin was oxidized with 10 mM $NaIO_4$ for 60 minutes at 4°C in dark and then oxidation was stopped by adding $NaHSO_3$ to a final concentration of 10 mM. The conjugation reaction was carried out using the oxidized Fetuin with diaminooxy PSA polymer (23kDa). The final concentration of polymer in the reaction mixture was 2.5 mM at pH of 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17mg/ml. The reaction was carried out at 4°C and sample was collected after 2 hours. Purified and unpurified conjugates were characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugate in SDS PAGE and this was also confirmed by western blotting.

Example 16

Coupling of Diaminooxy-PSA to Fetuin with Aniline to Act as a Nucleophilic Catalyst

[0094] 0.2 mg of Fetuin was oxidized with 10mM $NaIO_4$ for 30 minutes at 4°C in dark and then oxidation was stopped by adding $NaHSO_3$ to a final concentration of 5mM. The conjugation reaction was carried out using the oxidized Fetuin with diaminooxy PSA polymer (23kDa). The final concentration of polymer in the reaction mixture was 1.25mM. The final pH of reaction mixture was 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50mM or 3.17mg/ml. The final protein concentration in the reaction was 0.125mg/ml. 84.21µl of 200mM aniline solution was added to the 1.6ml of reaction mixture. The reaction was carried out at 4°C overnight.

Example 17

Coupling of Diaminooxy-PSA to Erythropoietin (EPO)

[0095] 0.2 mg of EPO was oxidized with 10 mM of $NaIO_4$ for 30 minutes at 4°C. The oxidation was stopped by adding $NaHSO_3$ to a final concentration of 5 mM. The conjugation reaction was carried out using the oxidized EPO with diaminooxy polymer of 23kDa. The final concentration of polymer in the reaction mixture was 1.25 mM. The final concentration

of EPO in the reaction mixture was 0.125 mg/ml. The final pH of the reaction mixture was around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50mM or 3.17mg/ml. The reaction was carried out at 4°C for 24 hours. Unpurified conjugate was characterized using SDS PAGE. A shift in the band was seen for the conjugate in SDS PAGE.

Example 18

Coupling of Diaminooxy-PSA to EPO with Aniline to act as a nucleophilic catalyst

[0096] 0.2mg of EPO was oxidized with 10mM $NaIO_4$ for 30 minutes at 4°C. The oxidation was stopped by adding $NaHSO_3$ to a final concentration of 5mM. The conjugation reaction was carried out using the oxidized EPO with diaminooxy PSA polymer (22kDa). The final concentration of polymer in the reaction mixture was 1.25mM. The final pH of the reaction mixture was around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50mM or 3.17mg/ml. The final protein concentration in the reaction was 0.125mg/ml. 84.21µl of 200mM aniline solution was added to the 1.6ml of reaction mixture. The reaction was carried out at 4°C for overnight. The conjugates were characterized using SDS PAGE. A shift in the band was seen in the conjugates. No adverse effect of aniline was observed on activity of the conjugates.

Example 19

Coupling of Diaminooxy-PSA to DNAse

[0097] For glycopolysialylation of DNAse, bovine pancreas DNAse was used for conjugation reaction. This source of DNAse was supplied as lyophilized powder, which was stored at -20° C. Prior to the reaction, this lyophilized powder was dissolved in sodium acetate buffer (pH 5.75). The polymer used for glycopolysialylation had a weight in the range of 10 kDa to 22 kDa. For oxidation of glycon moiety of DNAse, $NaIO_4$ was used as oxidizing agent to a final concentration of 1 mM. DNAse was oxidized at acidic pH of 5.75 at 4° C for 30 minutes. The oxidation was stopped by adding $NaHSO_3$ to a final concentration of 2 mM. After oxidation was complete, the conjugation reaction was carried out by addition of diaminooxy PSA polymer to a final concentration of 1.25 mM. $NaCNBH_3$ was added to the reaction mixture to a final concentration of 50 mM or 3.17 mg/ml and the polysialylation of the DNAse was preformed 4.0±1.0° C for at least 2 hours. The reactions were stopped with 25 molar excess of Tris over polymer. The conjugates were characterized using SDS PAGE

and western blotting. A shift in the band was seen for the conjugate in SDS PAGE and positive result was obtained from western blotting. Activity was measured as 95% (compared with the less than 50% observed in comparable conjugates made using aldehyde linker chemistry).

Example 20

Coupling of Diaminooxy (3 oxa-pentane-1,5-dioxyamine linker)-PSA to β-Galactosidase

[0098] For oxidation of β-Galactosidase, $NaIO_4$ was used at a concentration of 2 mM. 3 mg of β-Galactosidase was oxidized at acidic pH of 5.75 at 4° C for 30 minutes then oxidation was stopped by adding $NaHSO_3$ to a final concentration of 2 mM. The conjugation reaction was carried out using the oxidized β-Galactosidase with diaminooxy PSA polymer (23 kDa). The final concentration of polymer in the reaction mixture was 1.5 mM. The final concentration of β-Galactosidase in reaction mixture was 0.867 mg/ml. The final pH of reaction mixture was around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17mg/ml. The reaction was carried out at 4°C for 2 hours. Conjugates were characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugate in SDS PAGE and positive result was obtained from western blotting.

Example 21

Preparation of Hydrazide-Colominic Acid

[0099] We used the following protocol to prepare a PSA-hydrazide (colominic acid-hydrazide) using adipic acid dihydrazide. Analogous methods were used to make other PSA-hydrazides.

1 Dissolve 1g of activated colominic acid in ~10ml of 20mM sodium acetate pH 5.5±0.02. Final colominic acid concentration should be 62.5mg/ml

2 Dissolve 25-fold molar excess (over oxidized colominic acid "CAO") of adipic acid dihydrazide (MW= 174.2gms) in minimum amount of 20mM sodium acetate (pH 5.5 ±0.02) and add to solution from 1.

3 Amount of adipic acid dihydrazide to be added

$$= \frac{\text{Weight of CAO in grams} \times 25 \times \text{MW of adipic acid dihydrazide in gms}}{\text{MW of CAO in Daltons}}$$

$$= \frac{1 \times 25 \times 174.2}{}$$

15×10^3

= 0.290g

4 After adding adipic acid dihydrazide solution, make up the volume of colominic acid with sodium acetate to a final concentration of 62.5mg/ml. Therefore total reaction volume is 16ml.

5 Incubate the reaction mixture for 2±0.1 hr at 22.0± 1.0°C on shaker (22 oscillations per minute).

6 Prepare concentrated $NaCNBH_3$ solution (165 mg/ml) and add 0.5ml to solution from 1 so that the final concentration of this becomes 5.0 mg/ml in the final reaction mixture. Incubate the reaction mixture for 3.0±0.20 hours at 4.0±1.0°C on shaker (22 oscillations per minute).

7 Keep the reaction mixture in endotoxin-free, air tight container with excess 50ml of headspace for proper mixing (there should be enough space so that reaction mixture should not touch the cap of container).

8 After 3 hours reaction at 4°C, dilute the sample with 2mM triethanolamine (make the volume up to 50ml), at pH 8.0±0.02 to make final colominic acid concentration to 20 mg/ml.

9 Desalt the reaction mixture to remove excess of untreated adipic acid dihydrazide, $NaCNBH_3$ etc from the polymer. This can be done by GPC (using XK 50 Sephadex G-25 medium matrix; ≤1.8mg of CA/ml matrix; 35cm bed height; Column volume= 687ml) by observing UV 224nm and conductivity. Desalting is carried out with 20mM triethanolamine (pH 8.0±0.02) buffer.

10 After desalting, colominic acid-hydrazide is subjected to 1 cycle of ultrafiltration, 1 cycle of diafiltration using 20mM TEA, pH 8.0±0.02 and at least 3 cycles of diafiltration using 2mM TEA, pH 8.0±0.02. This can be done using 3kDa vivaflow cassettes.

11 Adjust the pH of desalted sample to pH 7.8-8.0. Optionally, freeze-dry the sample and consecutively keep it for secondary drying to remove excess of moisture.

Example 22

Coupling of Hydrazide-PSA to Erythropoietin

[00100] For oxidation of erythropoietin (EPO), $NaIO_4$ was used at a concentration of 10 mM. EPO (1 mg) was oxidized at pH 5.75 at 4°C for 30 minutes then oxidation was stopped by adding $NaHSO_3$ to a final concentration of 5 mM. The conjugation reaction was carried out using the oxidized EPO with hydrazide-PSA polymer. The molecular weight of the hydrazide-PSA used for conjugation was 24.34 kDa. The final concentration of hydrazide-

PSA in the reaction mixture was 1.25 mM. The final concentration of EPO in the reaction mixture was 0.125 mg/ml. The final pH of the reaction mixture was around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17 mg/ml. The reaction was carried out at 4°C for 24 hours. Conjugates were characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugate in SDS PAGE and a positive result was obtained from western blotting.

Example 23

Coupling of Hydrazide-PSA to β-Galactosidase

[00101] β-Galactosidase (0.5 to 4.5 mg) was oxidized with 0.625 to 2 mM of $NaIO_4$ for 30 minutes at 4°C. The oxidation was stopped by adding $NaHSO_3$ to a final concentration of 5 mM. The conjugation reaction was carried out using the oxidized β-galactosidase with hydrazide-PSA ranging from 24.34 kDa to 27.9 kDa. The final concentration of hydrazide-PSA in the reaction mixture was 1.25 mM. The final concentration of β-galactosidase in the reaction mixture was in a range from 0.125 mg/ml to 0.76 mg/ml. The final pH of reaction mixture should be around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17 mg/ml. The reaction was carried out at 4°C and samples were collected at 1, 2 and 24 hours. Purified and unpurified conjugate was characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugate in SDS PAGE and a positive result was obtained from western blotting. Activity was measured as 84%. Less than 50% activity was observed in comparable conjugates made using aldehyde linker chemistry.

Example 24

Coupling of Hydrazide-PSA to Fetuin

[00102] Fetuin (0.25 mg) was oxidized with NaIO4 (5 or 10 mM) for 30 or 60 minutes at 4°C. The oxidation was stopped by adding $NaHSO_3$ to a final concentration of 5 or 10 mM as appropriate to match the concentration of $NaIO_4$ used for oxidation. The conjugation reactions were carried out using the oxidized Fetuin with adipic acid dihydrazide-PSA polymer. The final concentration of the polymer in the reaction mixture was between 1.25 and 2.5 mM. The final pH of reaction mixture was around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17 mg/ml. The reaction was carried out at 4°C for 1 hour to 4 hours. The conjugates were characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugate in SDS PAGE for each set of reaction conditions and a positive result was obtained from western blotting.

[00103] A scaled-up reaction for 5 mg Fetuin followed by purification of the resulting conjugate was carried out. 5 mg Fetuin was oxidized with 10 mM $NaIO_4$ for 60 minutes at 4°C and then oxidation was stopped by adding $NaHSO_3$ to a final concentration of 10 mM. The conjugation reaction was carried out using the oxidized Fetuin with adipic acid dihydrazide-PSA polymer. The final concentration of polymer in the reaction mixture was 2.5 mM. The final pH of reaction mixture was around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17 mg/ml. The reaction was carried out at 4°C and samples were collected at 2 hours. Purified and unpurified conjugate was characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugate in SDS PAGE and a positive result was obtained from western blotting.

Example 25

Coupling of Hydrazide-PSA to DNAse

[00104] DNAse was oxidized with NaIO4 to a final concentration ranging from 0.2 mM to 2 mM for 30 minutes at 4°C. The oxidation reaction was stopped by adding $NaHSO_3$ to a final concentration of between 2 and 5 mM depending upon the concentration of $NaIO_4$ used for oxidation. Glycopolysialylation of oxidized DNAse was carried out by addition of hydrazide-PSA polymer to a final concentration of 1.25 mM to the oxidized DNAse. Sodium cyanoborohydride was added to the reaction mixture to a final concentration of 50 mM or 3.17 mg/ml and the glycopolysialylation of the DNAse was performed at 4°C for a time period ranging from 1 hour to 2 hours. The reactions were stopped with 25-fold molar excess of Tris over polymer. The conjugates were characterized using SDS PAGE and western blotting. A shift in the band was seen for the conjugates in SDS PAGE and a positive result was obtained from western blotting. The activity was measured as 49%.

Example 26

PEGylation of β-Galactosidase using Aminooxy Linker (3-oxa-pentane-1,5-dioxyamine)

[00105] β-Galactosidase (1 mg) was oxidized with 1.5 mM of $NaIO_4$ for 30 minutes at 4°C. The oxidation was stopped by adding $NaHSO_3$ to a final concentration of 1.5 mM.

[00106] The conjugation reaction was carried out using the oxidized β-Galactosidase with diaminooxy-PEG polymer (20 kDa). The final concentration of the polymer in the reaction mixture was 1.25 mM. The final concentration of β-Galactosidase in the reaction mixture was 1 mg/ml. The final pH of reaction mixture should be around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17 mg/ml. The reaction

was carried out at 4°C for 2 hours. Unpurified conjugate was characterized using SDS PAGE and a shift in the band was seen for the conjugate in SDS PAGE. The activity was measured as 59%.

Example 27

PEGylation of Erythropoietin using Aminooxy Linker

[00107] Erythropoietin (EPO; 0.2 mg) was oxidised with 5 or 10 mM $NaIO_4$ in 50 mM sodium acetate at pH 5.75 for 45 minutes at 4°C and then oxidation was stopped by adding $NaHSO_3$ to a final concentration of 5 or 10 mM (to match the concentration of $NaIO_4$ used for oxidisation). The conjugation reaction was carried out using the oxidised EPO with diaminooxy PEG polymer (20 kDa). The final concentration of the polymer in the reaction mixture was 1.5 mM. The final pH of reaction mixture should be around 5.75. Sodium cyanoborohydride was added to the reaction mixture to a concentration of 50 mM or 3.17 mg/ml. The final protein concentration in the reaction was 0.4 mg/ml. The conjugation reaction was carried out overnight at 4°C.

[00108] The invention thus provides conjugates of compounds other than blood coagulation proteins with water soluble polymers, in particular PSA and mPSA.

Claims:

1. A method of conjugating a water soluble polymer to an oxidized carbohydrate moiety of (1) a glycoprotein other than a blood coagulation protein, (2) a ganglioside, or (3) a drug delivery system comprising a carbohydrate group, comprising contacting the oxidized carbohydrate moiety with the water soluble polymer under conditions that allow conjugation,

wherein said water soluble polymer contains an aminooxy group and an oxime linkage is formed between the oxidized carbohydrate moiety and the aminooxy group on the water soluble polymer, or

wherein said water soluble polymer contains a hydrazide group and a hydrazone linkage is formed between the oxidized carbohydrate moiety and the hydrazide group on the water soluble polymer.

2. The method according to claim 1 wherein the water soluble polymer is polyethylene glycol (PEG) hydroxyethyl cellulose (HEC), dextrin or polyoxazoline.

3. The method according to claim 1 wherein the water soluble polymer is polysialic acid (PSA) or a modified PSA (mPSA).

4. The method according to claim 3 wherein the PSA or mPSA is colominic acid or modified colominic acid.

5. The method according to claim 3 or 4 wherein the PSA or mPSA comprises 2 – 500 sialic acid units.

6. The method according to any previous claim wherein the ganglioside comprises a glycosphingolipid (ceramide and oligosaccharide) with one or more sialic acids linked on the sugar chain.

7. The method according to any previous claim wherein the ganglioside comprises a ceramide linked to glucose, which is linked to a first galactose, which is linked to N-acetylgalactosamine, which is linked to a second galactose.

8. The method according to any one of claims 1-5 wherein the drug delivery system comprises a macromolecular drug delivery system, for instance an antibody

or a neoglycoprotein, or a synthetic polymers, for instance poly(hydroxypropylmethacrylamide), polylysine or polymerised alkyl cyanoacrylates.

9. The method according to any one of claims 1-5 wherein the drug delivery system comprises a particulate drug delivery system, for instance (i) a nanosphere or a microspheres, which comprises biodegradable materials such as albumin or semibiodegradable materials such as dextran and alkylcyanoacrylate polymers, (ii) a vesicle formed of nonionic surfactants, or (iii) a liposome.

10. The method according to any one of claims 1-5 wherein the glycoprotein is selected from cytokines such as interleukins, alpha-, beta-, and gamma-interferons, colony stimulating factors including granulocyte colony stimulating factors, fibroblast growth factors, platelet derived growth factors, phospholipase-activating protein (PUP), insulin, plant proteins such as lectins and ricins, tumor necrosis factors and related alleles, soluble forms of tumor necrosis factor receptors, interleukin receptors and soluble forms of interleukin receptors, growth factors, tissue growth factors, transforming growth factors such as TGFαs or TGFβs and epidermal growth factors, hormones, somatomedins, pigmentary hormones, hypothalamic releasing factors, antidiuretic hormones, prolactin, chorionic gonadotropin, follicle-stimulating hormone, thyroid-stimulating hormone, tissue plasminogen activator, immunoglobulins such as IgG, IgE, IgM, IgA, and IgD, monoclonal antibodies, erythropoietin (EPO), blood factors other than blood coagulation proteins, galactosidases, α-galactosidases, β-galactosidases, DNAses, fetuin, fragments thereof and fusion proteins comprising any of the above mentioned proteins or fragments thereof.

11. The method according to any previous claim, comprising oxidizing the carbohydrate moiety by incubating (1), (2) or (3) with sodium periodate ($NaIO_4$).

12. The method according to any previous claim, comprising oxidizing the water soluble polymer to form an aldehyde group on a terminal unit of the water soluble polymer, and reacting the oxidized water soluble polymer with an aminooxy linker or a hydrazide linker.

13. The method according to claim 12 comprising oxidizing the water soluble polymer using $NaIO_4$.

14. The method according to any previous claim comprising contacting the oxidized carbohydrate moiety with water soluble polymer in a buffer comprising a nucleophilic catalyst selected from aniline and aniline derivatives.

15. The method according to any previous claim, wherein said water soluble polymer contains an aminooxy group and an oxime linkage is formed between the oxidized carbohydrate moiety and the aminooxy group on the water soluble polymer.

16. The method according to claim 15 wherein the aminooxy group is formed by reacting oxidized water soluble polymer with an aminooxy linker, and the aminooxy linker is 3-oxa-pentane-1,5-dioxyamine or 3,6,9-trioxa-undecane-1,11-dioxyamine.

17. The method according to any one of claims 1-14, wherein said water soluble polymer contains a hydrazide group and a hydrazone linkage is formed between the oxidized carbohydrate moiety and the hydrazide group on the water soluble polymer.

18. The method according to claim 17 wherein the hydrazide group is formed by reacting oxidized water soluble polymer with a hydrazide linker.

19. The method according to any previous claim further comprising reducing an oxime linkage or a hydrazone linkage in the conjugated (1), (2) or (3) by incubation in the presence of a reducing compound.

20. The method according to claim 19 wherein the reducing compound is sodium cyanoborohydride ($NaCNBH_3$) or ascorbic acid (vitamin C).

21. A conjugated glycoprotein, ganglioside or drug delivery system obtainable by the method according to any previous claim.

22. A conjugated glycoprotein other than a blood coagulation protein, a ganglioside or a drug delivery system comprising:

(a) the glycoprotein, ganglioside or drug delivery system; and

(b) at least one aminooxy-water soluble polymer bound to the glycoprotein, ganglioside or drug delivery system of (a), wherein said aminooxy-water soluble polymer is attached to the glycoprotein, ganglioside or drug delivery system via one or more carbohydrate moieties.

23. A conjugated glycoprotein according to claim 22, wherein the water soluble polymer is PSA or mPSA.

24. A conjugated glycoprotein other than a blood coagulation protein, a ganglioside or a drug delivery system comprising:

(a) the glycoprotein, ganglioside or drug delivery system; and

(b) at least one hydrazide-water soluble polymer bound to the glycoprotein, ganglioside or drug delivery system of (a), wherein said hydrazide-water soluble polymer is attached to the glycoprotein ganglioside or drug delivery system via one or more carbohydrate moieties.

25. A conjugated glycoprotein according to claim 24, wherein the water soluble polymer is PSA or mPSA.