

SELF ADJUSTING INSTRUMENT

Field of the Invention

The present invention is related to the field of tools. Specifically the present invention relates to an instrument for cleaning and/or shaping and/or widening a channel, existing in or through a solid object.

Background of the Invention

Publications and other reference materials referred to herein, including references cited therein, are incorporated herein by reference in their entirety and are numerically referenced in the following text and respectively grouped in the appended Bibliography which immediately precedes the claims.

There are many situations in which it is required to use an instrument for cleaning out and/or shaping and/or widening a channel that exists in or passes through a solid object. One of the best examples illustrative of the problem and of the shortcomings of the prior art is from the field of dental instruments, specifically root canal procedures. Root canal procedure is one of the most demanding tasks for a dental surgeon. Root canal treatment consists of two stages: (a) shaping, cleaning, and widening of the root canal and (b) obturation of the canal space. The first stage is aimed at removing all tissue remnants, shaping the canal space and disinfecting it, while the second stage is aimed at sealing the root canal and preventing its recontamination. Failure to achieve either of those goals may result in

persistent apical periodontitis - associated with periapical bone resorption and occasional or chronic suppuration.

In the simplest case, in which the canal is relatively straight and has a relatively uniform circular cross-section, the work is carried out by starting with a small diameter instrument (known as a dental file) and replacing it with a series of increasingly larger diameter files until the desired final diameter of the canal is attained. If the canal is not straight, using the conventional stainless steel files will most probably result in a poor quality of treatment. In cases in which the curvature is not too great, nickel titanium alloy files are able to adapt themselves to the longitudinal curvature of the canal; thus achieving better results; however existing nickel-titanium alloy files cannot adapt themselves to changes in the shape or diameter of the canal, therefore a series of files must be used to clean out a canal as is the case with stainless steel files. Also the use of any type of existing file in a canal having non uniform or non circular cross-section results in a canal that is either not completely cleaned out or one having a circular cross-section, the uniform diameter of which is at least as large as the maximum width of the original canal.

The anatomy of a tooth is shown in Fig. 1. Topographically tooth 1 is divided into two sections. The crown 2, covered by enamel 4, is the visible part of the tooth. The root 3 is below the gums and anchors the tooth in place in the jaw bone. Within the dentin 6, which comprises the principal mass of the tooth, is located the pulp chamber 5 and one or more root canals 7, both of which are filled with pulp 8.

Figs. 2A to 2C illustrate the major steps of the root canal procedure. In the first step (shown in Fig. 2A) part of the crown is removed and the pulp is cleaned out of the pulp chamber. In the second step (Fig. 2B) the openings of the root canals are widened. Then (Fig. 2C) the canal system is shaped, cleaned, and widened, removing all pulp particles and infection. In a final step (not shown in the figures) the clean and disinfected root canals are obturated.

Endodontic failures are more common than the profession is willing to acknowledge. The commonly quoted success rates are based mainly on studies carried out in teaching institutes and/or by endodontists. Nevertheless, surveys carried out on the general public indicate that in association with up to 58% of the endodontically treated teeth a periapical lesion was evident (1).

This represents, most probably, a poor quality of treatment (1); nevertheless, it may also represent a basic flaw in the common approach to root canal treatment. Root canals are usually perceived as having a gradually tapering diameter with a round cross section (Fig. 3A). This may be true for many upper anterior teeth; however, it is far from reality in many of the bicuspid and molars. In these teeth ribbon-like root canals, with a flat cross section (Fig. 3B) are common (2). The flat dimension of these canals is at the bucco-lingual plane, which is not seen on a radiograph, and usually has its maximal width at 5 mm from the apex. This anatomy is especially pronounced in the second upper bicuspid, in distal roots of lower molars, as well as in many canines and lower incisors. Additionally, canals with a tear-shaped cross section (Fig. 3C) are common in roots that have two canals, such as the mesial roots of lower molars and those of upper first

bicuspid as well as in many of the mesio-buccal roots of upper molars. The fact that all of these anatomical variations are not seen on a regular periapical radiograph is one of the reasons for the common misconception and presents a major obstacle in achieving the goal of high quality endodontic treatment.

The traditional, common, approach for cleaning, widening, and shaping root canals utilizes hand files having round cross-sections and a standardized cylindro-conic shape. Sequential use of files of increasing diameter, with intermitted flushing with antiseptic solution, results in a canal in which a cylindro-conic gutta-pecha cone may intimately be fitted in the apical part of the canal and used as a "master cone". With the proper paste type sealer and accessory cones they are expected to seal the apical part of the canal. The common cleaning, widening, and shaping procedures are designed to adapt the apical part of the root canals to the form of these standardized master cones.

This common concept is based on the image of a root canal that has a round cross section, which may gradually be enlarged by round files to the shape of a standardized master cone. Although suitable for anterior teeth, when applied in many posterior root canals, this approach may often lead to failure. Cleaning, widening, and shaping a flat root canal with round files will frequently leave a remaining buccal and/or lingual recesses along the root canal filling, untouched and full of tissue remnants, bacteria, or both (3,4). This will inevitably result in failure. Recent studies indicate that this problem is much more common than previously appreciated (2, 3).

When using traditional hand-held stainless steel files some of these recesses are inevitably only partially cleaned. In Fig. 4 is shown a set of stainless steel K-files. A great deal of experience is necessary to choose the proper length and diameter as the canal is cleaned out from the top to the bottom. When the root canal curves it is only possible to follow the curvature by increasing the diameter of the canal. This problem is illustrated in Fig. 5A. If the curvature of the canal becomes too great, generally near the apex of the canal, then one of two undesirable situations arises. The first, shown in Fig. 5B, is that the process is terminated resulting in creation of a ledge in the canal and debris in the untreated lower part of the canal. The second alternative, shown in Fig. 5C, is that the procedure continues until perforation of the tooth occurs, also resulting in a false canal or apex enlargement. One other major difficulty encountered during root canal treatment is shown in Fig. 5D; if one of the solid files breaks and can not be removed, a not infrequent occurrence, then the root canal treatment fails and the tooth is usually removed.

The hand-held stainless steel instruments are currently gradually being replaced by nickel titanium rotary files. As in the case of K-files, current leading nickel titanium rotary files are used as series of instruments with gradually enlarging diameters but, unlike the stainless steel files, are able to adapt longitudinally to the canal shape. Nickel titanium rotary files are more efficient and allow the operator to complete a case in a somewhat shorter time. Unfortunately, this efficiency has a price: the prepared canal is of a perfect round cross section and the cleaning of the recesses in flat and tear-shaped canals is not done.

Recognition of the above problem has led some professional authorities to consider a further enlargement of the apical part of the canals, to a diameter that will include the flat remaining parts. The preparation of a root canal by enlargement for root canals having round, flat, and tear-shaped cross-sections is shown schematically in Figs. 6A, 6B, and 6C respectively. Such enlargement could not be safely done in bent root canals with traditional stainless steel instruments because of their rigidity (3). Rotary nickel titanium files made it possible to enlarge bent canals in a mesial root of a lower molar to accept a No. 45-50 gutta-percha master cone. Nevertheless, this approach has two short comings: it may frequently lead to either unwanted excessive local thinning of the remaining root canal wall (2) or to the use of a single-cone root canal filling in the apical third of the canal. The first may lead to a higher frequency of vertical root fractures, while the second was discarded long ago for its inferior sealing abilities. Furthermore, in many cases the diameter required to really include the recesses is so large that it will cause a perforation of the canal wall (2) (see Fig. 6B and Fig. 6C).

The issue of cleaning, widening, shaping, and obturation of root canals with non-round cross sections does not currently have an adequate, efficient solution.

It is therefore a purpose of the current invention to provide an instrument that is capable of changing its interior volume, contour, or both during use in cleaning and/or shaping and/or widening a channel, existing in or through a solid object, in order to shape itself to the channel's three-dimensional contour.

It is another purpose of the current invention to provide an endodontic file that is capable of cleaning and shaping and widening root canals having circular and/or non-circular cross sections.

It is another purpose of the current invention to provide an endodontic file whose contour varies during use thus allowing the use of a single file for an entire root canal procedure.

It is yet another purpose of the current invention to provide an endodontic instrument that is sufficiently flexible to allow it to adapt itself longitudinally to the curvature of the root canal up to its apical end.

It is another further purpose of the current invention to provide an endodontic file that requires significantly less time to perform root canal treatments than existing instruments.

It is a still further purpose of the current invention to provide an endodontic instrument that is significantly easier to use and has a significantly shorter learning curve than existing instruments used to perform root canal treatments.

Further purposes and advantages of this invention will appear as the description proceeds.

Summary of the Invention

The present invention can be realized in many different embodiments and has applications in many fields in which it is necessary to clean out and/or shape and/or widen a channel, existing in or through a solid object. Examples of such applications can be found, for example, in such widely differing fields as drilling for oil, dental surgery, and material machining. In order to best illustrate the many advantages of the instrument of the invention over existing tools, a specific embodiment of the invention for use in dental root canal treatment, one of the most demanding applications for instruments of this type, has been chosen as an illustrative and non-limiting example to be described herein.

In one aspect the present invention is an instrument for cleaning and/or shaping and/or widening a channel that exists in or through a solid object. The instrument is capable of changing its interior volume, contour, or both during use in order to shape itself to the channel's three-dimensional contour of the channel. The instrument of the invention is characterized in that it is a long narrow balloon, which is inserted into the channel and then inflated. A rod or wire can be inserted into the interior of the balloon and attached at the distal end.

At least a part of the outer surface of the balloon can be coated with a coating of an abrasive material, thereby allowing the instrument to remove material from the wall of the channel when relative motion takes place between the outer surface and the wall. In some embodiments the relative motion is translational motion. The abrasive material can be diamond powder, titanium nitride, or tungsten carbide.

The instrument of the invention can be designed and used such that during the procedure of cleaning and/or shaping and/or widening the channel, either a relatively uniform amount of material or a different amount of material can be removed from the wall of the channel along the entire insertion length of the instrument in the channel. As a result of the design of the instrument the cross-sectional shape of the channel,

along the entire insertion length of the instrument that is inserted into the channel is essentially the same after the procedure of cleaning and/or shaping and/or widening the channel as before the procedure.

The instrument of the invention can be an endodontic file.

In another aspect the invention is a method of using the instrument of the invention for cleaning and/or shaping and/or widening a channel that exists in or through a solid object. The method comprises the following steps:

- inserting the instrument into the channel;
- inflating the instrument;
- causing relative motion between the instrument and the wall of the channel; and
- deflating and removing the instrument from the channel when the cleaning and/or shaping and/or widening have been completed.

All the above and other characteristics and advantages of the invention will be further understood through the following illustrative and non-limitative description of preferred embodiments thereof, with reference to the appended drawings.

Brief Description of the Drawings

- Fig. 1 shows the anatomy of a tooth;
- Figs. 2A to 2C illustrate the major steps of the root canal procedure;
- Figs. 3A to 3C show root canals having different cross sectional shapes;
- Fig. 4 shows a set of stainless steel K-files;
- Figs. 5A to 5D show some of the problems encountered in using prior art files to perform root canal treatments;
- Figs. 6A to 6C show the stages, according to the prior art, in preparing root canals having different cross sectional shapes;

- Figs. 7A, 7B, and 7C are respectively perspective, front, and flattened-out, views of the instrument of the invention;
- Figs. 8A and 8B show cross-sectional views of the instrument of the invention before being inserted into the root canal and inside a tear shaped canal respectively;
- Figs. 9A, 9B, and 9C show schematically the preparation of a root canal, using the self adjusting instrument of the invention, for root canals having round, flat, and tear-shaped cross-sections respectively;
- Fig. 10 shows how the instrument of the invention adapts its shape as it is inserted up to the apical end of the root canal; and
- Figs. 11A to 11F show cross-sections of examples of different embodiments of the instrument of the invention.

Detailed Description of Preferred Embodiments

In general, the channels to be widened and/or cleaned and/or shaped by the instrument of the invention are relatively long and narrow. These channels will be described hereinbelow in terms of a single "longitudinal axis", which is the line defined by the loci of the center points of the channel along its length, and a multitude of "radial axes", wherein each such radial axis is defined by a line originating at a point on the longitudinal axis and perpendicular to the longitudinal axis at that point. Rotation of a given radial axis around its origin defines the localized "radial plane". The direction essentially parallel to the longitudinal direction will be known as the "longitudinal direction" and the direction essentially parallel to one of the radial axes will be known as the "radial direction". Because the instrument of the invention conforms to the shape of the canal similar terminology will be used to describe the principal axes of the instrument.

The instrument of the invention can be inserted completely to the end of the channel or only partially into the channel, in which case only part of the channel will be widened and/or shaped and/or cleaned. The length of the instrument that is inserted into the channel is known as the "insertion length" which term also indicates the depth of the channel that is worked on by the instrument.

As an illustrative, but non-limitative, example of the instrument of the invention embodiments of an endodontic file for performing root canal treatments will be described hereinbelow.

The preferred embodiment of the endodontic instrument of the invention, known herein as the SAF (self adjusting file) is a rotary nickel titanium instrument of a unique design. While current leading rotary files must be used as series of instruments with gradually enlarging diameters, the SAF is used as a single instrument for the whole procedure. When inserted into a narrow canal, whose nominal diameter is less than its own nominal diameter, the instrument is compressed, its superelastic property allowing it to adapt itself to the cross-sectional shape of the walls of the canal in each radial plane along the longitudinal axis of the canal. Rotating in the canal it removes tissue and debris from the canal and the canal wall. As the debris is removed from the canal wall, the super elastic property of the SAF causes it to gradually expand with time in the radial direction while continually maintaining contact with the canal wall at every point. Thus material is uniformly removed from the dentinal walls of the canal until the desired nominal diameter is achieved.

A preferred embodiment of the SAF is shown respectively in perspective, front, and flattened out, views in Figs. 7A, 7B, and 7C. The SAF 10 is made of a nickel titanium alloy (Nitinol) and originally is given a cylindrical shape. The walls of the upper end, the neck 12, are solid and are gripped by either the dental hand piece or are attached to a handle for manual use. The main part of the body of the SAF is an open, lattice-like structure made up of longitudinal elements 14, that run the length of the instrument from neck to tip 16 and short circumferential elements 18 that connect adjacent longitudinal elements. In the preferred embodiment shown in the figures, there are four longitudinal elements and the circumferential elements, in their undeformed state are arcs of a circle. In a radial plane containing circumferential elements, the circumferential elements that lie in that plane define the cross-sectional shape of the instrument in that plane. Both the circumferential and longitudinal elements have a flat rectangular blade-like cross section. After manufacture, the Nitinol cylinder is constrained in a mold and heat treated to give it its shape memory property while changing its shape to cylindrical-conic.

The surfaces of the instrument of the invention that are in contact with the walls of the canal are treated in some way to enable them to remove material from the wall as the instrument rotates. One possible treatment is to coat the surfaces with an abrasive material such as, for example, diamond powder, titanium nitride, and tungsten carbide, that will remove dentin from the canal wall by friction as the SAF is rotated, thus cleaning out and enlarging the inside of the root canal. In other embodiments, the surfaces in contact with the wall of the canal can be manufactured with roughened surfaces comprising, for example numerous small teeth as in a file or a rasp. Alternately, these surfaces can comprise a cutting edge

similar to the edge on a drill bit. In some embodiments of the instrument of the invention, the surfaces in contact with the canal wall can be relatively smooth and abrasive slurry can be introduced into the canal to be trapped between the instrument and the wall.

The material scraped from the wall of the canal passes through the openings in the lattice structure of the body of the SAF into the hollow interior from which it can easily be removed by rinsing or suction without stopping rotation of the instrument or withdrawing it from the root canal. In other embodiments, the debris can also be removed *via* the space between the canal wall and the instrument. The design allows for fluids, such as antiseptic or saline solution, to continuously flow into the root canal, either through the center of the instrument or between the outer surface of the instrument and the canal wall, while the instrument is working, thus saving valuable time and improving the debridement and disinfection procedures. The constant flow also increases the efficiency of filing and prevents clogging the canal with dentin-mud and debris. Another advantage of the hollow structure of the SAF is that, in the extreme case of instrument failure and breakage inside the canal, the separated part of the instrument of the invention can be easily and safely removed, using specially designed extractors, no matter what the position of the broken piece of the instrument in the root canal.

After part of the crown is removed and the pulp is cleaned out of the pulp chamber, and a sufficient access to the canal is obtained the SAF is inserted into the root canal. As the instrument is pushed into the canal, its superelasticity allows it to be guided to the apical end of the root canal by following the path of least resistance (through the pulp rather than the

much harder dentine). Prior art nickel titanium files can also adapt themselves to the canal shape longitudinally but are unable to change their volume and contour as can the SAF. Additionally the solid structure of the prior art files makes them less flexible than the hollow lattice-like structure SAF. In Fig. 10 is shown the SAF adapting its shape as it is inserted up to the apical end of the root canal.

The instrument is now moved relative to the walls of the root canal in order to carry out the cleaning, widening, and shaping process. The motion can be longitudinal, i.e. the instrument can be moved up and down in the canal; rotational; vibrational, i.e. the instrument can be caused to vibrate by connecting it to, for example, an ultrasound transducer; or a combination of these motions. In the preferred embodiment of the invention the SAF is rotated either manually or by means of a dental handpiece. As the instrument rotates, the SAF's super elastic property keeps its elements pressed against the root canal wall in all the radial planes along the length of the instrument.

Figs. 8A and 8B show cross-sectional views of the instrument of the invention outside of and inside a tear shaped root canal respectively. The views in the cross-sections shown in Figs 8A and 8B are in radial planes wherein each such radial plane is located at and contains a single set of circumferential elements. Since the axis of the SAF essentially lies on the longitudinal axis of the canal, each plane intersects the walls of the canal at right angles. The perimeter of the SAF in each of these planes is made up of eight segments - **14a** to **14d**, the longitudinal elements, and **18a** to **18d**, the circumferential elements. The material and structure of the SAF have three properties that allow it to carry out the desired function. Firstly, the

superelasticity of the alloy makes the device constructed from it extremely flexible, allowing it to be deformed to conform to the shape of the canal at the position at which it is located. Secondly, the diameter of the original cylindro-conic state of the instrument is greater than the diameter of the canal. Therefore the stress created in the alloy by the deformation from contact with the walls of the canal as the instrument is rotated and the super elastic property causing the instrument to try to return to its original cylindro-conic shape. The internal force exerted in attempting this return to the original shape constantly pushes the elements of the device against the inner wall of the canal. Thirdly each element made of the super elastic alloy has the property of being able to stressed/strained up to 8% to 10% from it's original shape, depending on the exact composition of the alloy, thus allowing the internal volume of the SAF to increase with time and its elements to remain in constant contact with the walls, even as material is continually being removed from them. As the instrument rotates each of the circumferential elements 18a to 18d changes in length and shape independently from the others, thus the instrument is able to conform to the local shape of the canal wall.

The fact that the circumference of the instrument is divided into four elements, each of which can independently change shape imparts to the SAF a degree of flexibility, an ability to adapt to the shape of the root canal, and the ability to expand in size that goes far beyond that of existing files. These properties can be further increased by building the instrument with a greater number of peripheral elements, however increased flexibility, etc. will be gained at the expense of the strength of the device.

Thus, in the plane shown, as the instrument rotates, its cross-sectional shape is constantly changing to conform to the shape of the canal wall and the length of the circumference of the device in that plane is constantly increasing as material is removed from the wall. This is to be compared to the situation with existing files in which the shape of the canal is changed to conform to the shape of the file and the files must constantly be replaced with files of larger diameter in order to clean, widen, and shape the canal.

The description given hereinabove applies for each successive set of circumferential elements located in different radial planes along the length of the instrument. The adaptation to the local shape of the canal and changes in contour and length of the circumferential elements that comprise each successive set is essentially independent of its neighbors. This behavior explains how the instrument of the invention can deal with the common situation described hereinabove in which the canal narrows along much of its length and then becomes wide near the apical tip before narrowing again. Because the instrument is moved (rotated) as a single unit, the amount of material removed from the canal wall, which mainly depends on how long the instrument is revolved, is essentially constant along the entire length of the portion of the instrument that is inserted into the canal.

For almost all cases, the deviations of the diameter of the root canal from its average diameter are such that the instrument of the invention can be designed to allow use of a single instrument to clean out the whole length of the canal. In the preferred embodiments of the invention, the outer surface of the instrument is uniformly treated to enable removal of material from the wall, in which case essentially the same amount of material will be removed from the wall of the canal at each radial plane along its entire

length. However, the skilled person will know how the instrument can be designed and treated to allow non-uniform removal of material at different positions along the length of the canal, if this result is desired for specific applications. Based on statistical information regarding the dimensions of root canals from a large number of teeth, a single nominal width can be determined for the instrument of the invention. It may be however, that it is preferable to provide instruments having several different nominal diameters, for example a small diameter for a narrow canal and a larger diameter for wide canals. In any case, once the correct size instrument has been selected, the entire cleaning, widening, and shaping procedure is then carried out using only that instrument which, once inserted into the canal, is only withdrawn at the end of the procedure. It is to be noted that in some cases, the channel to be worked on by the instrument of the invention may have an exceptionally widely varying cross section, in which case more than one instrument, having different nominal diameters, will have to be used to shape, widen, and clean the entire channel.

The preparation of a root canal, using the self adjusting instrument of the invention is shown schematically Figs. 9A, 9B, and 9C for root canals having round, flat, and tear-shaped cross-sections respectively. The figures are a series of images showing the stages of the cleaning, shaping, and widening step in the procedure. The images range from the untreated root canal on the left to the canal at the end of the procedure on the right. From the figures, it can be seen that the rotating SAF removes a relatively uniform layer from all inner surfaces of the canal wall and therefore the final shape of the cleaned out canal (right image) is very close to that of the original canal. The shaping and widening are done by removing a minimal amount of the canal wall and therefore without causing localized thinning of the root

wall as is the case in the prior art (see Figs. 6B and 6C). Using the SAF to clean out the root canal, the nominal diameter and shape of the canal at each radial plane along its length is preserved. In other words the shaped and cleaned canal does not have an essentially circular cross section having a uniform cross-sectional area along its length as is the case with the prior art.

Shaping, widening, and cleaning the root canal with one instrument, while flushing with a constant flow of antiseptic solution, may significantly cut down treatment time. Additionally shaping and cleaning the root canal with one instrument eliminates the necessity of the operator following complex and tricky flow charts in order to accomplish a simple root canal treatment procedure, as is demanded by current leading rotary file systems.

Heat-softened gutta-percha methods can be easily adapted for obturation of the prepared root canal obtained with the instrument of the invention.

Many variations in the choice of materials and especially in the design of the structure of the device are possible. For example, the device does not have to be built from Nitinol but other types of material, such as, for example, stainless steel, steel, plastic, nickel based alloys, and titanium based alloys can be chosen. Instead of having circumferential and longitudinal elements with a flat rectangular blade-like shape as described hereinabove the elements can have, for example, polygonal prism, rod-like, or curved shapes. Similarly, elements having polygonal (including rectangular, square and triangular), round, and curved cross sections can be used. The combination of original cylindrical shape of the instrument and cylindrical-conic shape after heat treatment, which is most suitable for root

canal work, can be replaced by other shapes which might be more suitable for specific applications. Additionally the structure of the instrument need not be the same as the preferred embodiment of the SAF described hereinabove. Figs. 11A to 11F show cross-sections of some examples of different embodiments of the instrument of the invention. The longitudinal elements are designated by numeral **20** and the circumferential elements **21**. Fig. 11A shows the SAF and Fig. 11B is a similar design except that, in this embodiment, only the outer surfaces of the longitudinal elements are in contact with the canal wall. Using the embodiment of Fig. 11B, the debris can be removed upwards through the space between the canal wall and the circumferential elements while fluid flows downwards through the center of the device, or *vice versa*. The embodiment of Fig. 11C is triangular shaped. The longitudinal elements can be round and covered with abrasive material or teeth or they can be triangular shaped with the outward facing apex acting as a cutting/scraping edge. The embodiment shown in Fig. 11D has a single square longitudinal element with four blades attached to it. The embodiments of Fig. 11E and Fig. 11F have a single longitudinal element from which project radially a multitude of blade-like or wire-like elements. The means of designing and manufacturing these and other embodiments of the instrument of the invention, including providing the necessary superelastic and shape memory properties is within the scope of the knowledge of skilled persons and therefore will not be discussed in further detail herein.

In another embodiment, the instrument of the invention comprises a long narrow balloon, which is inserted into the channel and then inflated. This embodiment can be realized in several ways. For, example, an instrument based on the design of the SAF can be built in which the circumferential

elements are removed and a balloon is mounted to the device along its longitudinal axis and inside the longitudinal elements. The balloon is attached to the device at the neck and to the distal ends of the longitudinal elements. The instrument is inserted into the canal with the balloon deflated. When in position, fluid is introduced into the interior of the balloon using conventional techniques and the balloon expands pushing the longitudinal elements against the walls of the channel. The outer surfaces of the longitudinal elements are treated or shaped in some way to enable them to remove material from the wall as the instrument is moved relative to the walls of the channel. With embodiments comprising a balloon, the relative motion is preferably translational, i.e. the instrument is alternately pushed and pulled in the direction of the longitudinal axis of the channel.

In an alternate embodiment, the device can comprise a balloon only which is coated with an abrasive material on its outer surface. To give the balloon sufficient rigidity, a rod or wire is inserted into the interior of the balloon and attached at the distal end. The balloon is inserted into the channel and then inflated pressing the sides of the balloon against the walls of the channel. The relative motion is preferably translational i.e. pushing and pulling the internal rod in the direction of the longitudinal axis of the channel will cause the balloon to move relative to the wall cleaning, shaping, and widening the channel. When the work is completed, the balloon is deflated and withdrawn from the channel.

Although embodiments of the invention have been described by way of illustration, it will be understood that the invention may be carried out with many variations, modifications, and adaptations, without departing from its spirit or exceeding the scope of the claims.

Bibliography

1. Saunders, WP, Saunders, EM, Sadiq, J, Cruickshank, E, Technical standard of root canal treatment in an adult Scottish sub-population, Br Dent J 182: 382-386, 1990.
2. Wu, M-K, R'oris, A, Borkis, D, Wesselink, PR, Prevalence and extent of long oval canals in the apical third, Oral Surg Oral Med Oral Pathol 89:739-743, 2000.
3. Tan, BT, Messer, H H, The quality of apical canal preparation using hand and rotary instruments with specific criteria for enlargement based on initial apical file size, J Endodon 28: 658-664, 2002.
4. Wu, M-K, Wesselink P R, A primary observation on the preparation and obturation of oval canals, In. Endod J 34:137-141, 2001.

Claims

1. An instrument for cleaning and/or shaping and/or widening a channel that exists in or through a solid object, said instrument capable of changing its interior volume, contour, or both during use in order to shape itself to the channel's three-dimensional contour of said channel;
characterized in that said instrument comprises a long narrow balloon, which is inserted into said channel and then inflated.
2. An instrument according to claim 1, comprising a rod or wire which is inserted into the interior of the balloon and attached at the distal end.
3. An instrument according to claim 1, wherein at least a part of the outer surface of the balloon is coated with a coating of an abrasive material;
thereby allowing said instrument to remove material from the wall of the channel when relative motion takes place between said outer surface and said wall.
4. An instrument according to claim 3, wherein the abrasive material is chosen from the group comprising:
 - diamond powder;
 - titanium nitride; and
 - tungsten carbide.
5. An instrument according to claim 3, wherein the relative motion is translational motion.
6. An instrument according to claim 1, wherein, during the procedure of cleaning and/or shaping and/or widening the channel, a relatively uniform amount of material is removed from the wall of said channel along the entire insertion length of said instrument in said channel.
7. An instrument according to claim 1, wherein, during the procedure of cleaning and/or shaping and/or widening the channel, a different amount of material is removed from the wall of said channel at

different positions along the insertion length of said instrument in said channel.

8. An instrument according to claim 1, wherein, as a result of the design of said instrument the cross-sectional shape of said channel, along the entire insertion length of said instrument that is inserted into said channel, is essentially the same after the procedure of cleaning and/or shaping and/or widening the channel as before said procedure.
9. An instrument according to claim 1, wherein said instrument is an endodontic file.
10. A method of using the instrument of claim 1 for cleaning and/or shaping and/or widening a channel that exists in or through a solid object said method comprising the following steps:
 - inserting said instrument into said channel;
 - inflating said instrument;
 - causing relative motion between said instrument and the wall of said channel; and
 - deflating and removing said instrument from said channel when said cleaning and/or shaping and/or widening have been completed.